



MRC Cognition  
and Brain  
Sciences Unit



UNIVERSITY OF  
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# EEG/MEG 4: Multimodal Integration and Prior Information

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COGNESTIC 2023

# Multimodal Dataset

## A multi-subject, multi-modal human neuroimaging dataset

[Daniel G Wakeman](#) & [Richard N Henson](#)

*Scientific Data* **2**, Article number: 150001 (2015) | [Cite this article](#)

<https://www.nature.com/articles/sdata20151>

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

### METHODS article

Front. Neurosci., 06 August 2018  
Sec. Brain Imaging Methods  
Volume 12 - 2018 | <https://doi.org/10.3389/fnins.2018.00530>

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## A Reproducible MEG/EEG Group Study With the MNE Software: Recommendations, Quality Assessments, and Good Practices

 Mainak Jas<sup>1</sup>  Eric Larson<sup>2</sup>  Denis A. Engemann<sup>3,4</sup>  Jaakko Leppäkangas<sup>1</sup>  
 Samu Taulu<sup>2,5</sup>  Matti Hämäläinen<sup>6</sup>  Alexandre Gramfort<sup>1,3,4\*</sup>

<https://www.frontiersin.org/articles/10.3389/fnins.2018.00530/full>





### METHODS article

Front. Neurosci., 24 April 2019  
Sec. Brain Imaging Methods  
Volume 13 - 2019 | <https://doi.org/10.3389/fnins.2019.00300>

This article is part of the Research Topic  
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## Multimodal Integration of M/EEG and f/MRI Data in SPM12

 Richard N. Henson<sup>1\*</sup>  Hunar Abdulrahman<sup>1</sup>  Guillaume Flandin<sup>2</sup>  Vladimir Litvak<sup>2</sup>

<https://www.frontiersin.org/articles/10.3389/fnins.2019.00300/full>

# How Can We Combine Measurement Modalities?

## “Converging Evidence”:

Compare results from different modalities, determine commonalities and differences.

## “(Asymmetric) Fusion”:

Use one modality as a constraint for another.

(e.g. EEG->fMRI, fMRI->EEG/MEG)

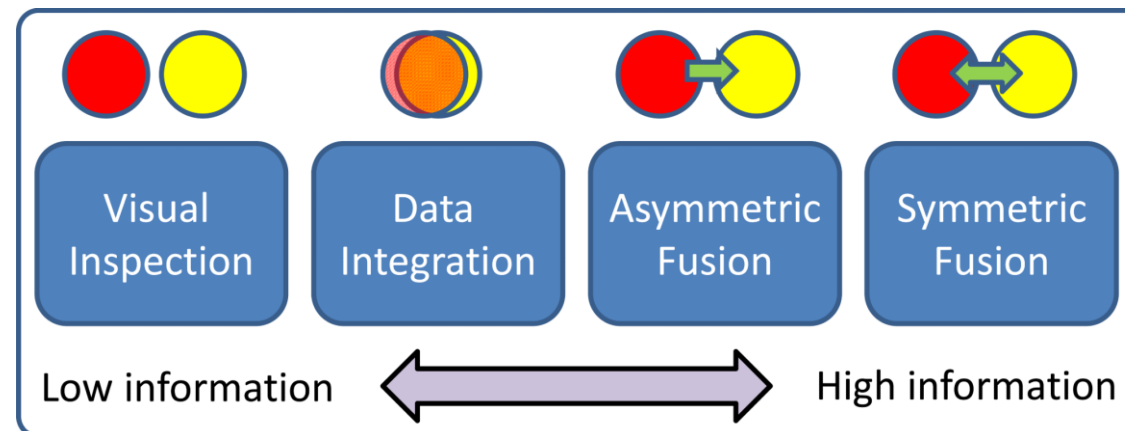
## “Neural Modelling” (“Symmetric Fusion”):

Use of a common neural model that accounts for signals in all modalities.

(e.g. EEG<->MEG)

e.g. Horwitz&Poeppel, HBM 2002; Henson et al., HBM 2010

Each of these options poses different challenges with respect to modelling assumptions and complexity.



# How Can We Combine Modalities?

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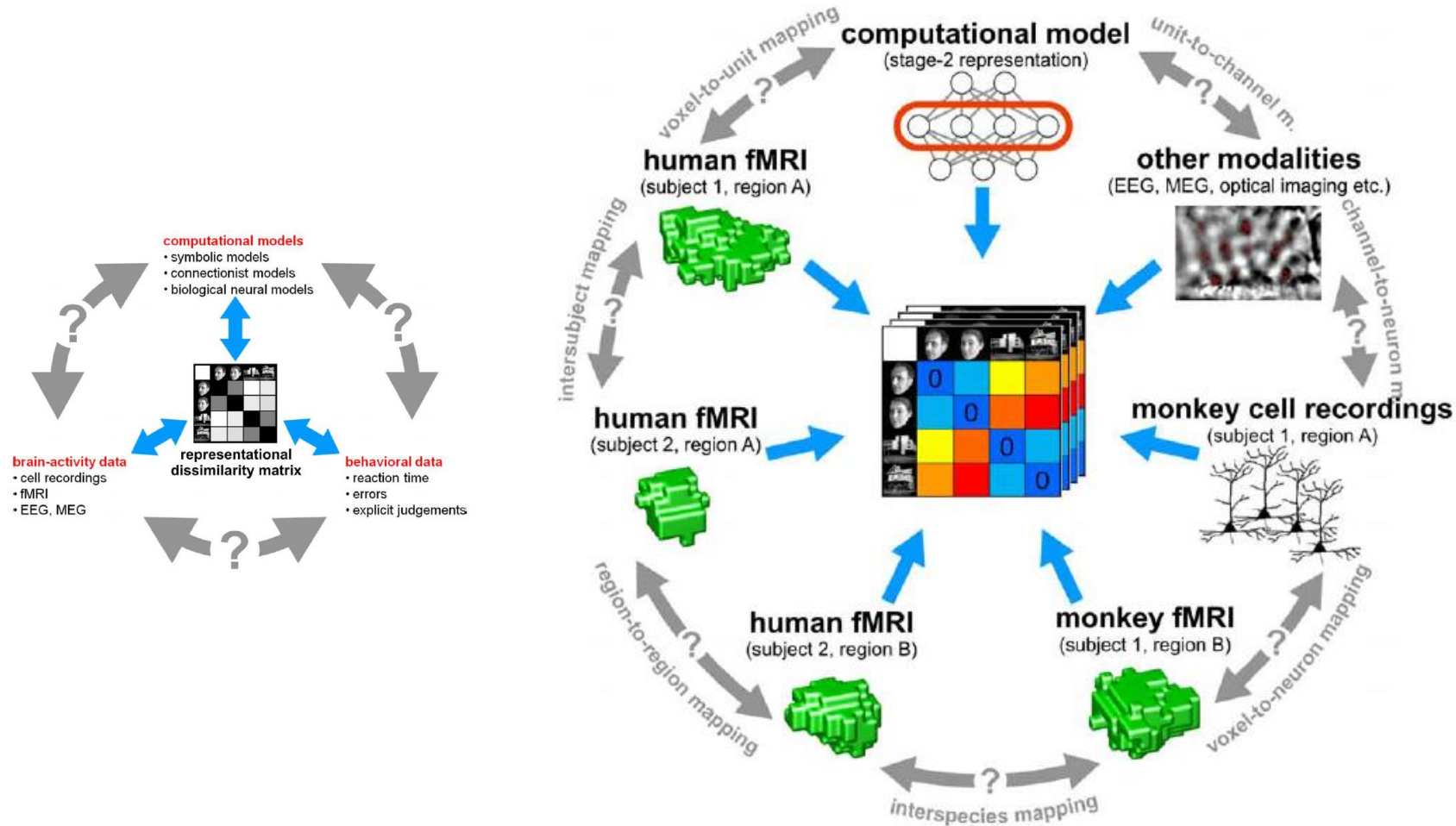
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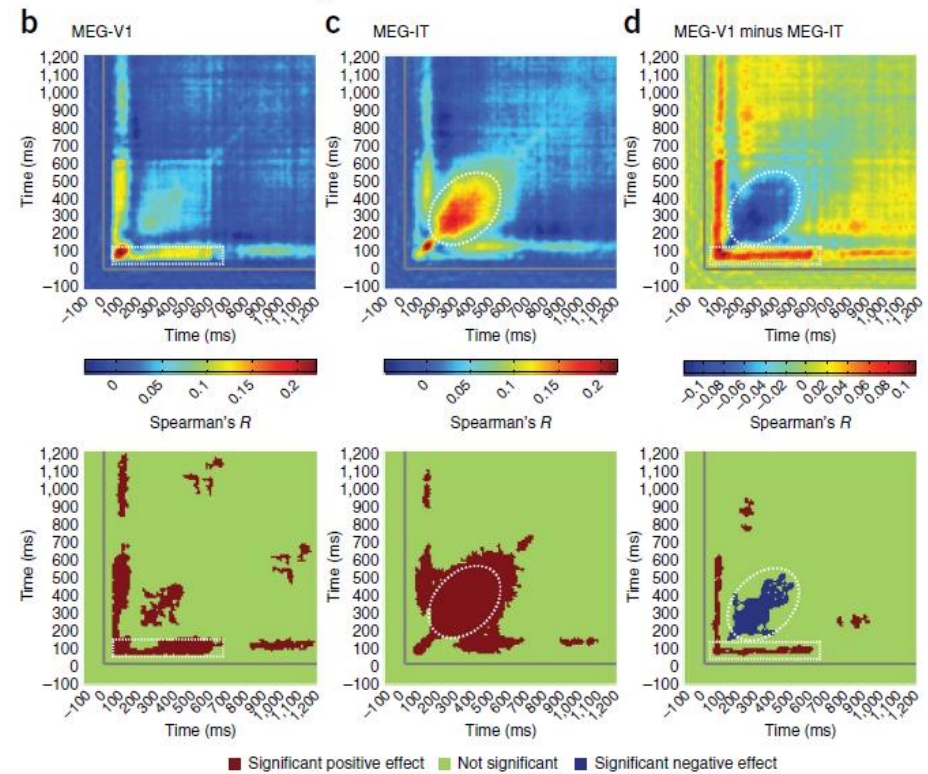
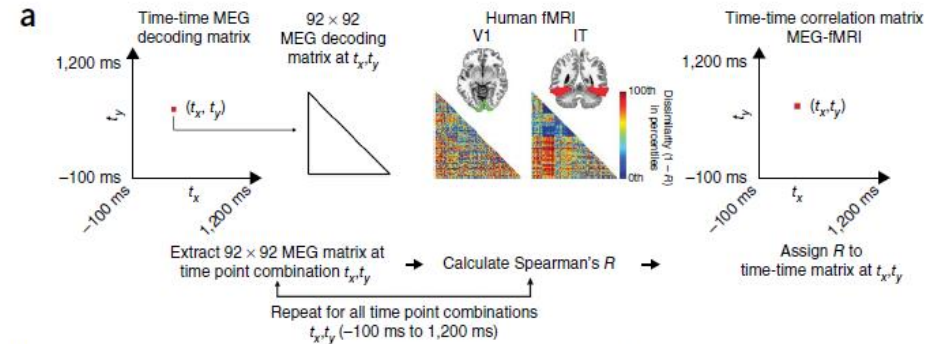
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# Comparing Representational Dissimilarity Across Neuroimaging Methods



# Comparing Representational Dissimilarity Across Neuroimaging Methods



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## **“Neural Modelling” (“Symmetric Fusion”):**

Use of a common neural model that accounts for signals in all modalities.

# Problems Integrating EEG/MEG And fMRI

1. Metabolic activity can occur without EEG/MEG activity.
2. EEG/MEG activity can occur without BOLD activity.
3. EEG/MEG and metabolic activity may have common sources, but are not fully spatially overlapping.
4. EEG/MEG and metabolic activity have different time courses.

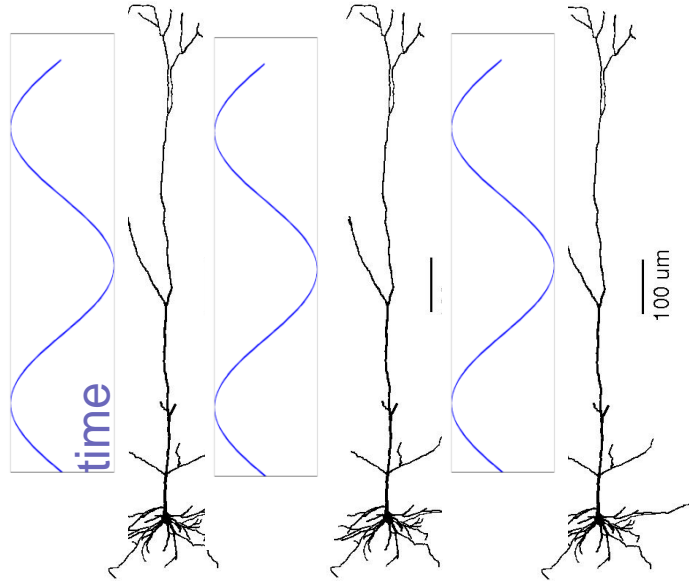
Note: Usually EEG/MEG and fMRI are acquired in different sessions, causing:

- a) inter- and intra-subject variability (same or different subjects in different sessions)
- b) differences in scanning position (supine, seated)
- c) differences in scanning environment (e.g. scanner noise)

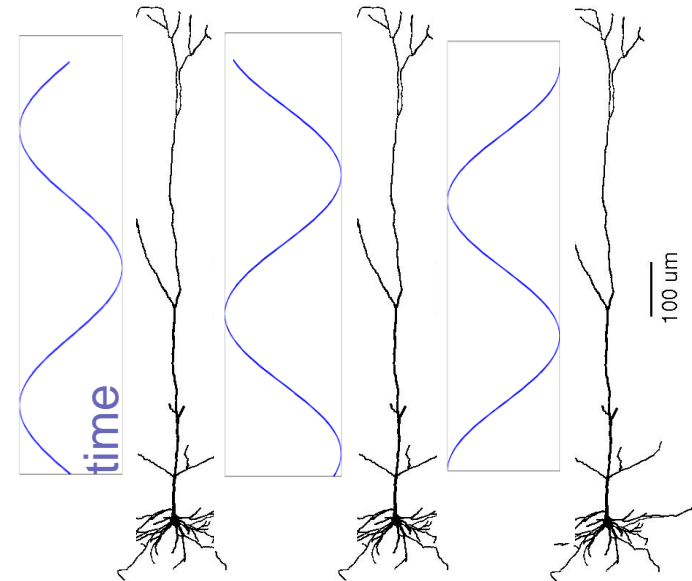


# Problems Integrating EEG/MEG And fMRI

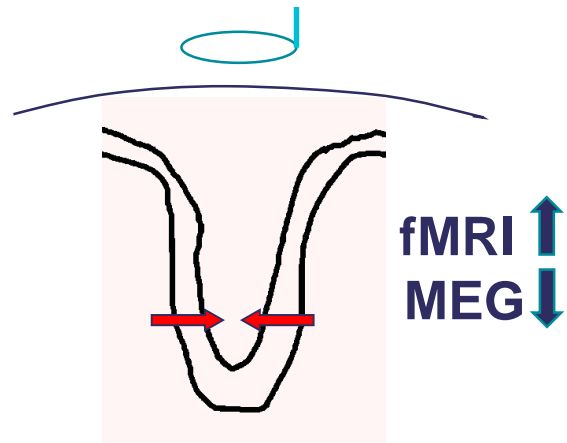
Synchronous: fMRI↑ MEG↑



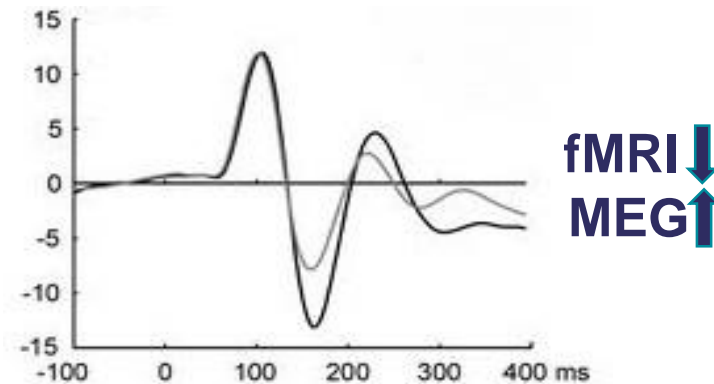
Asynchronous: fMRI↑ MEG↓



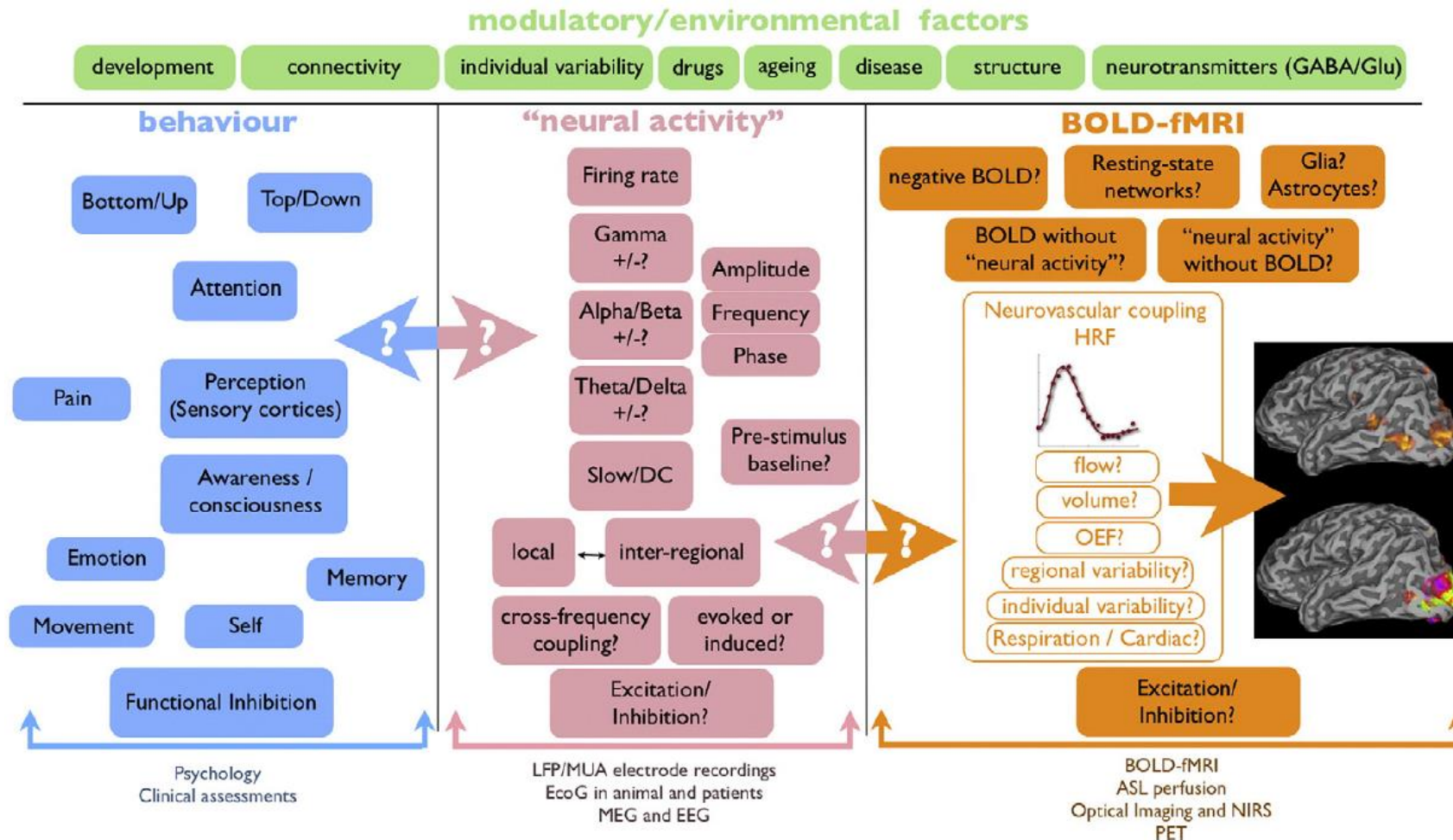
Source Configuration



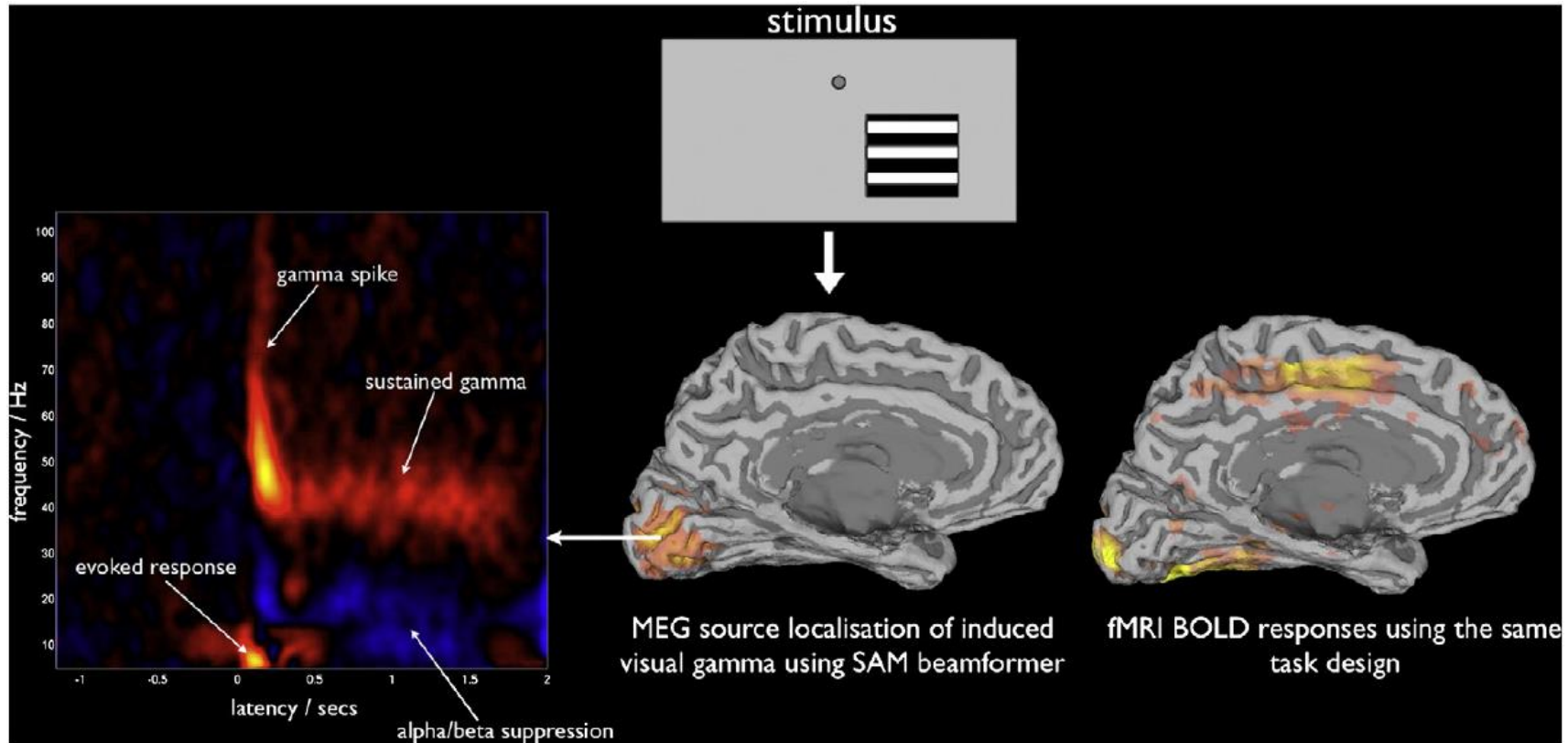
Time Scale



# Which “Neural Activity” Do You Mean?



# Which “Neural Activity” Do You Mean?



# Problems Integrating EEG/MEG And fMRI

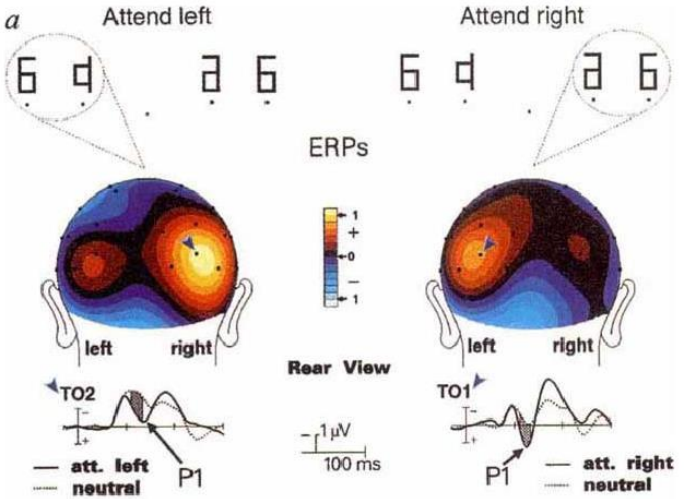
Liu et al., PNAS 1998:

- 1) “**Fundamental mis-specifications** can arise because EEG and MEG and fMRI measure physically different aspects of brain function.”
- 2) “**Experimental mis-specifications** refer to measurement or estimation errors that can be corrected, at least in theory”.

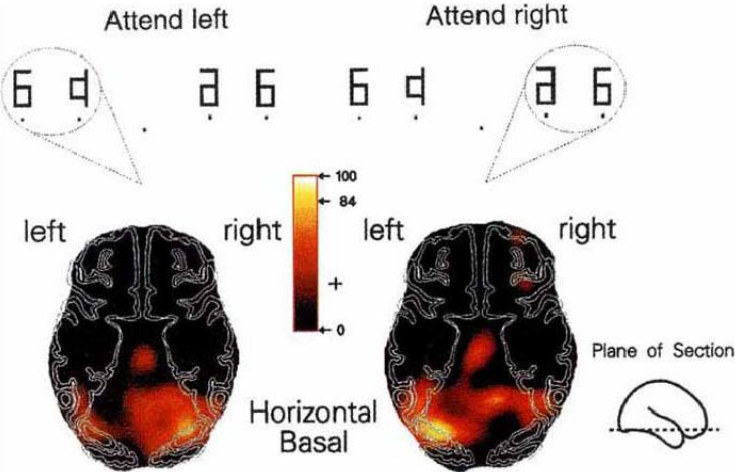
# Multimodal Integration

## Hypothesis-Guided Dipole Modelling

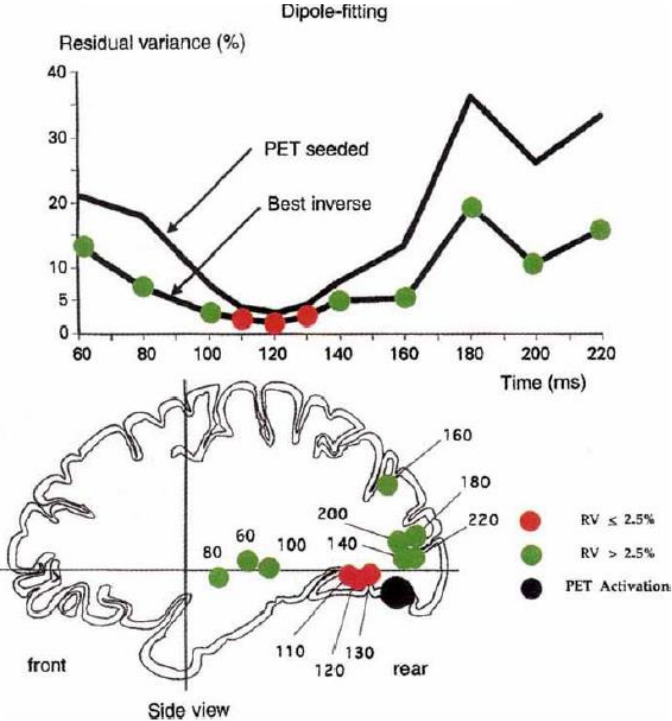
ERPs



PET



### PET-constrained Dipole Modelling



# “Weighting” and “Priors”

$$P(\mathbf{j}(r,t) | \mathbf{x}(t) \ \& \ f(r,t)) = \frac{P(\mathbf{x}(t) | \mathbf{j}(r,t)) P(f(r,t) | \mathbf{j}(r,t)) P(\mathbf{j}(r,t))}{P(\mathbf{x}(t) \ \& \ f(r,t))}$$

If source strengths and priors can be modelled as multivariate Gaussian distributions, then the maximum a posteriori probability (MAP) estimate is the minimum norm estimate:

$$\hat{\mathbf{s}}(t) = \mathbf{W}\mathbf{x}(t), \text{ where } \mathbf{W} = \mathbf{R}\mathbf{A}^T (\mathbf{A}\mathbf{R}\mathbf{A}^T + \mathbf{C})^{-1}$$

**A:** Leadfield

**R/C:** Source/noise covariance

$0 < R_{ii} < 1$

depending on fMRI

# Relative Weighting of fMRI

Ideally, this requires knowledge about “fMRI visible” and “fMRI invisible” sources –  
if we knew those, we wouldn’t need source estimation anymore.

“The optimal fMRI weighting, which depends on the confidence in the hypothesis that neuronal and hemodynamic activity are tightly coupled, currently cannot be determined *a priori*.”

Liu et al., PNAS 1998

# Relative Weighting of fMRI

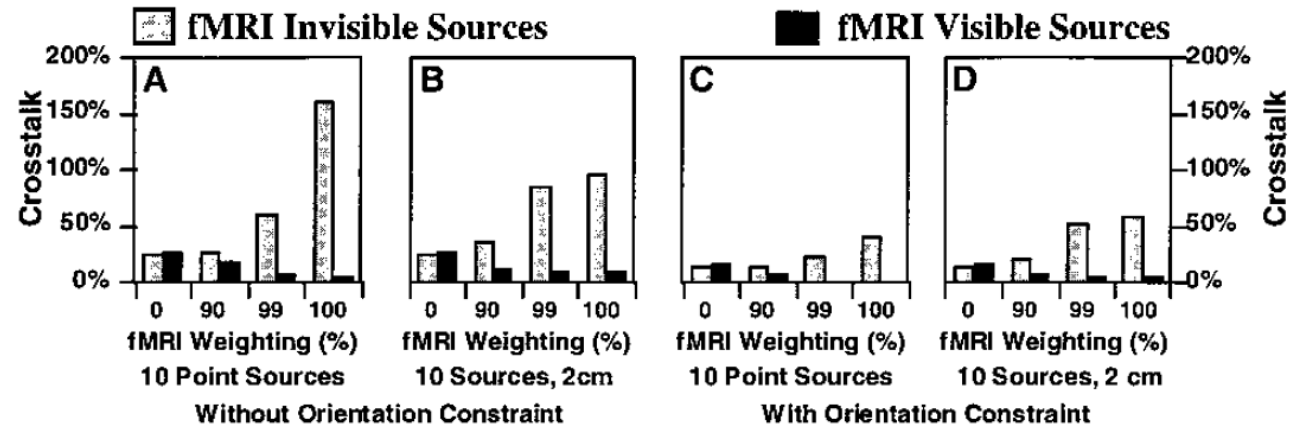


FIG. 3. Crosstalk versus relative fMRI weighting. Crosstalk is shown for 10 sources (point and 2 cm in diameter), with and without orientation constraint. The relative fMRI weighting was either 0%, 90%, 99%, or 100%. The optimal fMRI weighting requires a compromise between resolving fMRI visible sources (i.e., higher fMRI weighting) and minimizing distortion from fMRI invisible sources (i.e., lower fMRI weighting). The results indicate that a 90% fMRI weighting greatly reduces the crosstalk from fMRI visible sources, while only slightly increasing the crosstalk from fMRI invisible sources.



# Relative Weighting of fMRI

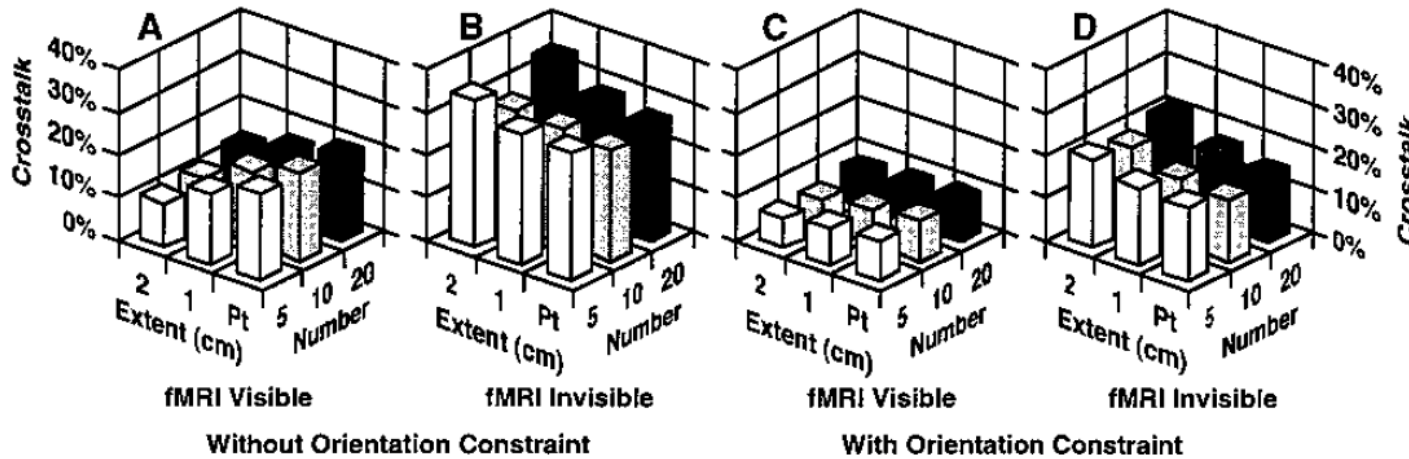
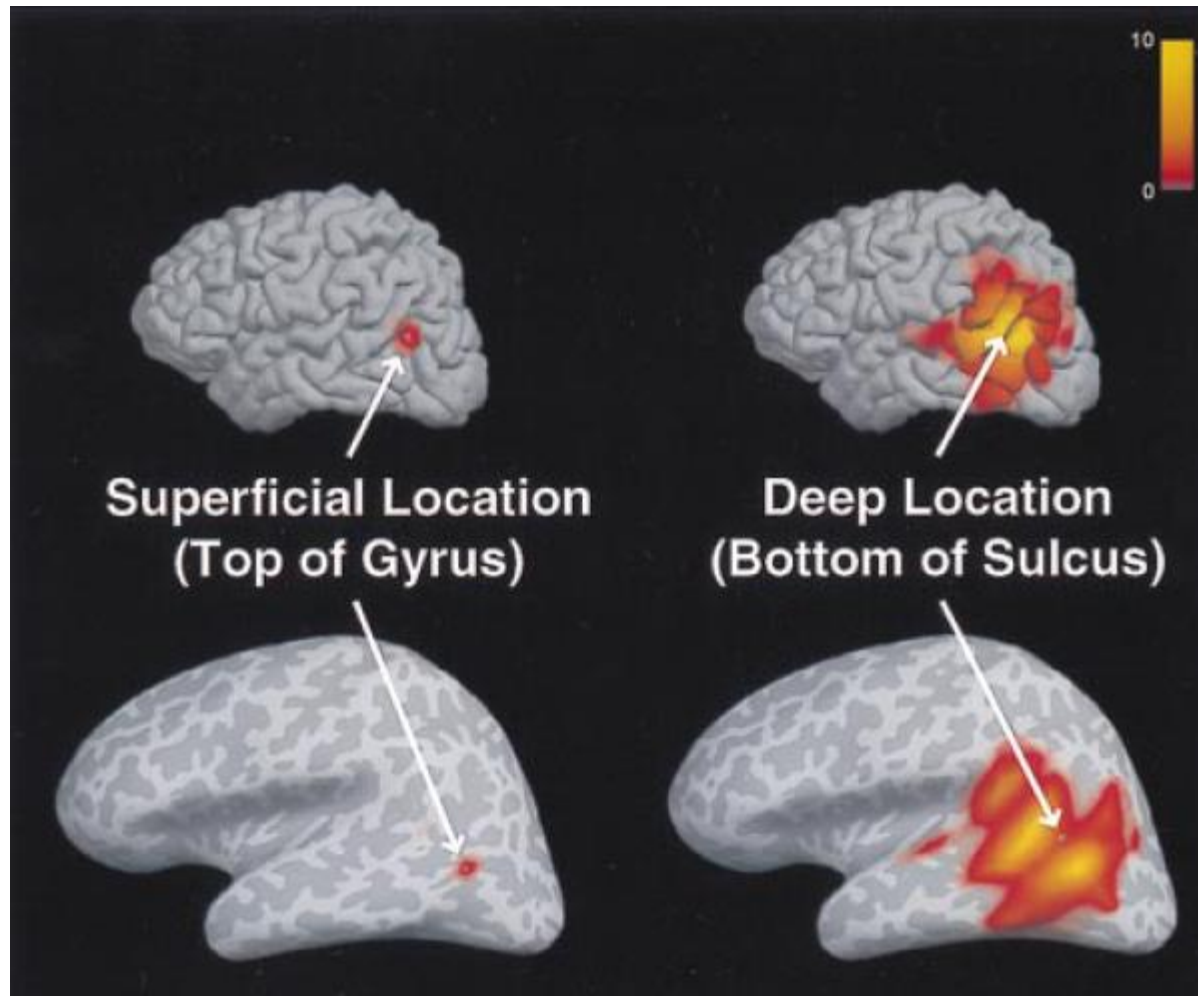


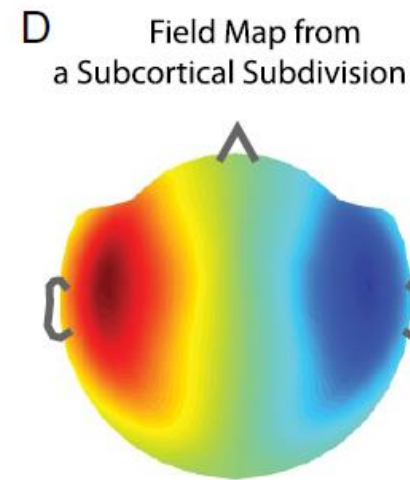
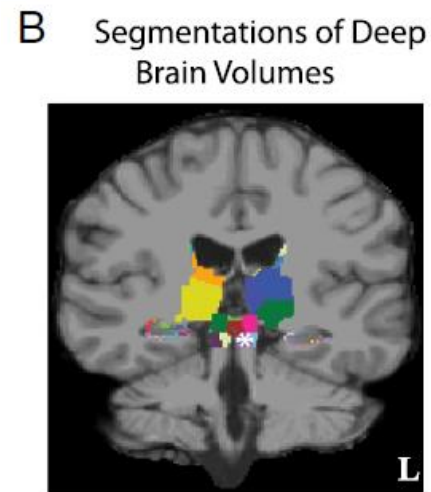
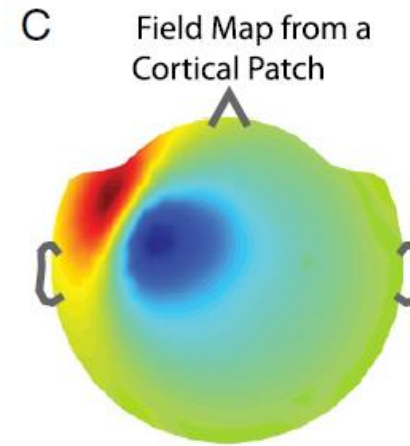
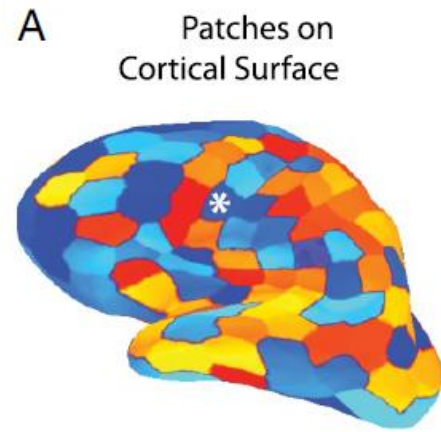
FIG. 4. Crosstalk versus extent and number of sources. Crosstalk is shown for a variety of extents and numbers of sources. The extent of sources was either point, 1 cm or 2 cm in diameter, and the number of sources was 5, 10, or 20 (indicated by different gray scale). A partial fMRI weighting of 90% was used in these simulations. The results indicate that the crosstalk is relatively independent of source extent and number. This demonstrates that the proposed linear estimation method is appropriate for modeling multiple, extended areas of activation, as typically encountered in functional neuroimaging studies.



# (How) Can We Estimate Deep Sources?

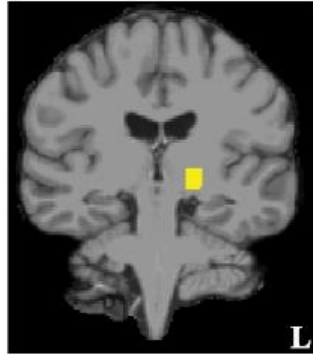


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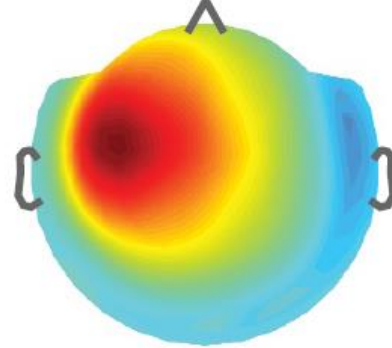


# (How) Can We Estimate Deep Sources?

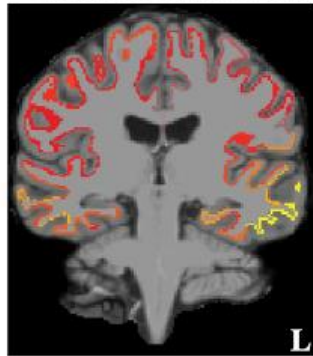
A Subcortical Current



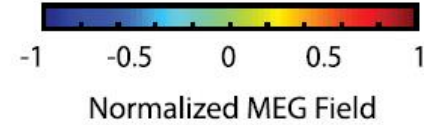
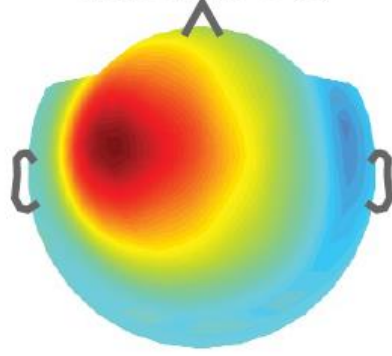
B Subcortical Field Pattern



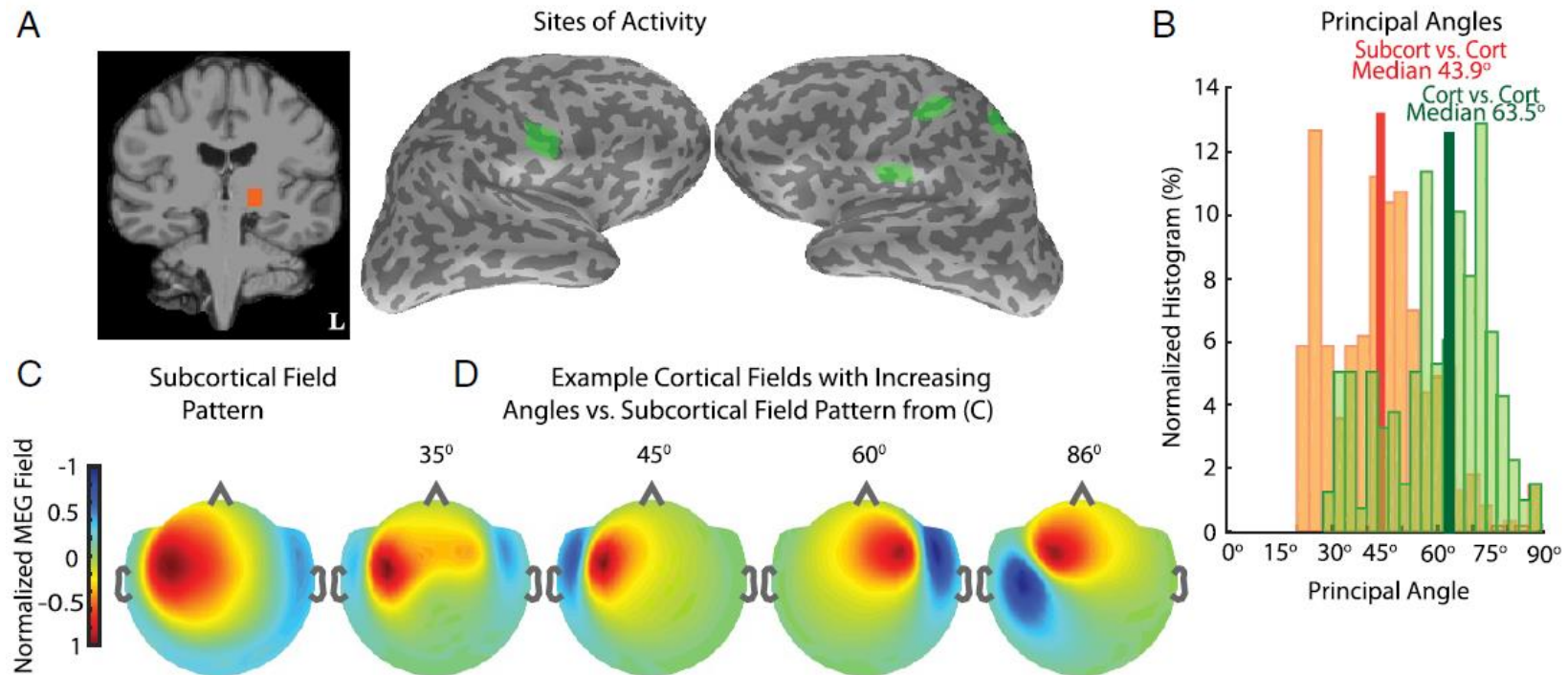
C Best Fitting Cortical Current Distribution



D Cortical Field Pattern most Similar to (B)

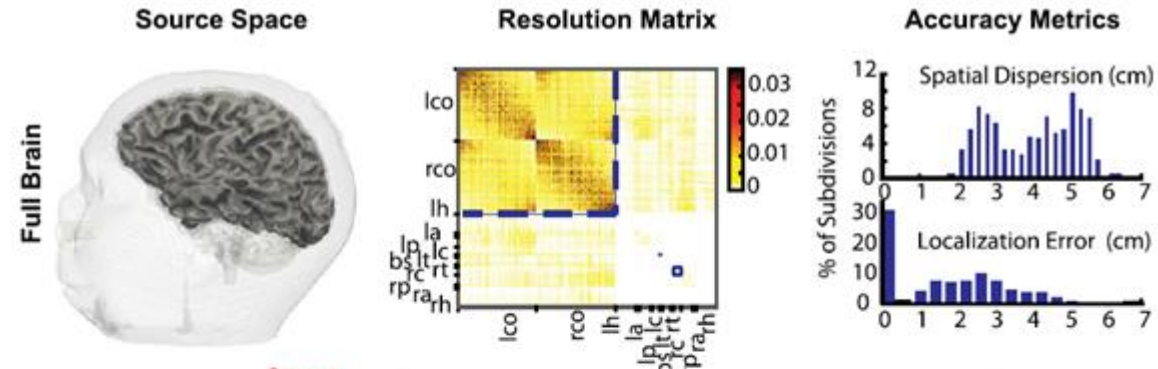


# (How) Can We Estimate Deep Sources?



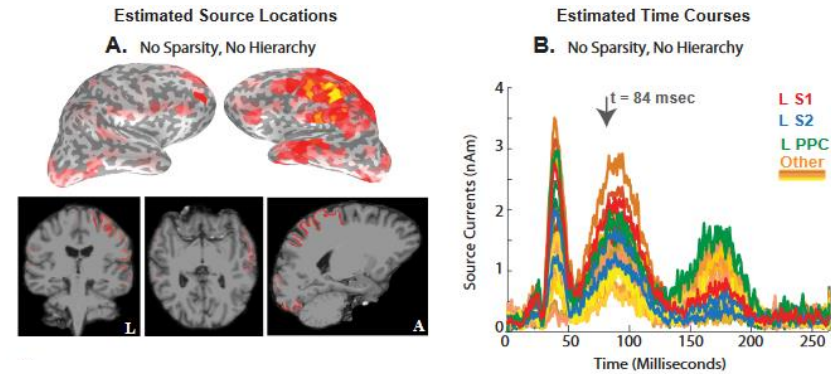
# (How) How Can We Estimate Deep Sources?

## The Importance Of Sparsity



# (How) How Can We Estimate Deep Sources?

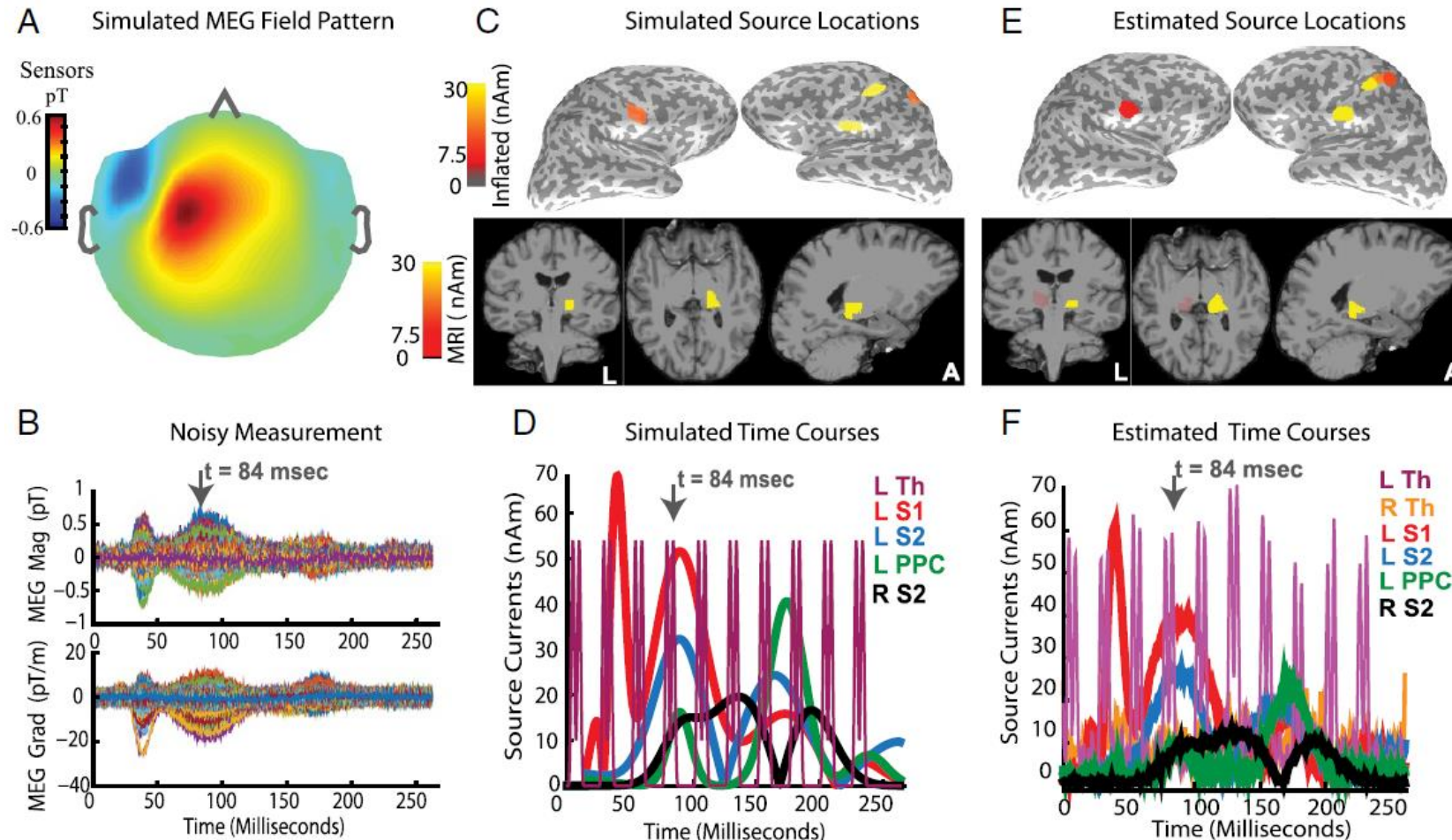
## Sparsity And Hierarchy Are Key





# (How) How Can We Estimate Deep Sources?

## The Importance Of Sparsity



# Conclusions

- Priors lead to a bias of your solution towards what you already know.
- The link between the physiology of EEG/MEG and fMRI is not well understood.  
The usefulness of priors depends on the individual case.
- Priors can be implemented as weightings or source covariance matrices in the (Bayesian) minimum-norm framework.
- Prior information on the location and sparsity of sources is particularly useful (required) for deep sources.



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