



MRC Cognition
and Brain
Sciences Unit



UNIVERSITY OF
CAMBRIDGE

EEG/MEG 2: Head and Forward Modelling

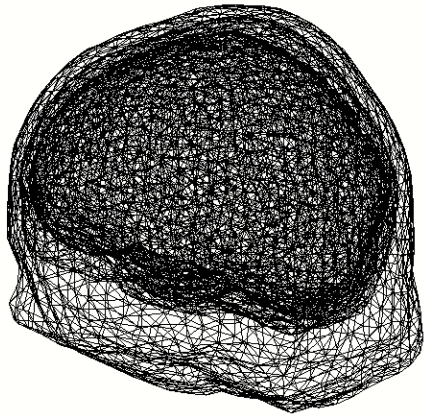
Olaf Hauk

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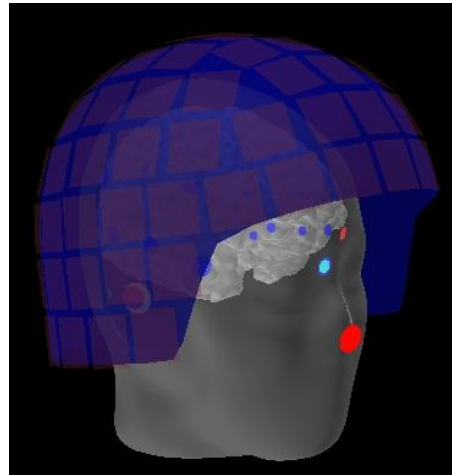
COGNESTIC 2023

Ingredients for Source Estimation

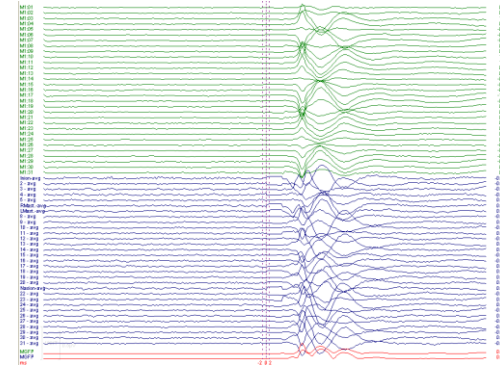
Volume Conductor/
Head Model



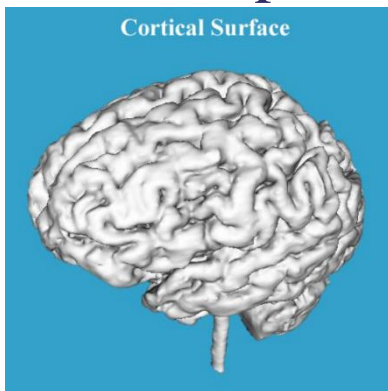
Coordinate
Transformation



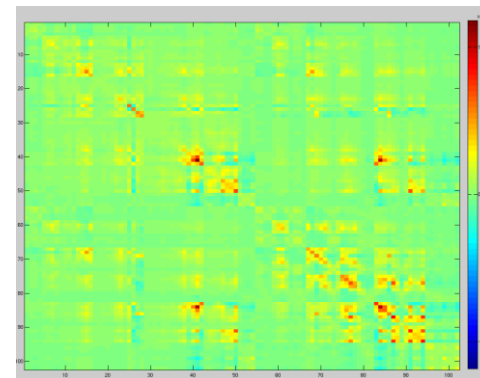
MEG data



Source Space

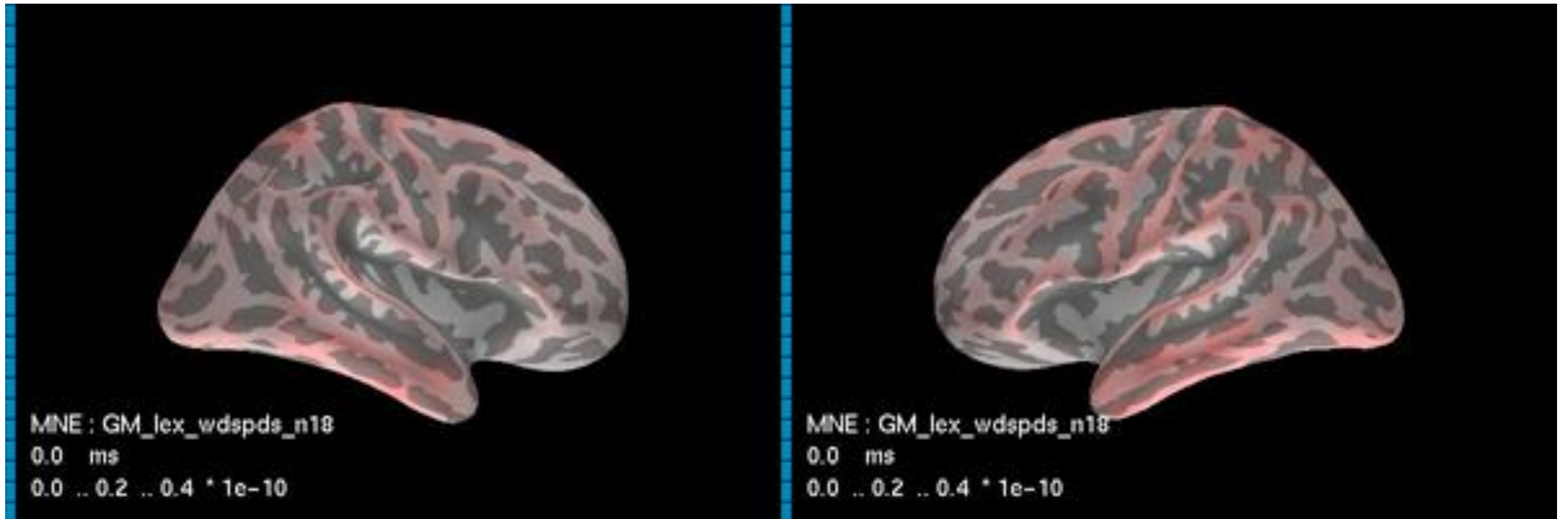


Noise/Covariance Matrix



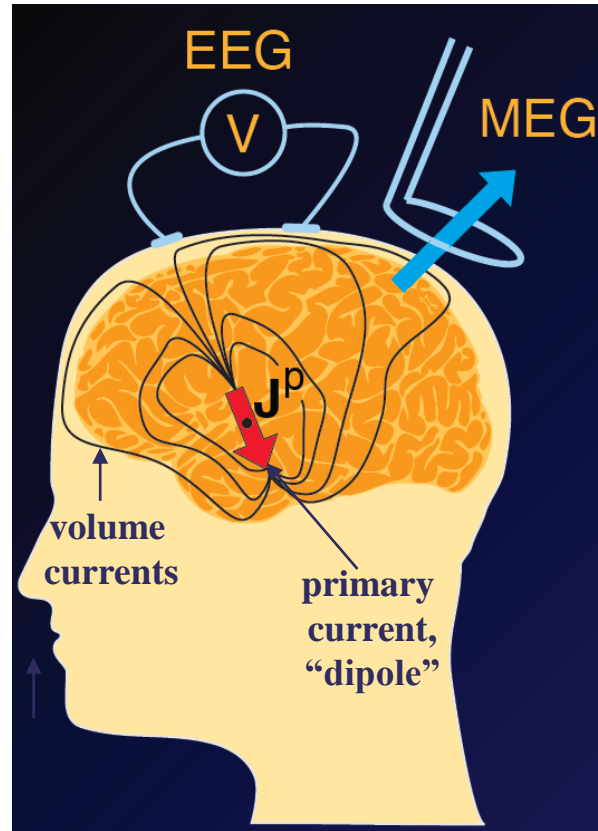
Our Goal: Spatio-Temporal Brain Dynamics

“Brain Movies”

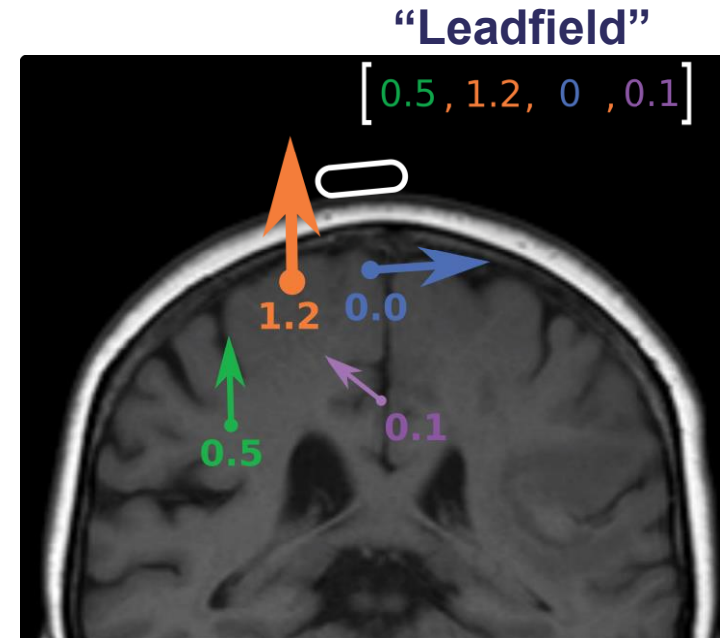


We Have To First State The Forward Problem In Order To Solve The Inverse Problem

EEG/MEG measure the primary sources indirectly

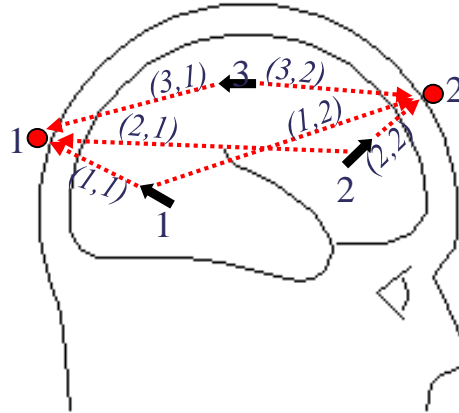


Sensors are differently sensitive to different sources



Hauk, Stenroos, Tieder. In: Supek S, Aine C (eds), "Magnetoencephalography: From Signals to Dynamic Cortical Networks, 2nd Ed."

The EEG/MEG Forward Problem



data	“leadfield”	dipoles	?	dipoles	inverse	data
$\begin{matrix} \bullet \\ \bullet \end{matrix} \begin{pmatrix} d_1 \\ d_2 \end{pmatrix}$	$= \begin{pmatrix} 0.5 & 0 & 0.3 \\ 0 & 1 & -0.3 \end{pmatrix}$	$\begin{pmatrix} j_1 \\ j_2 \\ j_3 \end{pmatrix}$	$\xrightarrow{\text{inversion}}$	$\begin{pmatrix} j_1 \\ j_2 \\ j_3 \end{pmatrix}$	$= \begin{pmatrix} 1.5034 & 0.1241 \\ 0.2483 & 0.9379 \\ 0.8276 & -0.2069 \end{pmatrix}$	$* \begin{pmatrix} d_1 \\ d_2 \end{pmatrix}$

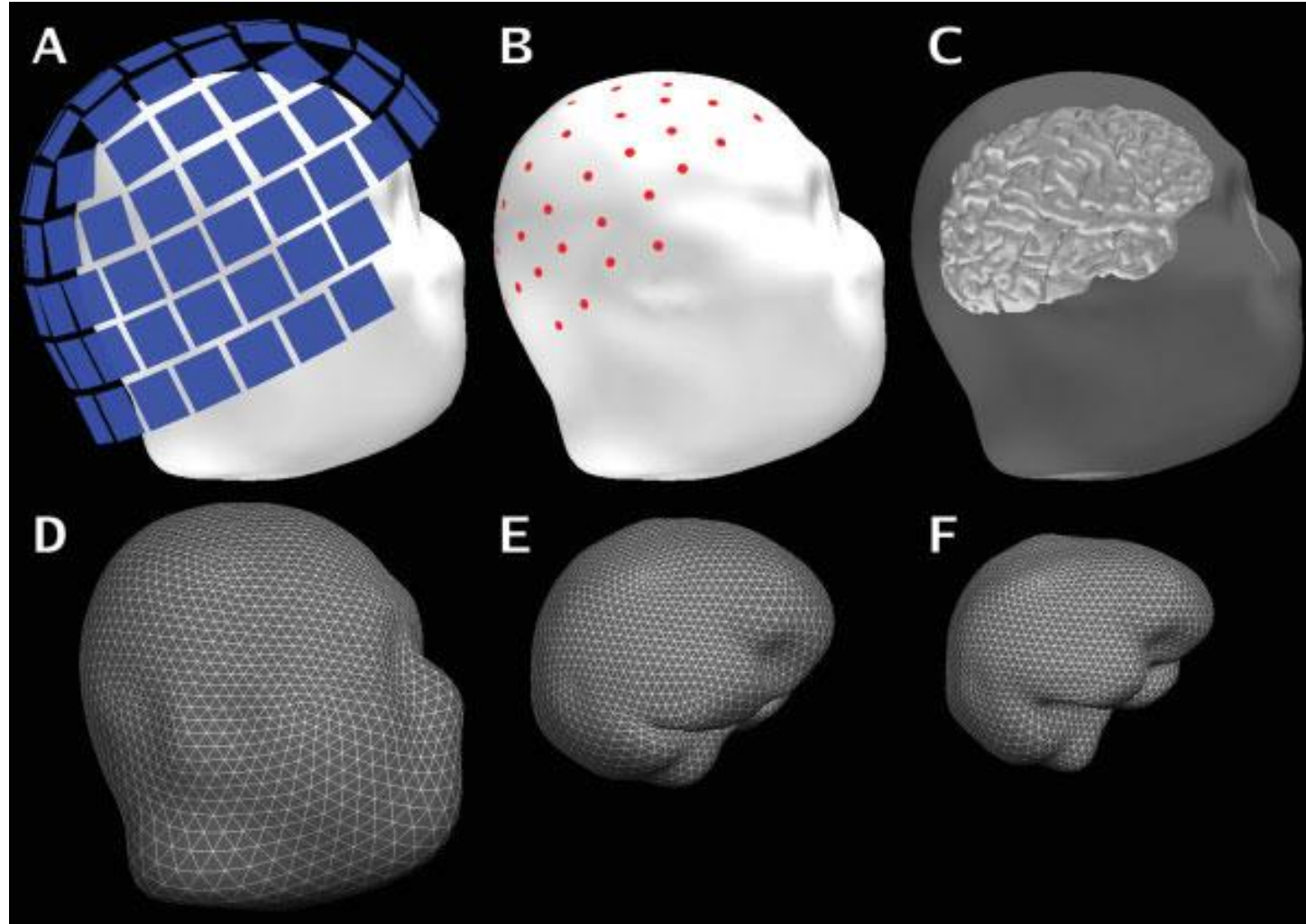
$$j_1 + j_2 = 1$$

under-determined problem, no unique solution

$$\mathbf{d} = \mathbf{L}\mathbf{j}$$

d: data (n_sensors x 1) **L**: “leadfield” (n_sensors x n_dipoles), **j**: dipoles (n_dipoles x 1)
 Usually n_dipoles >> n_sensors.

Ingredients for a head model

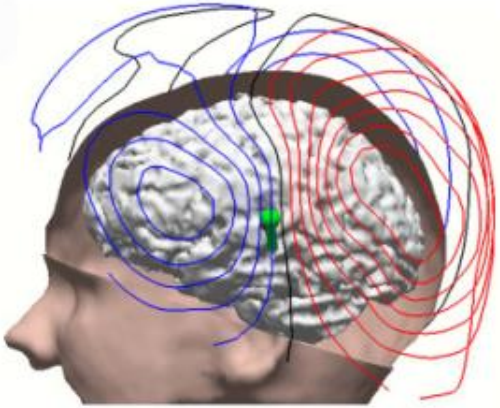


Goldenholz et al., HBM 2009
<https://pubmed.ncbi.nlm.nih.gov/18465745/>

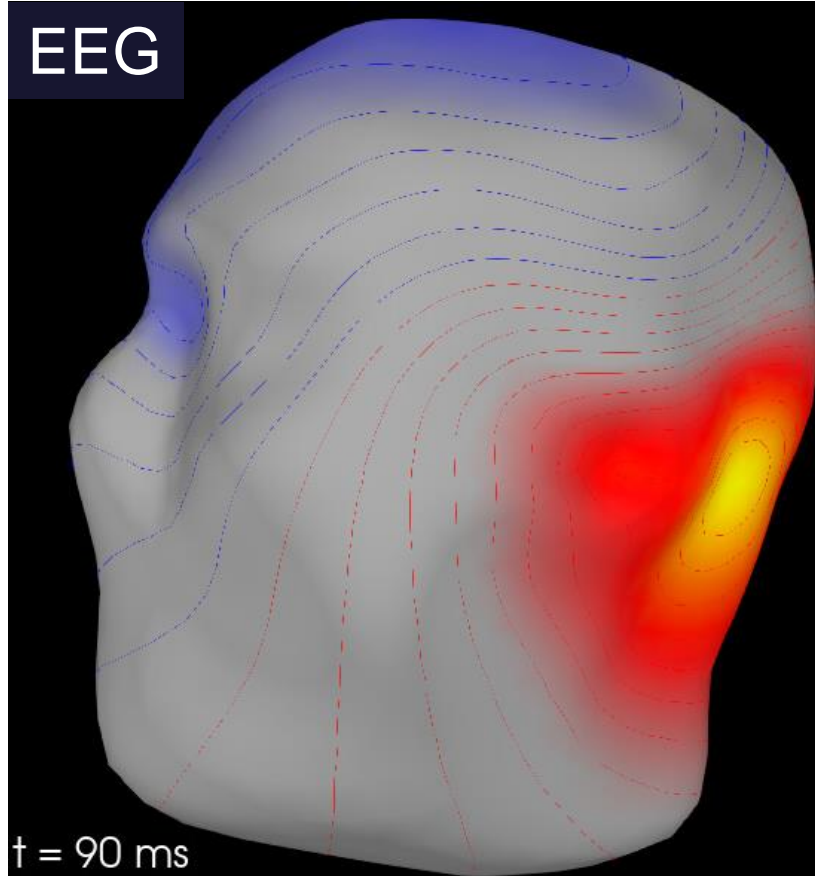
If you don't have individual MRIs: Standard head models and spherical approximations are available.

Example: Auditorily Evoked Activity

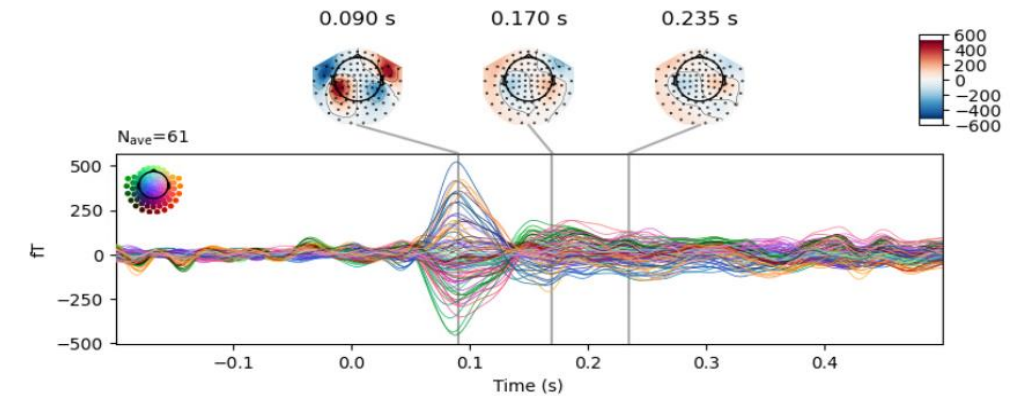
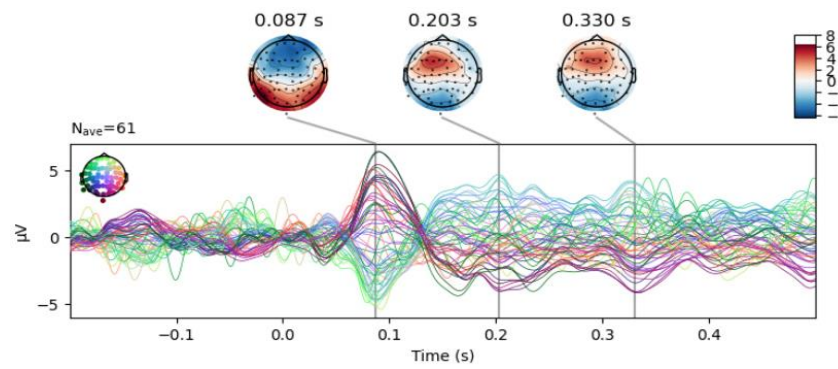
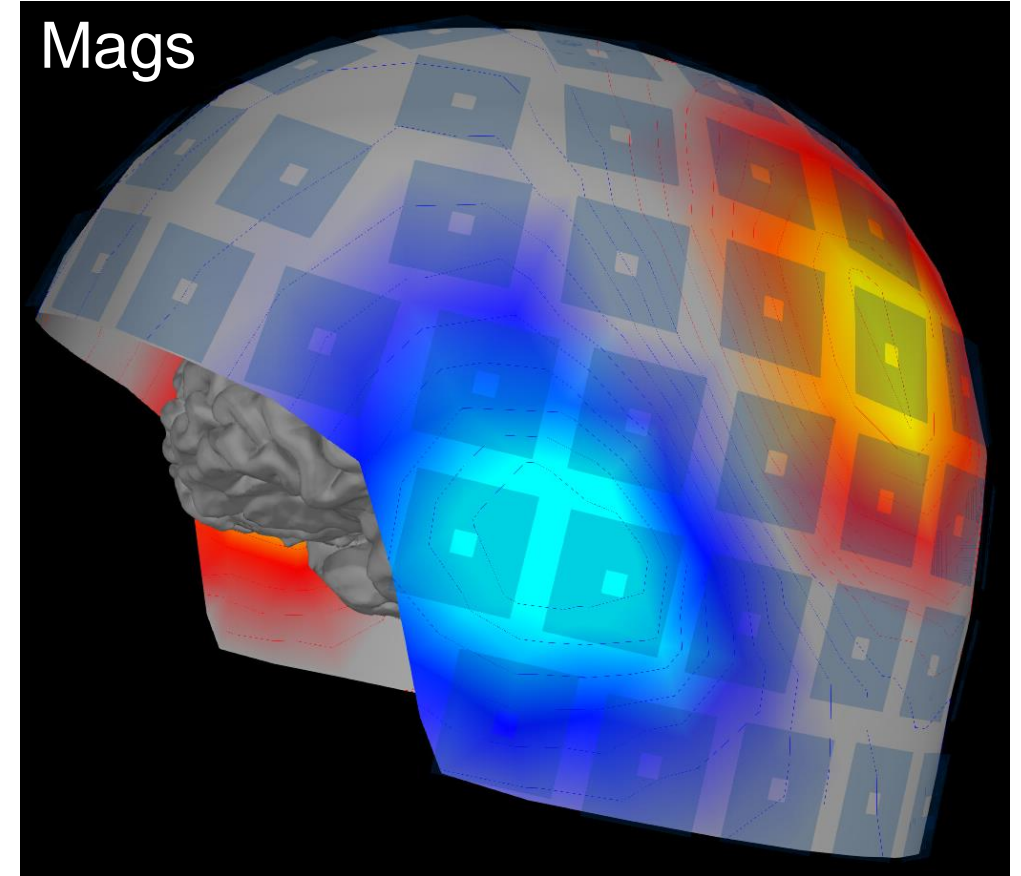
Tone to right ear



EEG

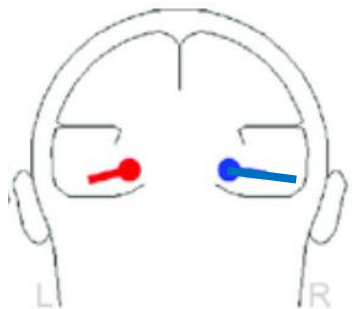


Mags

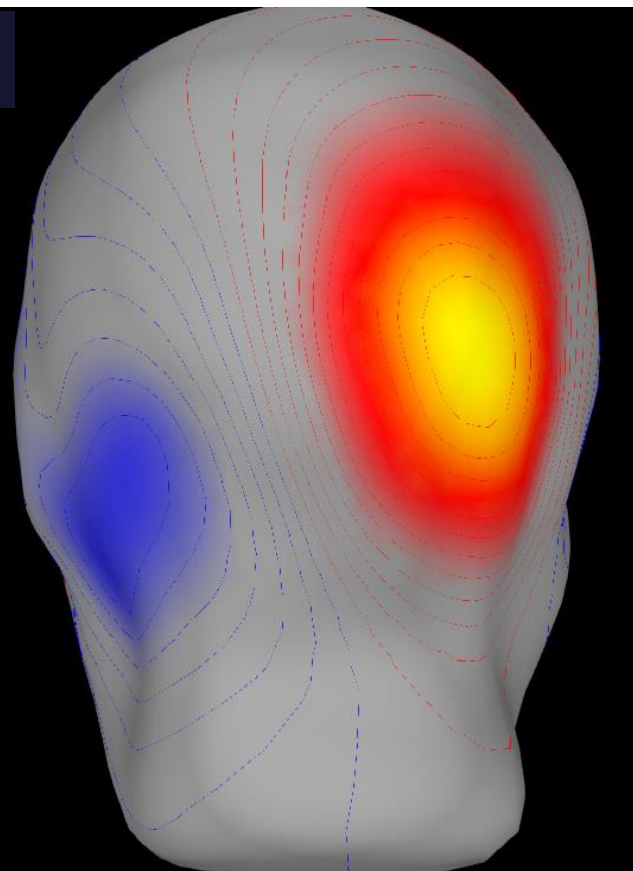


Example: Visually Evoked Activity ~100 ms

Checkerboard to
left visual field

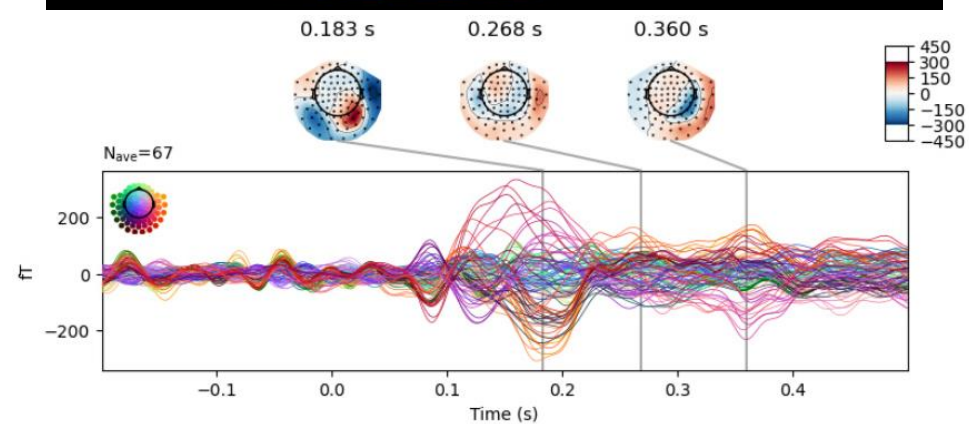
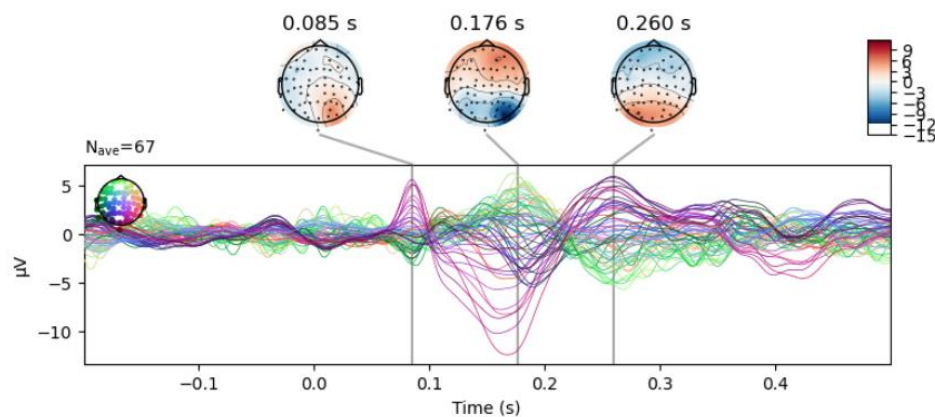
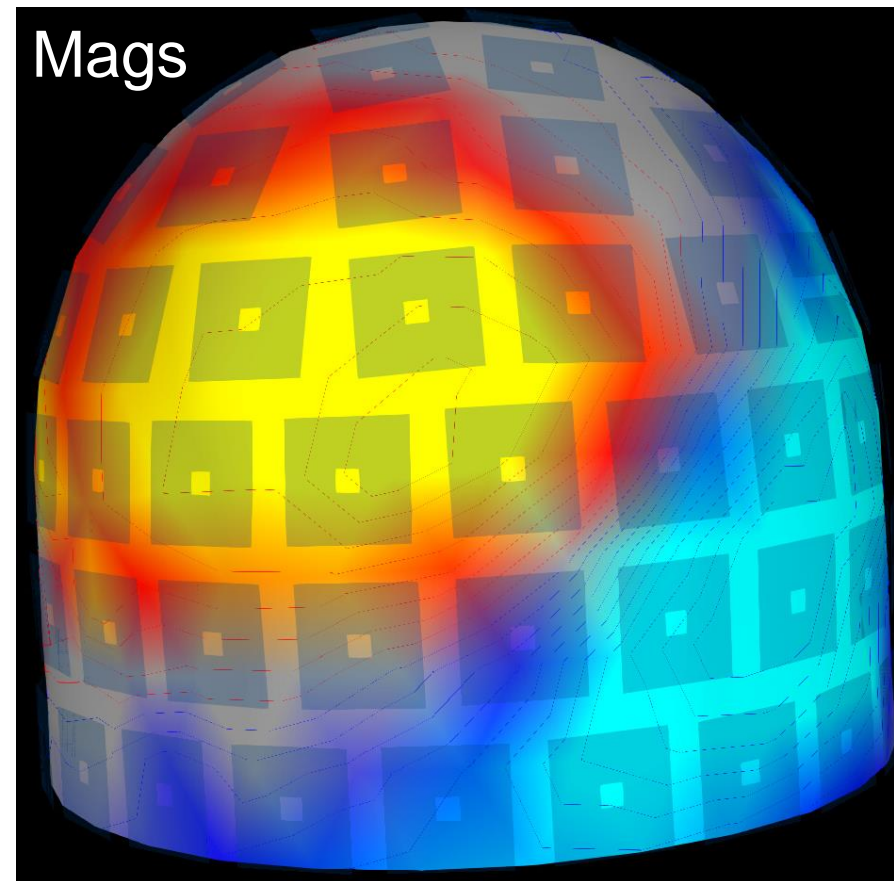


EEG



$t = 90 \text{ ms}$

Mags

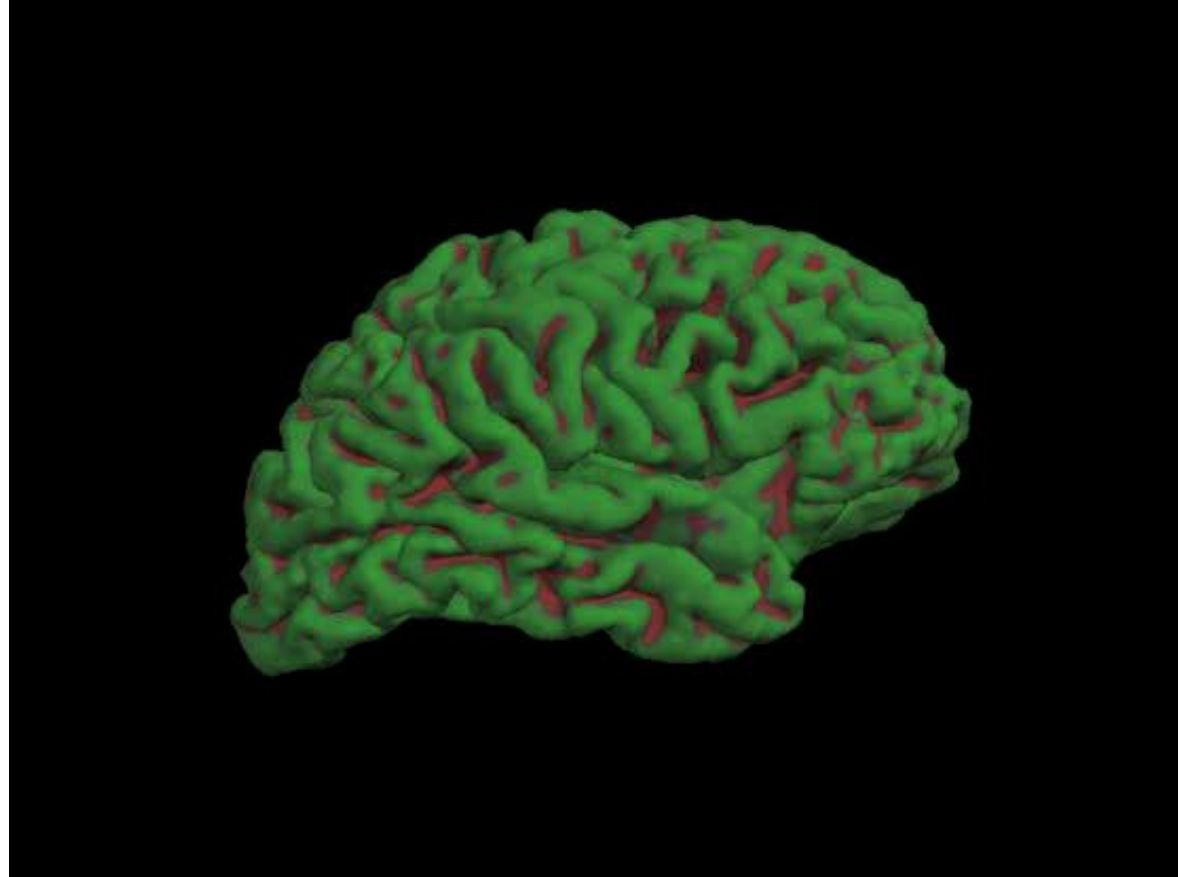


The Forward Problem and Head Modelling

Source Spaces

Source Space

Where active sources may be located, e.g. grey matter, 3D volume



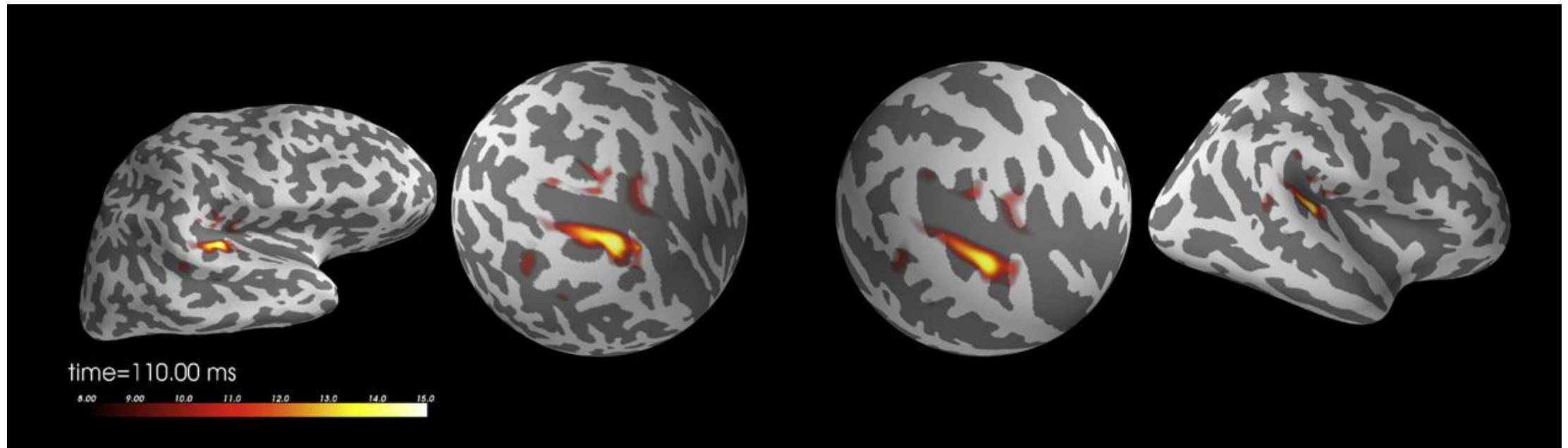
<http://www.cogsci.ucsd.edu/~sereno/movies.html>

Sometimes “standard head models” are used, when no individual MRIs available.

SPM uses the same “canonical mesh” as source space for every subjects, but adjusts it individually.

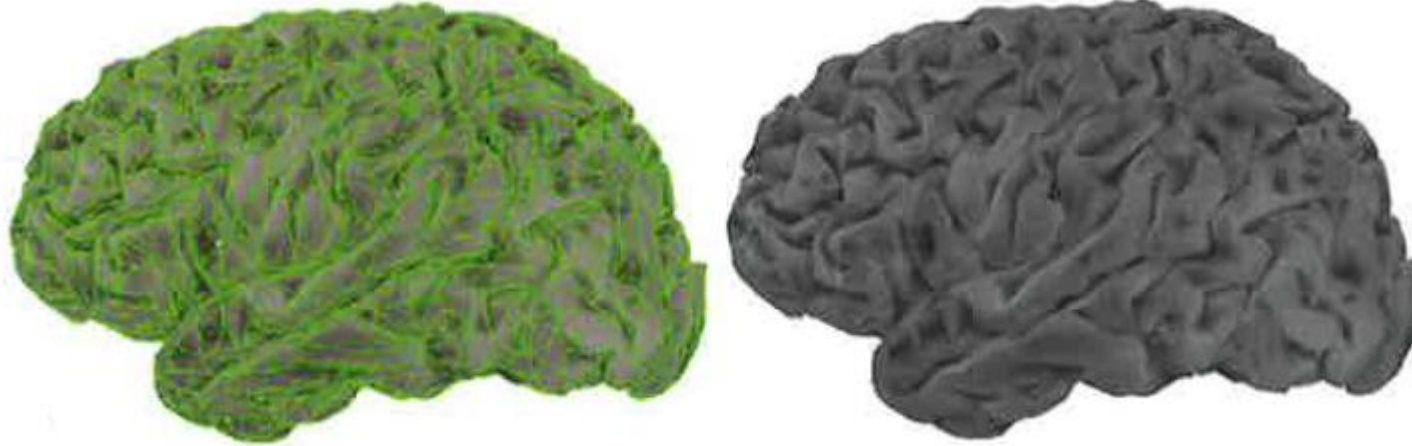
Normalising (Morphing) Cortical Surfaces

Morphing from individual to standard brain

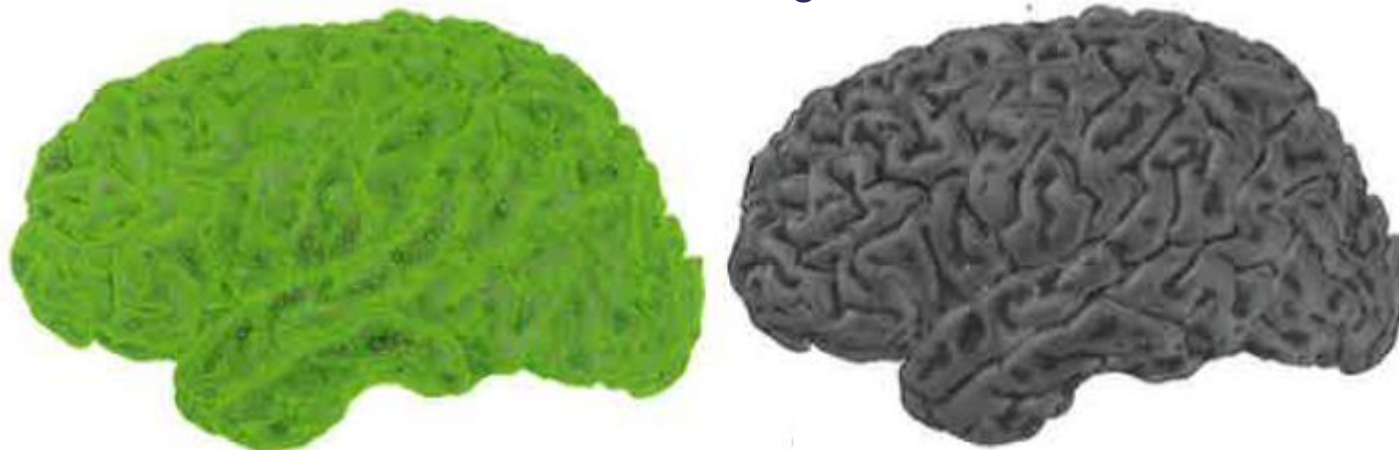


Spatial Sampling of Cortical Surfaces

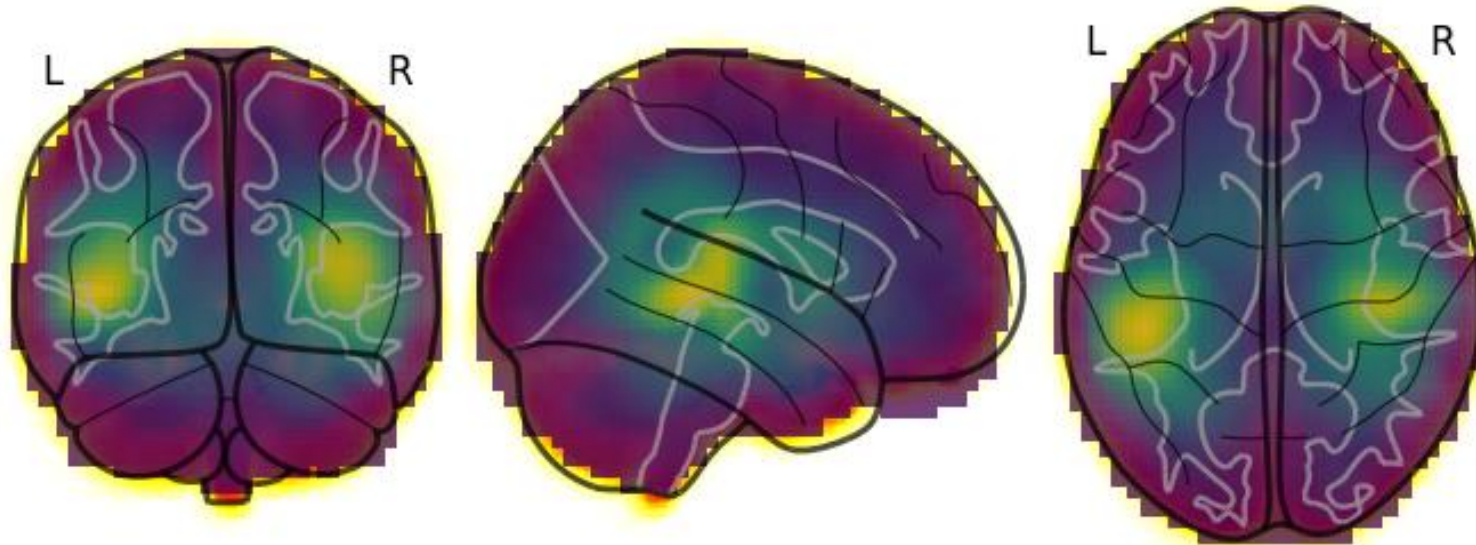
10.034 vertices, 20.026 triangles of 10 mm² surface area
Sufficient for most EEG/MEG applications



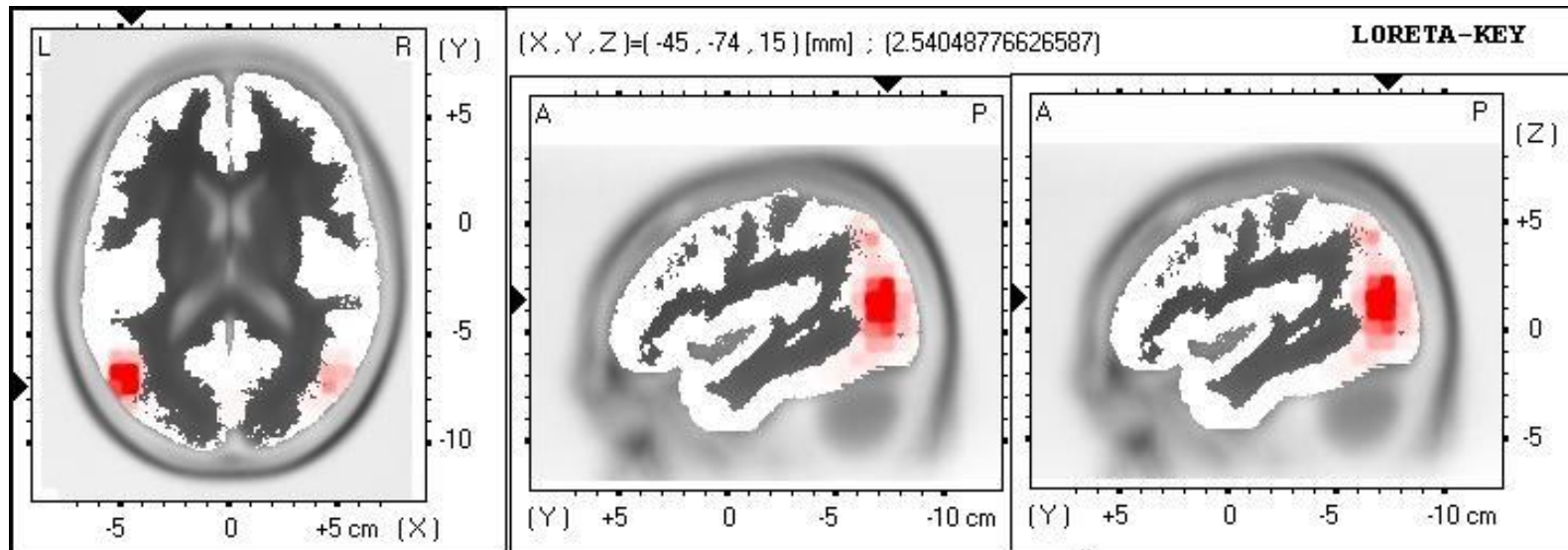
79.124 vertices, 158.456 triangles of 1.3 mm² surface area



Volumetric Source Spaces Are Possible

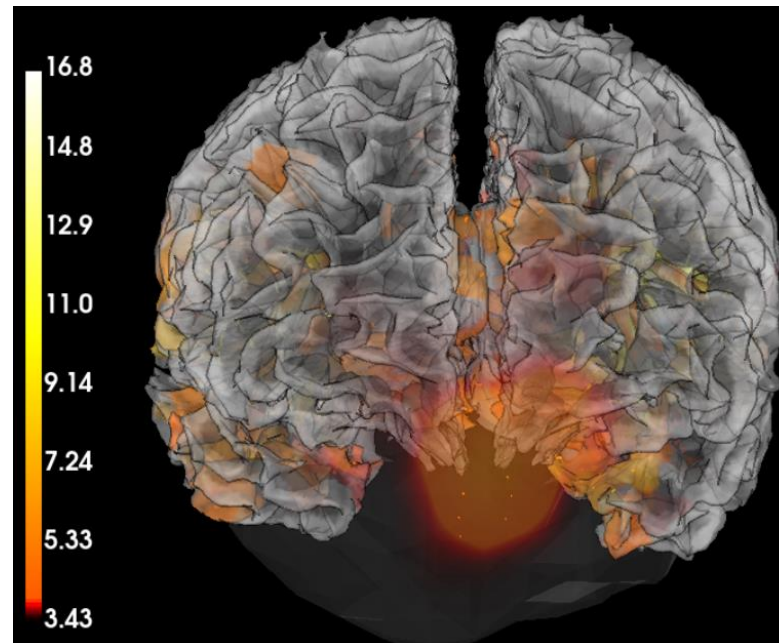
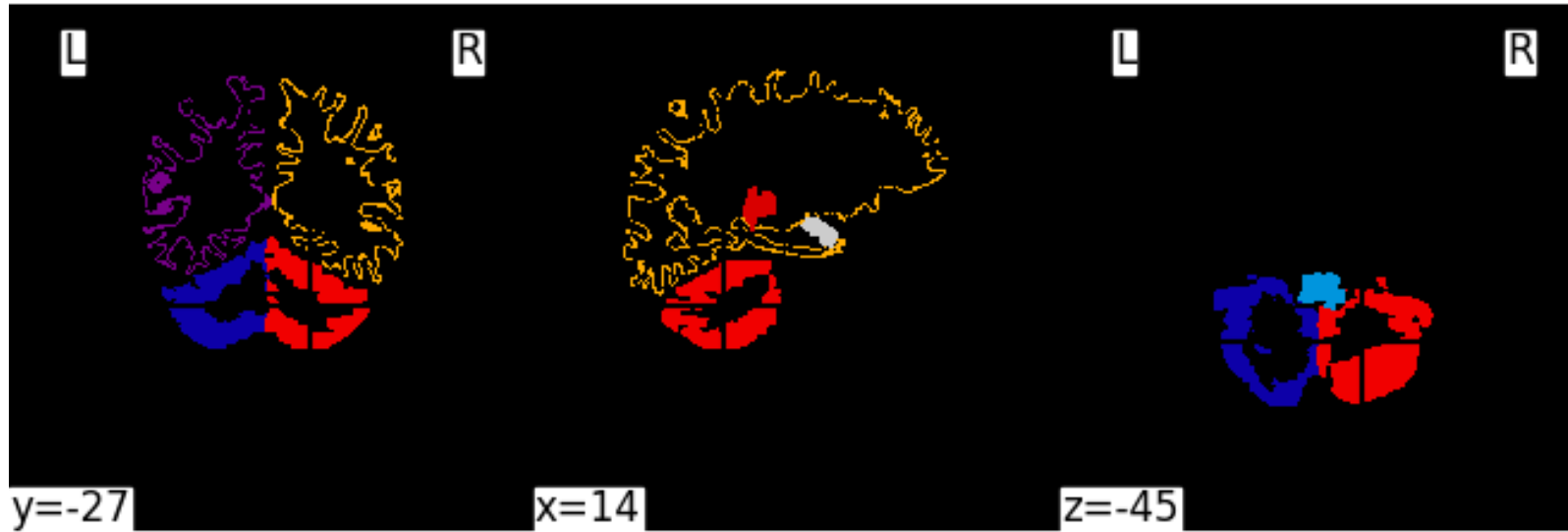


https://mne.tools/dev/auto_examples/inverse/morph_volume_stc.html



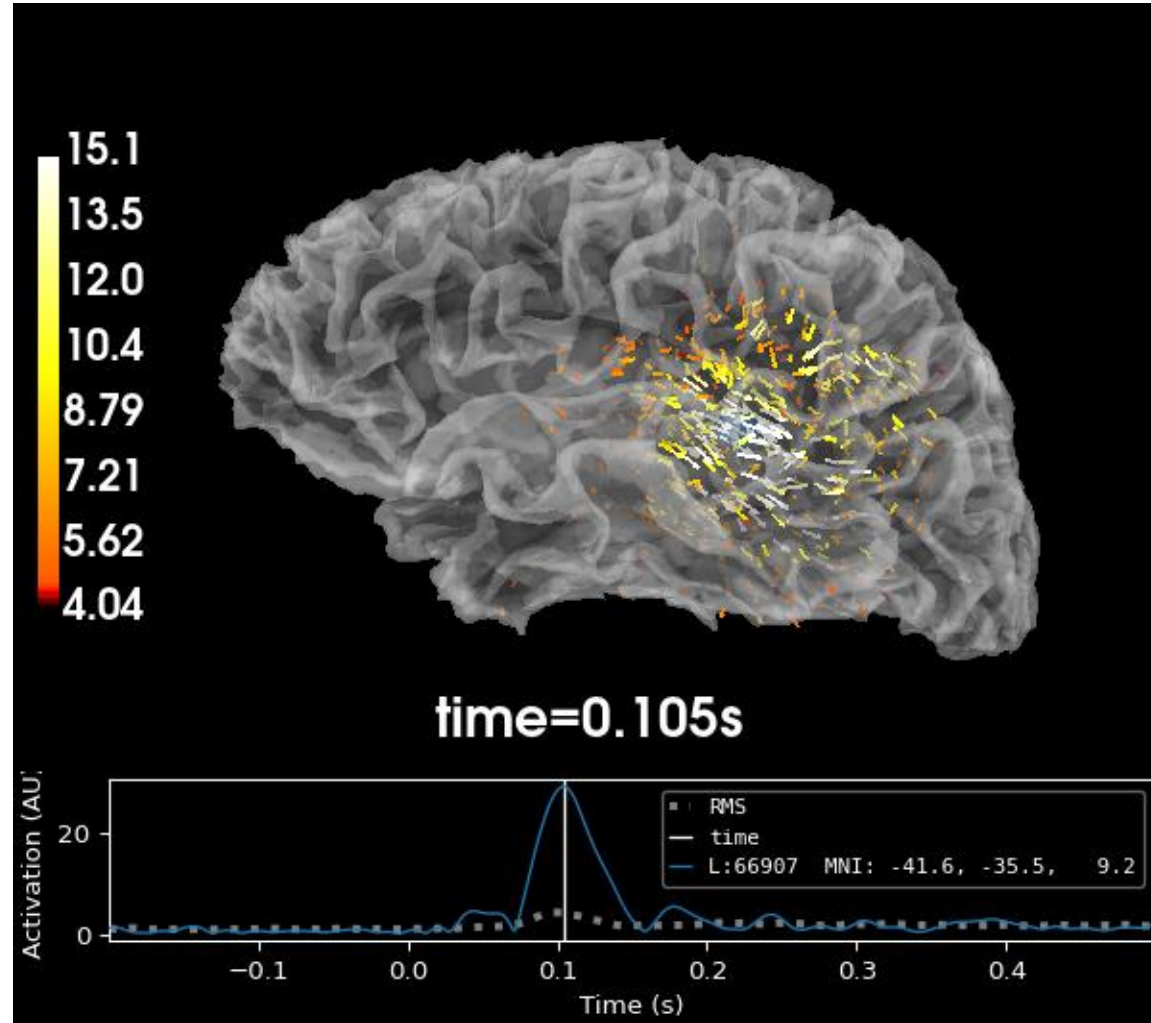
Mixed Source Spaces

Cortical and Sub-Cortical Sources

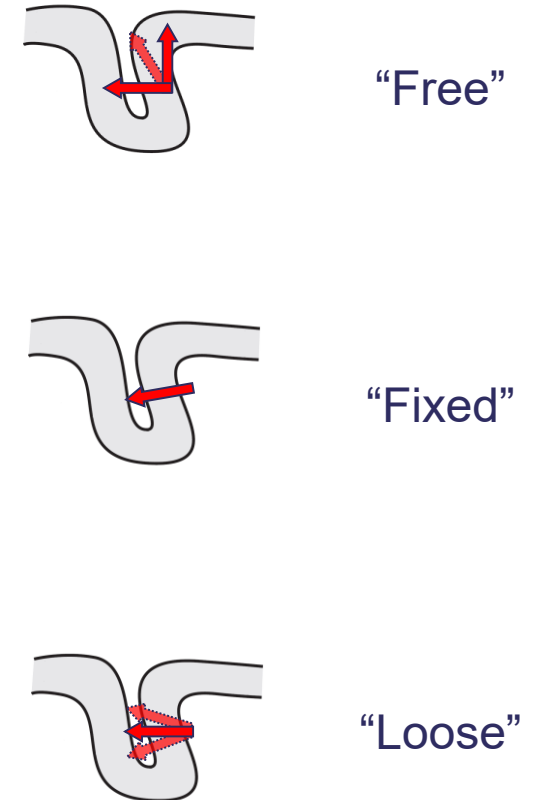


Source Orientations

Current sources have a direction and/or orientation.

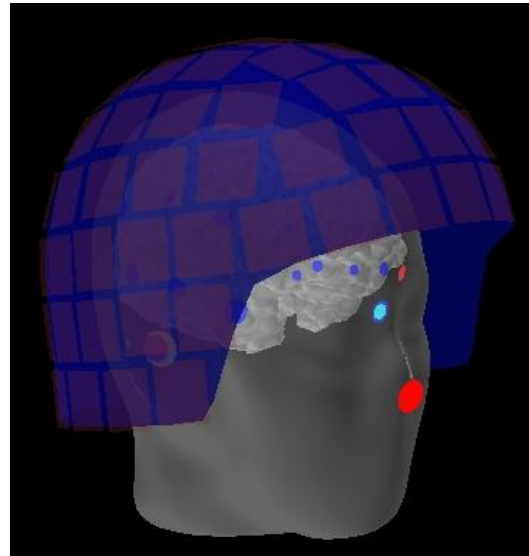


Constraints on source orientation:

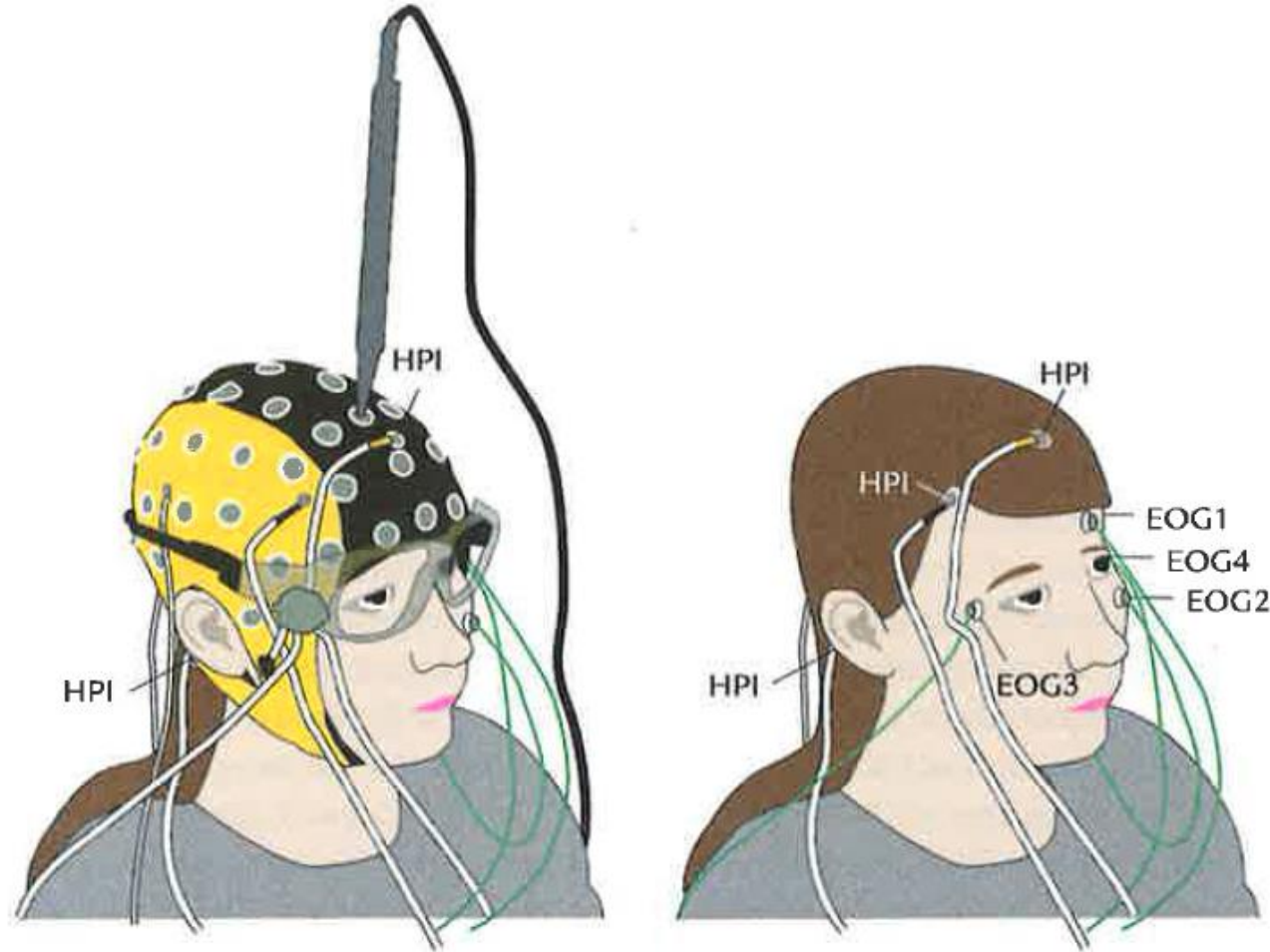


Coregistration of EEG/MEG and MRI Spaces

Coordinate
Transformation



Coregistration of EEG/MEG and MRI Spaces

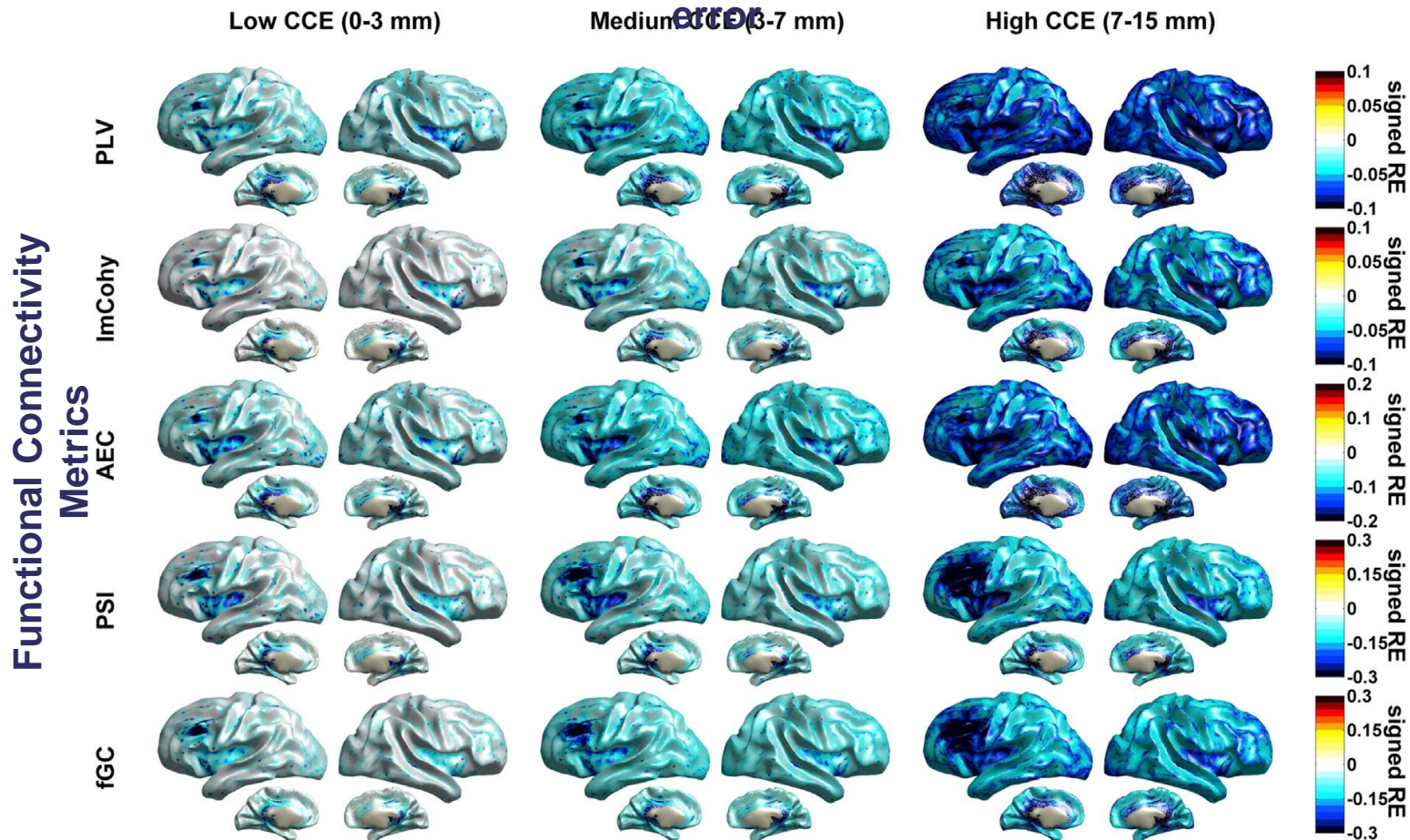


MNE-Python tutorial: <https://www.youtube.com/watch?v=ALV5qqMHLIQ>

Accurate Coregistration Is Important

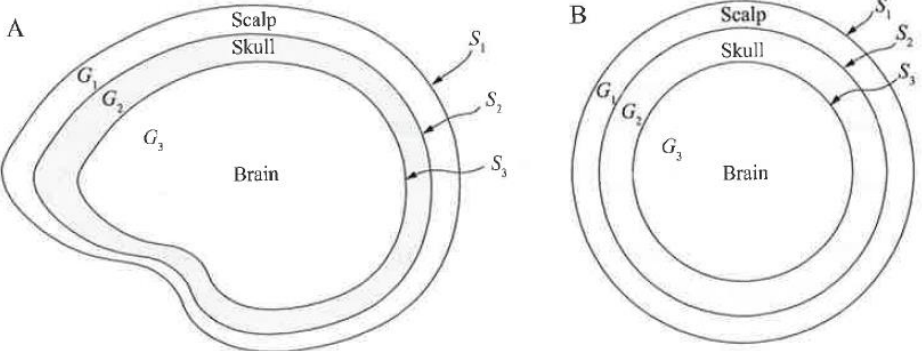
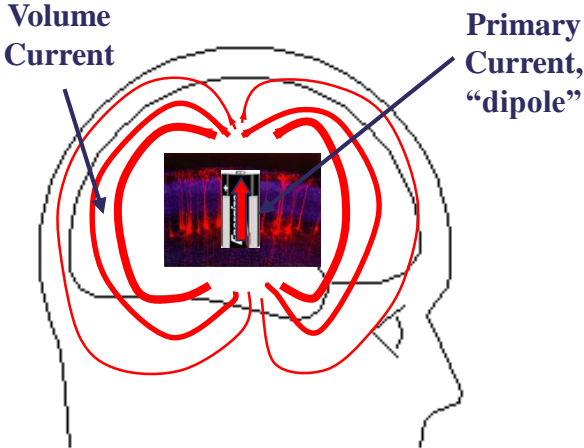
Coregistration errors affect the forward model, and therefore everything that follows.

For example, connectivity analysis:
3 levels of coregistration



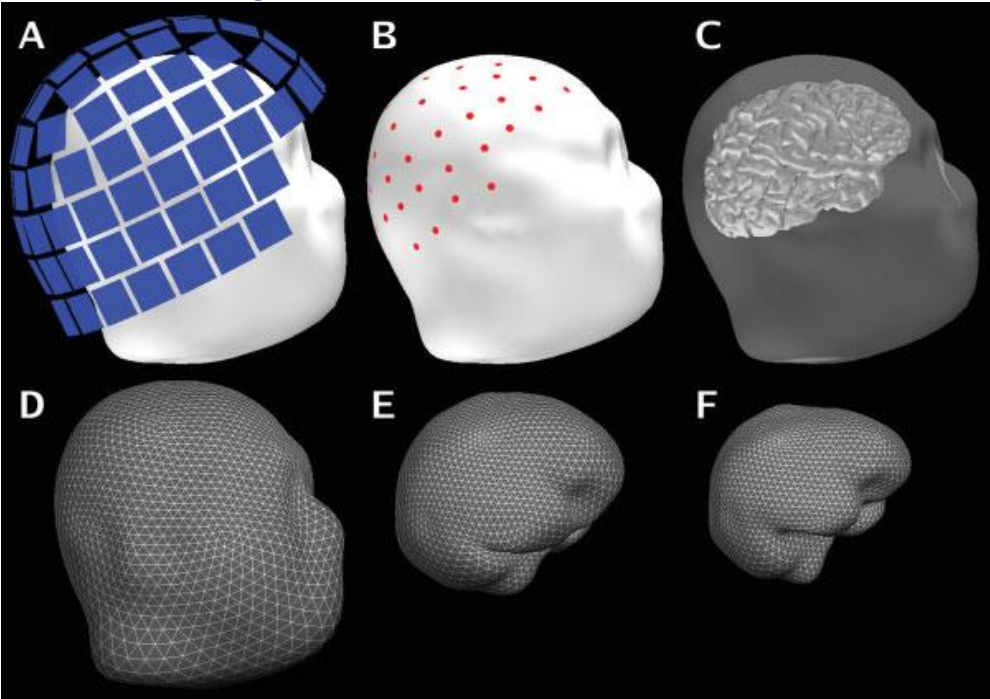
Head Models

Boundary Element Model (BEM)



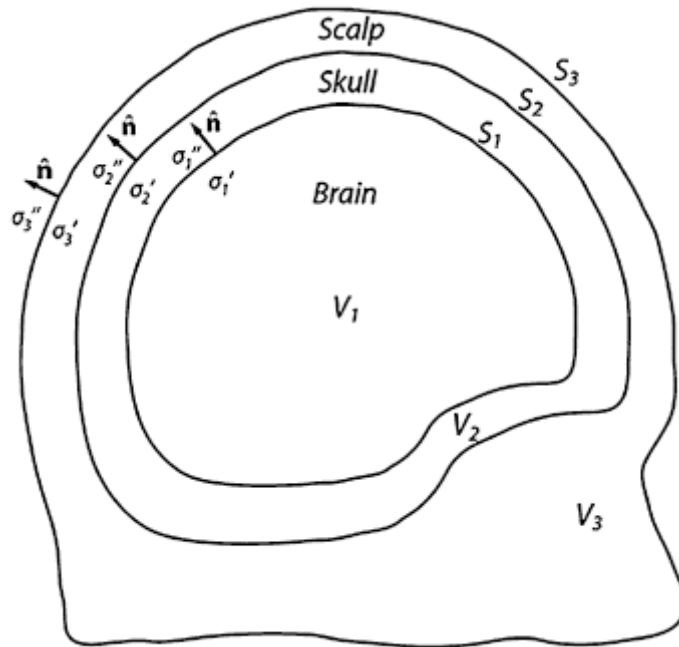
Ilmoniemi and Sarvas, "Brain Signals", MIT 2019

Ingredients for a head model



Goldenholz et al., HBM 2009

Boundary Element Model (BEM)



Heller & Volegov, in Magnetoencephalography by Supek & Aine (eds), Springer 2019

Electric potential

$$\sigma(\mathbf{r}) V(\mathbf{r}) = \frac{1}{4\pi} \sum_j (\sigma_j' - \sigma_j'') \int_{S_j} dS_j' \mathbf{n}(\mathbf{r}') \cdot \frac{\mathbf{r}' - \mathbf{r}}{|\mathbf{r}' - \mathbf{r}|^3} V(\mathbf{r}') + \frac{1}{4\pi} \int_V d^3r' \mathbf{J}^p(\mathbf{r}') \cdot \frac{\mathbf{r} - \mathbf{r}'}{|\mathbf{r} - \mathbf{r}'|^3},$$

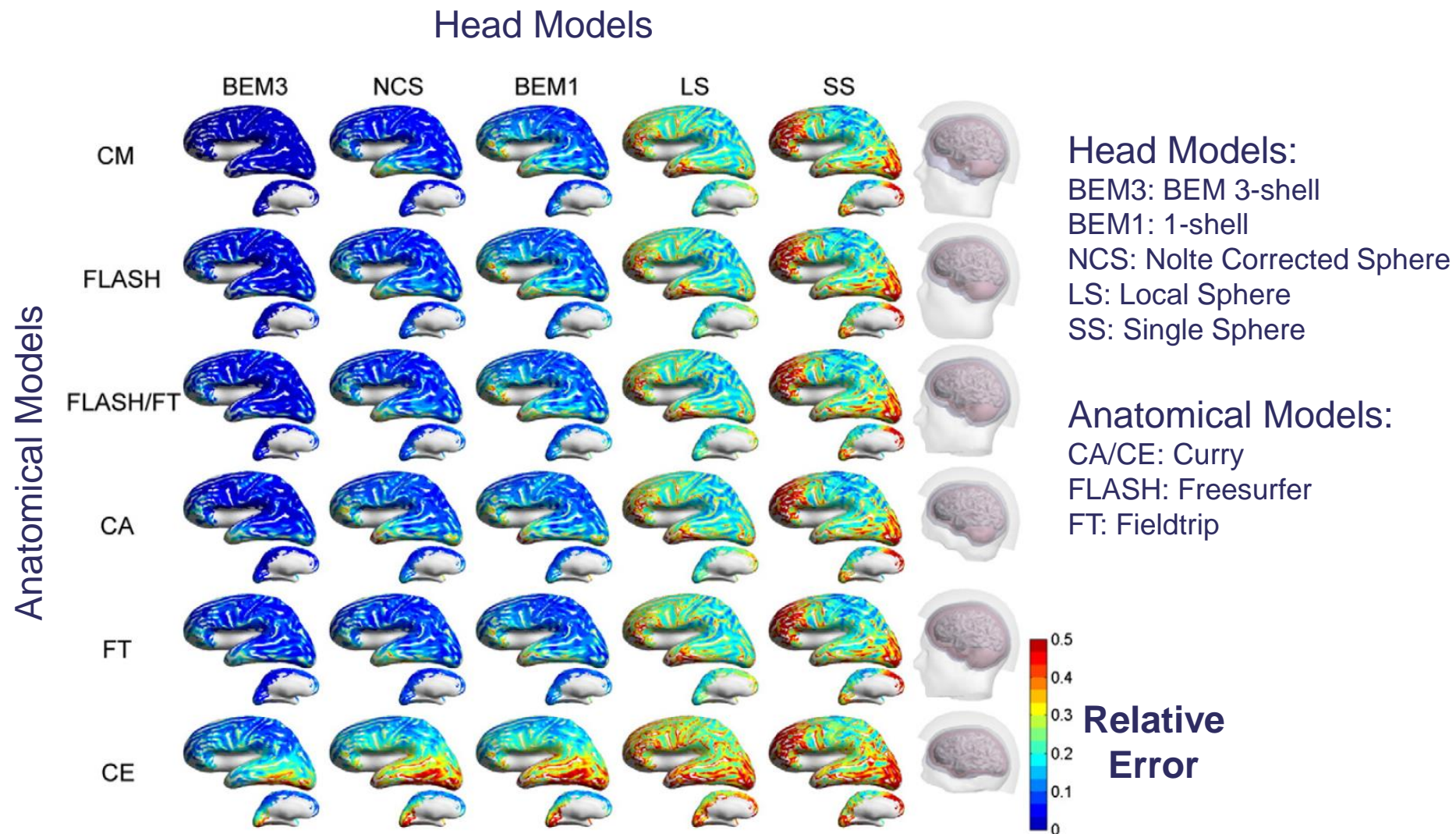
Magnetic Field

$$\mathbf{B}^p(\mathbf{r}) = \frac{\mu_0}{4\pi} \int_V \mathbf{J}^p(\mathbf{r}') \times \nabla' \frac{1}{|\mathbf{r} - \mathbf{r}'|} d^3r',$$

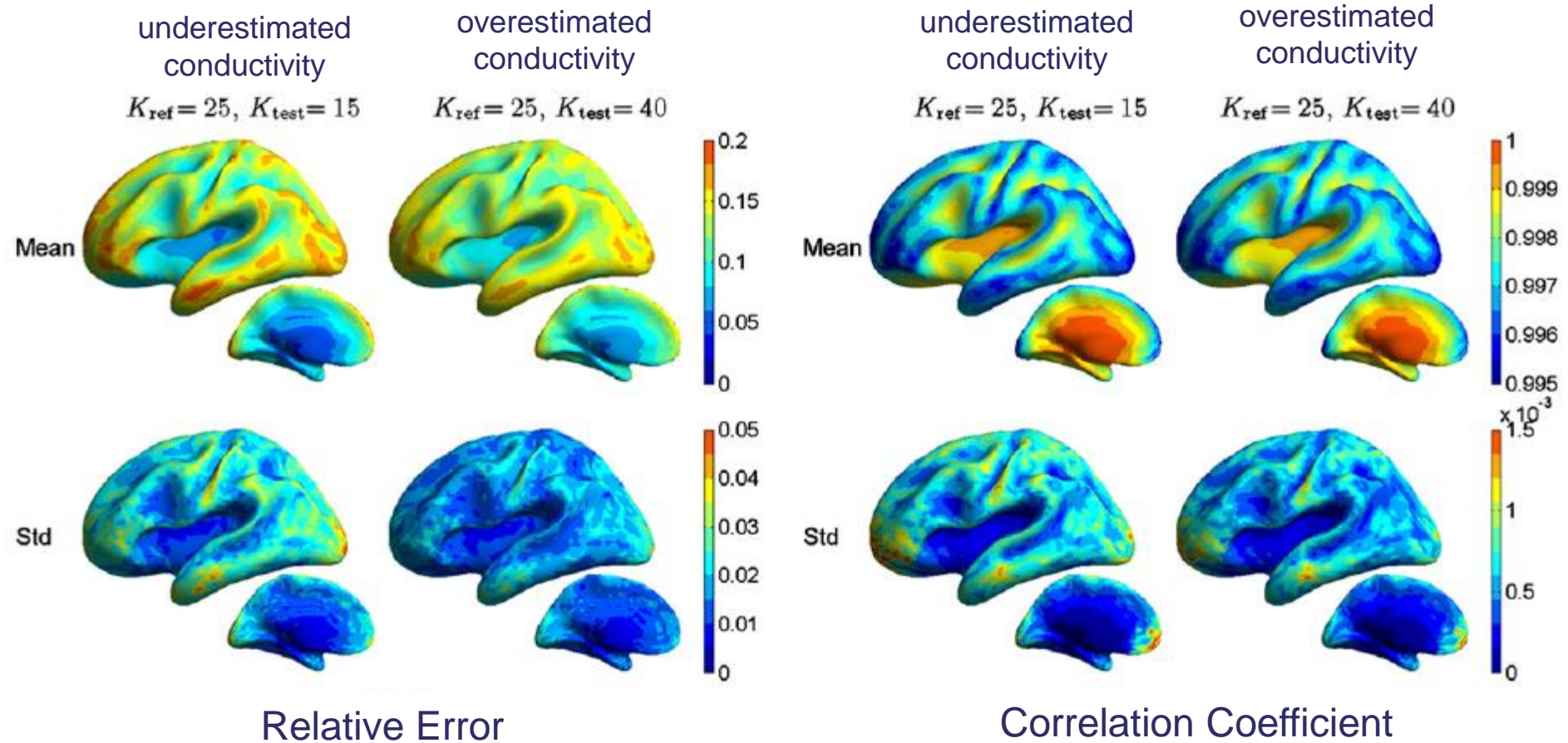
$$\mathbf{B}^R(\mathbf{r}) = -\frac{\mu_0}{4\pi} \sum_i \sigma_i \int_{V_i} \nabla' V(\mathbf{r}') \times \nabla' \frac{1}{|\mathbf{r} - \mathbf{r}'|} d^3r',$$

- Volume currents depend on conductivity distribution within the whole head volume.
- EEG measurements on the scalp are the result of volume currents, and are strongly affected by head geometry.
- MEG measurements are the sum of magnetic fields from primary and volume currents, but the magnetic fields of currents close to the source are much stronger than at larger distances.
- Thus, MEG signals are less affected by head geometry (e.g. skull and scalp). We usually only use one compartment (inner skull) for MEG (unless in combination with EEG).

The Effect of Head Model Accuracy for MEG



Boundary Element Models Are Relatively Robust Against Conductivity Errors

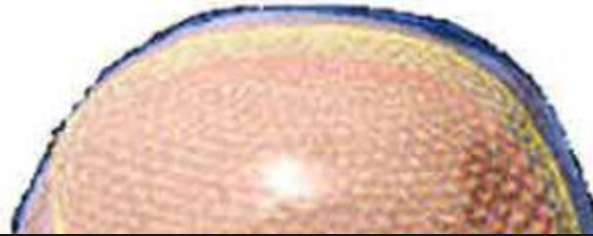


Head Models With Different Levels of Detail

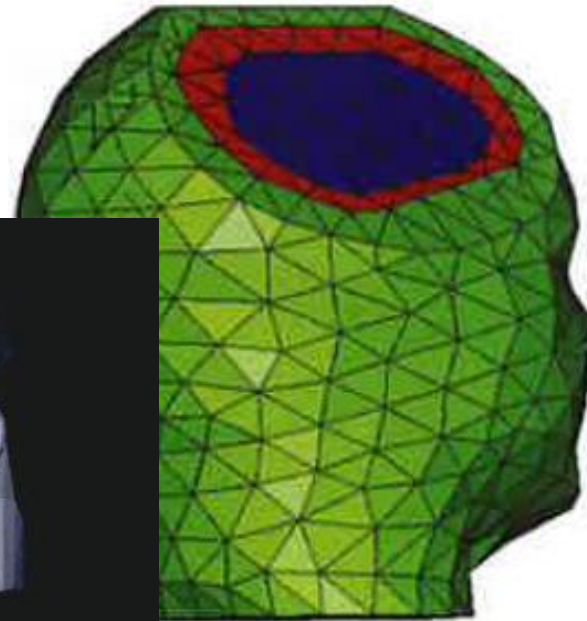
Spheres



Boundary Element Model
(BEM)



Finite Element Model
(FEM)



Kraftwerk, 1986

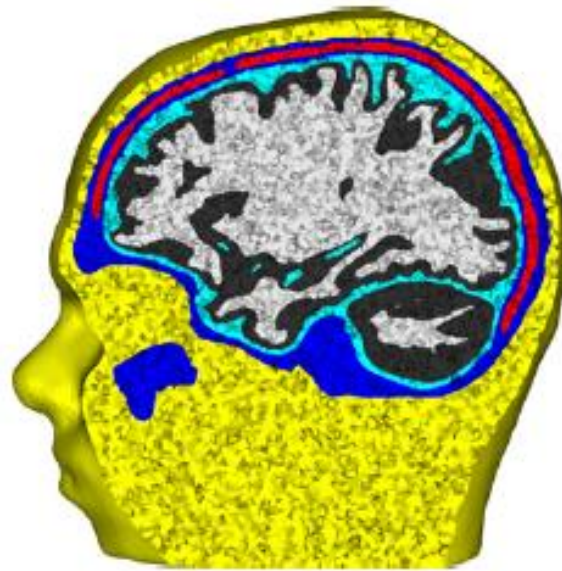
Finite Element Models (FEMs)

The use of 3-layer (brain, skull, scalp) BEM models based on individual MRI images is state-of-the-art for EEG/MEG source estimation.

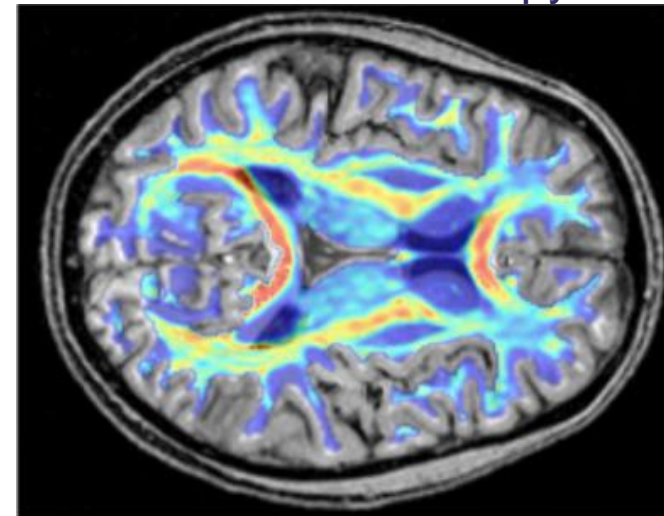
For MEG-only, single shell BEMs and local/corrected sphere models can provide reasonable approximations.

But heads are more complex:

White Matter
Gray Matter
CSF
Skull
Compacta
Skull
Spongiosa
Skin



Fractional Anisotropy



Vorwerk et al., NI 2014

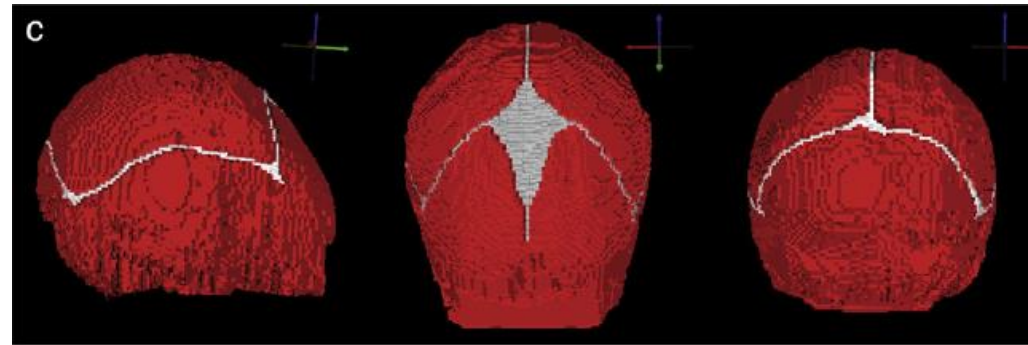
It is not obvious how to translate this into more accurate estimate for conductivity distributions.

Conductivities Of Tissues Can Only Be Approximated

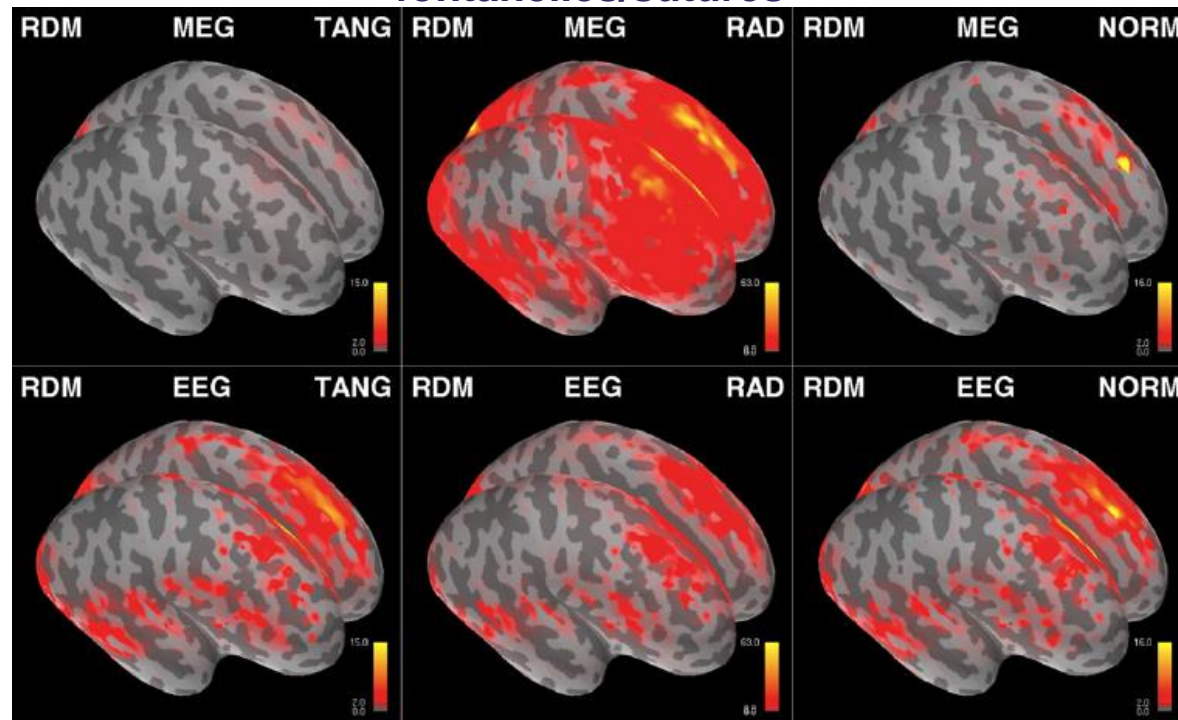
Table 2 Isotropic conductivity values of single tissue types used in human head volume conductor modeling

Tissue	Conductivity in S/m	Reference
Brain gray matter	0.45	Logothetis et al. 2007
Brain white matter	0.1	Akhtari et al. 2010
Spinal cord and cerebellum	0.16	Haueisen et al. 1995
Cerebrospinal fluid	1.79	Baumann et al. 1997
Hard bone (compact bone)	0.004	Tang et al. 2008
Soft bone (spongiform bone)	0.02	Akhtari et al. 2002
Blood	0.6	Gabriel et al. 2009
Muscle	0.1	Gabriel et al. 1996, 2009
Fat	0.08	Gabriel et al. 2009
Eye	1.6	Pauly and Schwan 1964 ; Lindenblatt and Silny 2001
Scalp	0.43	Geddes and Baker 1967
Soft tissue	0.17	Haueisen et al. 1995
Internal air	0.0001	Haueisen et al. 1995

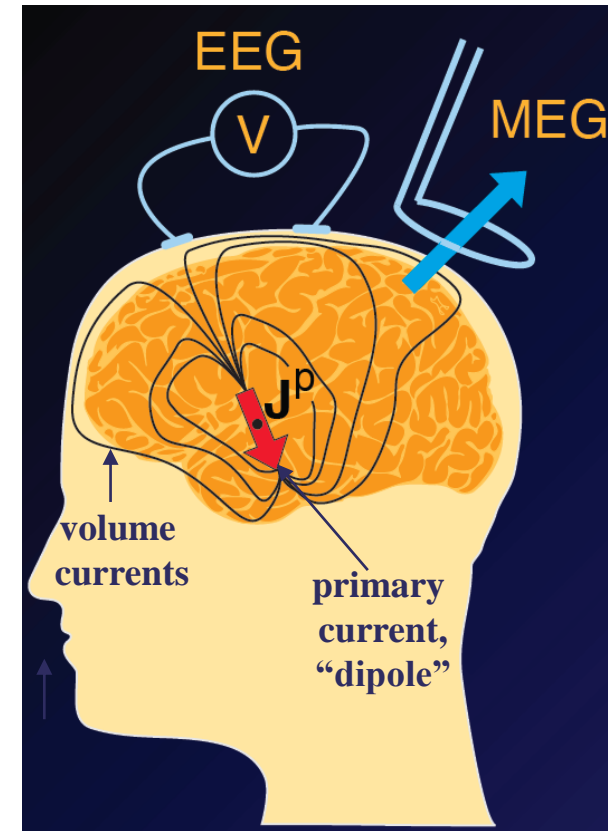
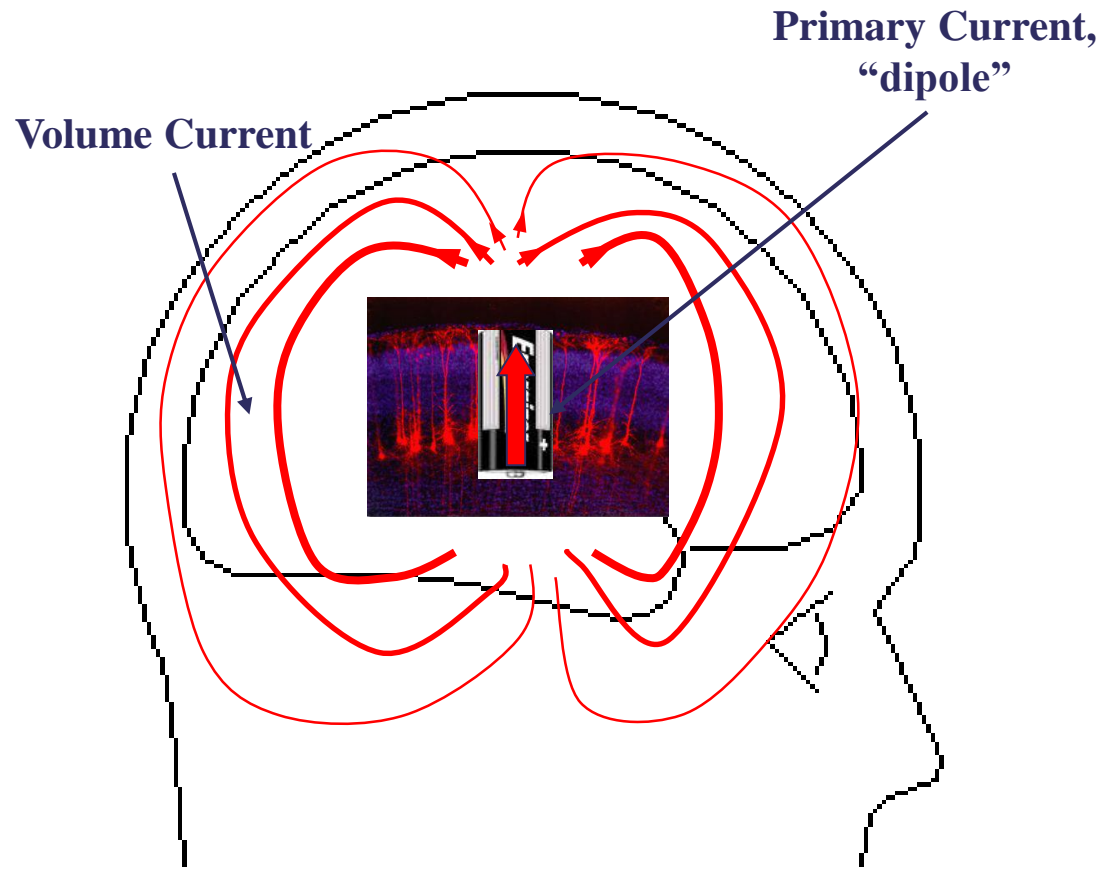
Infant Skulls – Fontanelles and Sutures



Relative error between models with and without fontanelles/sutures



Different Sensitivities of EEG and MEG



<http://www.nmr.mgh.harvard.edu/meg/pdfs/talks/>

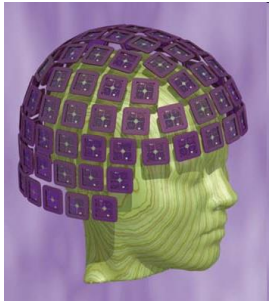
All effects are instantaneous.
Volume currents affect both EEG and MEG –
but EEG more than MEG

Different Sensors and their Sensitivities (Leadfields)

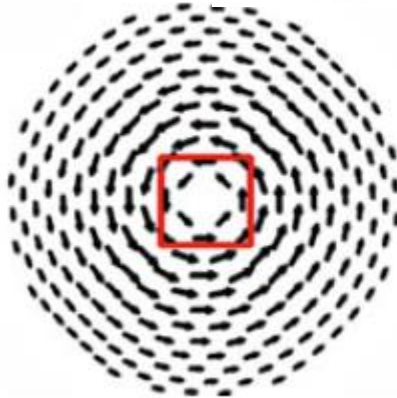
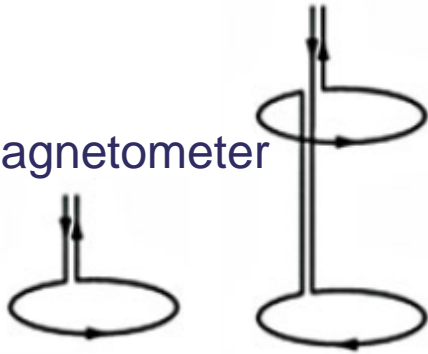
Leadfields are “sensitivity profiles” of individual sensors.

Each sensor is maximally sensitive to sources oriented along the arrows, and insensitive to sources perpendicular to the arrows.

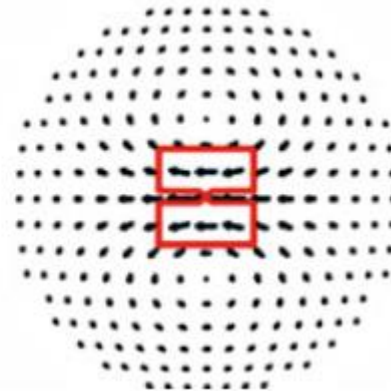
Axial Gradiometer



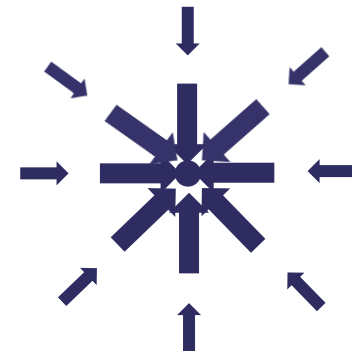
Magnetometer



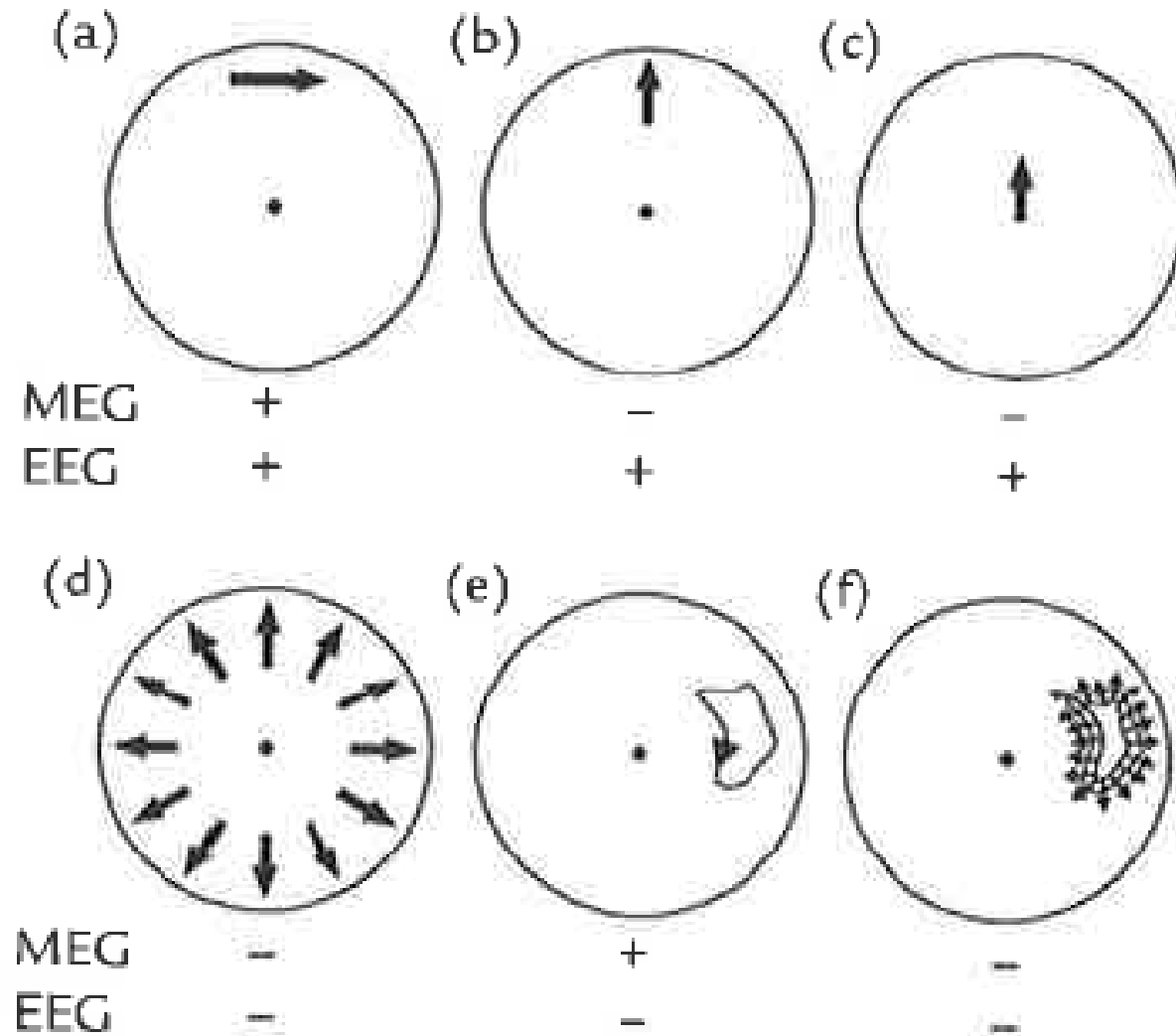
Planar Gradiometer(s)



EEG Electrode



EEG and MEG Are Differentially Sensitive To Radial and Tangential Sources

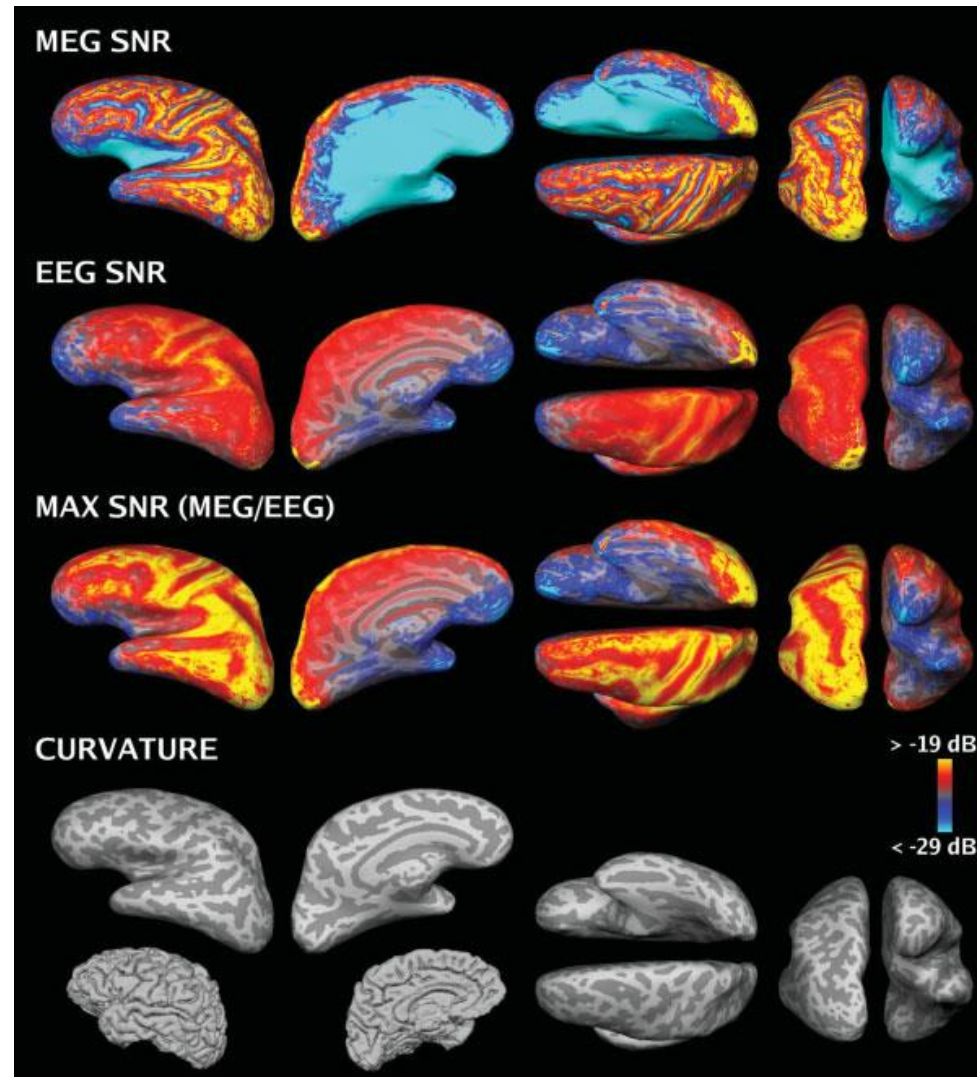


MEG is relatively insensitive to radial currents, and therefore also to deep currents.

Some complex source distributions may not produce EEG or MEG signals.

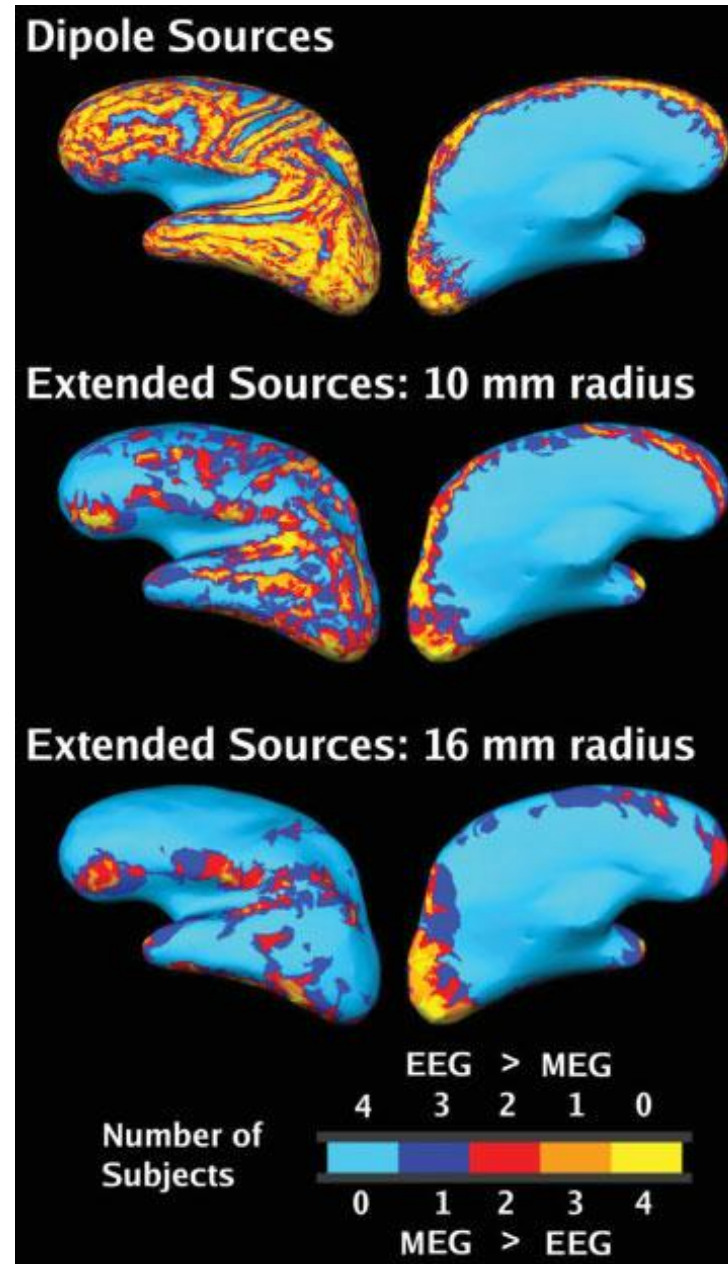
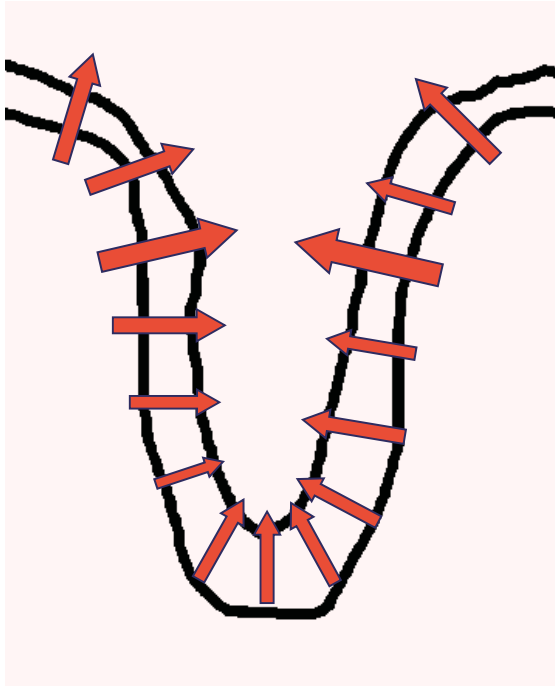
Sensitivity Maps

Sensor type, coverage and distance to sources strongly affect sensitivity and spatial resolution



MEG Is Less Sensitive To Spatially Extended Sources Than EEG

Distributed source around sulcus



Conclusion – Head Modelling

3-compartment BEM models are currently state-of-the-art for EEG/MEG source estimation.

Single-shell approximations are still common for MEG.

More detailed head models may increase accuracy, but require more accurate data and information, such as accurate MRI segmentations and conductivity values. (see e.g. Vorwerk et al., BioMeg Eng Online 2018) for Fieldtrip FEM pipeline)

There is no right or wrong, there are only different approximations – know your limits.

Fixing Head Models

https://mne.tools/stable/auto_tutorials/forward/80_fix_bem_in_blender.html



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Thank you

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