

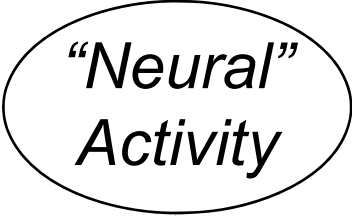
# Multi-modal integration of MEG, EEG & fMRI

Rik Henson

MRC CBU, Cambridge

# Multi-modal Integration

*Causes (hidden):*



*Generative (Forward) Models:*

Head Model

Head Model

Balloon Model

*(inversion)*

?

*Data:*

MEG

EEG

fMRI

? (future)

# Multi-modal Integration

*Causes (hidden):*



*Symmetric  
Integration  
(Fusion)*

*Generative  
(Forward)  
Models:*

Head  
Model

Head  
Model

Balloon  
Model

?

*Data:*

MEG

EEG

fMRI

? (future)

*Asymmetric  
Integration*

# Talk Overview



1. MEG + EEG symmetric integration (fusion)
2. M/EEG + fMRI asymmetric integration

# Symmetric Integration of MEG+EEG

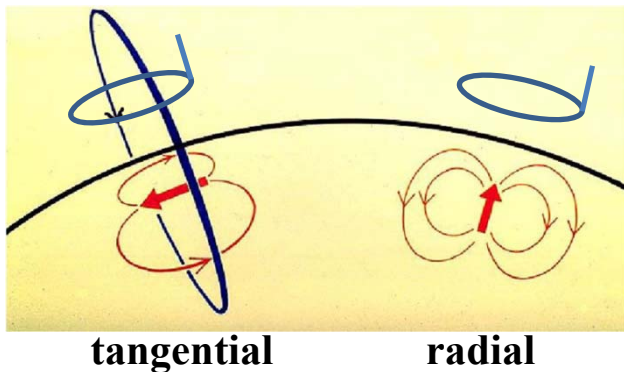
## Background



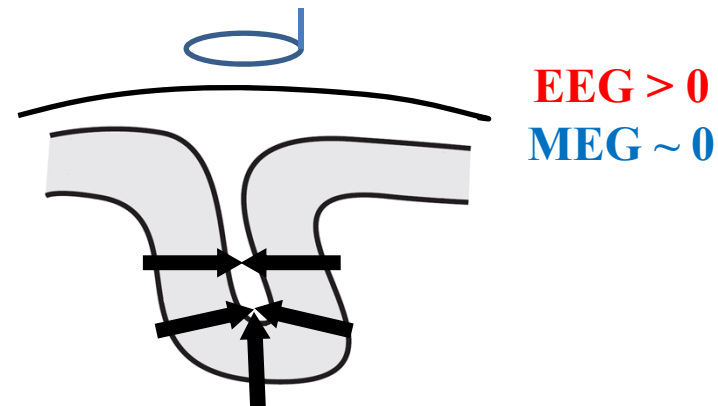
- MEG generally has superior spatial resolution than EEG (less blurred by skull/scalp)
- MEG cannot detect radial component of current sources; EEG can!

# Symmetric Integration of MEG+EEG Background

Dipolar Sources

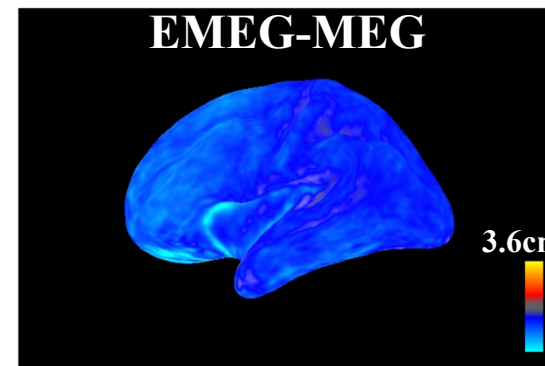
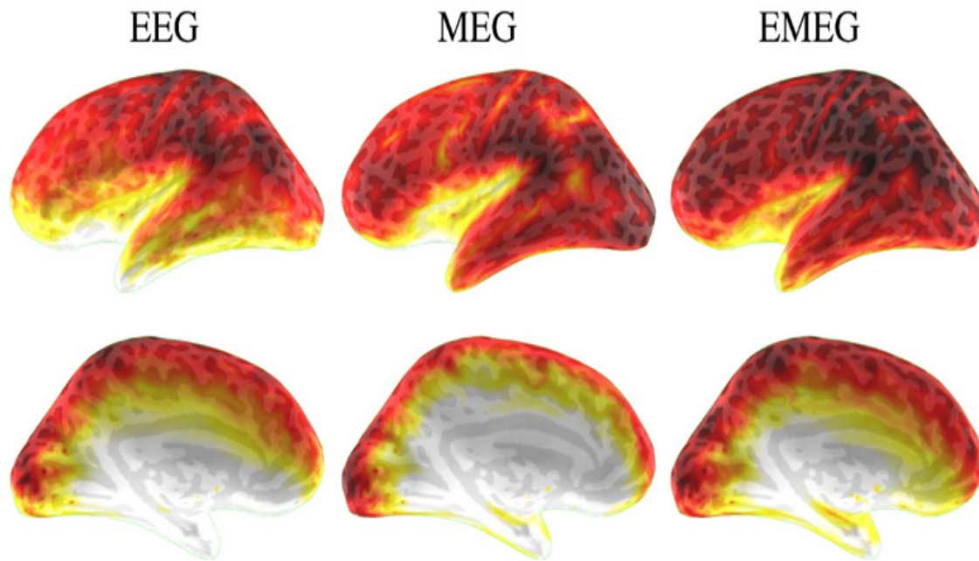


Extended Sources



Ahlfors et al., HBM 2010

Spatial Extent



Stenroos & Hauk, in prep

# Symmetric Integration of MEG+EEG

## Background



- MEG generally has superior spatial resolution than EEG (less blurred by skull/scalp)
- MEG cannot detect radial component of current sources; EEG can!
- And few practical problems acquiring concurrent EEG (apart from extra time attaching electrodes)
- ...but EEG data is more sensitive to head geometry and conductivity (potentially biasing any joint-localisation)...
- ...and has different noise characteristics...

# MEG Linear Forward Model

Given  $n$  sensors and  $p$  sources fixed in location and orientation (e.g, on a cortical mesh), then linear Forward Model (for single timepoint):

$$\begin{bmatrix} d_1 \\ \vdots \\ d_n \end{bmatrix} = \begin{bmatrix} L_{11} & L_{12} & \cdots & L_{1p} \\ \vdots & \ddots & & \vdots \\ L_{n1} & \cdots & \cdots & L_{np} \end{bmatrix} \begin{bmatrix} s_1 \\ s_2 \\ \vdots \\ s_p \end{bmatrix} + \begin{bmatrix} e_1 \\ \vdots \\ e_n \end{bmatrix}$$

$d$  = Data  
 $s$  = Sources  
 $L$  = Leadfields  
 $e$  = Error (noise)

$n$  sensors  
 $p \gg n$  sources  
 $n$  sensors  $\times$   $p$  sources  
 $n$  sensors...

Equivalent matrix format:

$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

Assume sensor noise is zero-mean Gaussian with error covariance  $\mathbf{C}^{(e)}$ :

$$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$$

Assume sources similarly Gaussian with source covariance  $\mathbf{C}^{(s)}$ :

$$\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$$



# MEG Linear Forward Model

## Assumptions to Solve

$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$   
 $\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$

$d$  = Data  
 $s$  = Sources  
 $L$  = Leadfields  
 $e$  = Error (noise)

$n$  sensors  
 $p \gg n$  sources  
 $n$  sensors  $\times$   $p$  sources  
 $n$  sensors...

General solution is:

*Hauk (2004), Neuroimage*

$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d}$$

$\lambda$  = Regularisation (hyperparameter)

But how calculate  $\mathbf{C}^{(e)}$  and  $\mathbf{C}^{(s)}$  ?

# MEG Linear Forward Model Assumptions to Solve

One approach is to model sources and noise by variance components:

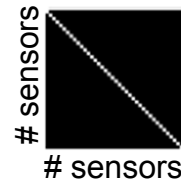
$$C = \sum_i \lambda_i Q_i$$

C = Sensor/Source covariance  
Q = Covariance components  
 $\lambda$  = Hyper-parameters

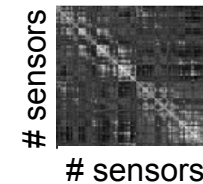
*Friston et al (2008) Neuroimage*

## 1. Sensor components, $Q_i^{(e)}$ (error):

“IID” (white noise):

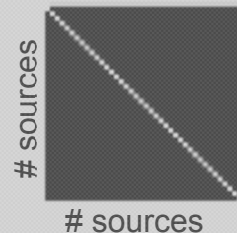


Empty-room:

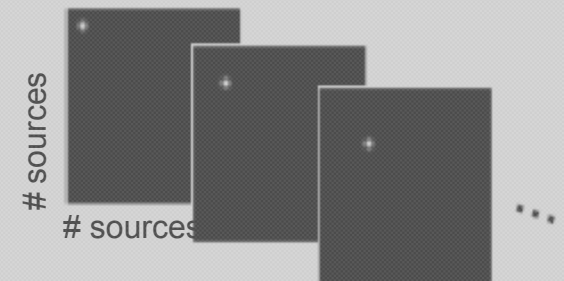


## 2. Source components, $Q_i^{(s)}$ (priors/regularisation):

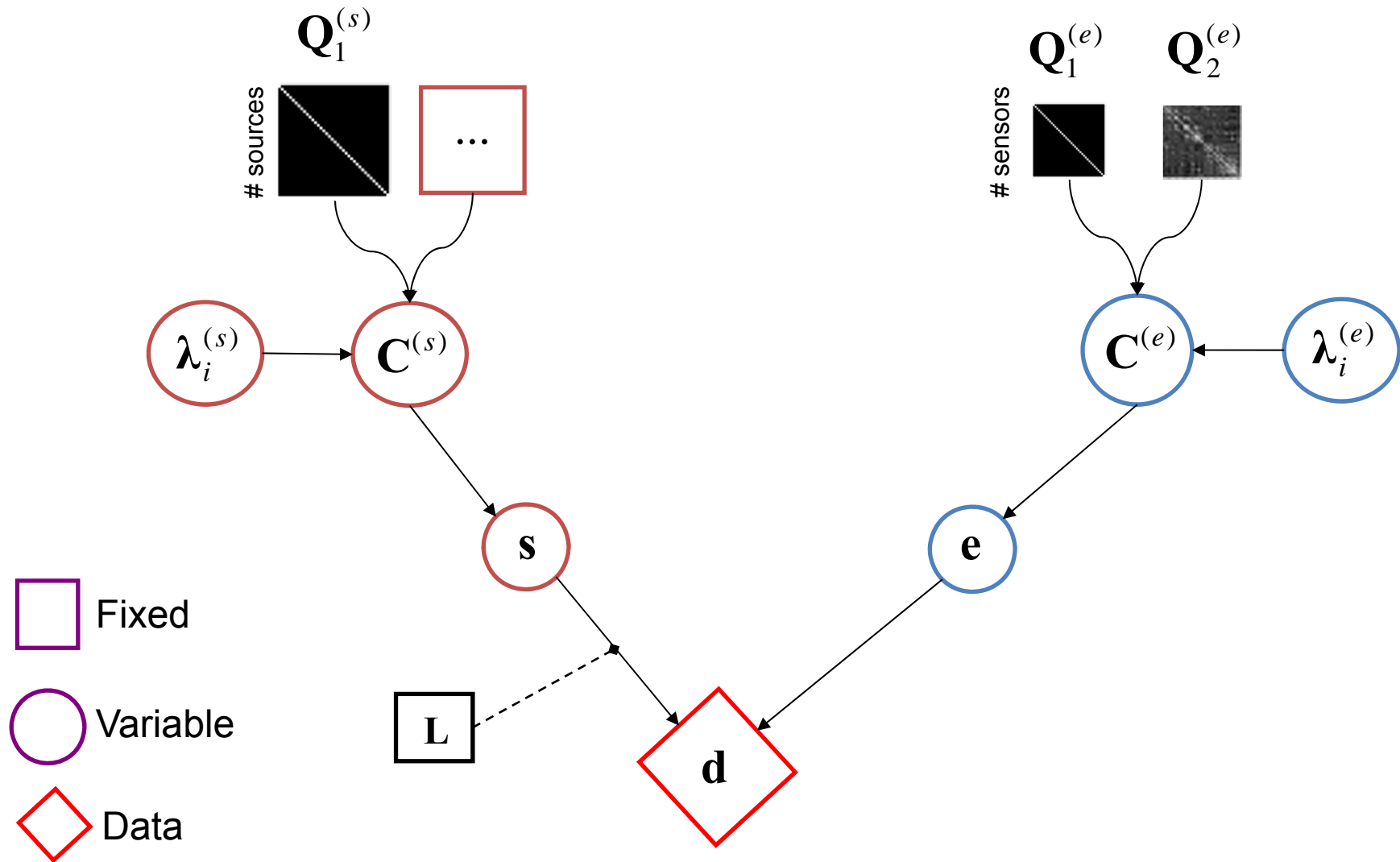
“IID” (min norm):



Multiple Sparse Priors (MSP):



# MEG Generative Model



# Symmetric Integration of MEG+EEG Generative Model

For fusing MEG and EEG, we can simply concatenate the MEG+EEG data:

$$\begin{bmatrix} \mathbf{d}_{(MEG)} \\ \mathbf{d}_{(EEG)} \end{bmatrix} = \begin{bmatrix} \mathbf{L}_{(MEG)} \\ \mathbf{L}_{(EEG)} \end{bmatrix} \mathbf{s} + \begin{bmatrix} \mathbf{e}_{(MEG)} \\ \mathbf{e}_{(EEG)} \end{bmatrix} \quad \begin{array}{l} \mathbf{e} \sim N(0, \mathbf{C}^{(e)}) \\ \mathbf{s} \sim N(0, \mathbf{C}^{(s)}) \end{array}$$

Note same sources, eg, for Minimum (L2) Norm solution:

$$\mathbf{C}^{(s)} = \mathbf{I} \quad \hat{\mathbf{s}} = \mathbf{L}^T (\mathbf{L}\mathbf{L}^T + \hat{\mathbf{C}}^{(e)})^{-1} \mathbf{d}$$

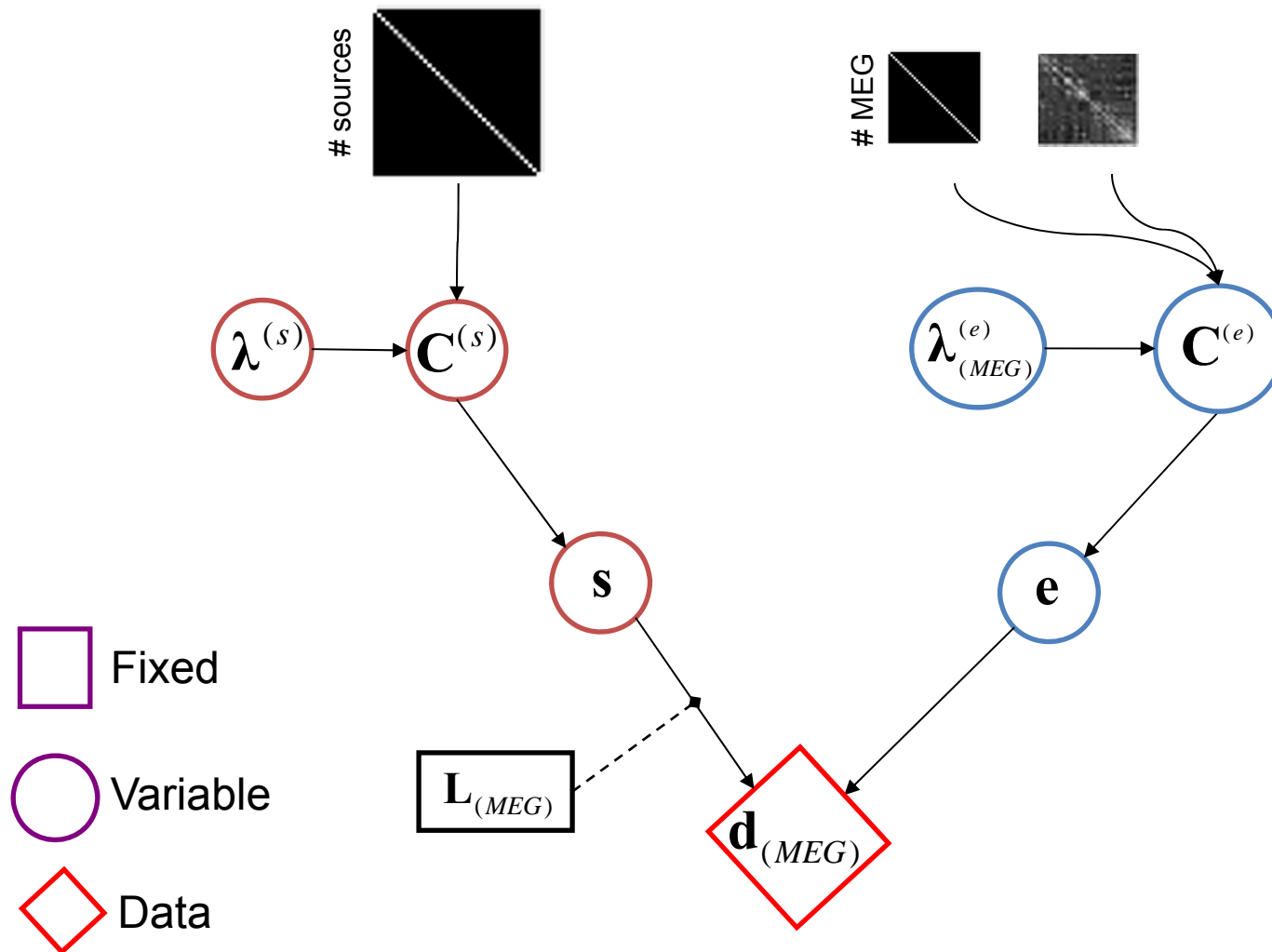
Noise expressed by MEG and EEG terms (e.g, white noise):

$$\hat{\mathbf{C}}^{(e)} = \lambda_1^{(e)} \mathbf{Q}_{(MEG)}^{(e)} + \lambda_2^{(e)} \mathbf{Q}_{(EEG)}^{(e)} \quad \mathbf{Q}_{(MEG)}^{(e)} = \begin{array}{c} \# \text{ sensors} \\ \blacksquare \\ \# \text{ sensors} \end{array} \quad \mathbf{Q}_{(EEG)}^{(e)} = \begin{array}{c} \# \text{ sensors} \\ \blacksquare \\ \# \text{ sensors} \end{array}$$

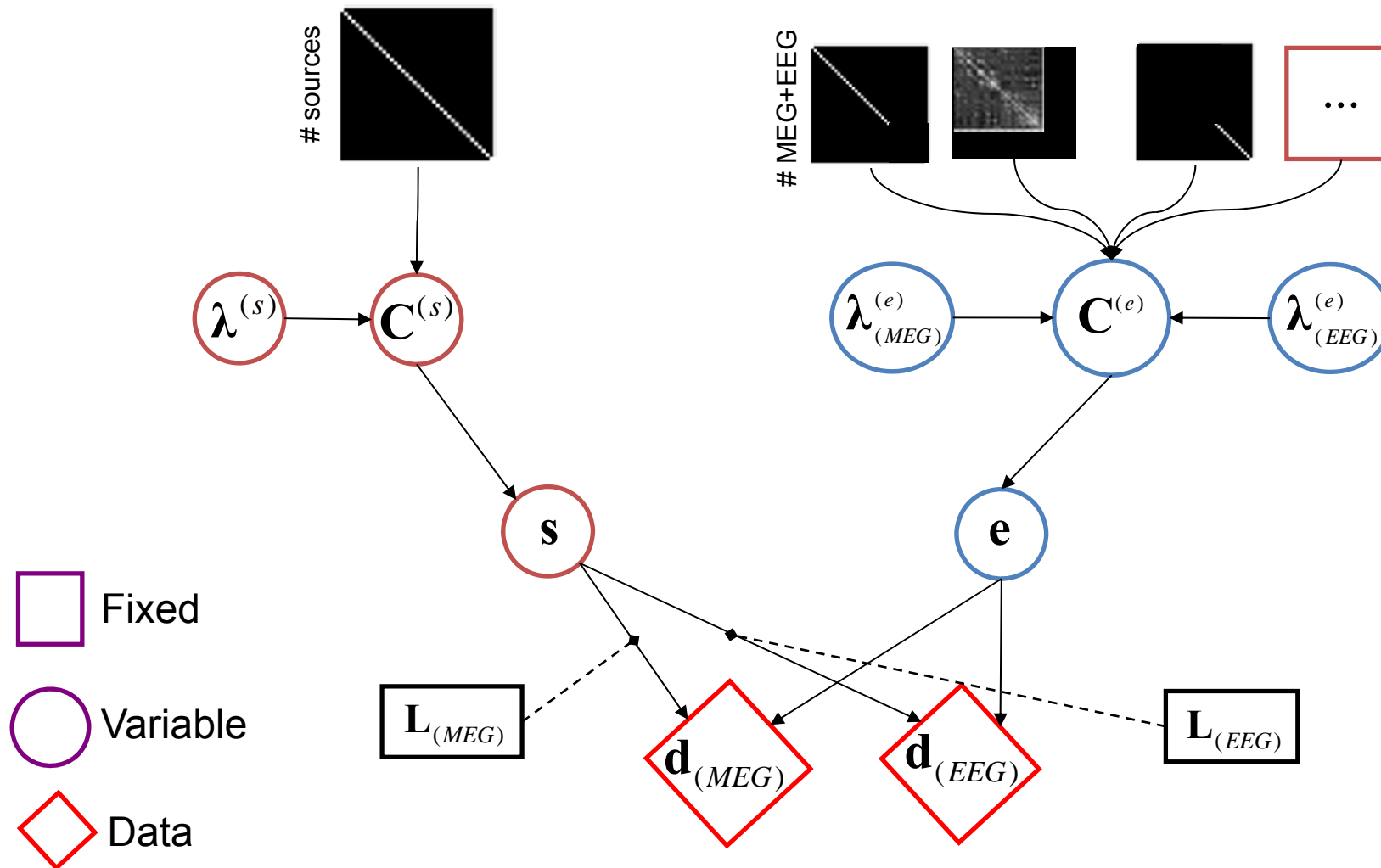
The separate hyperparameters allow for different noise levels (SNR)

The multiple hyperparameters are estimated by maximising **model evidence**  
(using a variational Bayesian approach, eg EM algorithm)

# Symmetric Integration of MEG+EEG Generative Model



# Symmetric Integration of MEG+EEG Generative Model



# One final problem...

- Though this allows for different additive noise levels in MEG and EEG...
- ...we are assuming mapping from common electrical sources to sensor values (in terms of Tesla and Volts) is known precisely...
- ...whereas in reality, this depends on several unknowns (e.g, precise conductivity of skull/scalp)
- One solution is to scale data/leadfields to have same variance:

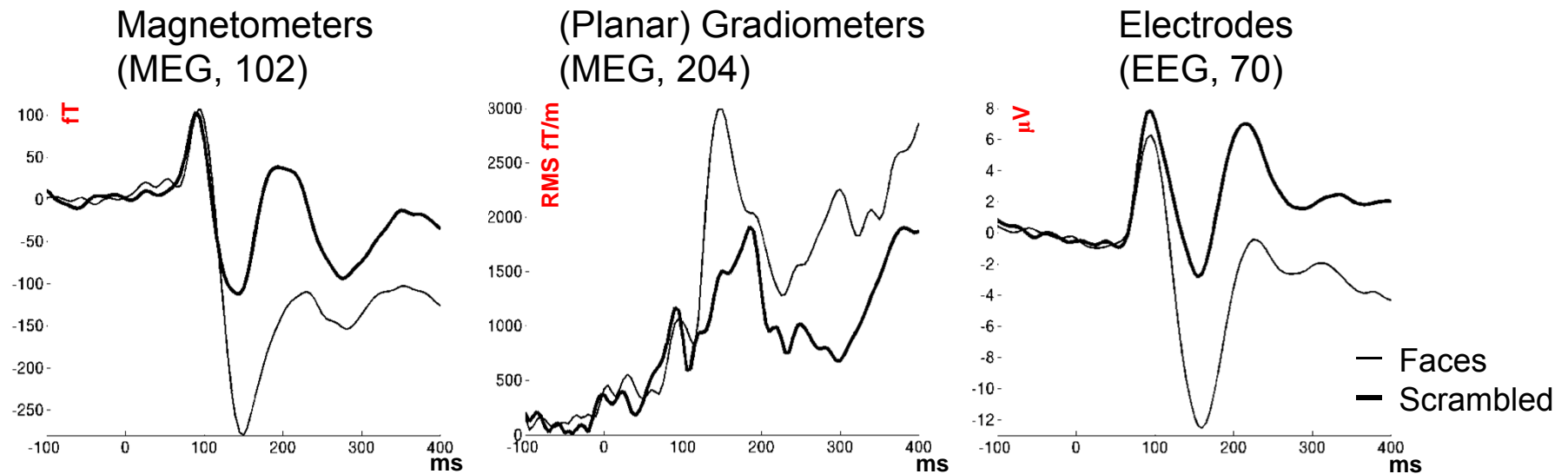
$$\tilde{Y}_i = \frac{Y_i}{\sqrt{\frac{1}{n_i} \text{tr}(Y_i Y_i^T)}}$$

$$\tilde{L}_i = \frac{L_i}{\sqrt{\frac{1}{n_i} \text{tr}(L_i L_i^T)}}$$

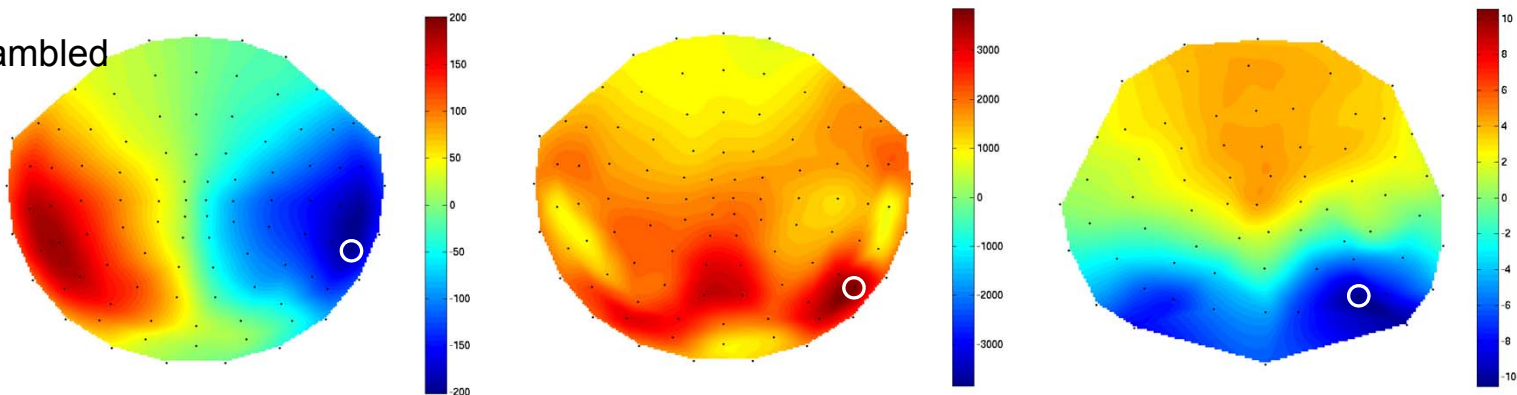
$i$  =  $i$ th modality, ie MEG or EEG  
 $n_i$  = Number of sensors for modality  $i$

# Symmetric Integration of MEG+EEG Example

ERs from 12 subjects for 3 simultaneously-acquired Neuromag sensor-types:

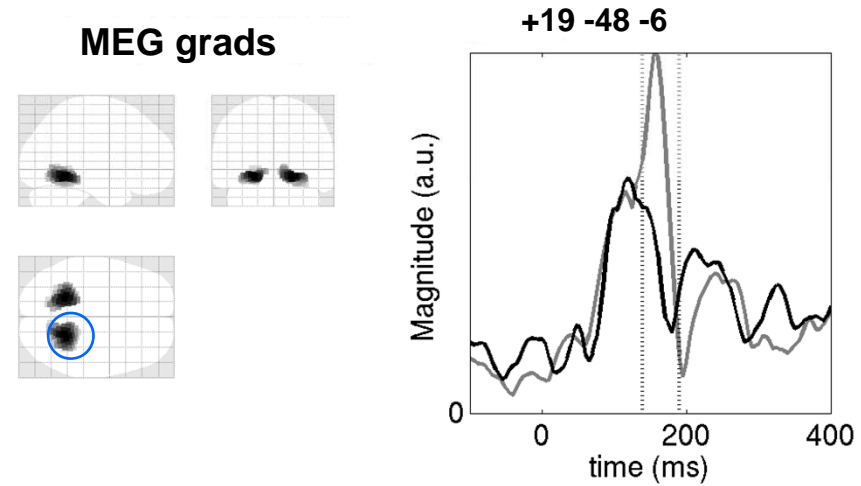
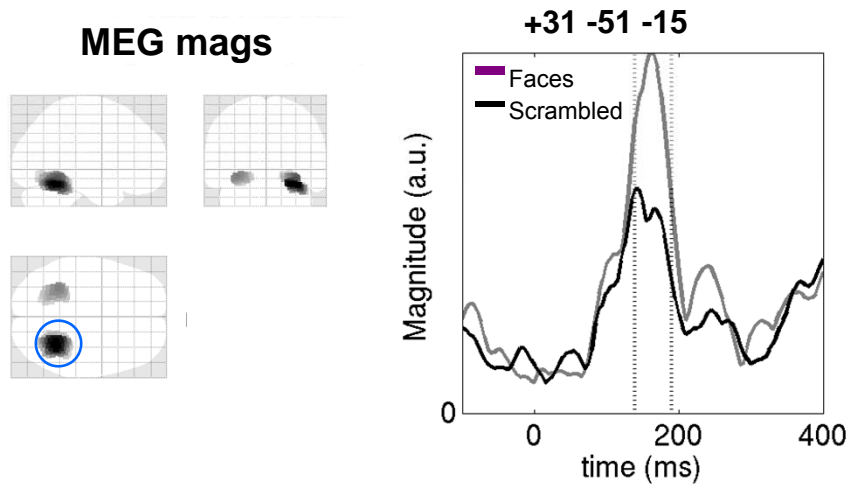


Faces - Scrambled  
150-190ms

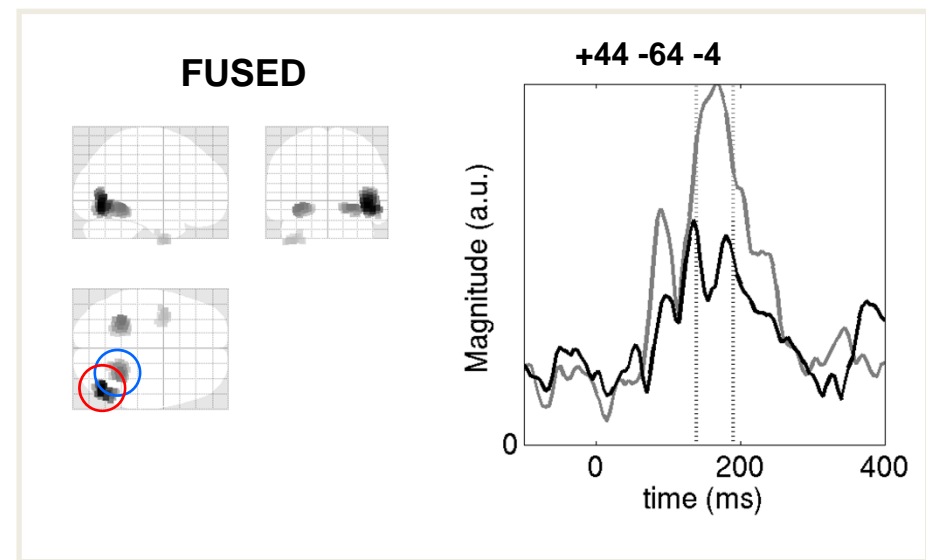
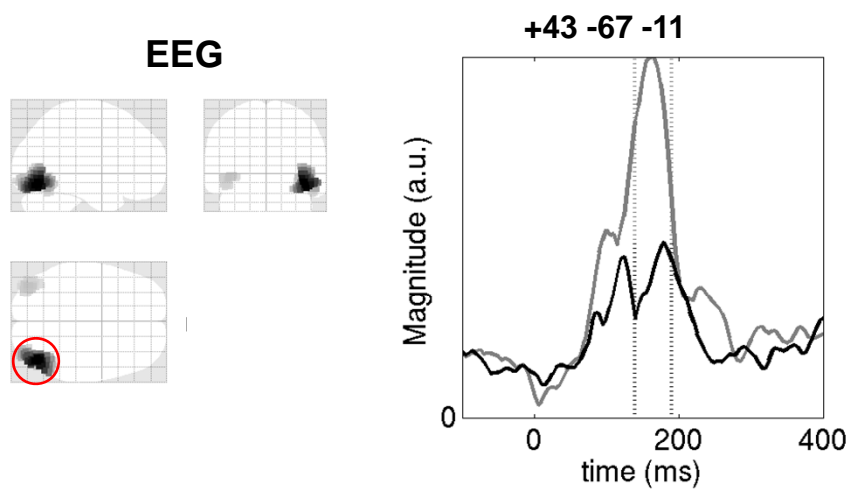




# Symmetric Integration of MEG+EEG



Faces – Scrambled, 150-190ms



IID noise for each modality; common MSP for sources

Henson et al (2009) Neuroimage

# Other Approaches to M/EEG fusion

- Estimate noise covariance from pre-stimulus baseline (**b**):

$$\mathbf{C}^{(e)} = \begin{bmatrix} \text{cov}(\mathbf{b}_{(MEG)}) & \mathbf{0} \\ \mathbf{0} & \text{cov}(\mathbf{b}_{(EEG)}) \end{bmatrix}$$

*Molins et al (2008), Neuroimage*

(which can also be used to pre-whiten data and leadfields, scaling to noise units)...  
...but downside is that **baseline contains source activity**, so not estimate of true sensor noise

- Maximise mutual information between MEG and EEG

*Baillet et al (1999), IEEE*

- Re-parameterise leadfields in terms of radial/tangential components

*Huang et al (2007), Neuroimage*

# Talk Overview

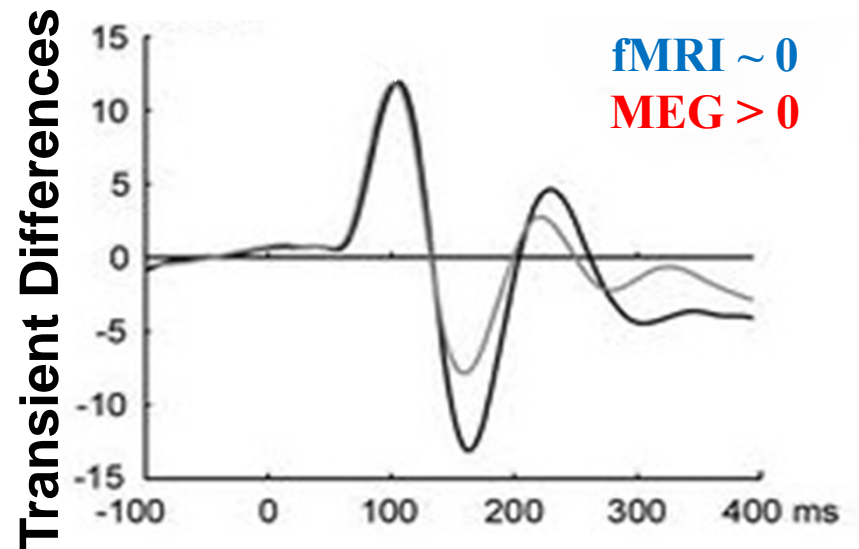
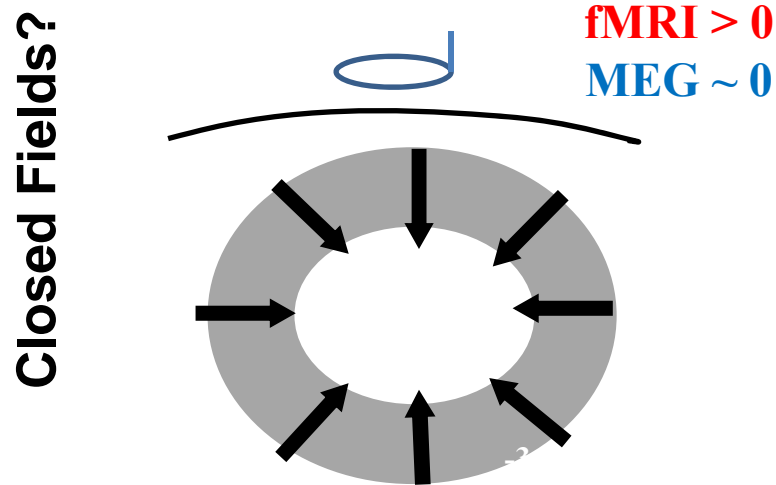
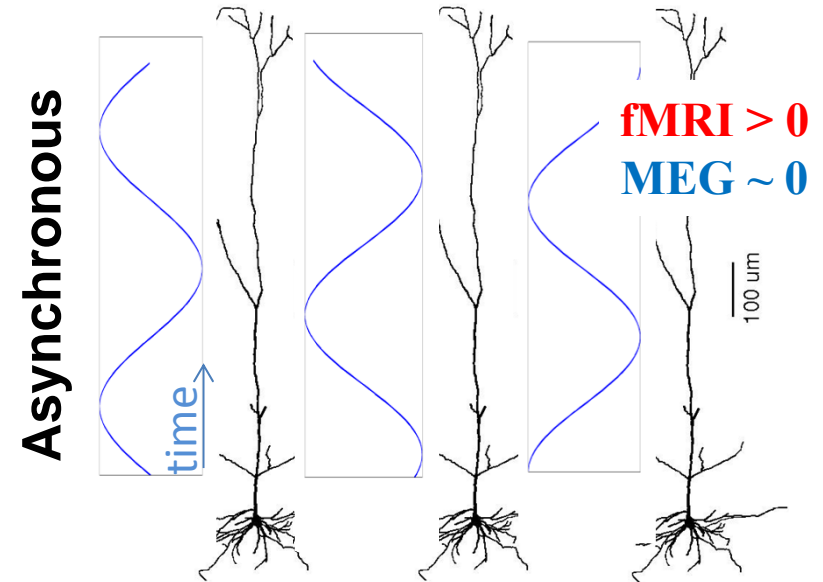
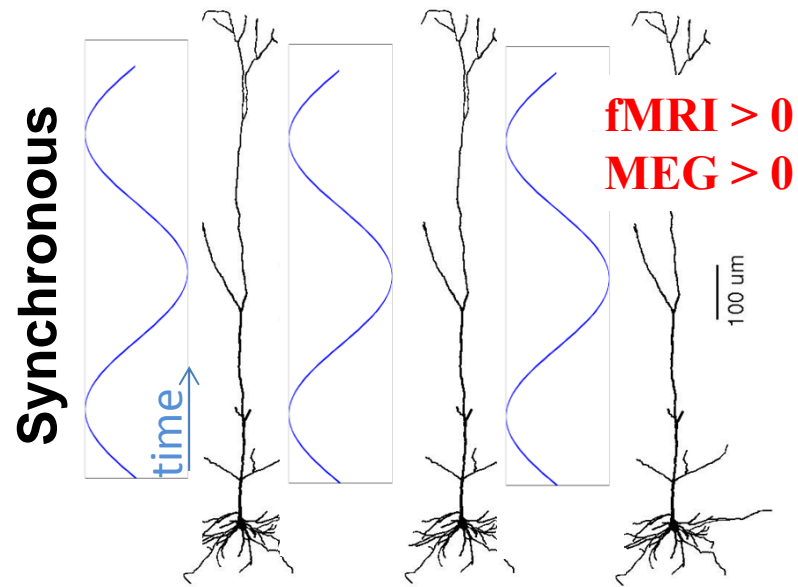
1. MEG + EEG symmetric integration (fusion)
- 2. M/EEG + fMRI asymmetric integration**

# Asymmetric Integration of MEG+fMRI Background



- fMRI has superior spatial resolution (~mm) than M/EEG, but inferior temporal resolution (integrating over seconds)
- fMRI and M/EEG measure similar, but not identical, neural activity
- Eg, some source configurations give detectable fMRI signal, but no detectable M/EEG signal...
- ...and vice versa

# Asymmetric Integration of MEG+fMRI Background



# Asymmetric Integration of MEG+fMRI Background



- fMRI has superior spatial resolution (~mm) than M/EEG, but inferior temporal resolution (integrating over seconds)
- fMRI and M/EEG measure similar, but not identical, neural activity
- Eg, some source configurations give detectable fMRI signal, but no detectable M/EEG signal...
- ...and vice versa
- Use fMRI as a **soft**, rather than **hard**, constraint on localisation of sources of M/EEG data...

# Asymmetric Integration of MEG+fMRI

Specifying (co)variance components (priors/regularisation):

$$C = \sum_i \lambda_i Q_i$$

C = Sensor/Source covariance  
Q = Covariance components  
 $\lambda$  = Hyper-parameters

1. Sensor components,  $Q_i^{(e)}$  (error):

“IID” (white noise):

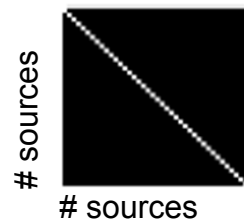


Empty-room:

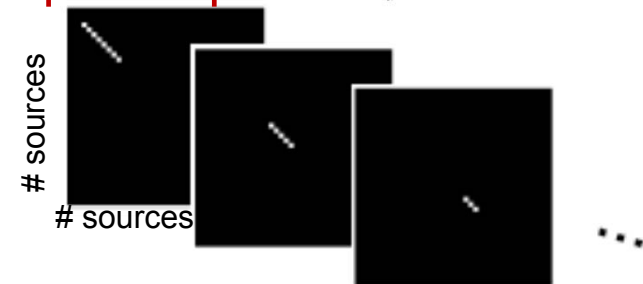


2. Each suprathreshold fMRI cluster becomes a separate prior  $Q_i^{(s)}$

“IID” (min norm):



fMRI Priors:



# Asymmetric Integration of MEG+fMRI

General solution again:

$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d} \quad \mathbf{e} \sim N(0, \mathbf{C}^{(e)})$$
$$\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$$

Now source covariance expressed as number of fMRI clusters:

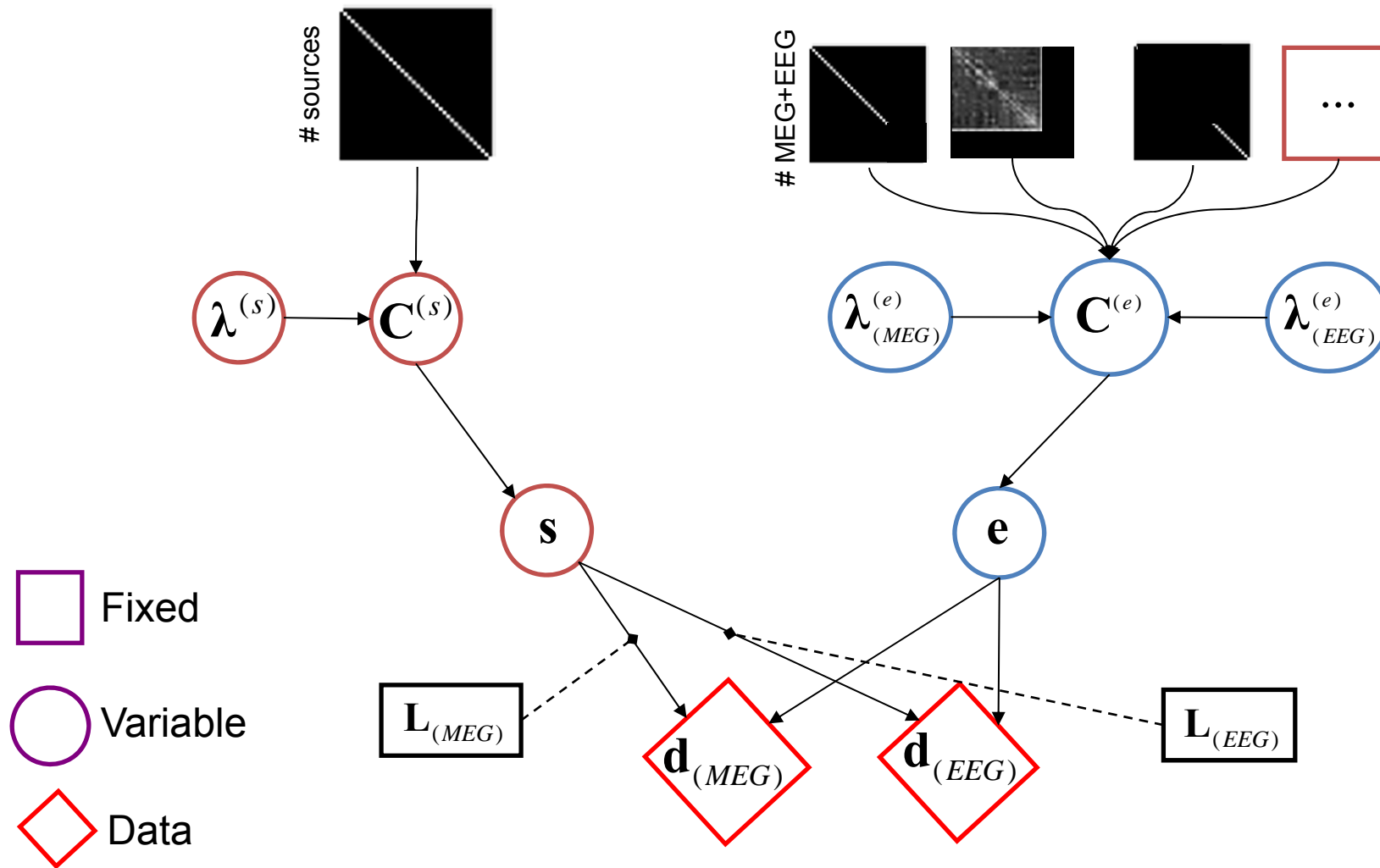
$$\mathbf{C}^{(s)} = \lambda_1^{(s)} \mathbf{Q}_{(fMRI1)}^{(s)} + \lambda_2^{(s)} \mathbf{Q}_{(fMRI2)}^{(s)} + \dots$$

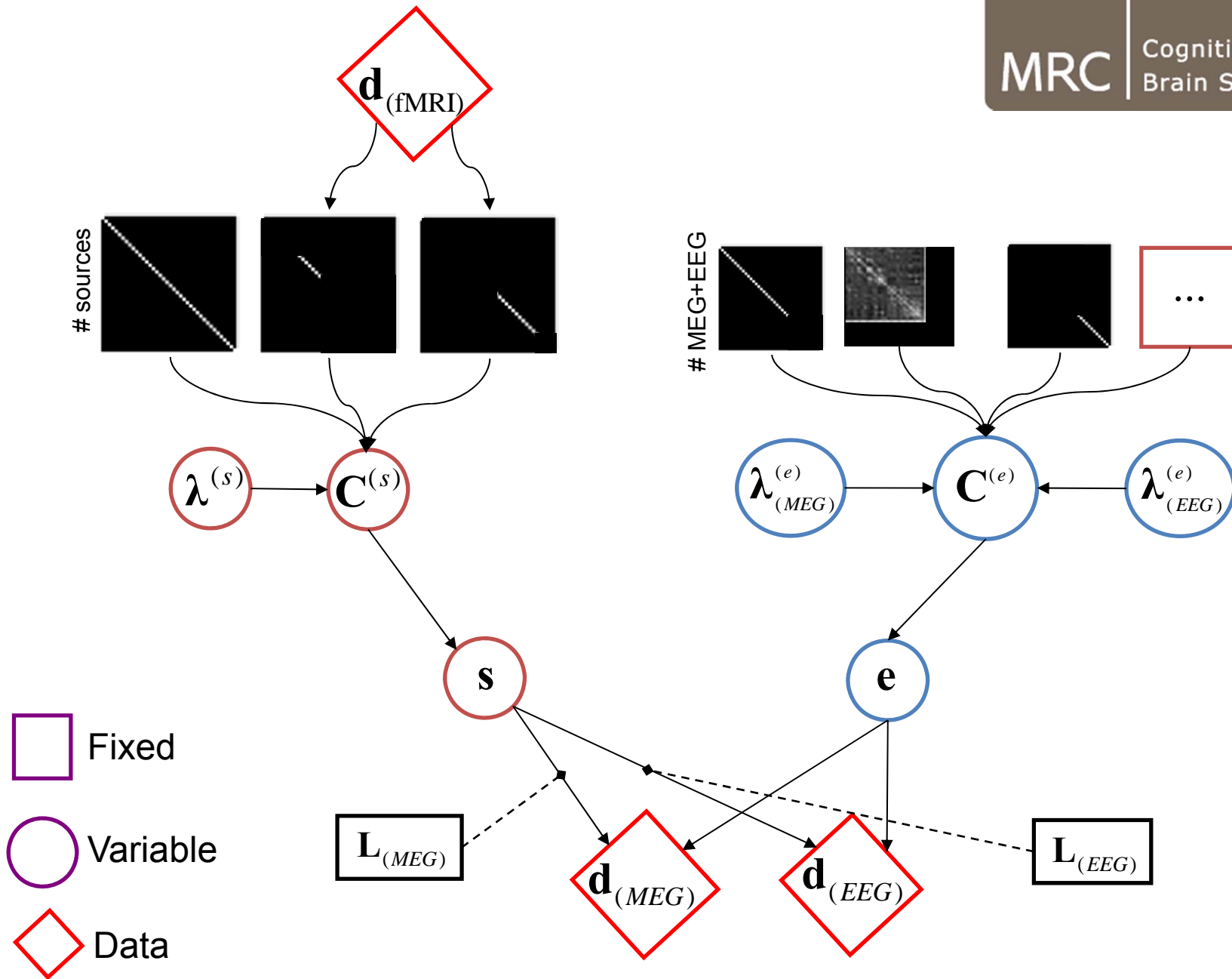
When  $\mathbf{Q}_i^{(s)}$  does not help maximise model evidence,  $\lambda_i^{(s)} \rightarrow 0$ ,  
i.e, constraints ignored...

...catering for situations where fMRI signal does not reflect same activity as in M/EEG signal (e.g, occurring later than time-window than M/EEG data)

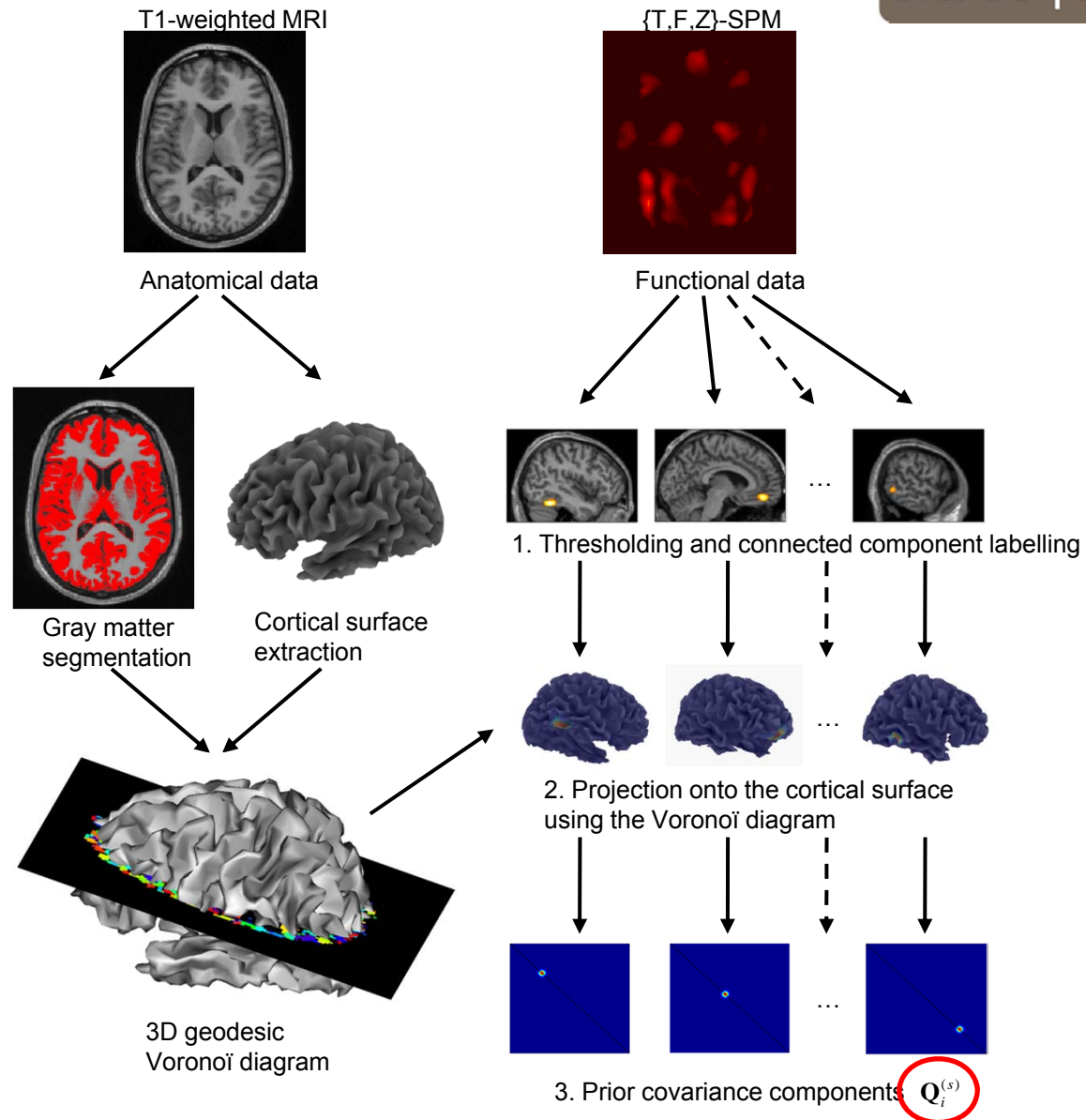


# Symmetric Integration of MEG+EEG Generative Model

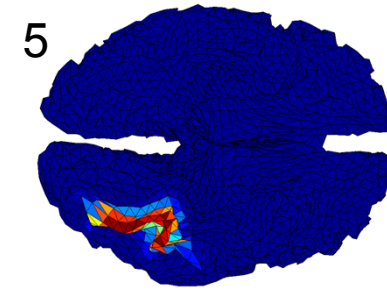
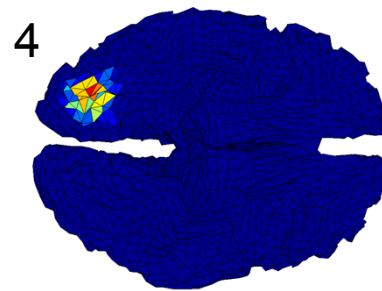
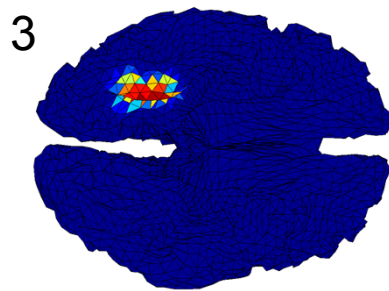
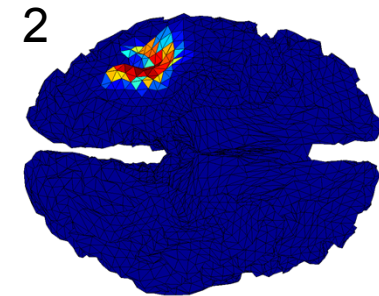
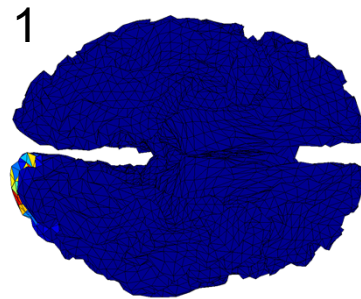
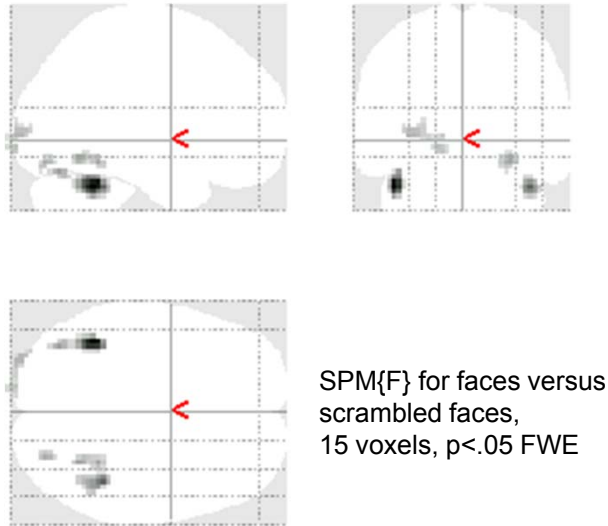




# Asymmetric Integration of M/EEG+fMRI

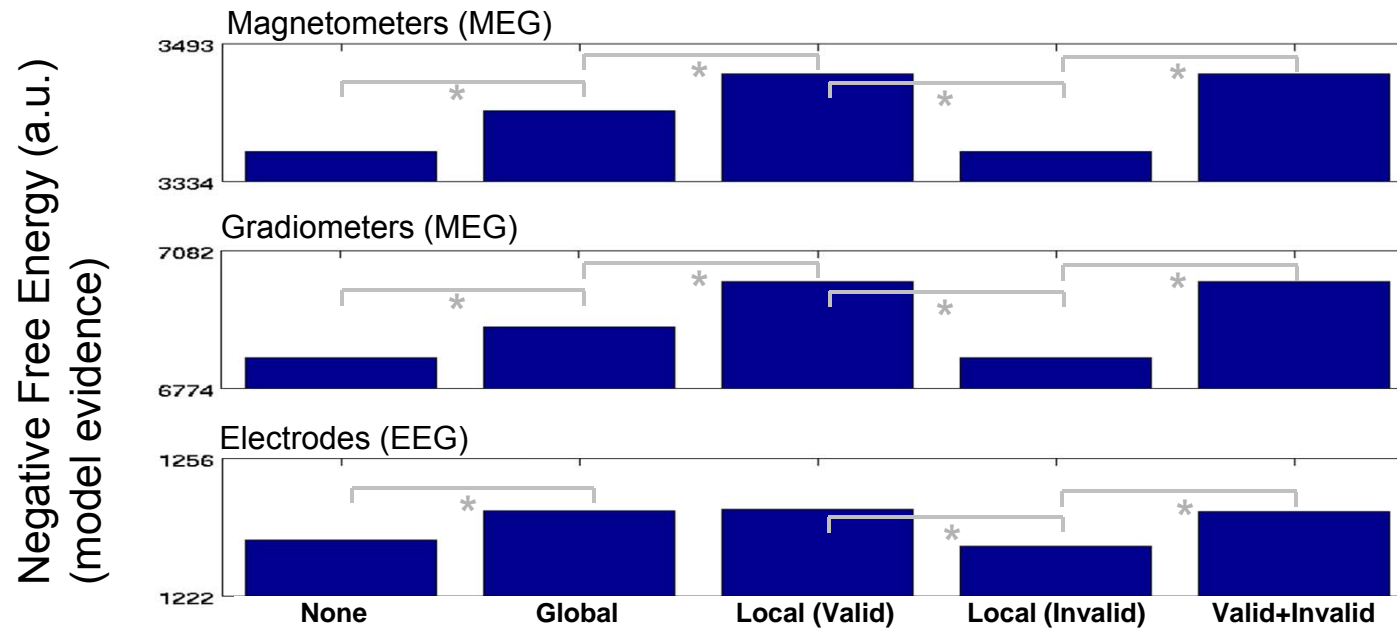


# Asymmetric Integration of M/EEG+fMRI



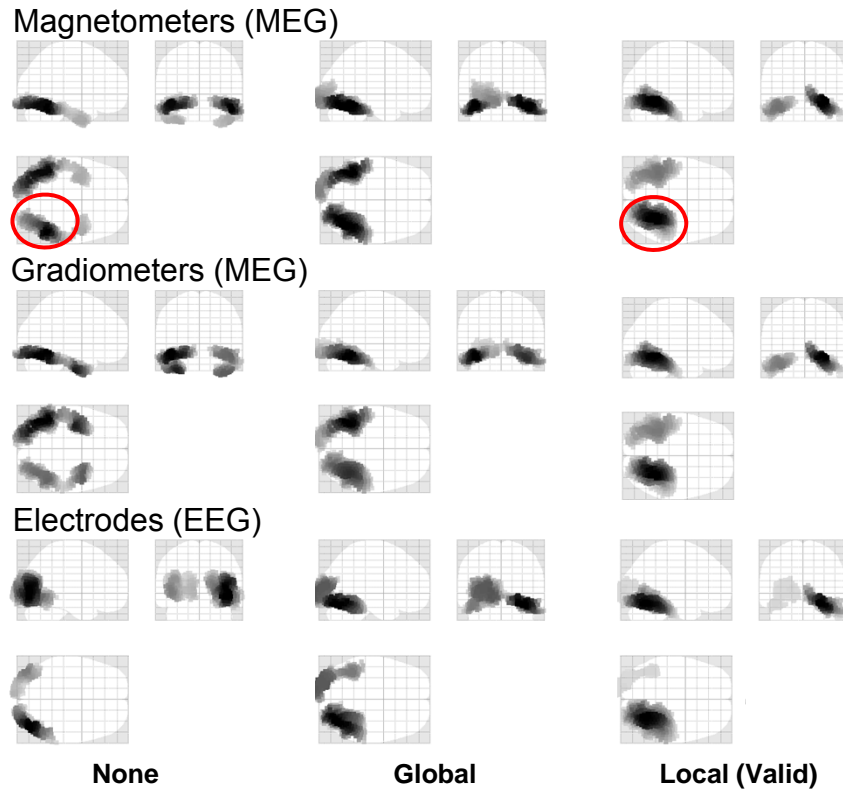
5 clusters from SPM of fMRI data from separate group of (18) subjects in MNI space

# Asymmetric Integration of M/EEG+fMRI



# Asymmetric Integration of M/EEG+fMRI

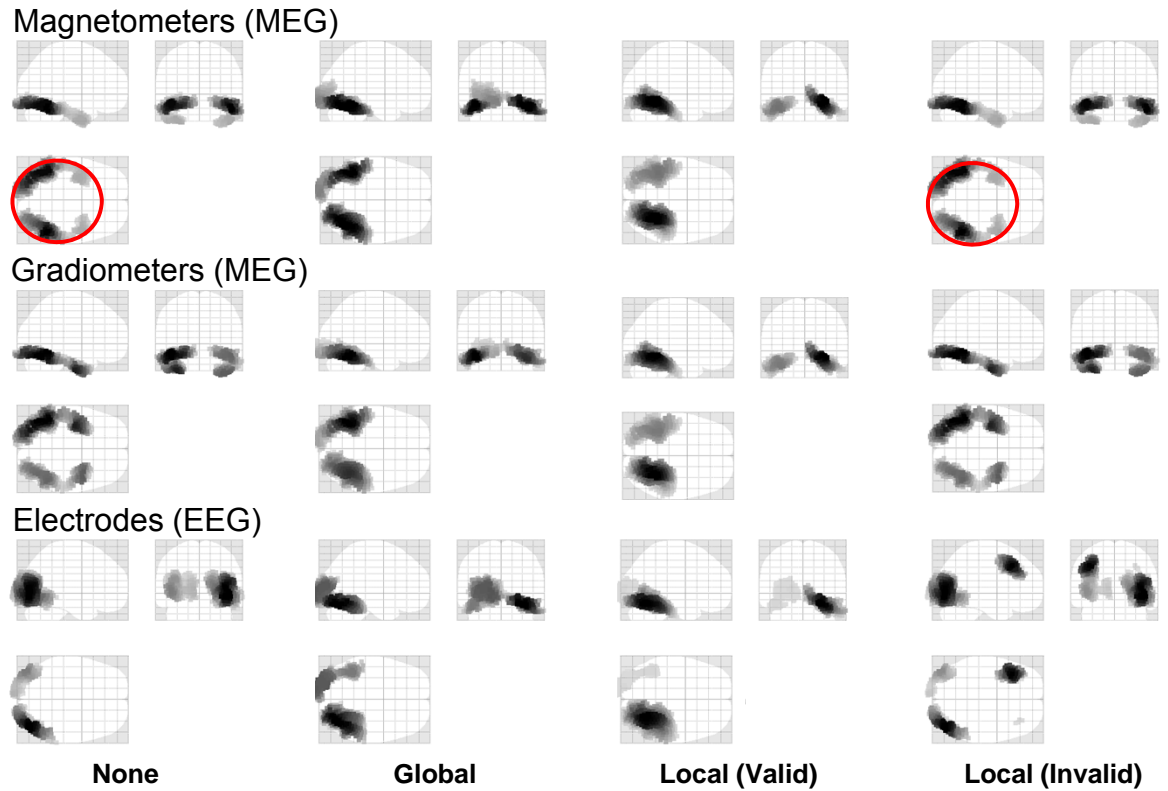
IID sources and IID noise (L2 MNM)



fMRI priors counteract superficial bias of Min Norm

# Asymmetric Integration of M/EEG+fMRI

## IID sources and IID noise (L2 MNM)



Invalid priors generally discounted (at least for MEG)

- Adding a single, global fMRI prior increases model evidence
- Adding **multiple** valid priors increases model evidence further
- Adding invalid priors does not necessarily increase model evidence, particularly in conjunction with valid priors  
Helpful if some fMRI regions produce no MEG/EEG signal  
(or arise from neural activity at different times)
- Can counteract superficial bias of, e.g, minimum-norm
- Makes some allowance for different sensitivities of fMRI and M/EEG to certain types of neural activity



# Other Approaches to fMRI/MEG/EEG



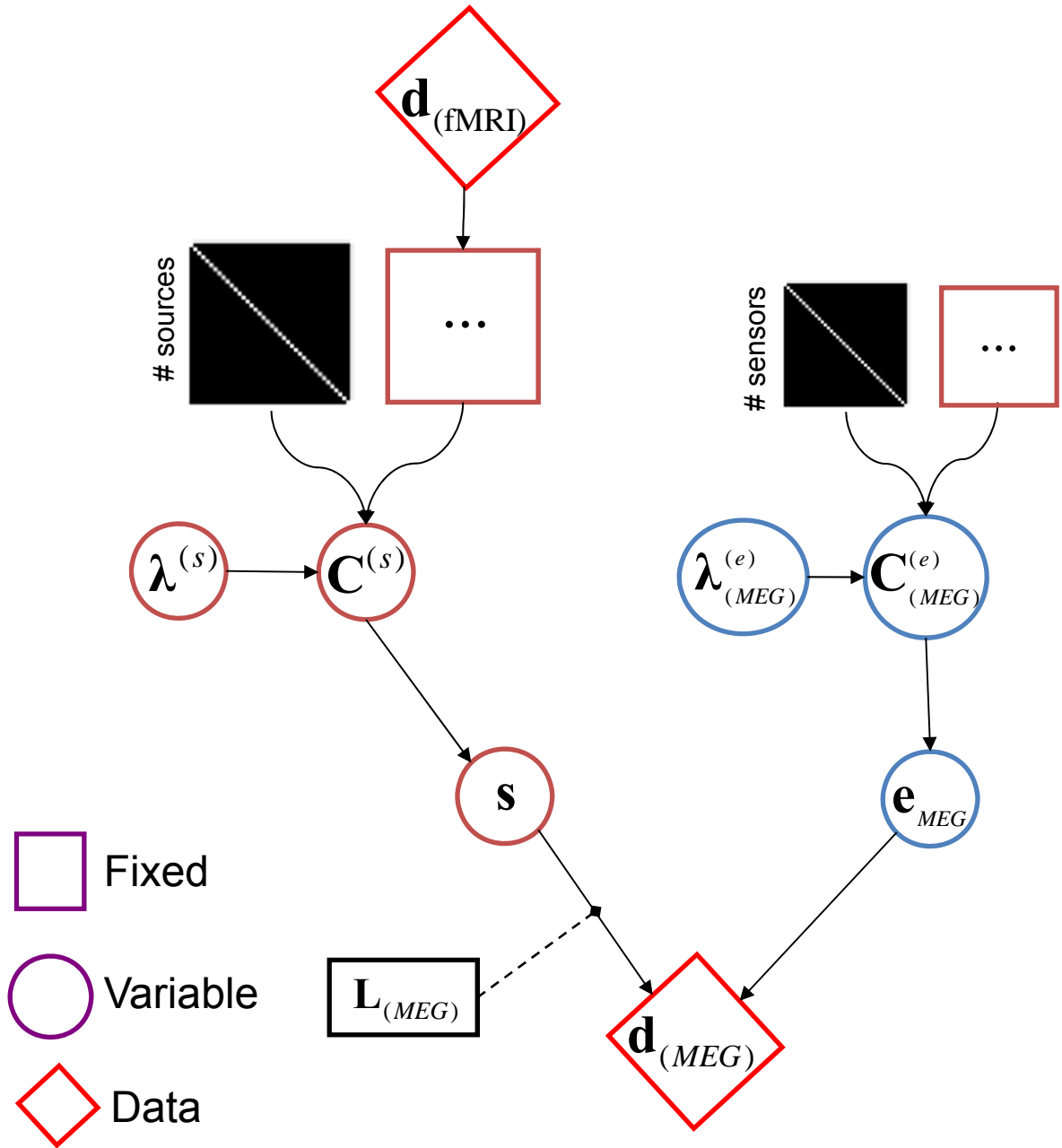
## Symmetric Integration (fusion) of fMRI and M/EEG

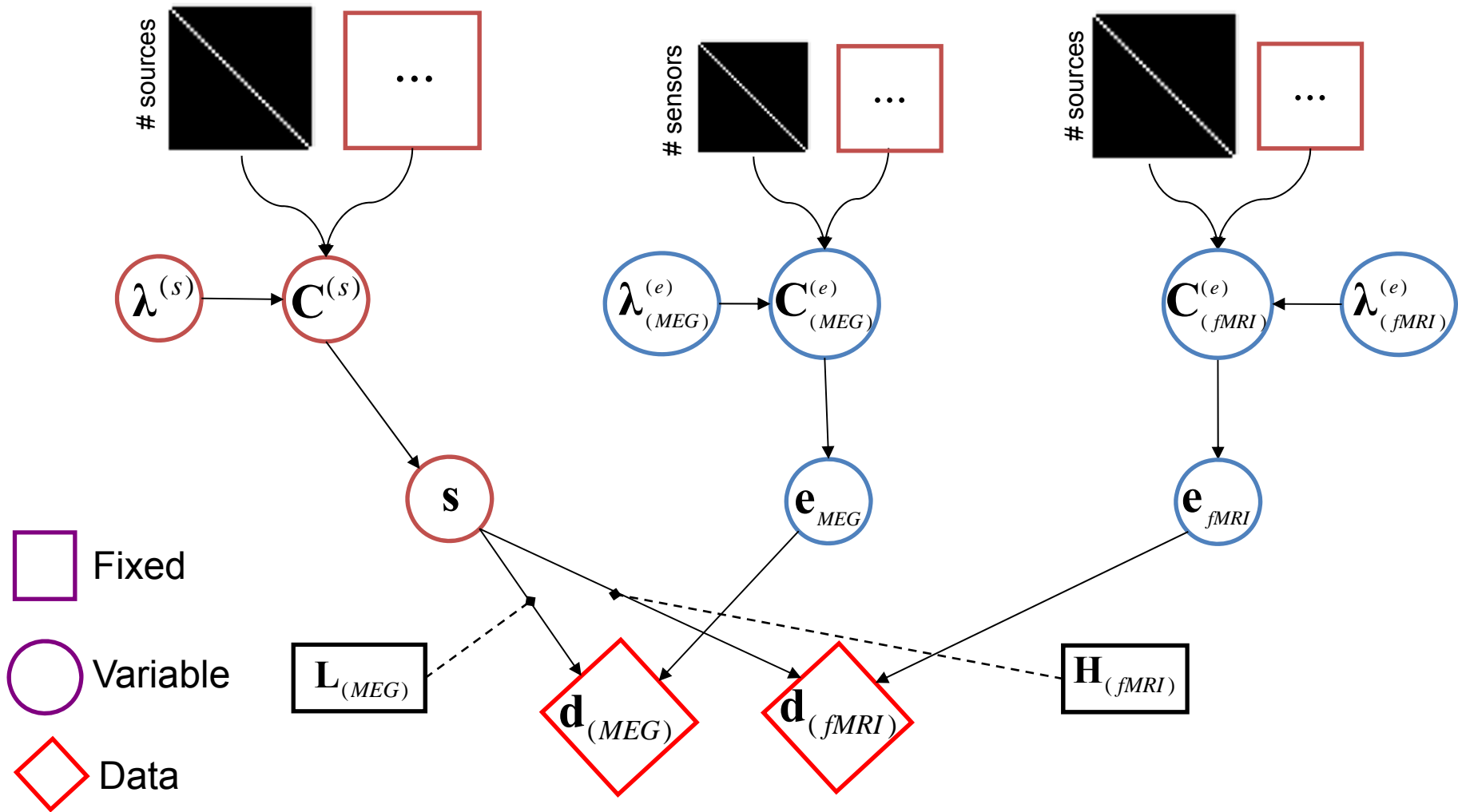
- e.g based on ROIs:

*Ou et al (2010), Neuroimage*

- e.g, full biophysical model

*Sotero & Trujillo-Barreto (2008), Neuroimage*



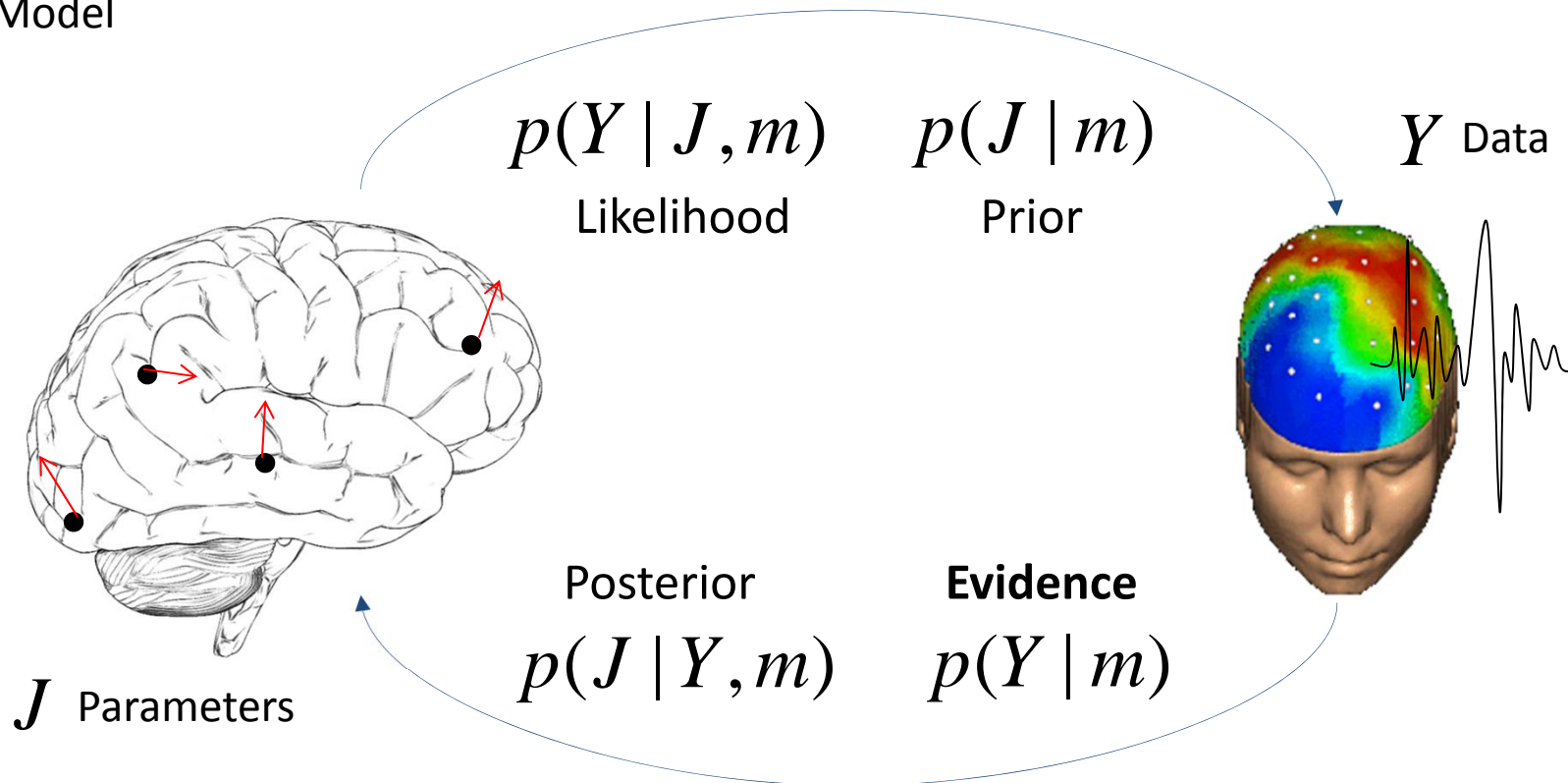


The End

# Bayesian Perspective

## Forward Problem

$m$  Model



## Inverse Problem

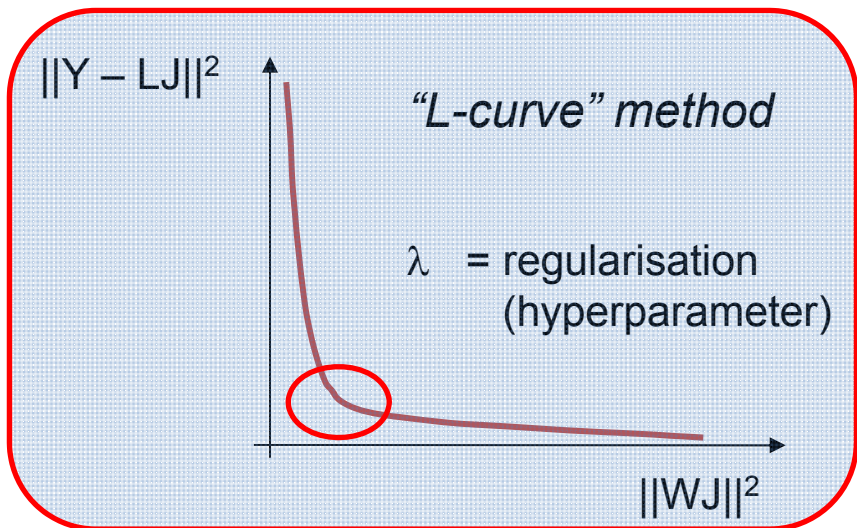
# Inverse Problem: Standard L2-norm

$$\mathbf{Y} = \mathbf{L}\mathbf{J} + \mathbf{E} \quad \mathbf{E} \sim N(\mathbf{0}, \mathbf{C}^{(e)})$$

$$\mathbf{J} = \arg \min \left\{ \left\| \mathbf{C}^{(e)-1/2} (\mathbf{Y} - \mathbf{L}\mathbf{J}) \right\|^2 + \lambda \left\| \mathbf{W}\mathbf{J} \right\|^2 \right\}$$

$$= (\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T [\mathbf{L} (\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T + \lambda \mathbf{C}^{(e)}]^{-1} \mathbf{Y}$$

“Tikhonov Solution”



- $\mathbf{W} = \mathbf{I}$  “Minimum Norm”
- $\mathbf{W} = \mathbf{D}\mathbf{D}^T$  “Loreta” ( $\mathbf{D}$ =Laplacian)
- $\mathbf{W} = \text{diag}(\mathbf{L}^T \mathbf{L})^{-1}$  “Depth-Weighted”
- $\mathbf{W}_p = \text{diag}(\mathbf{L}_p^T \mathbf{C}_y^{-1} \mathbf{L}_p)^{-1}$  “Beamformer”
- $\mathbf{W} = \dots$

# Inverse Problem: Equivalent PEB

Parametric Empirical Bayesian (PEB) 2-level hierarchical form:

$$\mathbf{Y} = \mathbf{L}\mathbf{J} + \mathbf{E}^{(e)} \quad \mathbf{E}^{(e)} \sim N(0, \mathbf{C}^{(e)})$$

$$\mathbf{J} = \mathbf{0} + \mathbf{E}^{(j)} \quad \mathbf{E}^{(j)} \sim N(0, \mathbf{C}^{(j)})$$

$\mathbf{C}^{(e)} = n \times n$  Sensor (error) covariance

$\mathbf{C}^{(j)} = p \times p$  Source (prior) covariance

Likelihood:

$$p(\mathbf{Y} | \mathbf{J}) = N(\mathbf{L}\mathbf{J}, \mathbf{C}^{(e)})$$

Prior:

$$p(\mathbf{J}) = N(0, \mathbf{C}^{(j)})$$

Posterior:

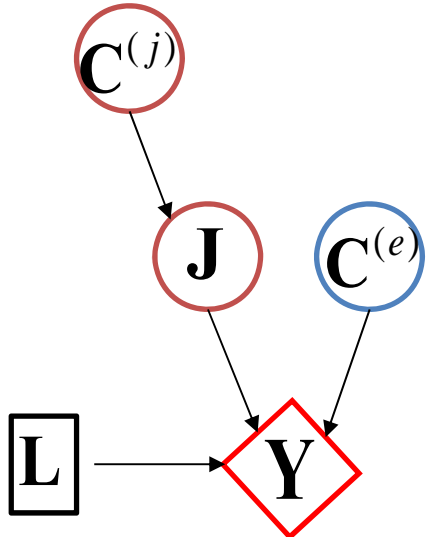
$$p(\mathbf{J} | \mathbf{Y}) \propto p(\mathbf{Y} | \mathbf{J})p(\mathbf{J})$$

Maximum A Posteriori (MAP) estimate:

$$\hat{\mathbf{J}} = \mathbf{C}^{(j)}\mathbf{L}^T [\mathbf{L}\mathbf{C}^{(j)}\mathbf{L}^T + \mathbf{C}^{(e)}]^{-1} \mathbf{Y}$$

cf Classical Tikhonov:

$$(\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T [\mathbf{L}(\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T + \lambda \mathbf{C}^{(e)}]^{-1} \mathbf{Y} \Rightarrow \mathbf{C}^{(j)} = (\mathbf{W}^T \mathbf{W})^{-1}$$



# PEB: Estimation

1. Obtain Restricted Maximum Likelihood (ReML) estimates of the hyperparameters ( $\lambda$ ) by maximising the variational “free energy” ( $F$ ):

$$\hat{\lambda} = \max_{\lambda} p(\mathbf{Y} | \lambda) = \max_{\lambda} F$$

2. Obtain Maximum A Posteriori (MAP) estimates of parameters (sources,  $\mathbf{J}$ ):

$$\hat{\mathbf{J}} = \max_{\mathbf{J}} p(\mathbf{J} | \mathbf{Y}, \hat{\lambda}) = \max_{\mathbf{J}} F$$

3. Maximal  $F$  approximates Bayesian (log) “model evidence” for a model,  $m$ :

$$\ln p(\mathbf{Y} | m) = \ln \int \int p(\mathbf{Y}, \mathbf{J}, \lambda | m) d\mathbf{J} d\lambda \approx F(\mathbf{Y}, \hat{\boldsymbol{\alpha}}, \hat{\boldsymbol{\Sigma}}) \quad m = \{\mathbf{L}, \mathbf{Q}, \boldsymbol{\eta}, \boldsymbol{\Omega}\}$$

$$F(\mathbf{Y}, \hat{\boldsymbol{\alpha}}, \hat{\boldsymbol{\Sigma}}) \propto \underbrace{-\text{tr}(\mathbf{C}^{-1} \mathbf{Y} \mathbf{Y}^T) - \ln |\mathbf{C}|}_{\text{Accuracy}} \underbrace{- (\hat{\boldsymbol{\alpha}} - \boldsymbol{\eta})^T \boldsymbol{\Omega}^{-1} (\hat{\boldsymbol{\alpha}} - \boldsymbol{\eta}) + \ln |\hat{\boldsymbol{\Sigma}} \boldsymbol{\Omega}^{-1}|}_{\text{Complexity}}$$

(...where  $\hat{\boldsymbol{\alpha}}$  and  $\hat{\boldsymbol{\Sigma}}$  are the posterior mean and covariance of hyperparameters)

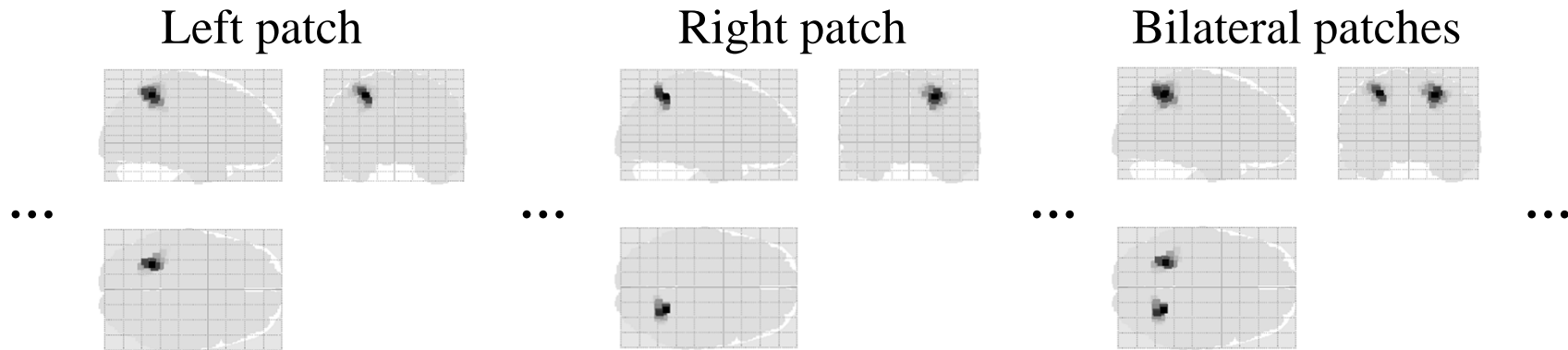


# PEB: Multiple Sparse Priors

Hyperpriors allow the extreme of 100's source priors, or MSP

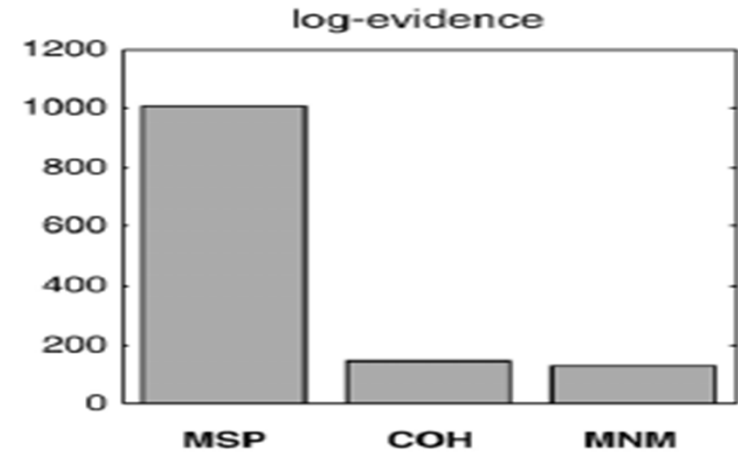
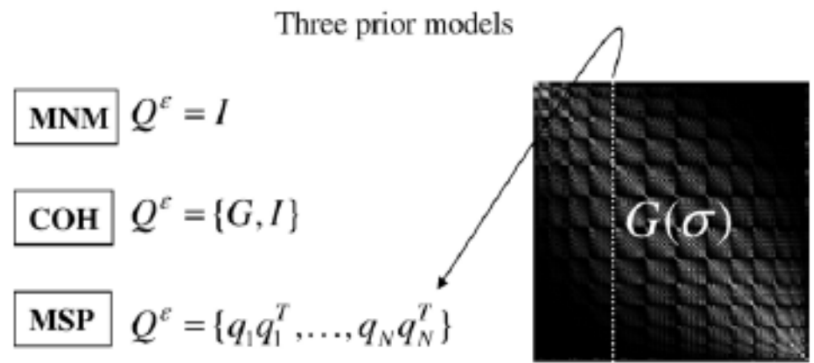


$$G(\sigma) = [q_1, \dots, q_N] = \sum_{i=0}^8 \frac{\sigma^i}{i!} A^i \approx \exp(\sigma A)$$

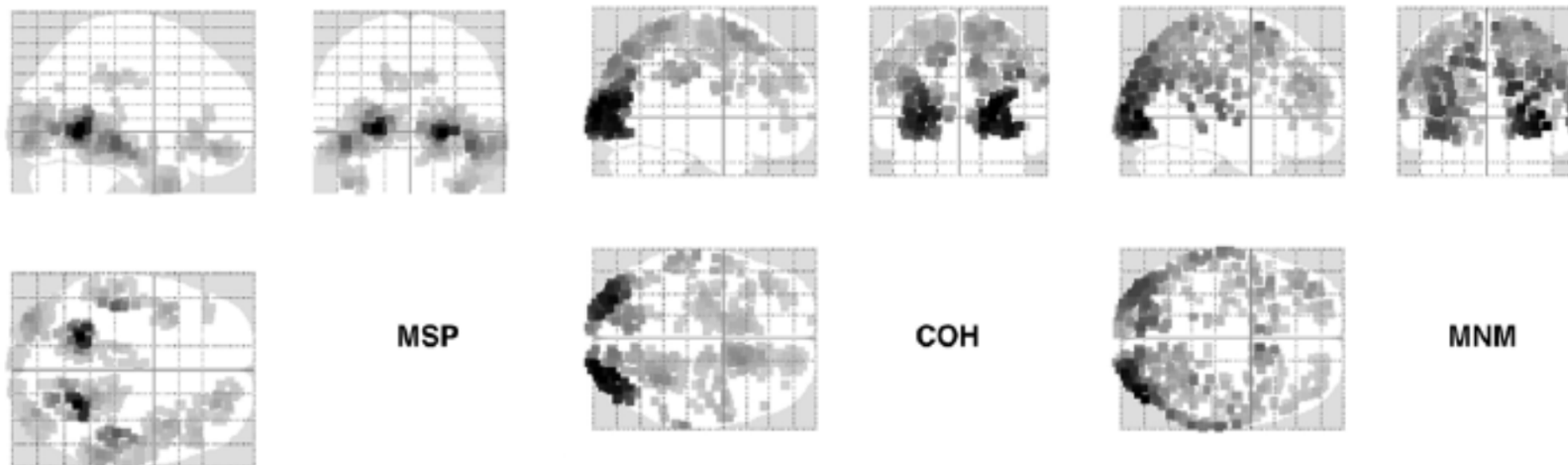


# PEB: Multiple Sparse Priors

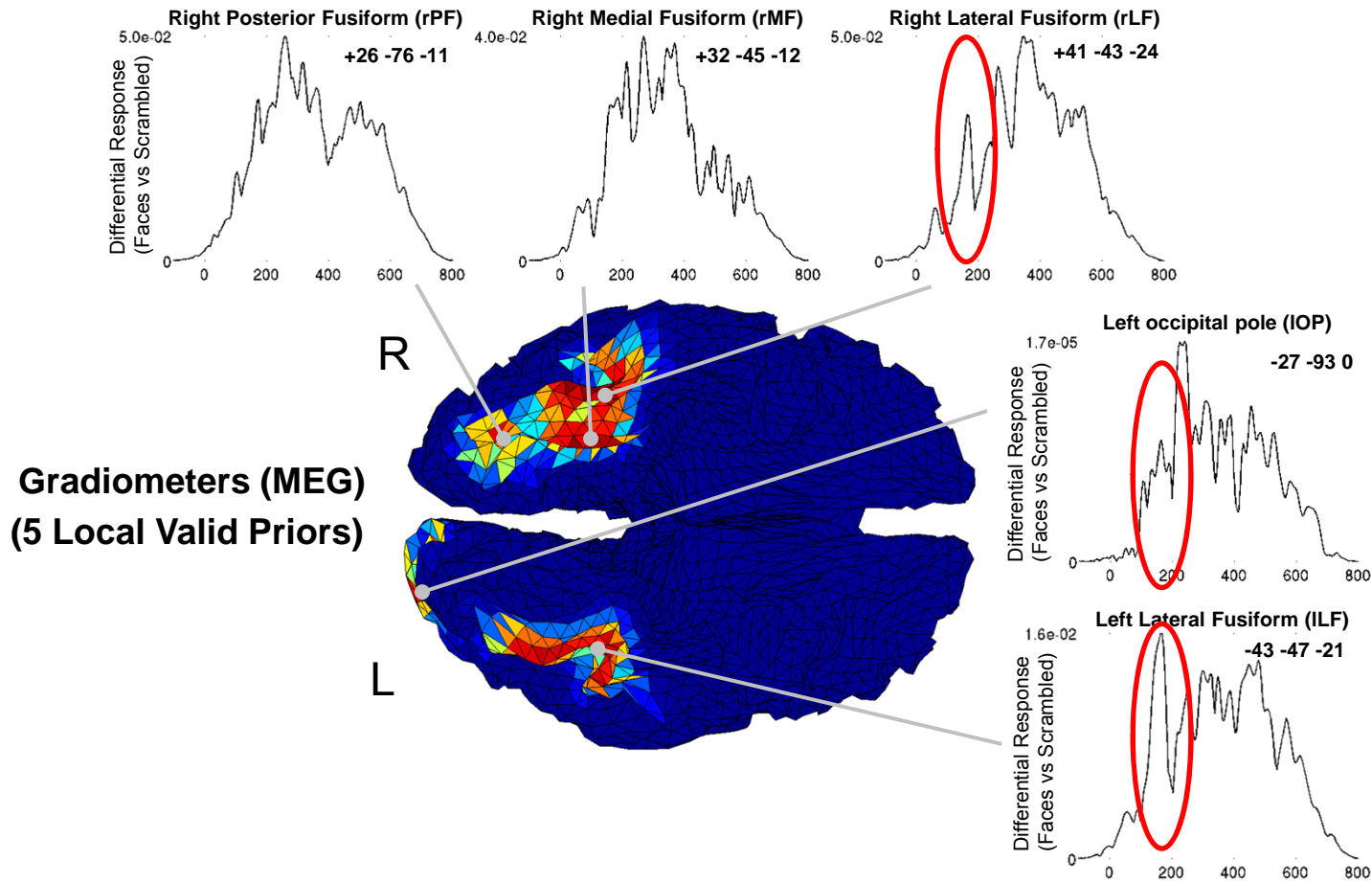
Hyperpriors allow the extreme of 100's source priors, or MSP



$$G(\sigma) = [q_1, \dots, q_N] = \sum_{i=0}^8 \frac{\sigma^i}{i!} A^i \approx \exp(\sigma A)$$



# Asymmetric Integration of M/EEG+fMRI



NB: Priors affect variance, not precise timecourse...

# PEB Summary



## Summary:

- **Automatically** “regularises” in principled fashion...
- ...allows for **multiple** constraints (priors)...
- ...to the extent that multiple (100’s) of sparse priors possible (MSP)...
- ...(or multiple error components or multiple fMRI priors)...
- ...furnishes estimates of **model evidence**, so can compare constraints