

Multi-modal integration

Rik Henson

MRC CBU, Cambridge

Data-driven vs Model-driven

1. Data-driven in sense that no model that links specific features of one modality with features of another (still employ some form of statistical model), eg ICA, CCA

2. Model-driven in sense that either:
 - 2.1 test specific feature relations across modalities, eg SEM

 - 2.2 has a generative model of both modalities, eg PEB

Symmetric vs Asymmetric

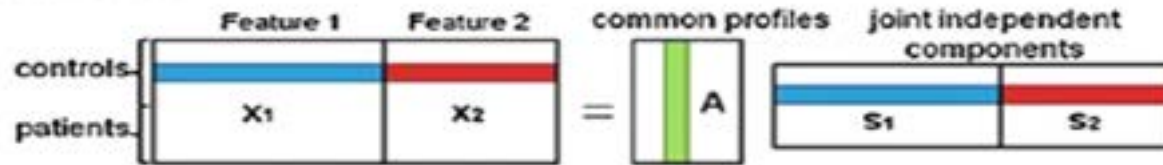
1. Symmetric integration (“fusion”) fits each modality simultaneously
2. Asymmetric integration uses one modality to model another modality

(Most data-driven approaches are symmetric; many, but not all, model-driven approaches are asymmetric)

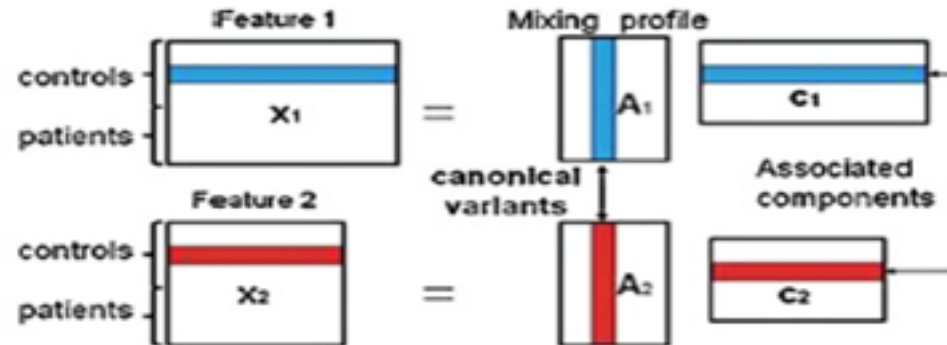
Some Data-Driven Methods

1. Linked Matrix Factorisation methods (ICA, CCA, PLS)
2. Representational Similarity Analysis (RSA)
3. Graph Theory

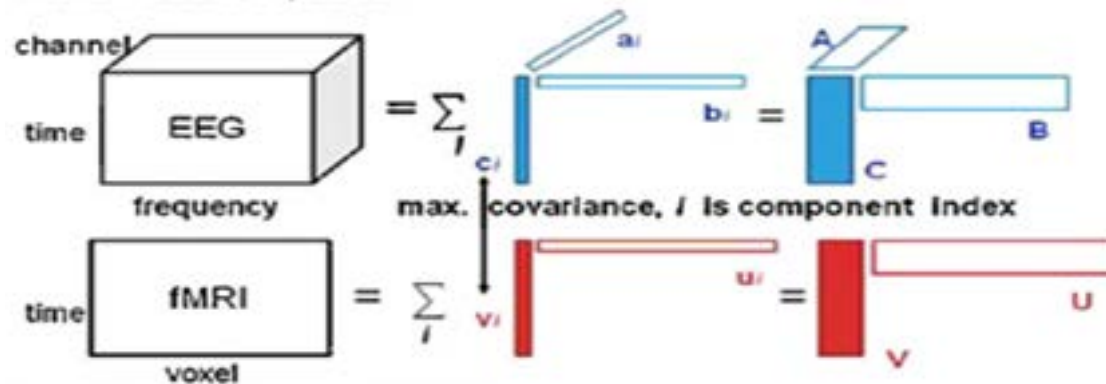
Joint ICA



mCCA

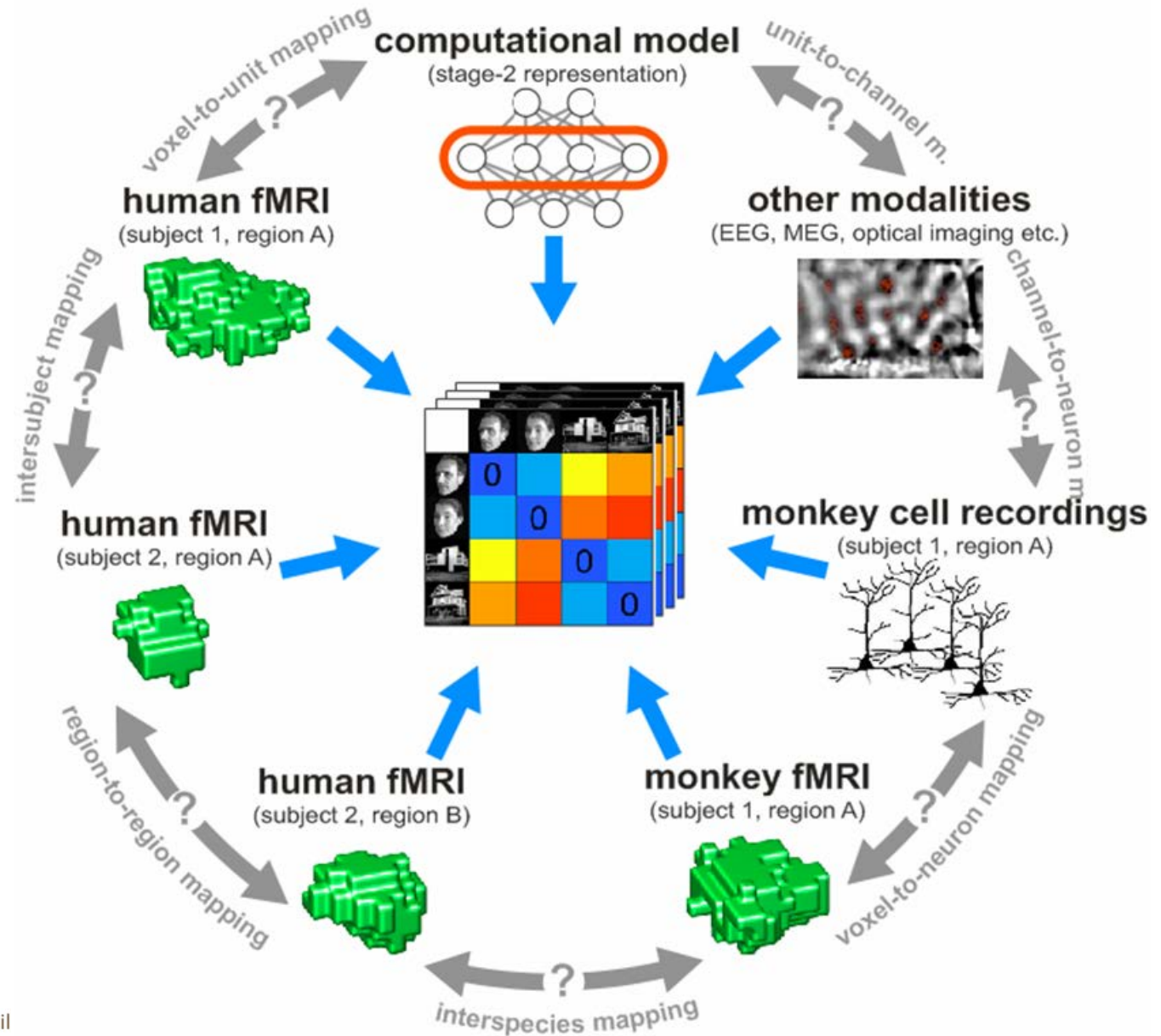


Partial Least Squares



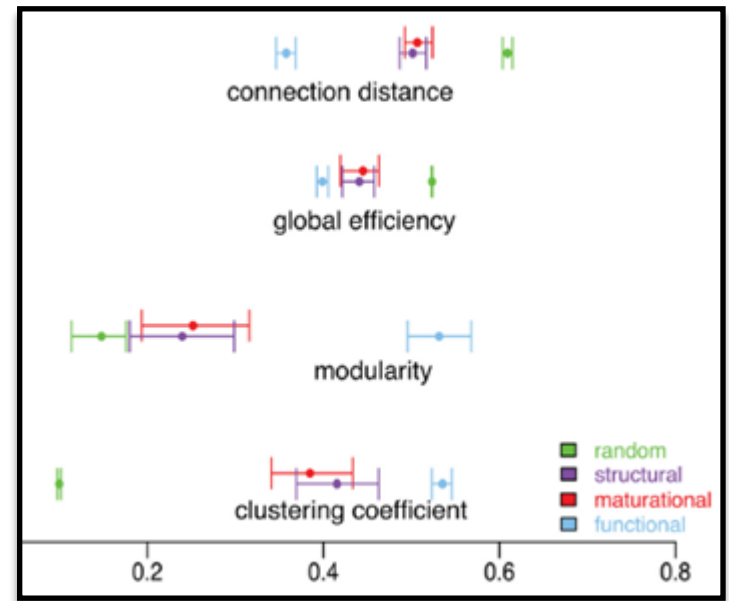
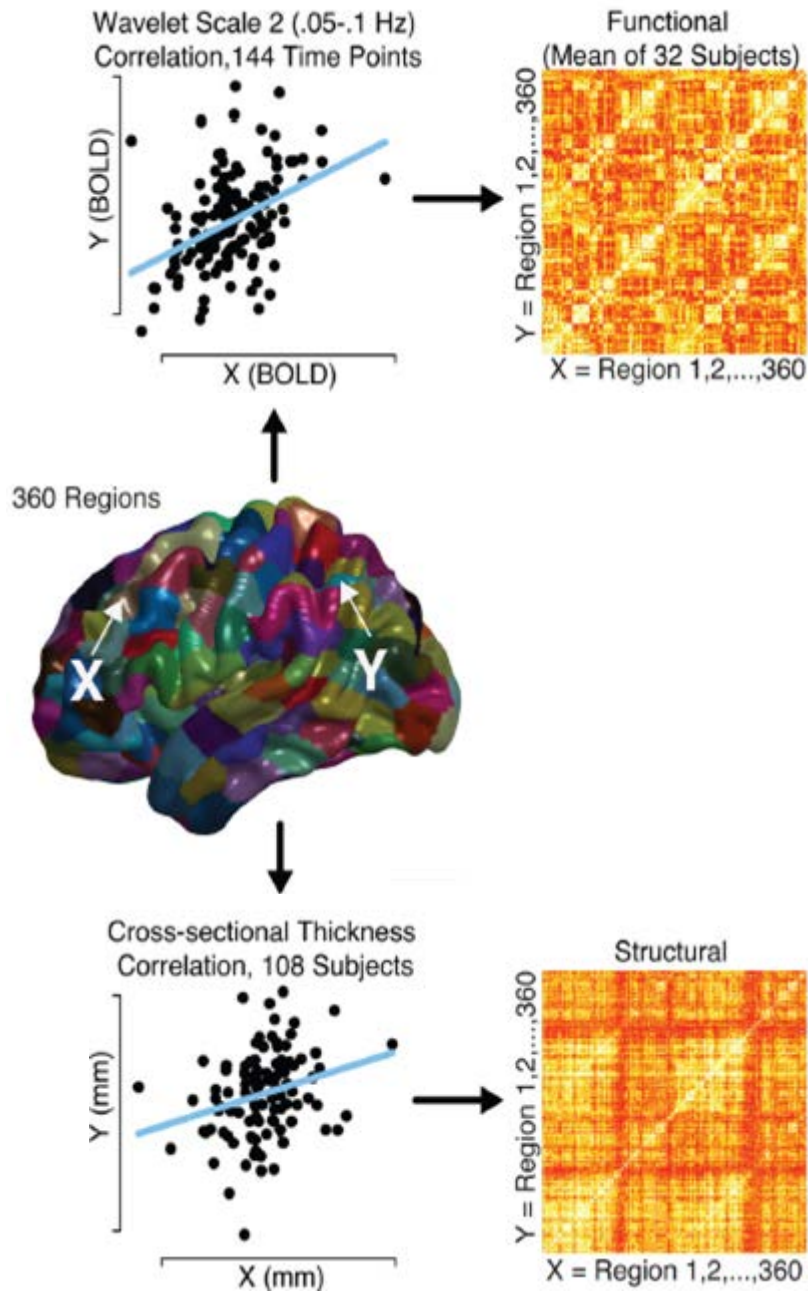
Some Data-Driven Methods

1. Linked Matrix Factorisation methods (ICA, PLS, CCA)
2. **Representational Similarity Analysis (RSA)**
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Some Data-Driven Methods

1. Linked Matrix Factorisation methods (ICA, PLS, CCA)
2. Representational Similarity Analysis (RSA)
3. Graph Theory



...or can even compare graphs with different nodes, eg fMRI ROIs and MEEG sensors...

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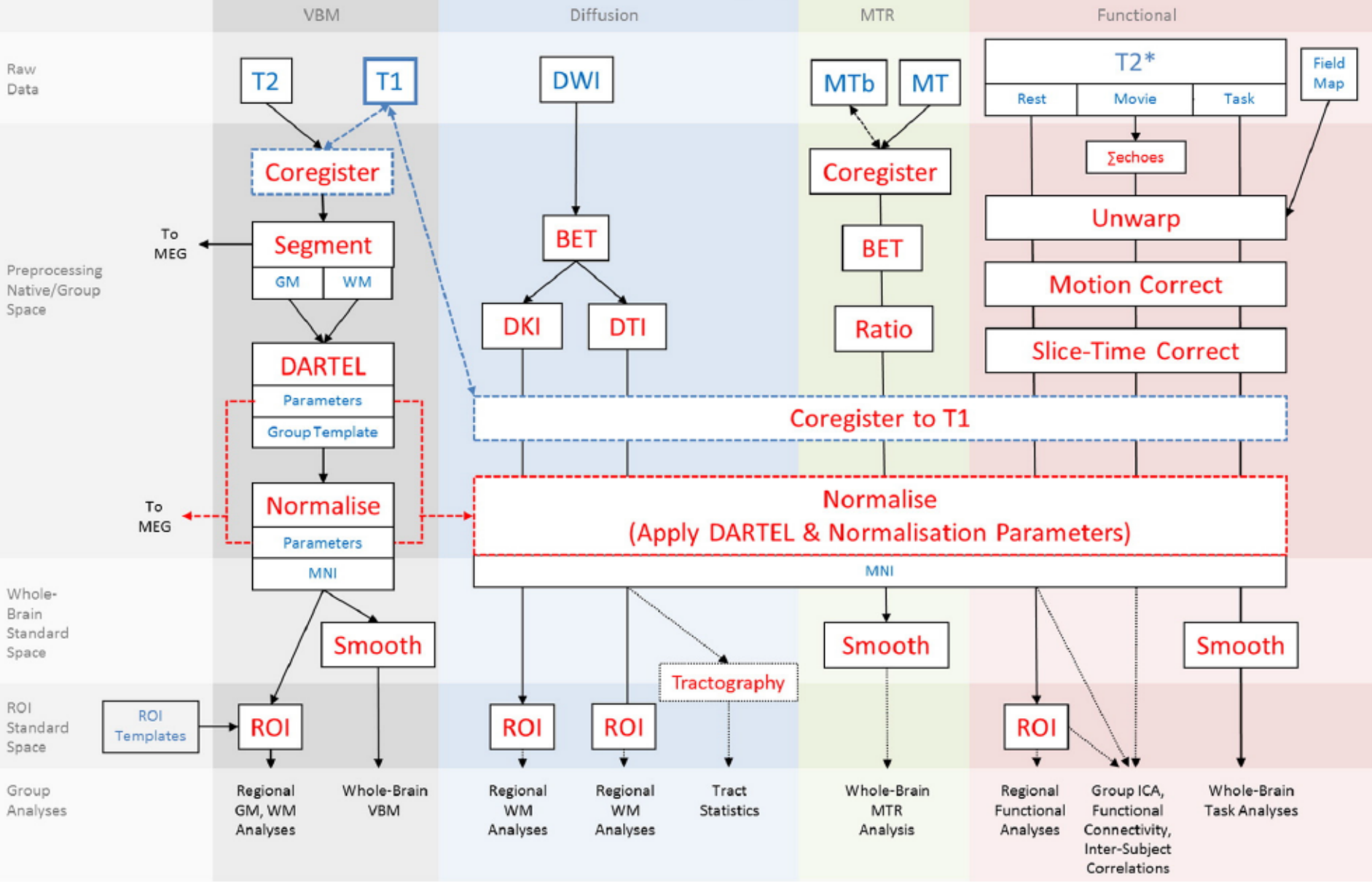
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Some Model-Based Examples (local CamCAN examples)

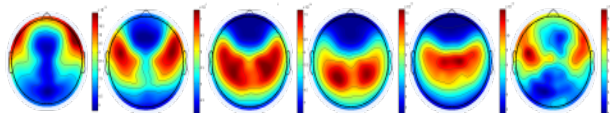
1. Combining T1-, T2-, Diffusion- and MT-weighted images for segmentation and normalisation
2. Univariate mediation: Using MEG to separate effects of age on neural vs vascular responsivity in fMRI
3. Univariate mediation: Using DKI to investigate effects of age on MEG latency
4. Multivariate Structural Equation Modelling (SEM) to separate GM and WM contributions to executive function

MRI Processing Pipelines

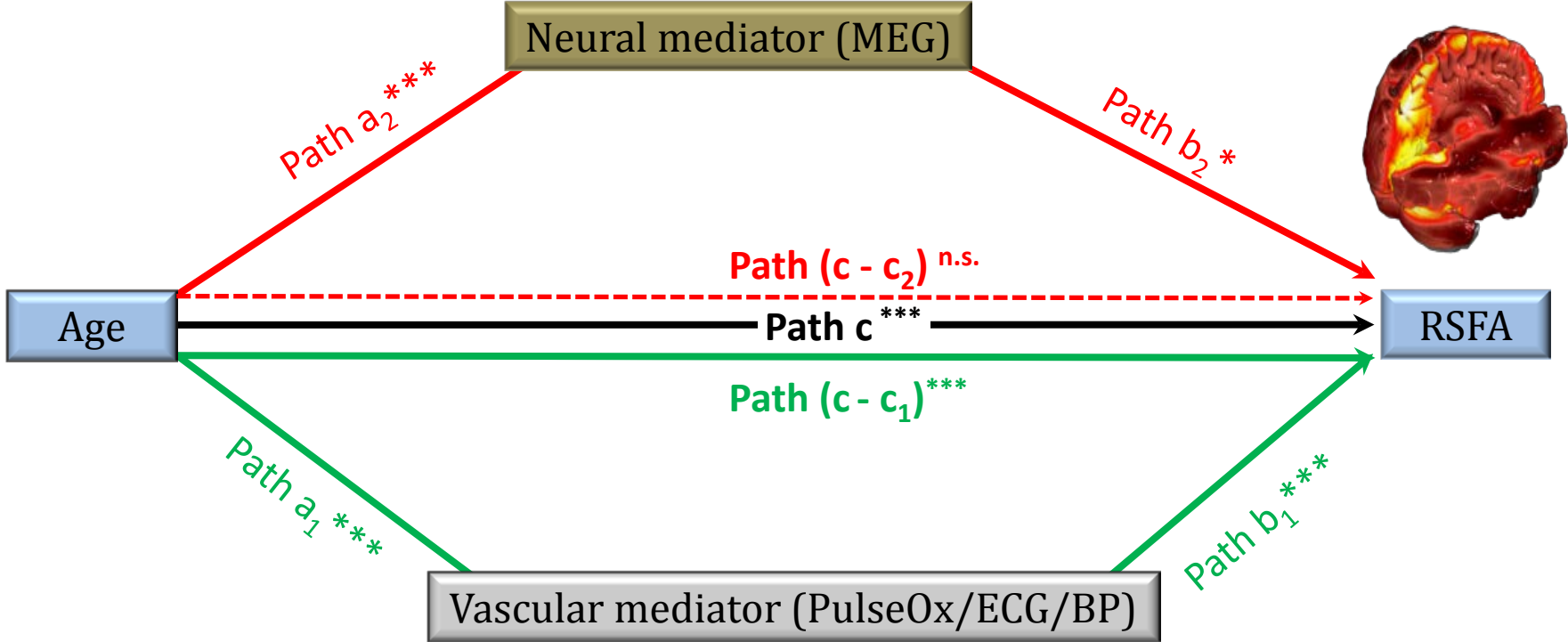
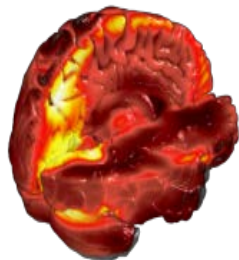


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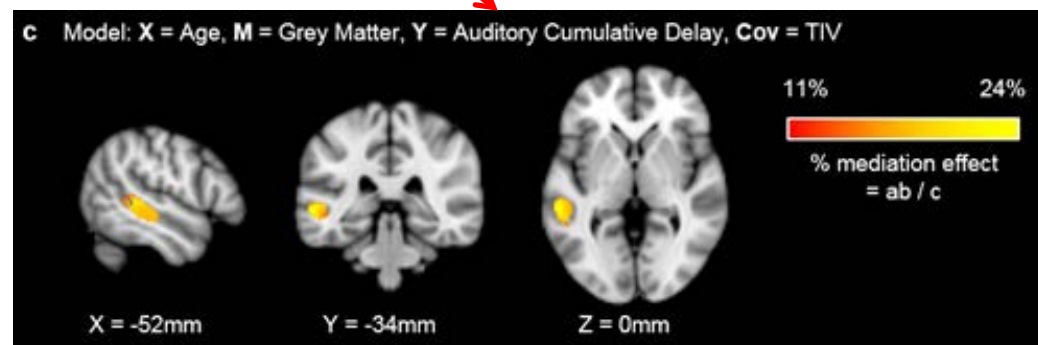
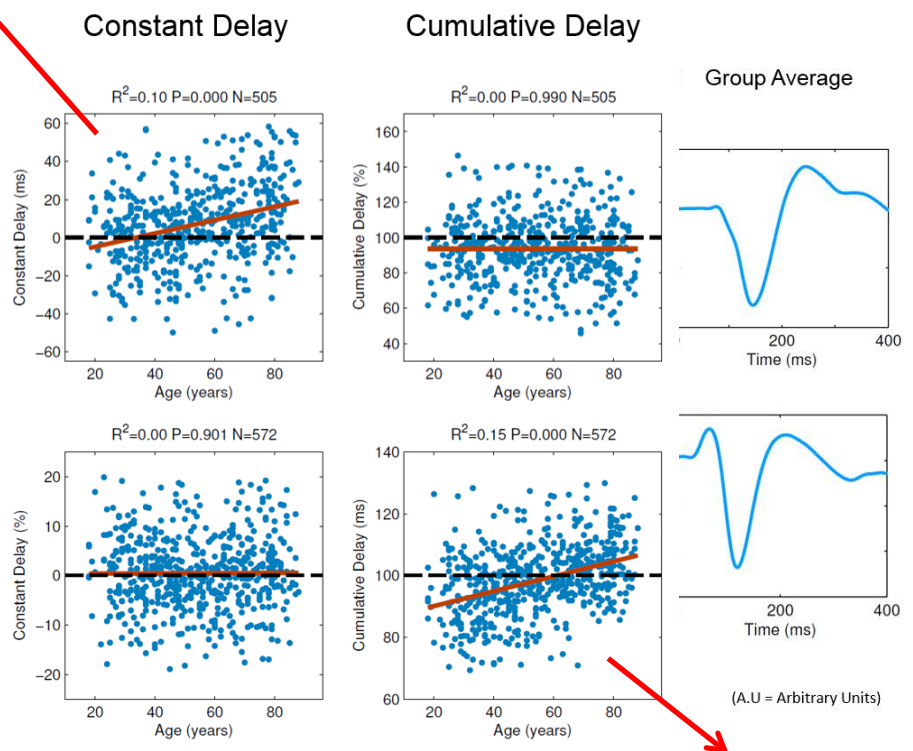
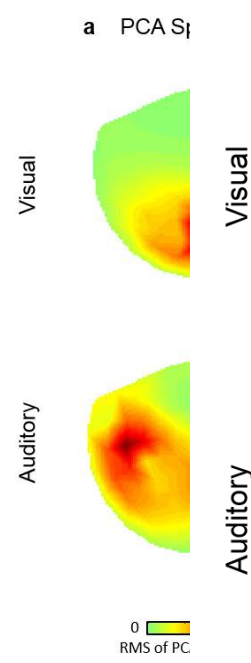
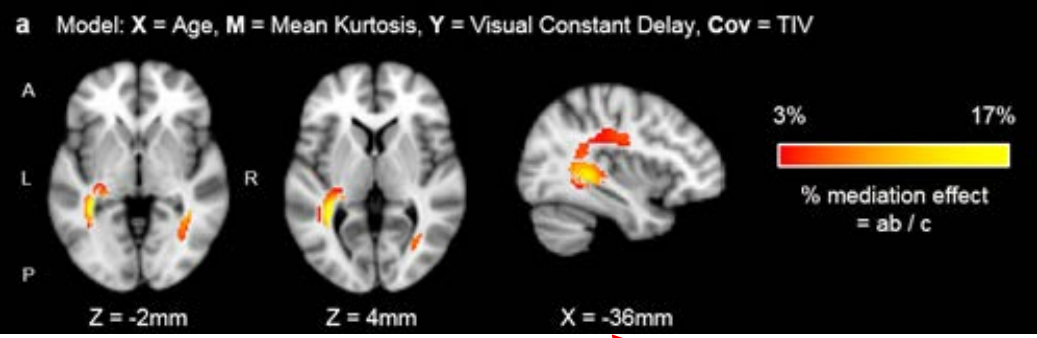


Neural mediator (MEG)



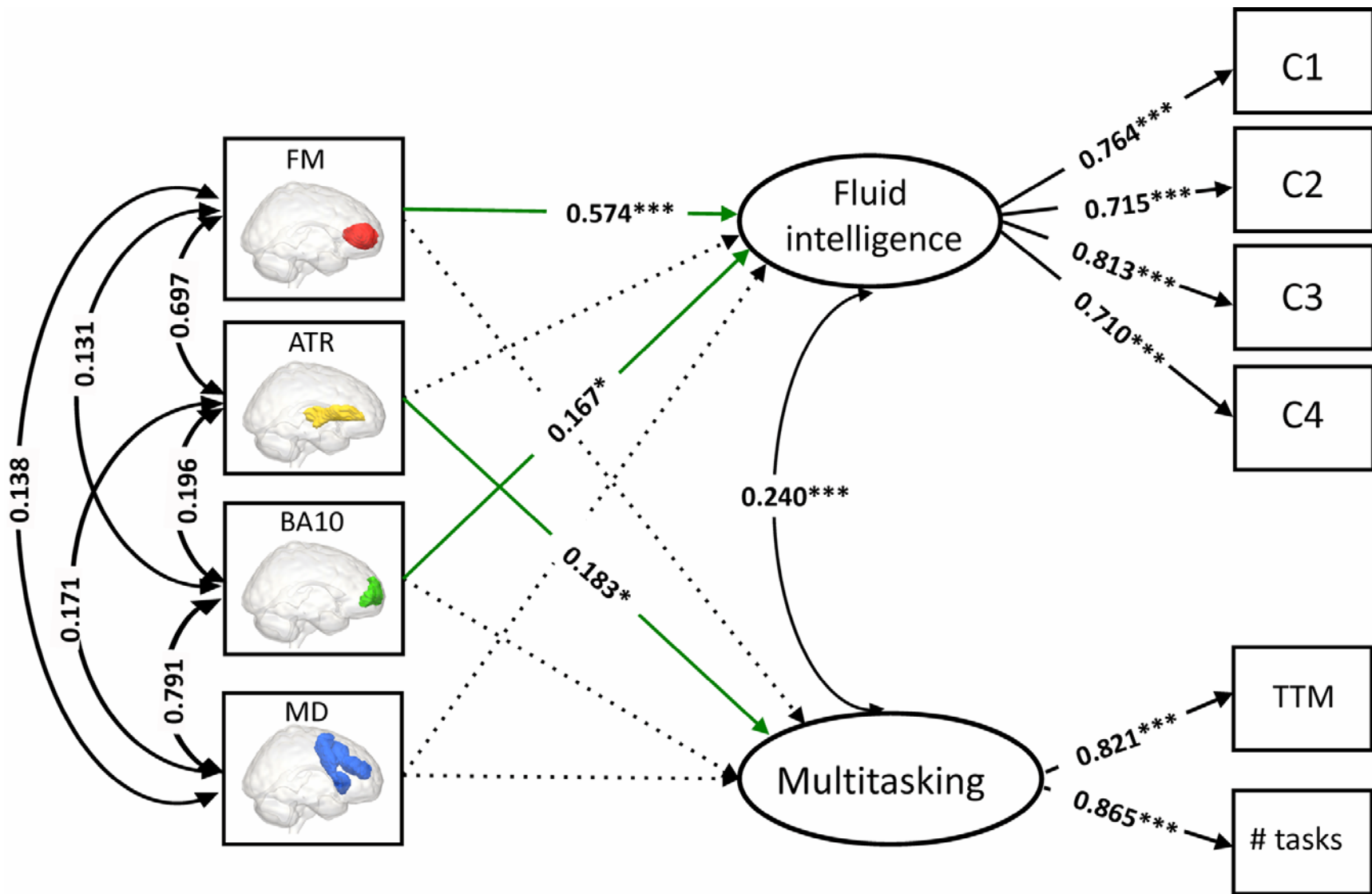
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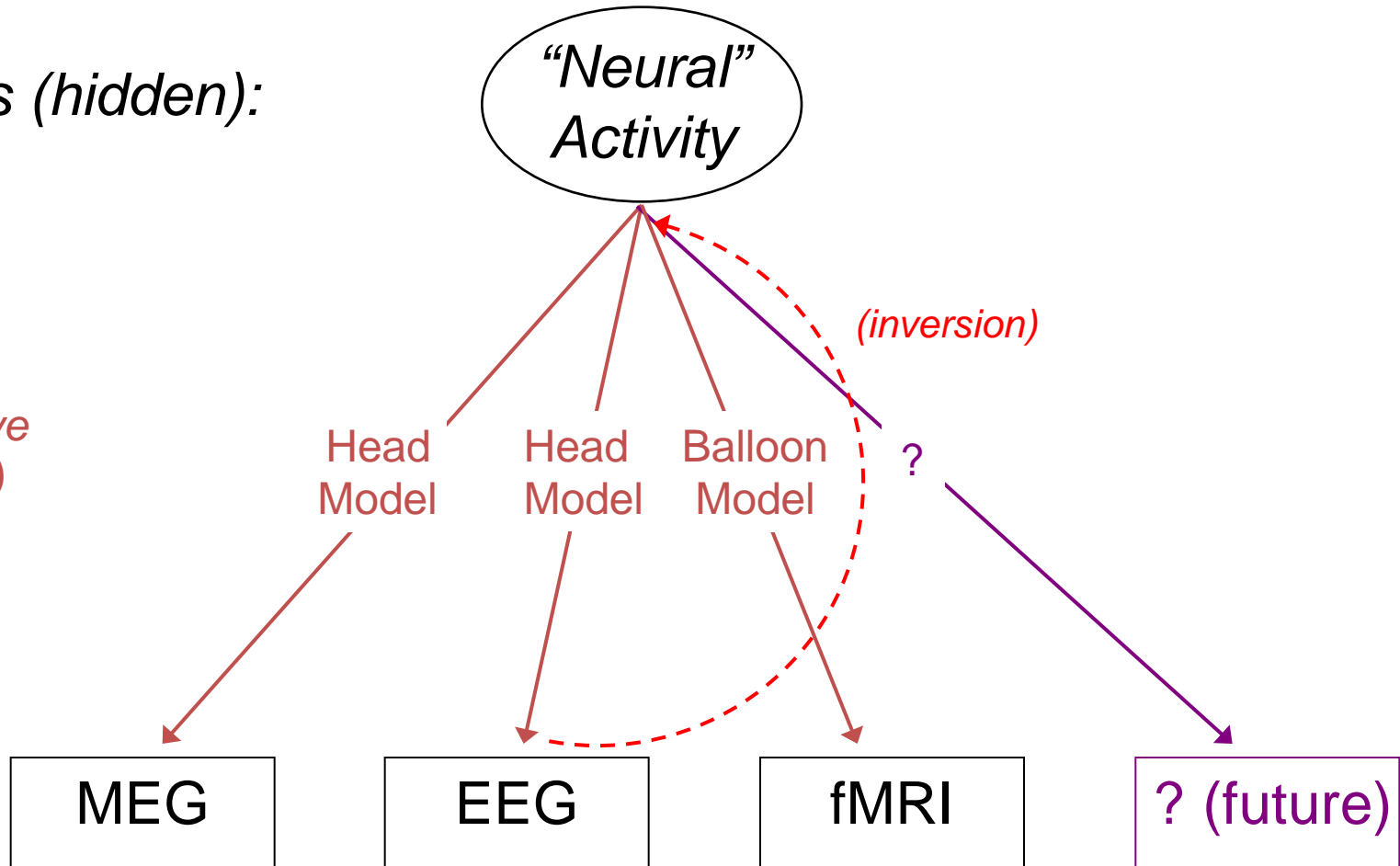
Multi-modal integration of MEG, EEG & fMRI

Multi-modal Integration

Causes (hidden):

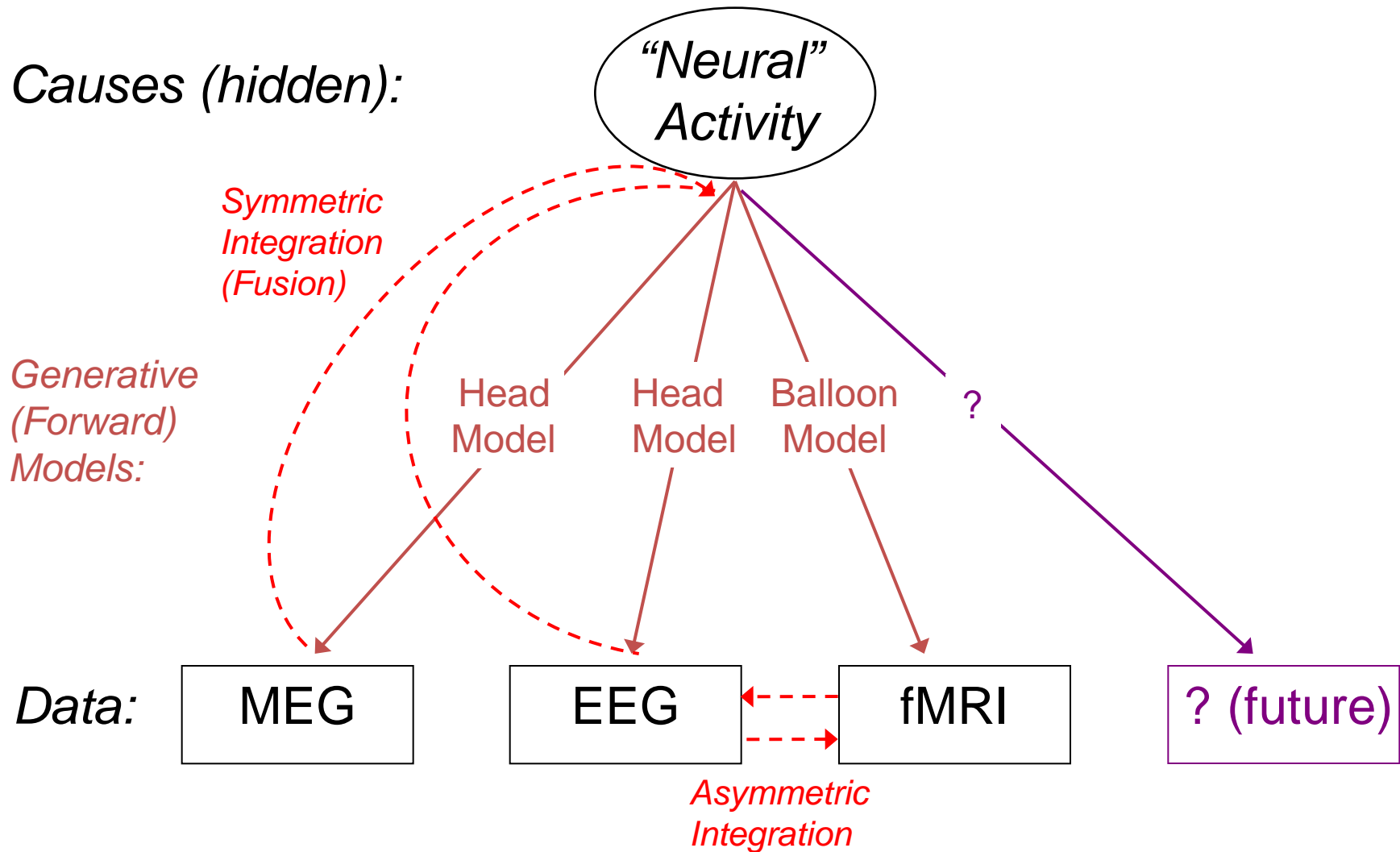
*Generative
(Forward)
Models:*

Data:



Multi-modal Integration

Causes (hidden):



Examples

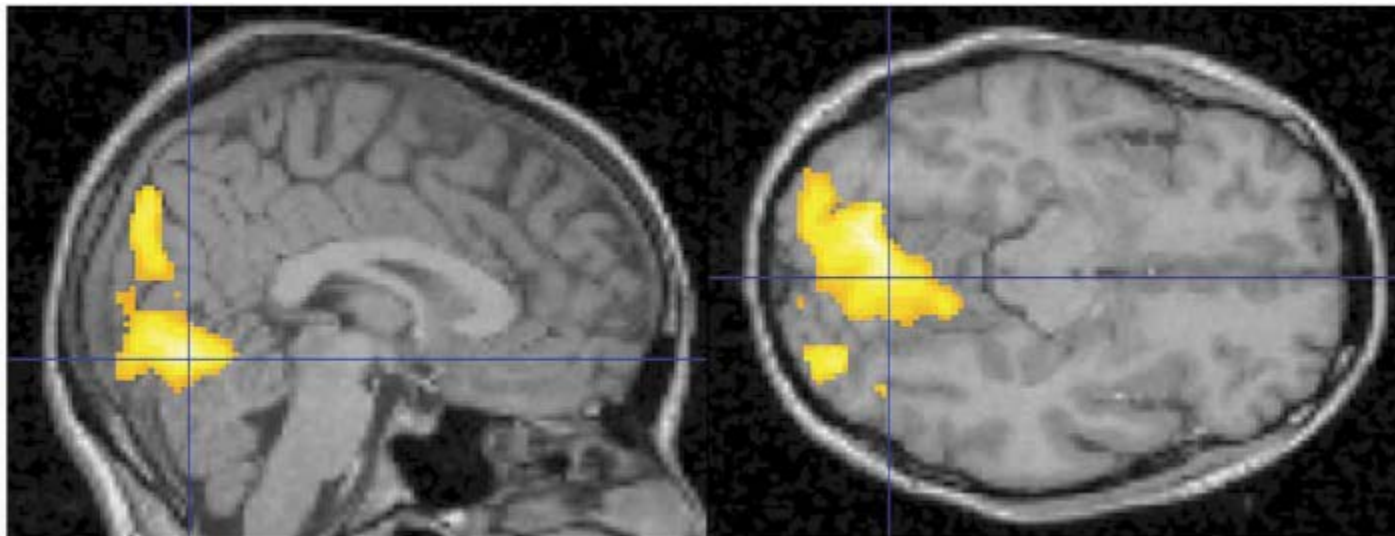
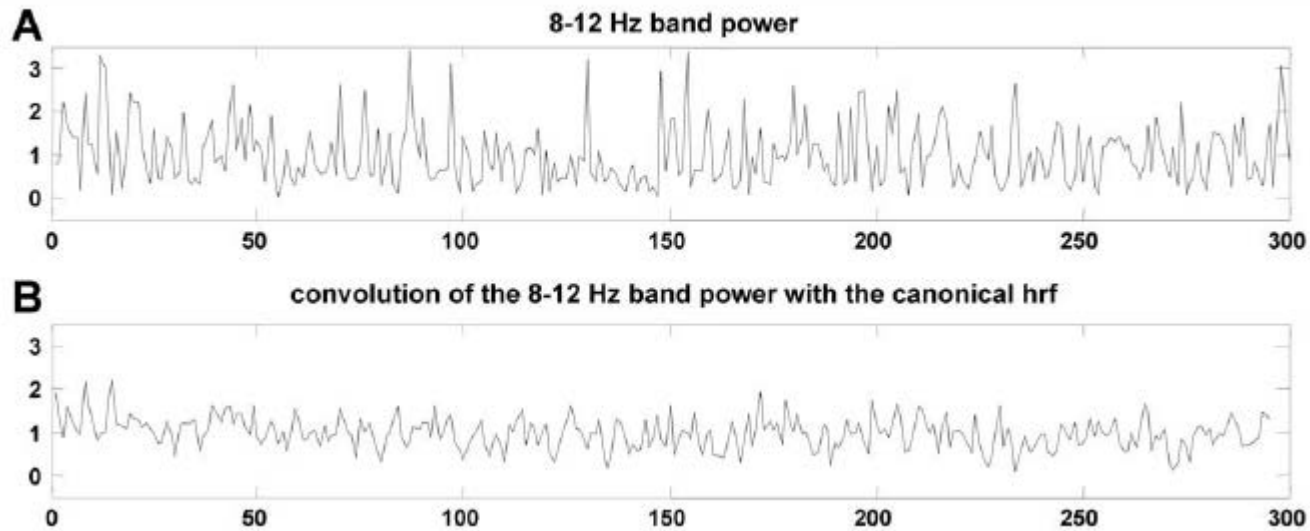
1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Concurrent EEG and fMRI

H. Laufs et al. / NeuroImage 19 (2003) 1463–1476



Examples

1. EEG \rightarrow fMRI asymmetric integration
- 2. fMRI \rightarrow M/EEG asymmetric integration**
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Examples

1. EEG \rightarrow fMRI asymmetric integration

(Background: The M/EEG inverse problem)

3. MEG \leftrightarrow EEG symmetric integration (fusion)

Given n sensors and p sources fixed in location and orientation (e.g, on a cortical mesh), then linear Forward Model (for single timepoint):

$$\begin{bmatrix} d_1 \\ \vdots \\ d_n \end{bmatrix} = \begin{bmatrix} L_{11} & L_{12} & \cdots & L_{1p} \\ \vdots & \ddots & & \vdots \\ L_{n1} & \cdots & \cdots & L_{np} \end{bmatrix} \begin{bmatrix} s_1 \\ s_2 \\ \vdots \\ s_p \end{bmatrix} + \begin{bmatrix} e_1 \\ \vdots \\ e_n \end{bmatrix}$$

d = Data

s = Sources

L = Leadfields

e = Error (noise)

n sensors

$p \gg n$ sources

n sensors \times p sources

n sensors...

Equivalent matrix format:

$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

Assume sensor noise is zero-mean Gaussian with error covariance $\mathbf{C}^{(e)}$:

$$e \sim N(0, \mathbf{C}^{(e)})$$

Assume sources similarly Gaussian with source covariance $\mathbf{C}^{(s)}$:

$$s \sim N(0, \mathbf{C}^{(s)})$$

M/EEG Linear Forward Model Assumptions to Solve

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$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$
$$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$$
$$\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$$

d = Data

s = Sources

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e = Error (noise)

n sensors

$p \gg n$ sources

n sensors \times p sources

n sensors...

General solution is:

Hauk (2004), Neuroimage

$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d}$$

λ = Regularisation (hyperparameter)

But how calculate $\mathbf{C}^{(e)}$ and $\mathbf{C}^{(s)}$?

MEG Linear Forward Model Assumptions to Solve

One approach is to model sources and noise by variance components:

$$\mathbf{C} = \sum_i \lambda_i \mathbf{Q}_i$$

\mathbf{C} = Sensor/Source covariance

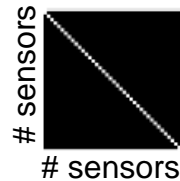
\mathbf{Q} = Covariance components

λ = Hyper-parameters

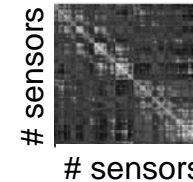
Friston et al (2008) Neuroimage

1. Sensor components, $\mathbf{Q}_i^{(e)}$ (error):

“IID” (white noise):

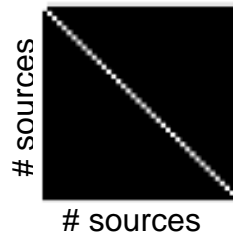


Empty-room:

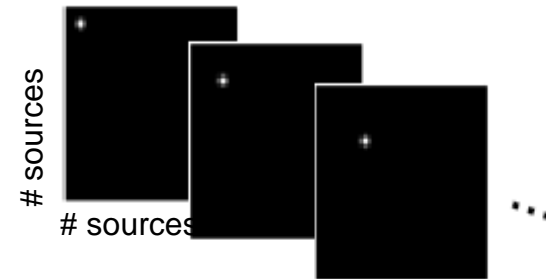


2. Source components, $\mathbf{Q}_i^{(s)}$ (priors/regularisation):

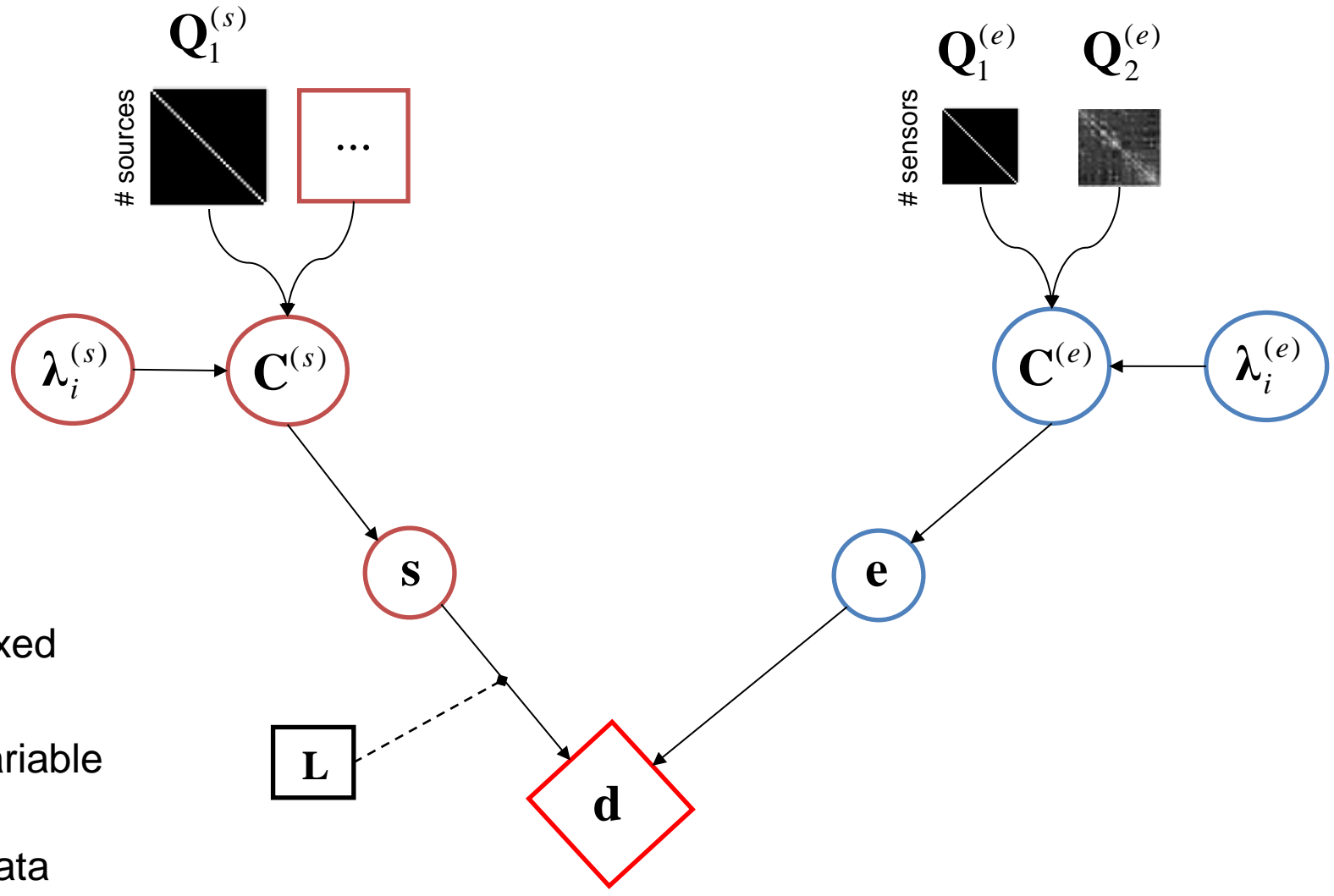
“IID” (min norm):



Multiple Sparse Priors (MSP):



MEG Generative Model



M/EEG Linear Forward Model Assumptions to Solve

$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$
 $\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$

d = Data
 s = Sources
 L = Leadfields
 e = Error (noise)

n sensors
 $p \gg n$ sources
 n sensors \times p sources
 n sensors...

General solution is:

Hauk (2004), Neuroimage

$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d}$$

λ = Regularisation (hyperparameter)

But how calculate $\mathbf{C}^{(e)}$ and $\mathbf{C}^{(s)}$?

Specify multiple (covariance) priors, and estimate their weighting (hyperparameters) by maximising **model evidence**

(using a variational Bayesian approach, eg EM algorithm)

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Asymmetric Integration of MEG+fMRI Background

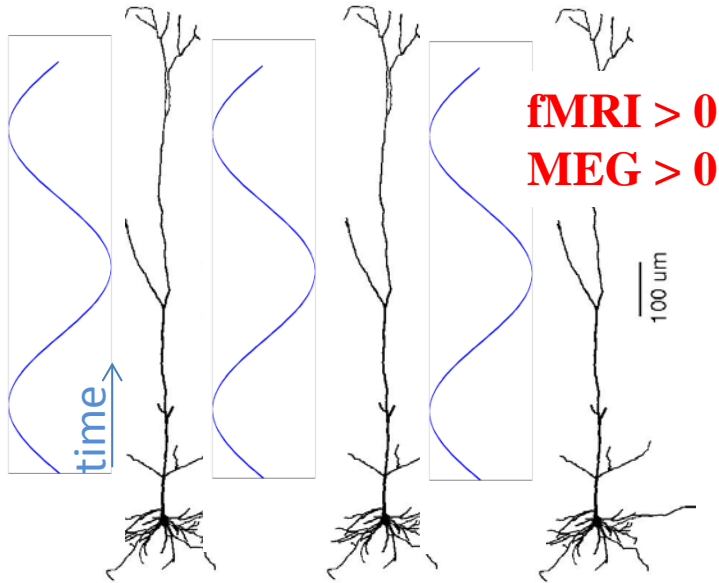
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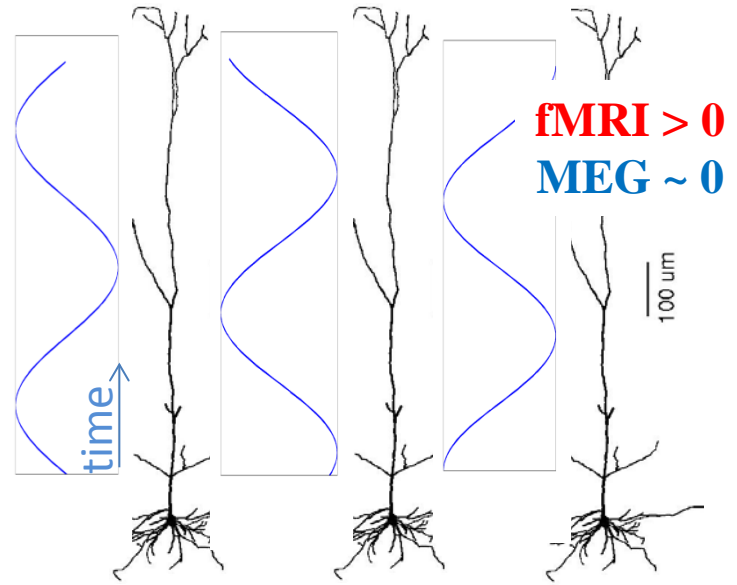
- fMRI has superior spatial resolution (~mm) than M/EEG, but inferior temporal resolution (integrating over seconds)
- fMRI and M/EEG measure similar, but not identical, neural activity
- Eg, some source configurations give detectable fMRI signal, but no detectable M/EEG signal...
- ...and vice versa

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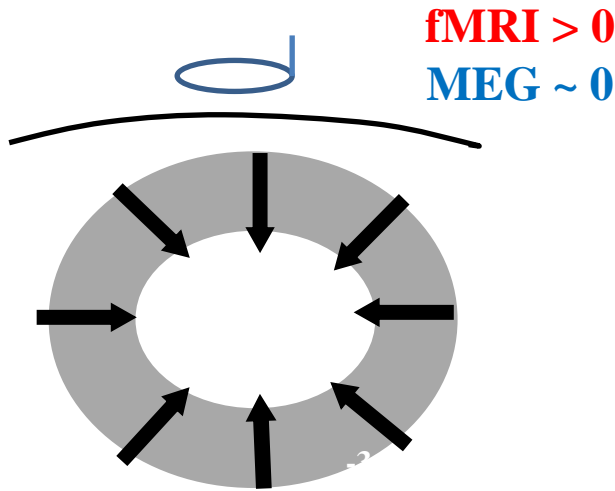
Synchronous



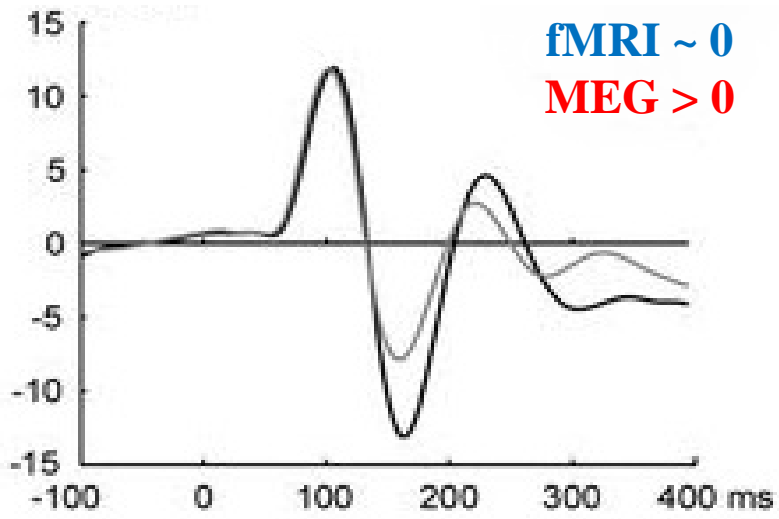
Asynchronous



Closed Fields?



Transient Differences



Asymmetric Integration of MEG+fMRI Background

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- fMRI has superior spatial resolution (~mm) than M/EEG, but inferior temporal resolution (integrating over seconds)
- fMRI and M/EEG measure similar, but not identical, neural activity
- Eg, some source configurations give detectable fMRI signal, but no detectable M/EEG signal...
- ...and vice versa
- Use fMRI as a **soft**, rather than **hard**, constraint on localisation of sources of M/EEG data...

Specifying (co)variance components (priors/regularisation):

$$\mathbf{C} = \sum_i \lambda_i \mathbf{Q}_i$$

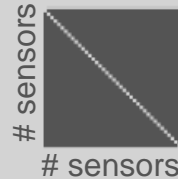
\mathbf{C} = Sensor/Source covariance

\mathbf{Q} = Covariance components

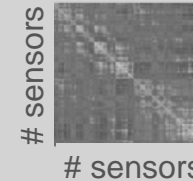
λ = Hyper-parameters

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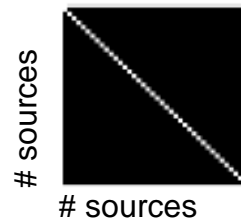


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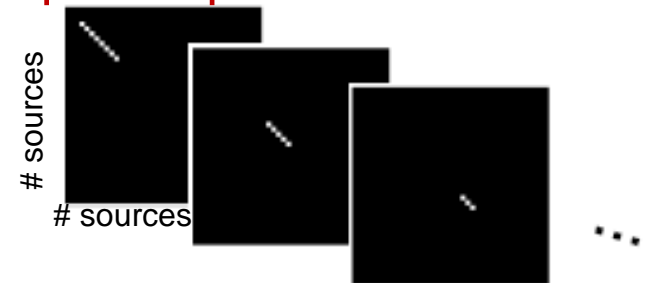


2. Each suprathreshold fMRI cluster becomes a separate prior $\mathbf{Q}_i^{(s)}$

“IID” (min norm):



fMRI Priors:



General solution again:

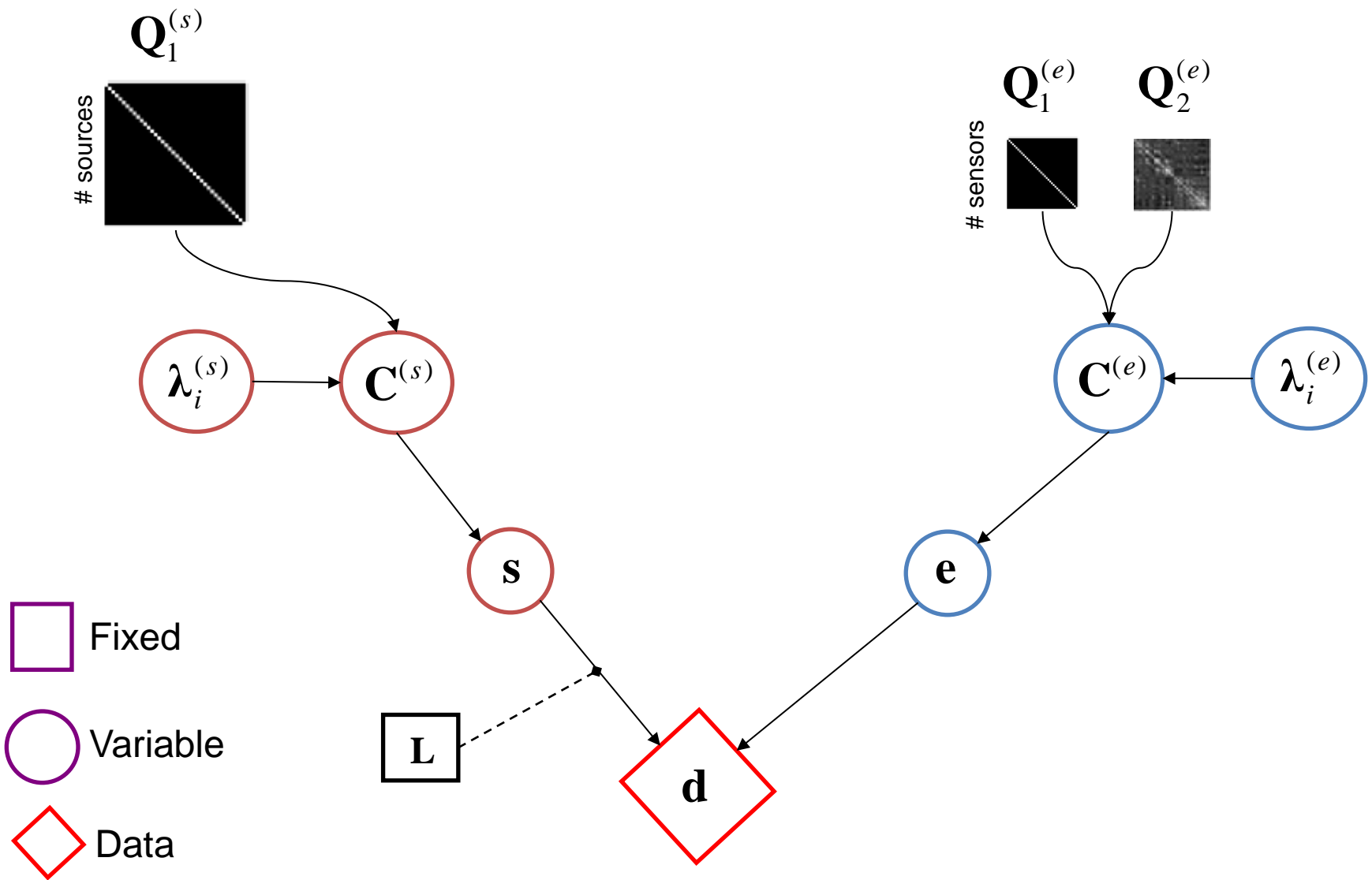
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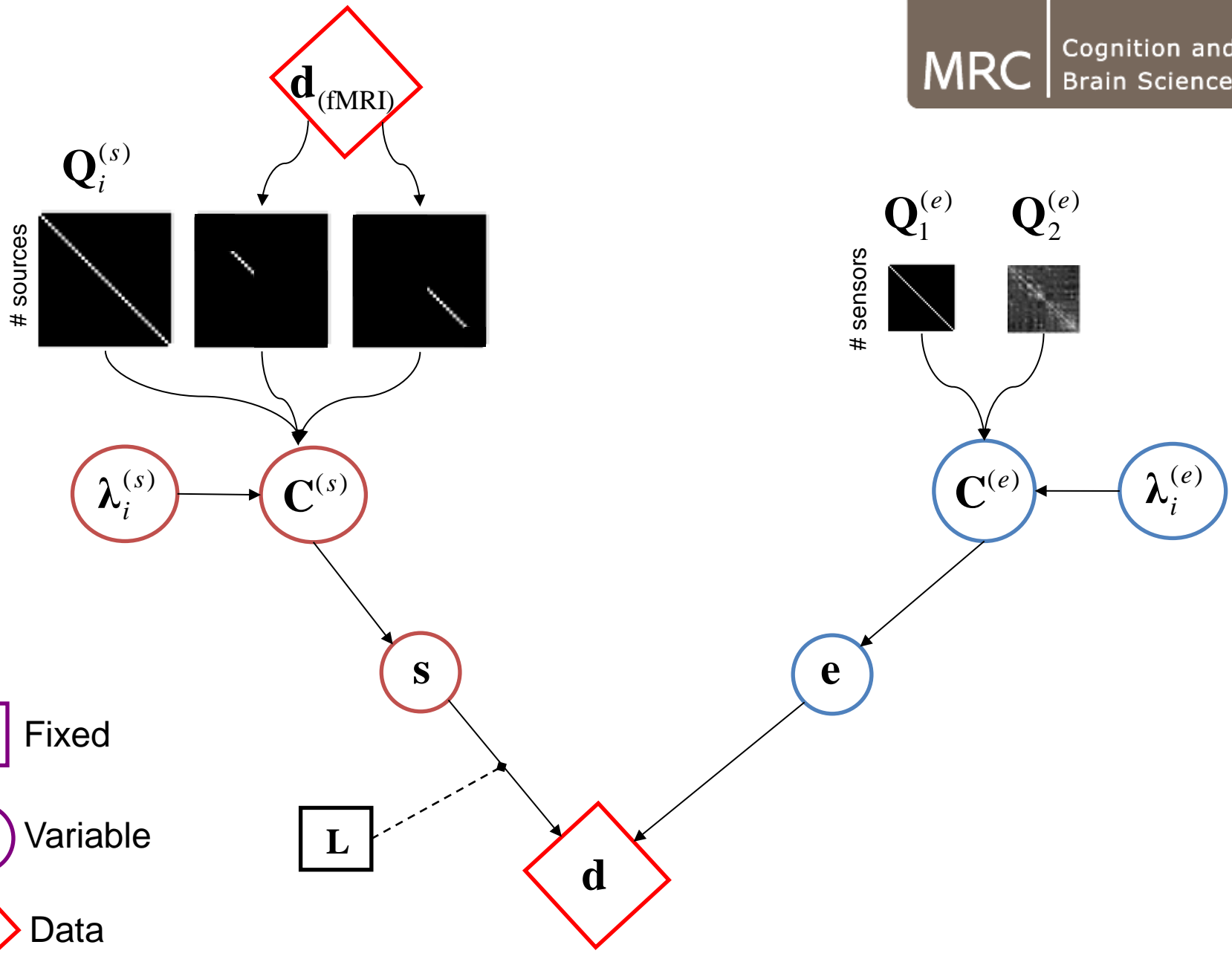
Now source covariance expressed as number of fMRI clusters:

$$\mathbf{C}^{(s)} = \lambda_1^{(s)} \mathbf{Q}_{(fMRI1)}^{(s)} + \lambda_2^{(s)} \mathbf{Q}_{(fMRI2)}^{(s)} + \dots$$

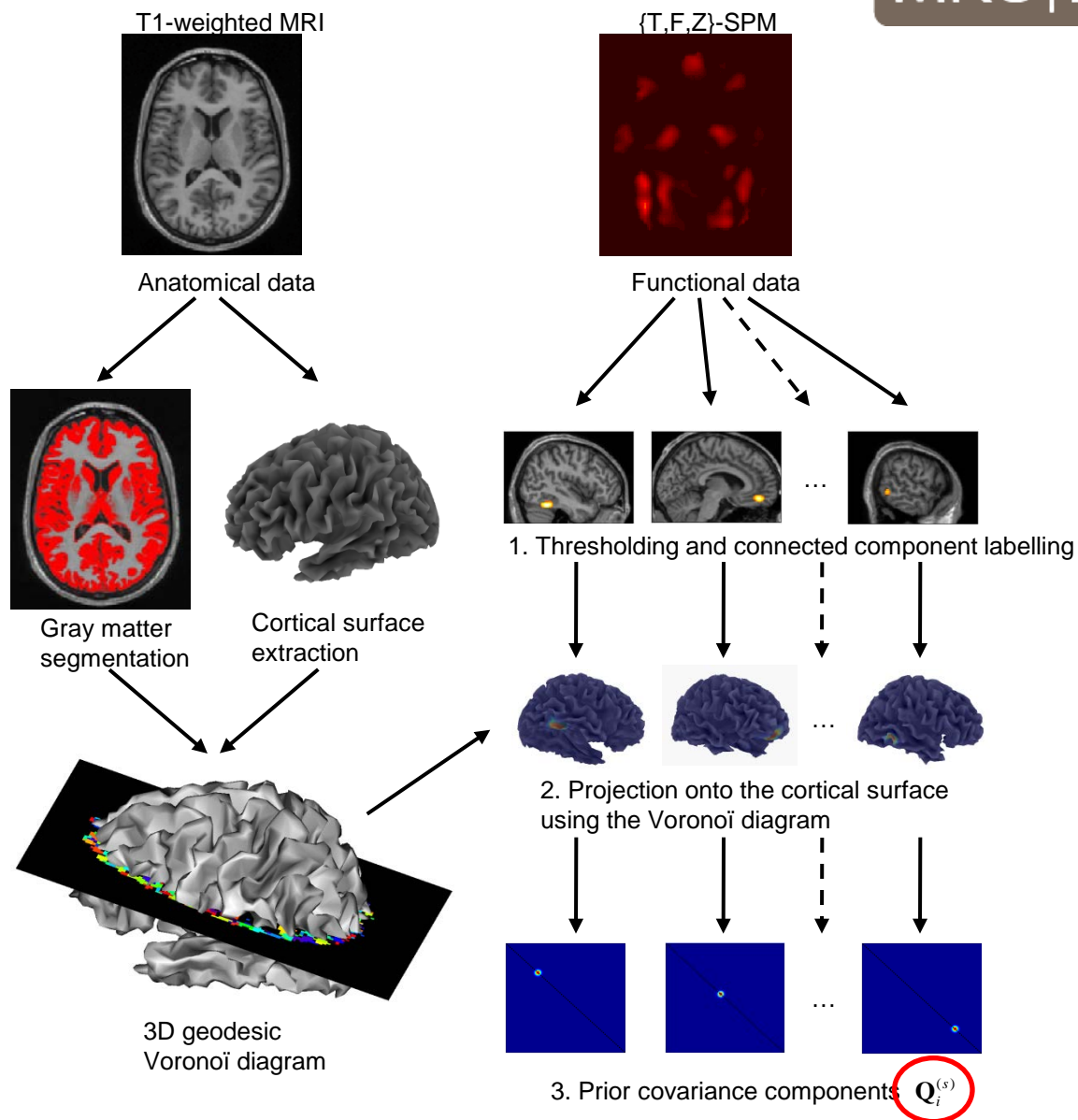
When $\mathbf{Q}_i^{(s)}$ does not help maximise model evidence, $\lambda_i^{(s)} \rightarrow 0$,
i.e. constraints ignored...

...catering for situations where fMRI signal does not reflect same activity as in M/EEG signal (e.g. occurring later than time-window than M/EEG data)

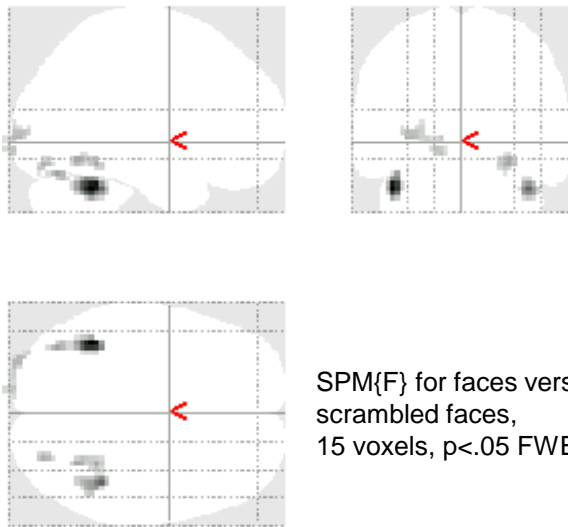




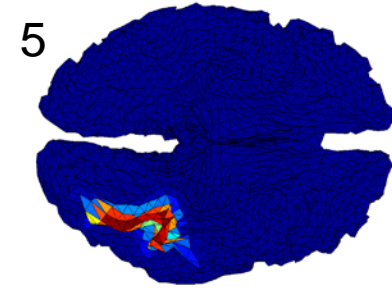
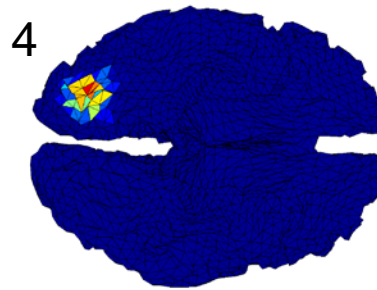
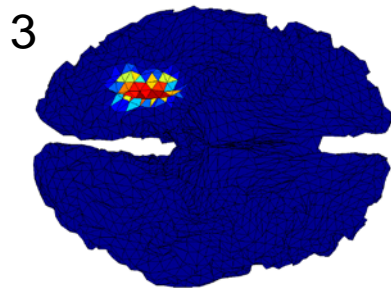
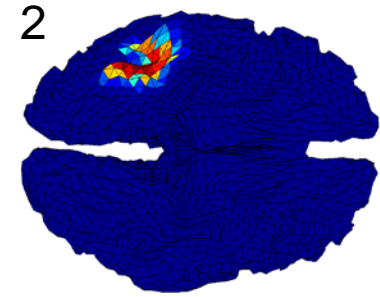
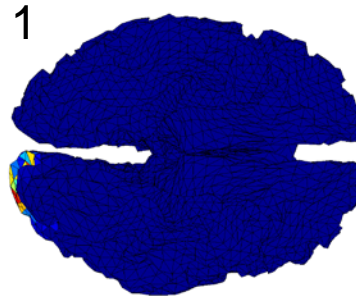
Asymmetric Integration of M/EEG+fMRI



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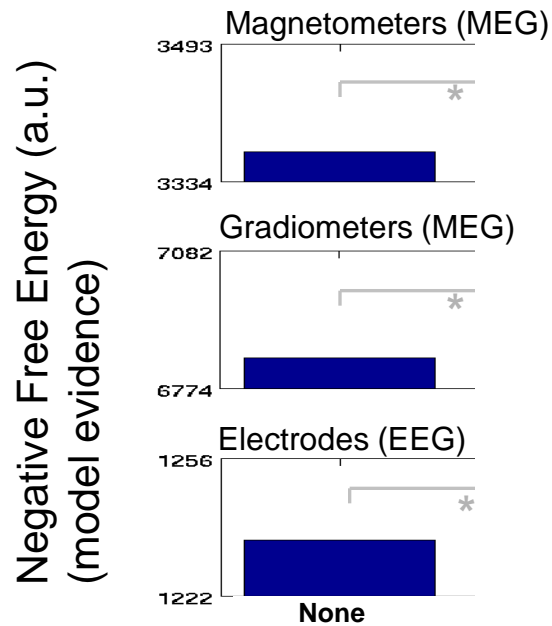


SPM{F} for faces versus
scrambled faces,
15 voxels, $p < .05$ FWE

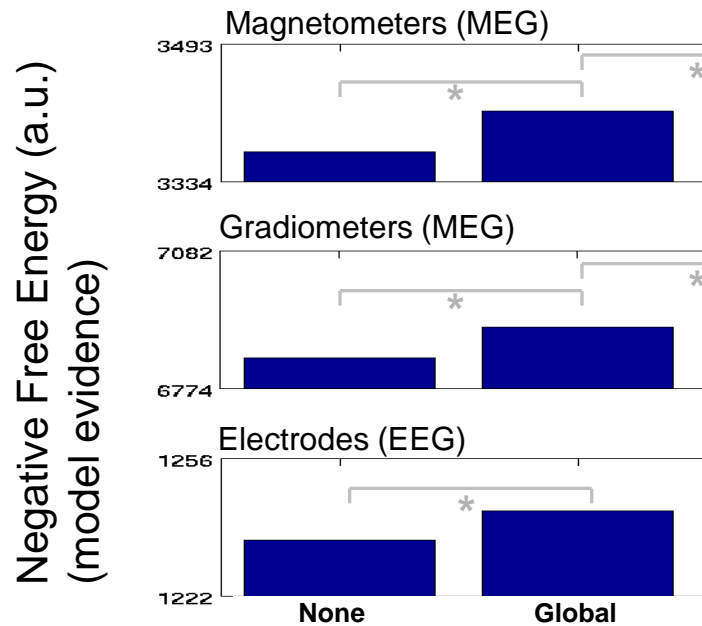


5 clusters from SPM of fMRI data from separate group of (18) subjects in MNI space

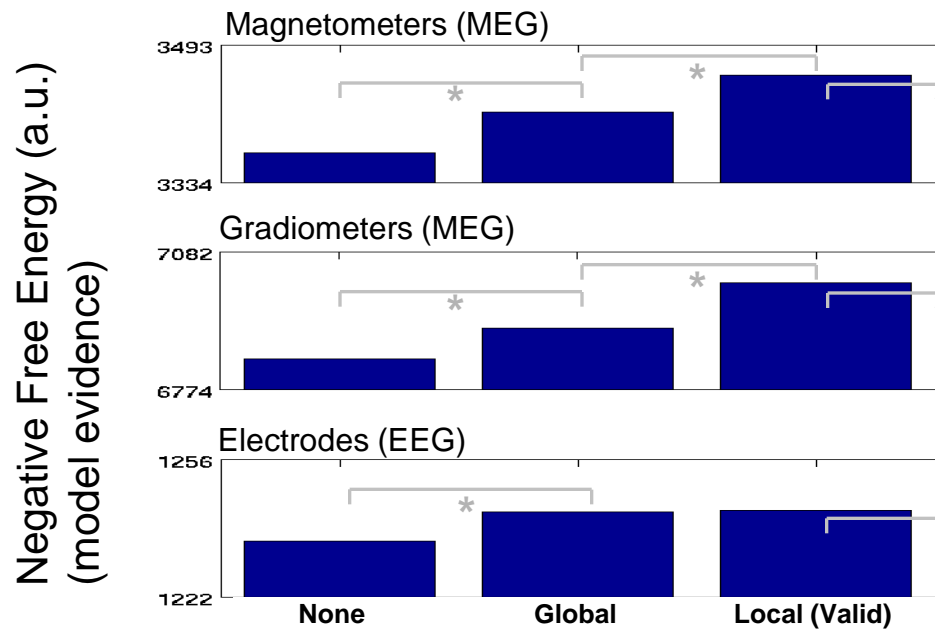
Asymmetric Integration of M/EEG+fMRI



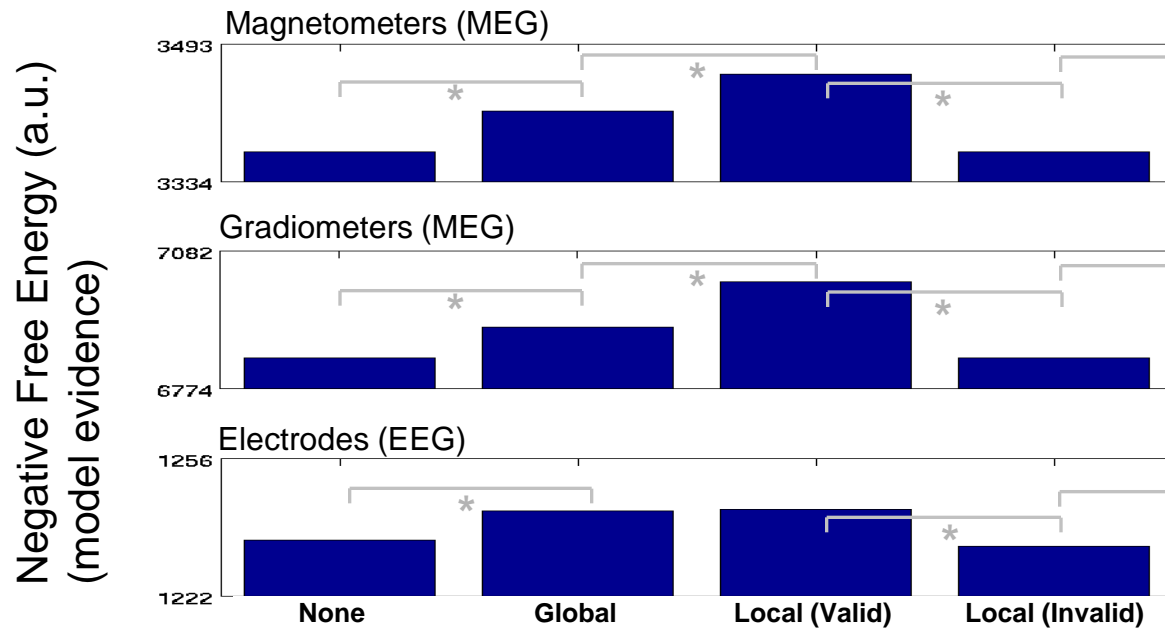
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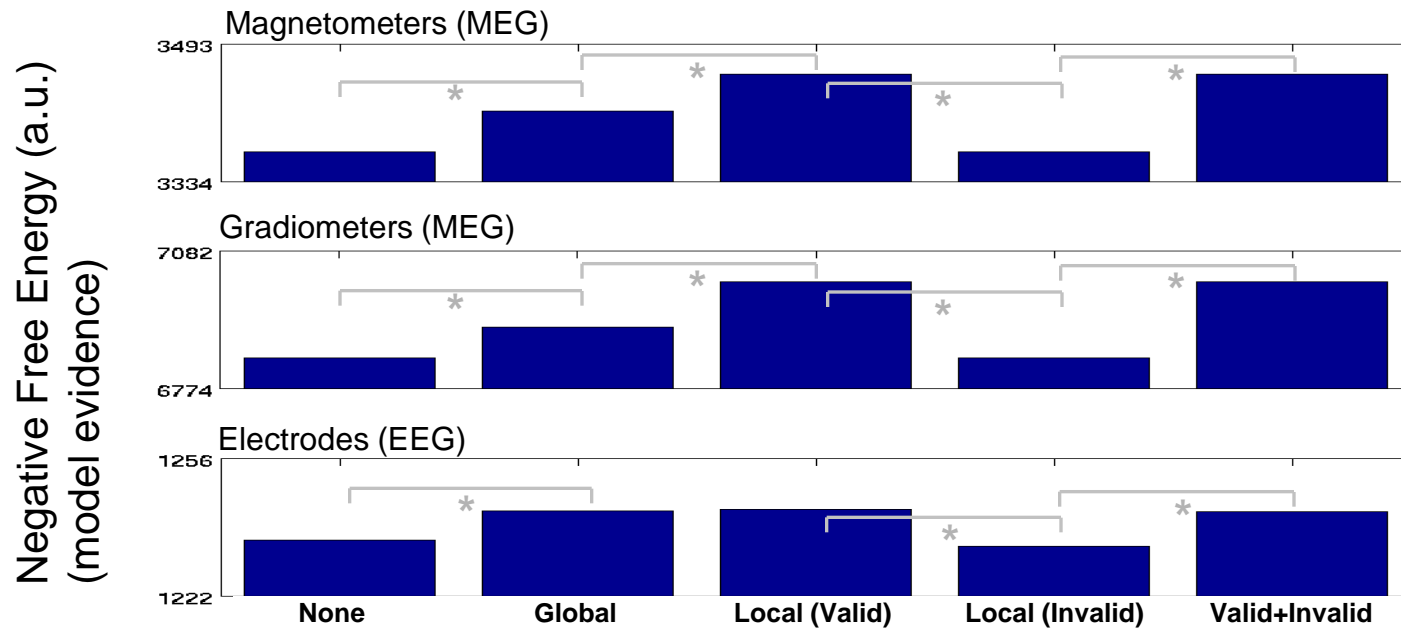
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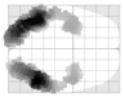
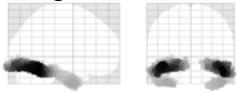
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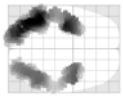
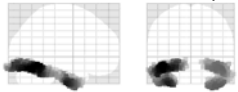
Asymmetric Integration of M/EEG+fMRI

IID sources and IID noise (L2 MNM)

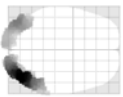
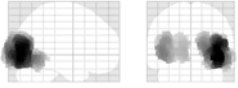
Magnetometers (MEG)



Gradiometers (MEG)



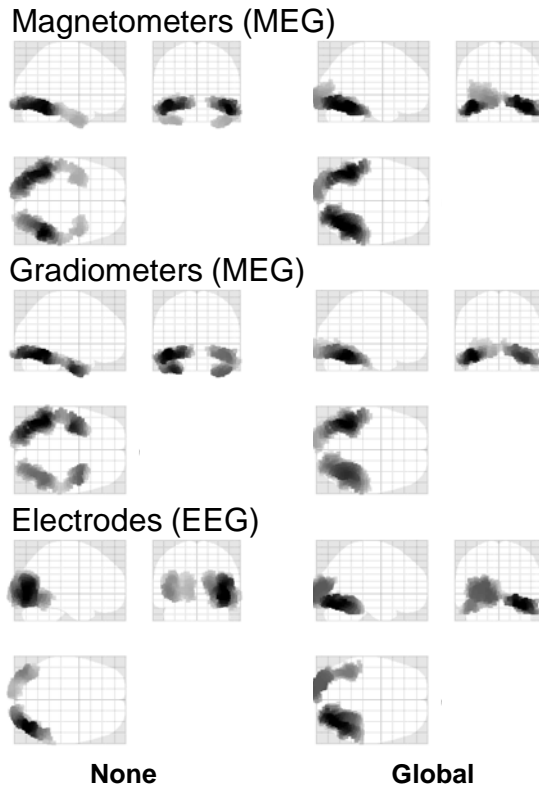
Electrodes (EEG)



None

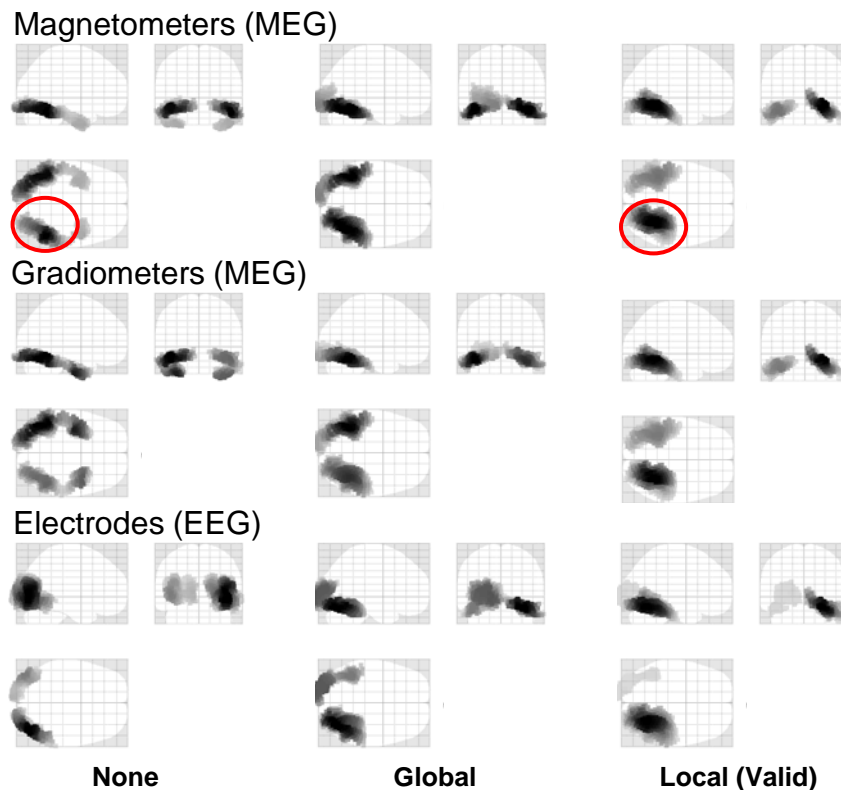
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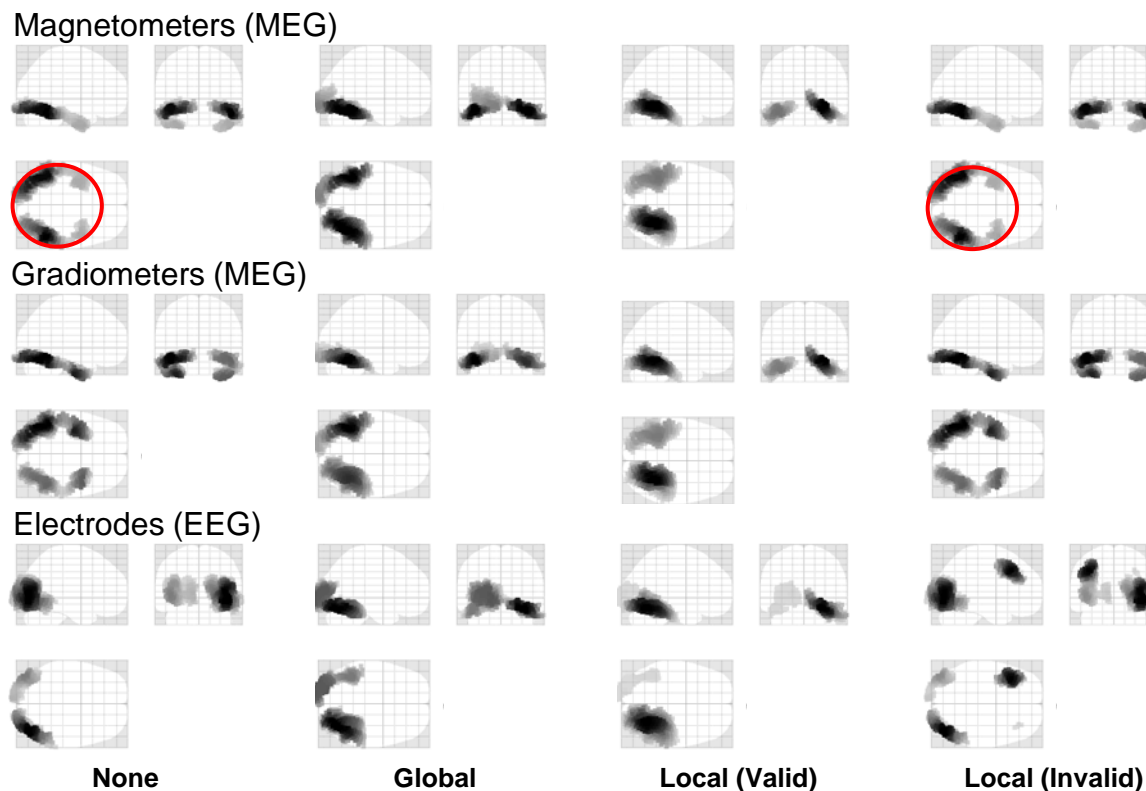
IID sources and IID noise (L2 MNM)



fMRI priors counteract superficial bias of Min Norm

Asymmetric Integration of M/EEG+fMRI

IID sources and IID noise (L2 MNM)



Invalid priors generally discounted (at least for MEG)

- Adding a single, global fMRI prior increases model evidence
- Adding **multiple** valid priors increases model evidence further
- Adding invalid priors does not necessarily increase model evidence, particularly in conjunction with valid priors
Helpful if some fMRI regions produce no MEG/EEG signal (or arise from neural activity at different times)
- Can counteract superficial bias of, e.g, minimum-norm
- Makes some allowance for different sensitivities of fMRI and M/EEG to certain types of neural activity

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Symmetric Integration of MEG+EEG

Background

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Brain Sciences Unit

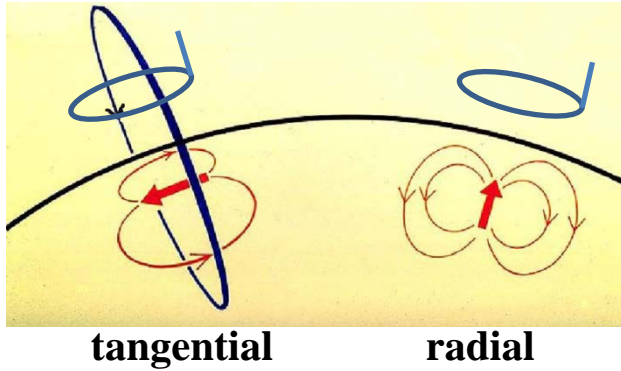
- MEG generally has superior spatial resolution than EEG (less blurred by skull/scalp)
- MEG cannot detect radial component of current sources; EEG can!

Symmetric Integration of MEG+EEG Background

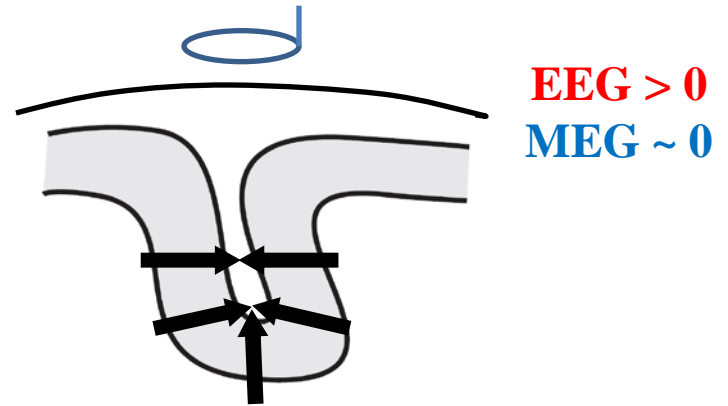
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Dipolar Sources

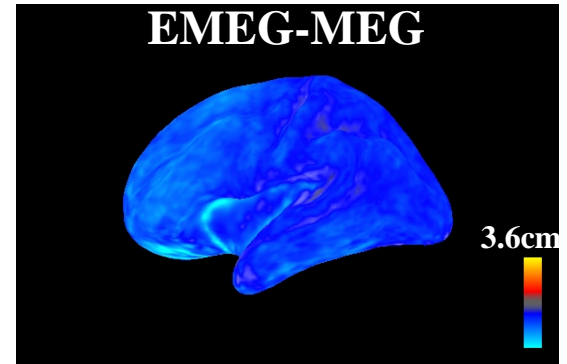
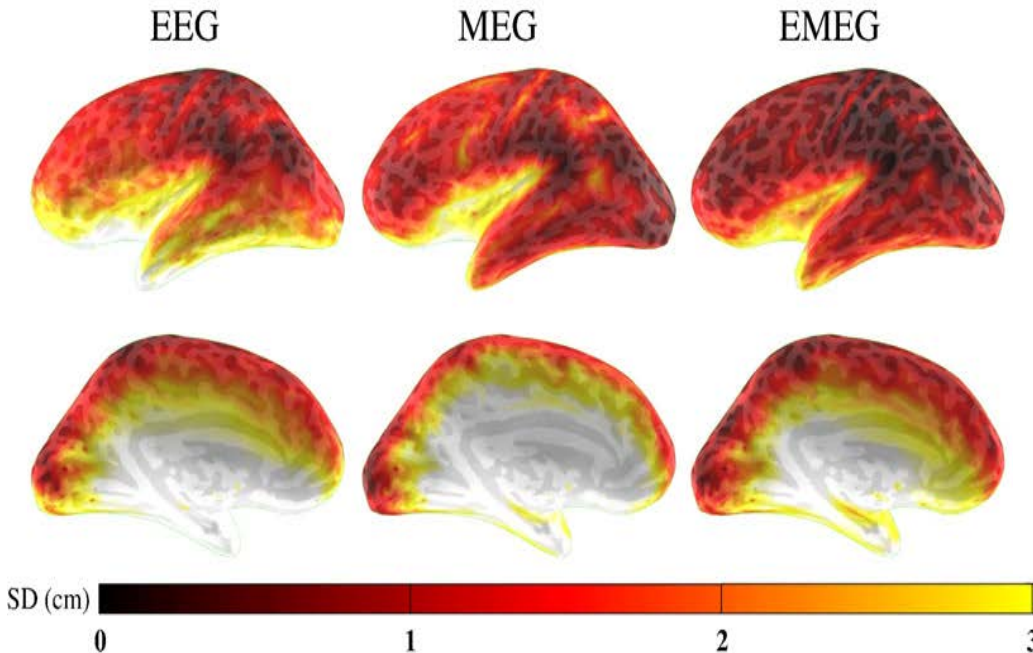


Extended Sources



Ahlfors et al., HBM 2010

Spatial Extent



Stenroos & Hauk, in prep

Symmetric Integration of MEG+EEG

Background

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- MEG generally has superior spatial resolution than EEG (less blurred by skull/scalp)
- MEG cannot detect radial component of current sources; EEG can!
- And few practical problems acquiring concurrent EEG (apart from extra time attaching electrodes)
- ...but EEG data is more sensitive to head geometry and conductivity (potentially biasing any joint-localisation)...
- ...and has different noise characteristics...

Symmetric Integration of MEG+EEG Generative Model

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For fusing MEG and EEG, we can simply concatenate the MEG+EEG data:

$$\begin{bmatrix} \mathbf{d}_{(MEG)} \\ \mathbf{d}_{(EEG)} \end{bmatrix} = \begin{bmatrix} \mathbf{L}_{(MEG)} \\ \mathbf{L}_{(EEG)} \end{bmatrix} \mathbf{s} + \begin{bmatrix} \mathbf{e}_{(MEG)} \\ \mathbf{e}_{(EEG)} \end{bmatrix} \quad \begin{array}{l} \mathbf{e} \sim N(0, \mathbf{C}^{(e)}) \\ \mathbf{s} \sim N(0, \mathbf{C}^{(s)}) \end{array}$$

Noise expressed by MEG and EEG terms (e.g, white noise):

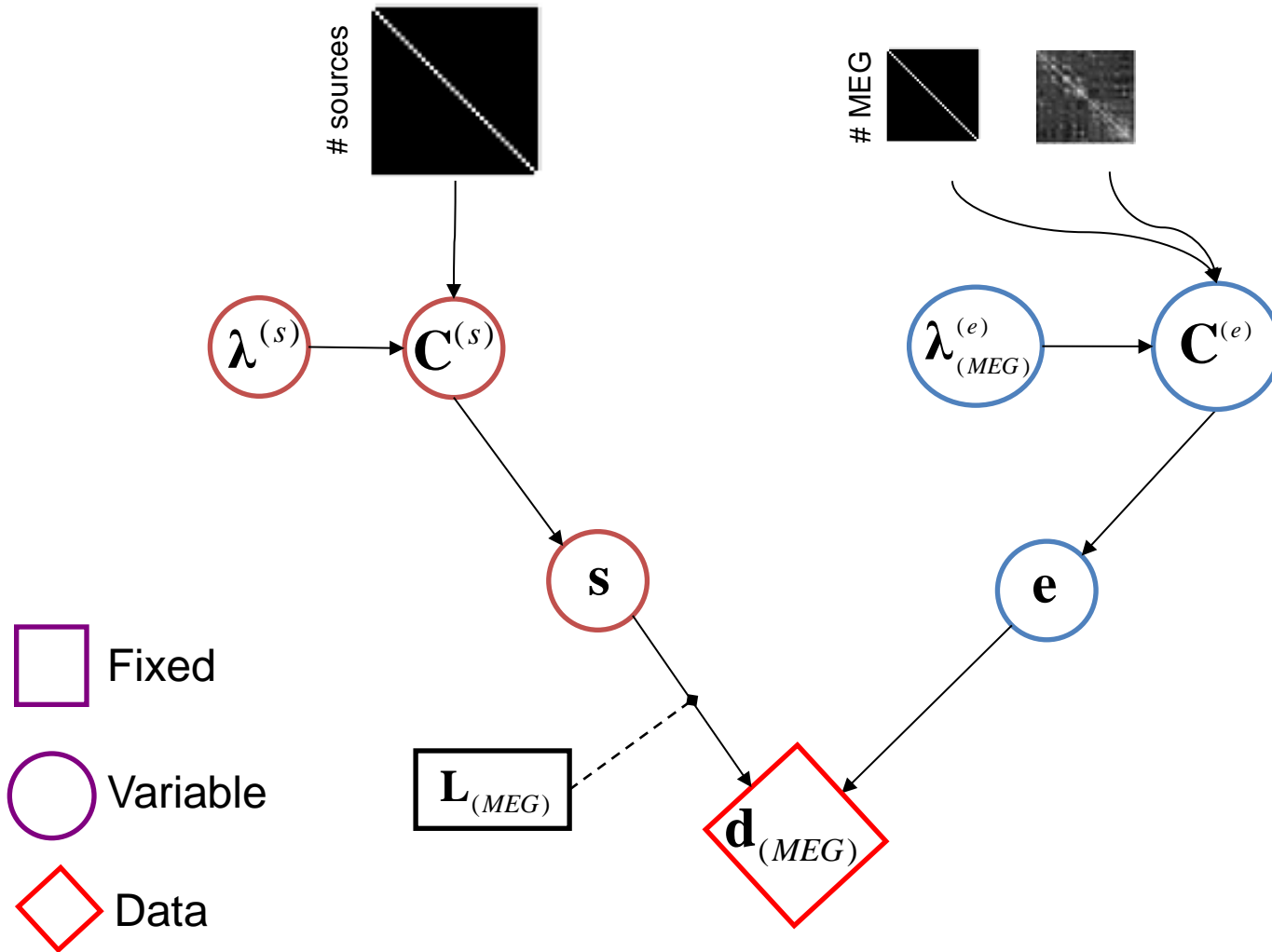
$$\hat{\mathbf{C}}^{(e)} = \lambda_1^{(e)} \mathbf{Q}_{(MEG)}^{(e)} + \lambda_2^{(e)} \mathbf{Q}_{(EEG)}^{(e)} \quad \mathbf{Q}_{(MEG)}^{(e)} = \begin{array}{c} \# \text{ sensors} \\ \begin{array}{|c|} \hline \text{[Diagonal Matrix]} \\ \hline \end{array} \\ \# \text{ sensors} \end{array} \quad \mathbf{Q}_{(EEG)}^{(e)} = \begin{array}{c} \# \text{ sensors} \\ \begin{array}{|c|} \hline \text{[Diagonal Matrix]} \\ \hline \end{array} \\ \# \text{ sensors} \end{array}$$

The separate hyperparameters allow for different noise levels (SNR)

Symmetric Integration of MEG+EEG Generative Model

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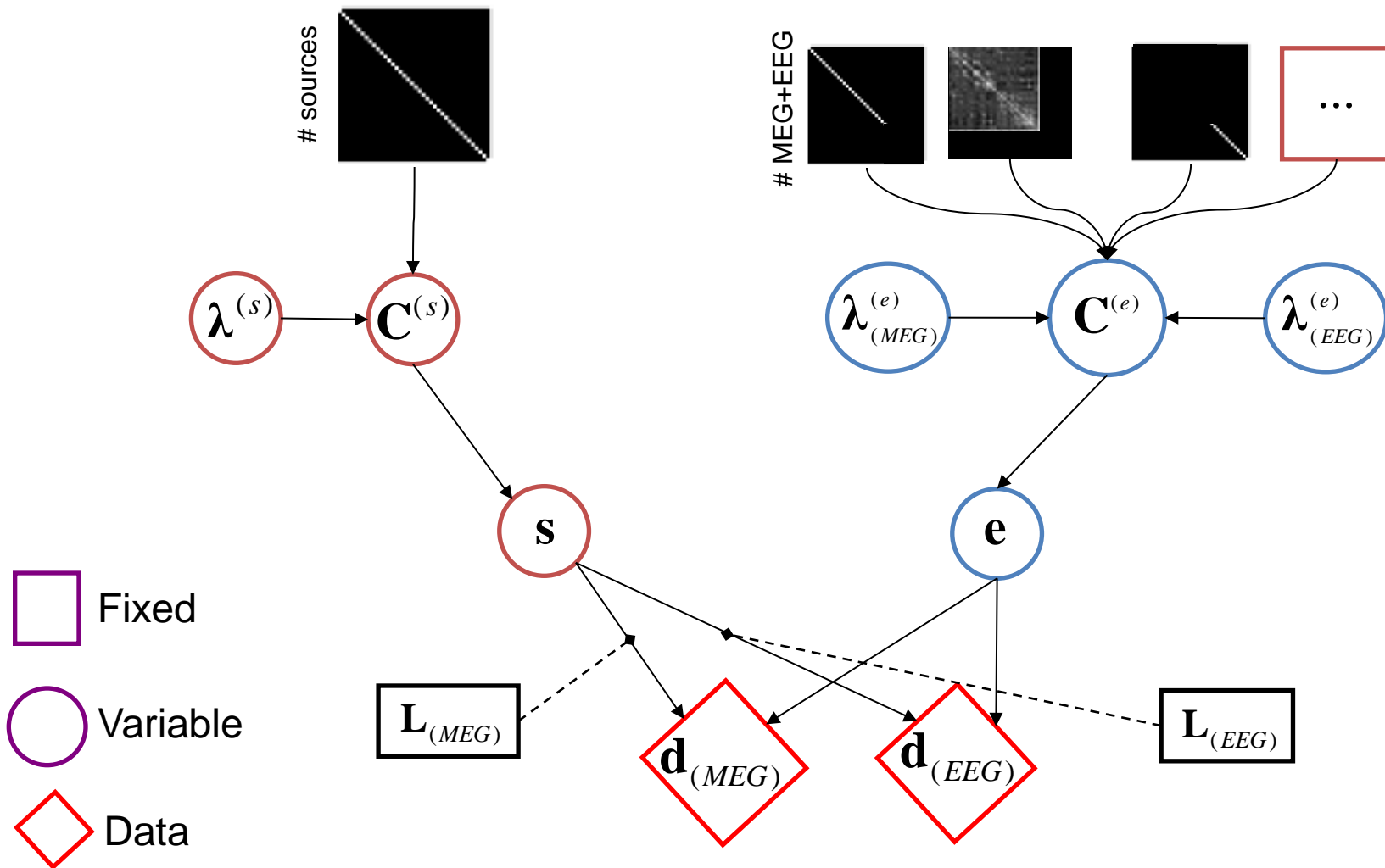
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Symmetric Integration of MEG+EEG Generative Model

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One final problem...

- Though this allows for different additive noise levels in MEG and EEG...
- ...we are assuming mapping from common electrical sources to sensor values (in terms of Tesla and Volts) is known precisely...
- ...whereas in reality, this depends on several unknowns (e.g, precise conductivity of skull/scalp)
- One solution is to scale data/leadfields to have same variance:

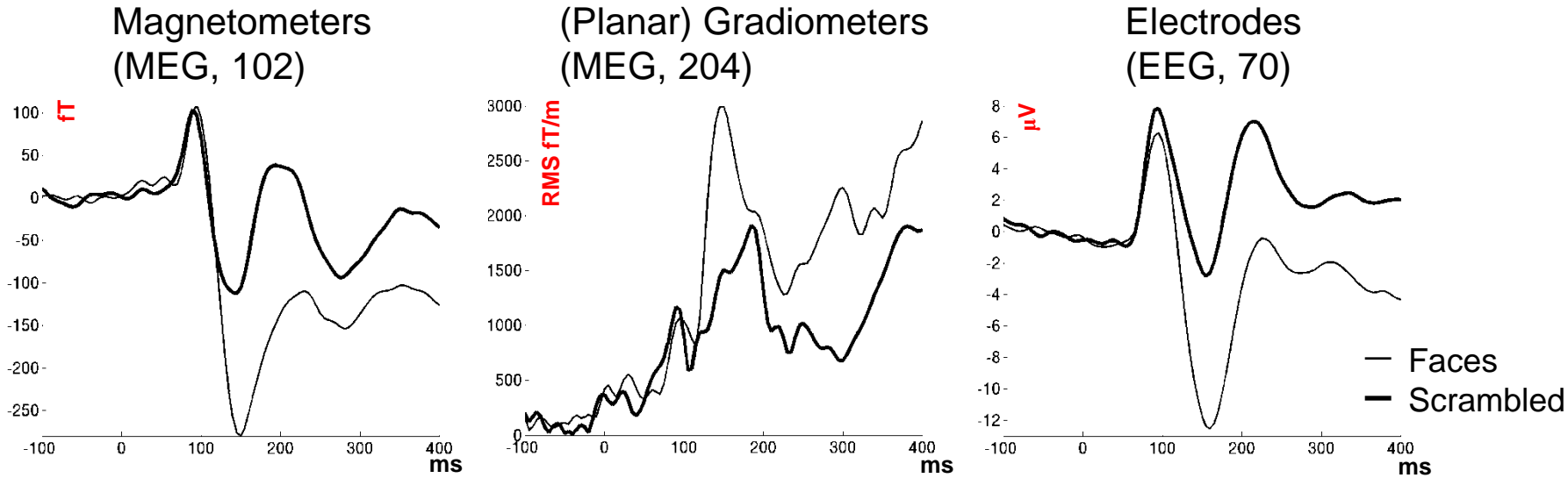
$$\tilde{Y}_i = \frac{Y_i}{\sqrt{\frac{1}{n_i} \text{tr}(Y_i Y_i^T)}}$$

$$\tilde{L}_i = \frac{L_i}{\sqrt{\frac{1}{n_i} \text{tr}(L_i L_i^T)}}$$

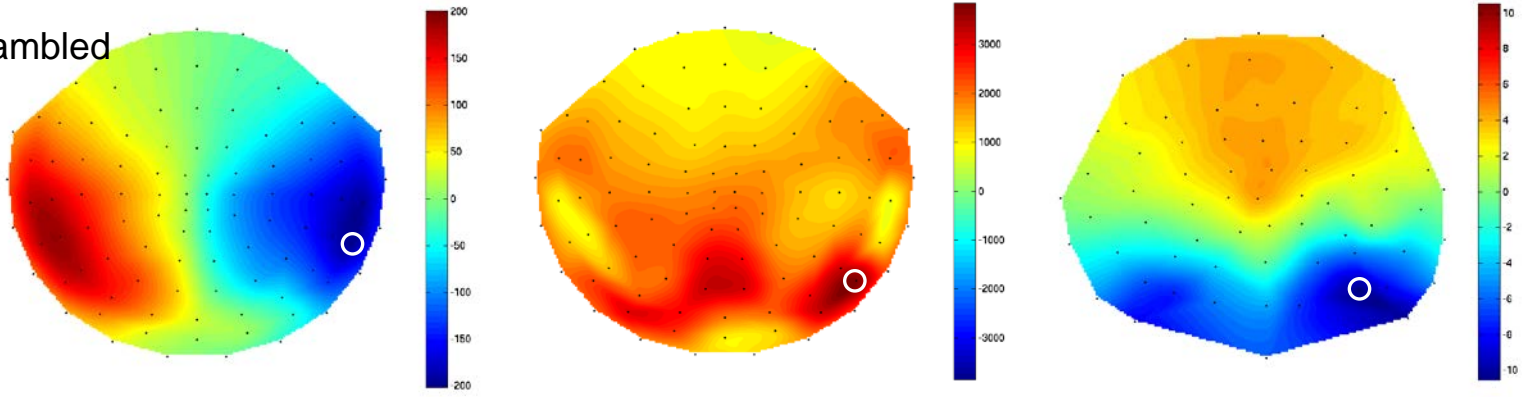
i = i th modality, ie MEG or EEG
 n_i = Number of sensors for modality i

Symmetric Integration of MEG+EEG Example

ERs from 12 subjects for 3 simultaneously-acquired Neuromag sensor-types:



Faces - Scrambled
150-190ms

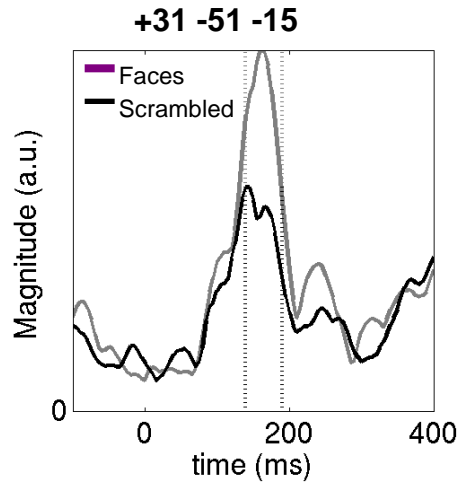
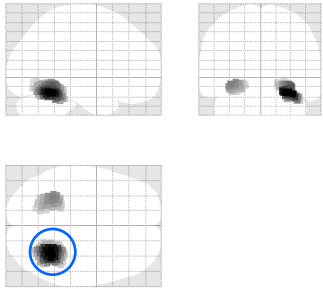


Symmetric Integration of MEG+EEG

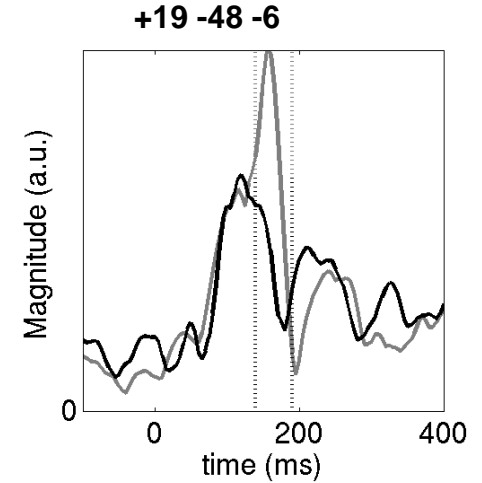
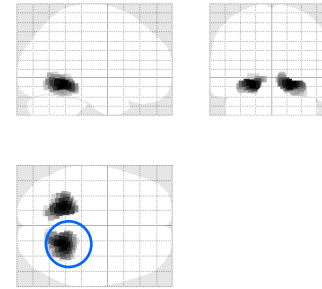
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MEG mags

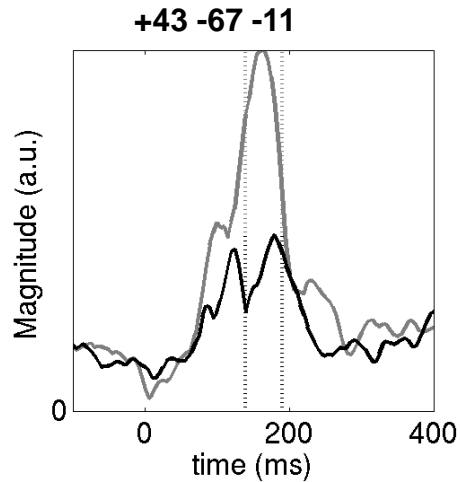
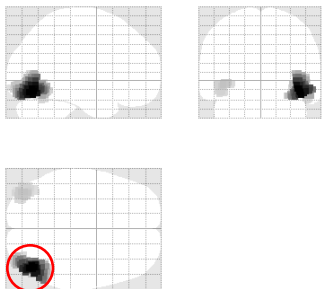


MEG grads

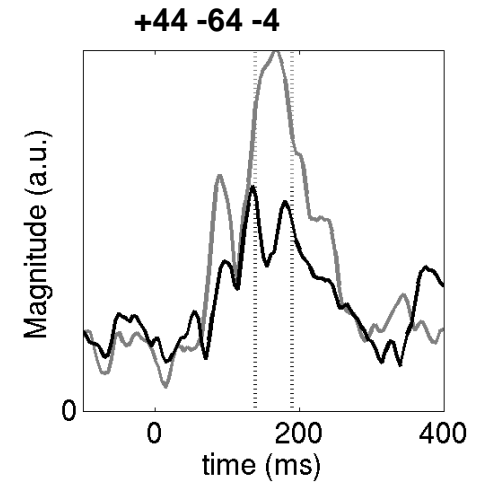
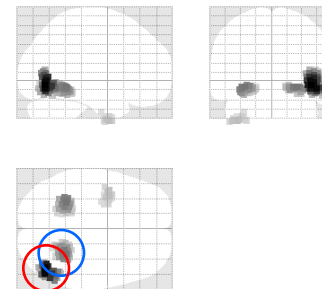


Faces – Scrambled, 150-190ms

EEG



FUSED



- Estimate noise covariance from pre-stimulus baseline (\mathbf{b}):

$$\mathbf{C}^{(e)} = \begin{bmatrix} \text{cov}(\mathbf{b}_{(MEG)}) & \mathbf{0} \\ \mathbf{0} & \text{cov}(\mathbf{b}_{(EEG)}) \end{bmatrix}$$

Molins et al (2008), Neuroimage

(which can also be used to pre-whiten data and leadfields, scaling to noise units)...

...but downside is that **baseline contains source activity**, so not estimate of true sensor noise

- Maximise mutual information between MEG and EEG

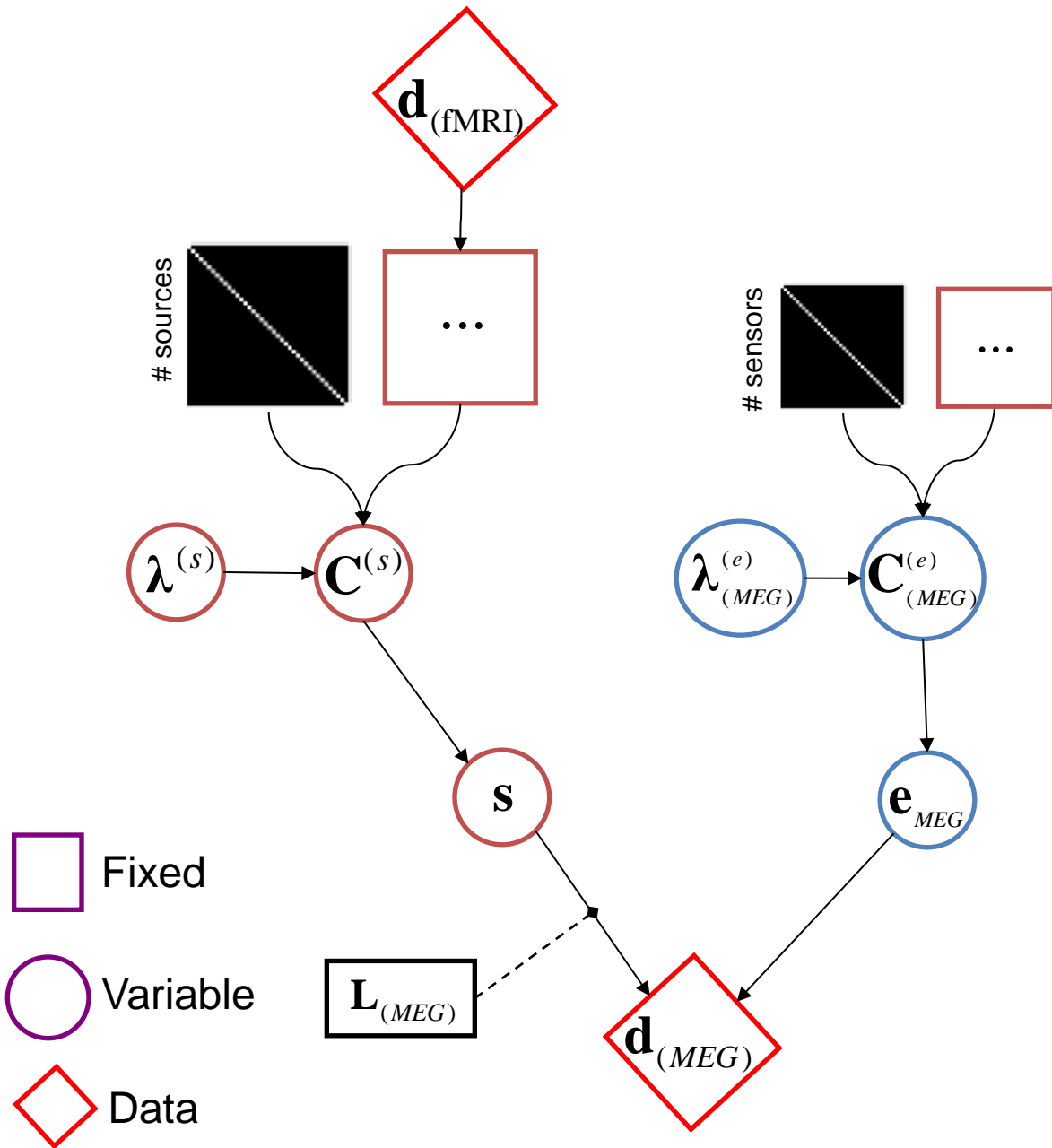
Baillet et al (1999), IEEE

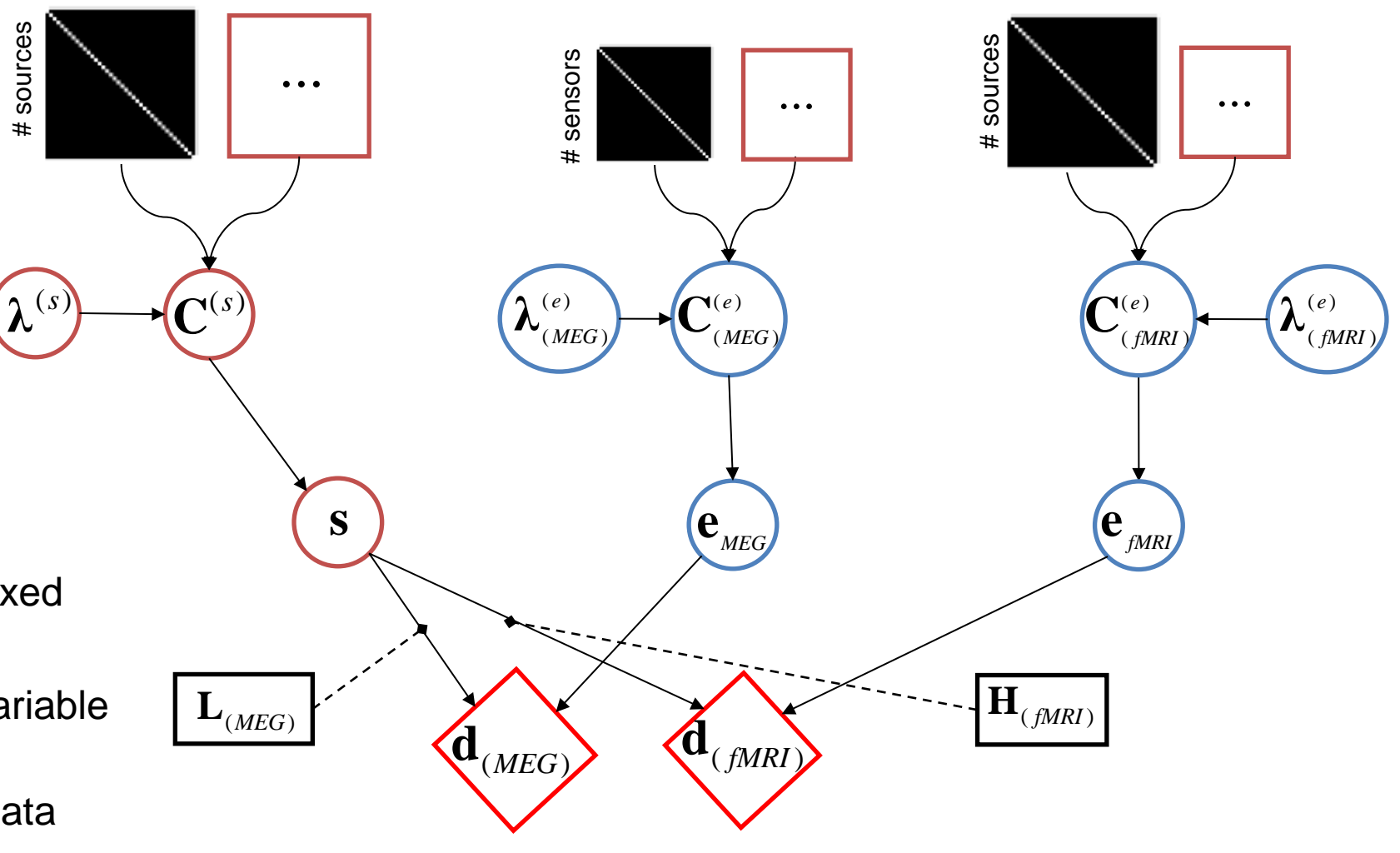
- Re-parameterise leadfields in terms of radial/tangential components

Huang et al (2007), Neuroimage

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)
4. fMRI \leftrightarrow MEG \leftrightarrow EEG fusion?





Data-driven, symmetric approaches:

- Linked Matrix Factorisation methods (ICA, CCA, PLS)
- Representational Similarity Analysis (RSA)
- Graph Theory

Model-driven, asymmetric approaches:

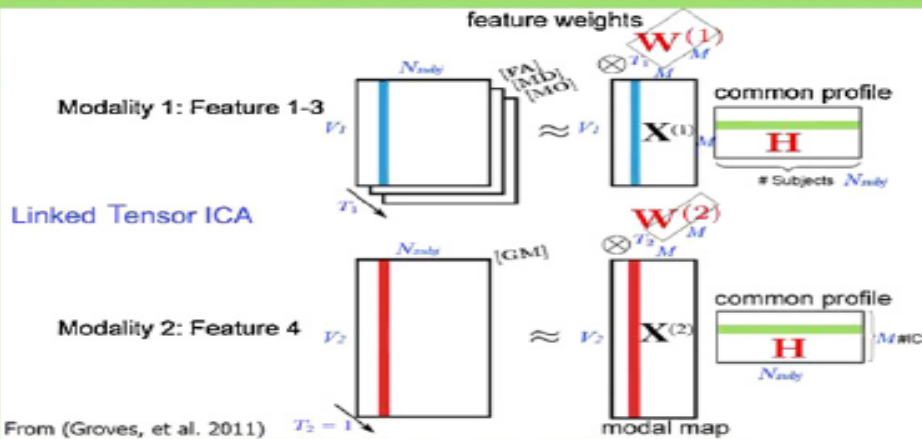
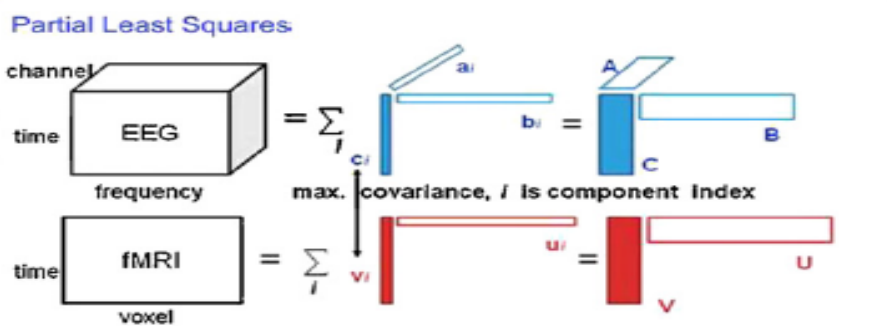
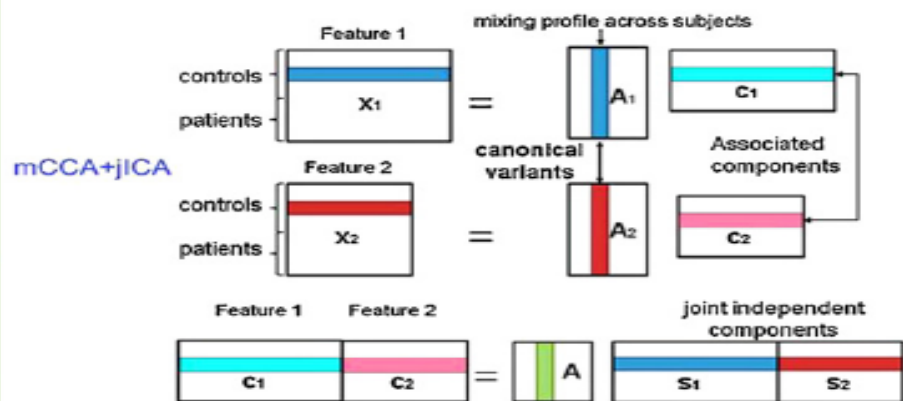
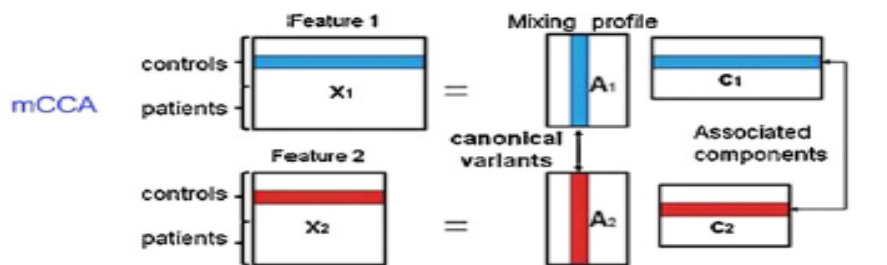
- Regression / Mediation / SEM

Model-driven, symmetric approaches:

- Generative models (eg PEB)

The End

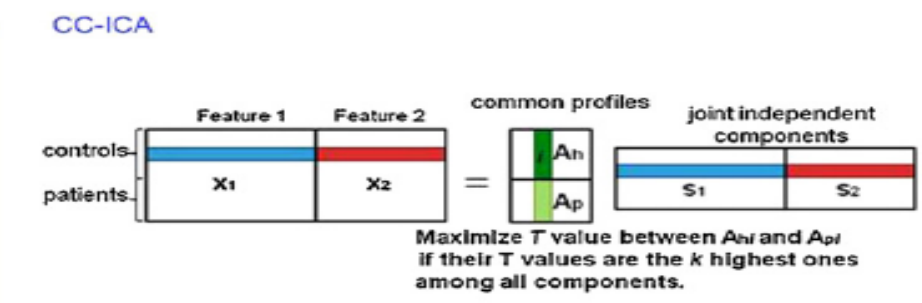
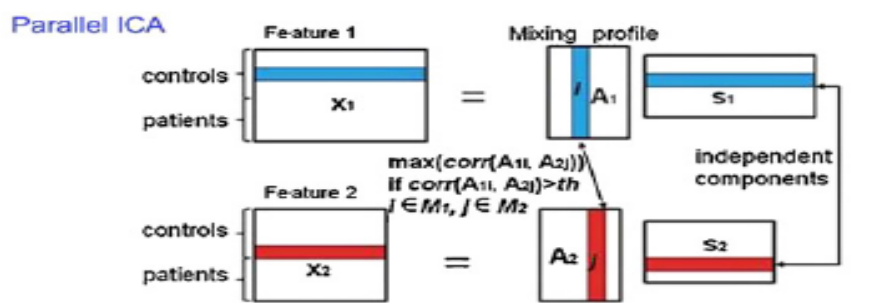
Blind Multivariate Fusion Methods



From (Martinez-Montes, et al. 2004)

From (Groves, et al. 2011)

Semi-Blind Multivariate Fusion Methods



Inverse Problem: Standard **L2**-norm

$$\mathbf{Y} = \mathbf{L}\mathbf{J} + \mathbf{E} \quad \mathbf{E} \sim N(\mathbf{0}, \mathbf{C}^{(e)})$$

$$\mathbf{J} = \arg \min \left\{ \left\| \mathbf{C}^{(e)-1/2} (\mathbf{Y} - \mathbf{L}\mathbf{J}) \right\|^2 + \lambda \left\| \mathbf{W}\mathbf{J} \right\|^2 \right\}$$

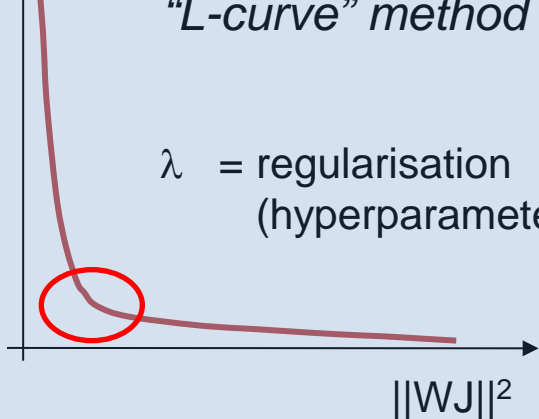
$$= (\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T [\mathbf{L} (\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T + \lambda \mathbf{C}^{(e)}]^{-1} \mathbf{Y}$$

“Tikhonov Solution”

$\|\mathbf{Y} - \mathbf{L}\mathbf{J}\|^2$

“L-curve” method

λ = regularisation
(hyperparameter)



$$\mathbf{W} = \mathbf{I}$$

“Minimum Norm”

$$\mathbf{W} = \mathbf{D}\mathbf{D}^T$$

“Loreta” (\mathbf{D} =Laplacian)

$$\mathbf{W} = \text{diag}(\mathbf{L}^T \mathbf{L})^{-1}$$

“Depth-Weighted”

$$\mathbf{W}_p = \text{diag}(\mathbf{L}_p^T \mathbf{C}_y^{-1} \mathbf{L}_p)^{-1}$$

“Beamformer”

$$\mathbf{W} = \dots$$

Inverse Problem: Equivalent PEB

Parametric Empirical Bayesian (PEB) 2-level hierarchical form:

$$\mathbf{Y} = \mathbf{L}\mathbf{J} + \mathbf{E}^{(e)} \quad \mathbf{E}^{(e)} \sim N(0, \mathbf{C}^{(e)})$$

$$\mathbf{J} = 0 + \mathbf{E}^{(j)} \quad \mathbf{E}^{(j)} \sim N(0, \mathbf{C}^{(j)})$$

$\mathbf{C}^{(e)} = n \times n$ Sensor (error) covariance

$\mathbf{C}^{(j)} = p \times p$ Source (prior) covariance

Likelihood:

$$p(\mathbf{Y} | \mathbf{J}) = N(\mathbf{L}\mathbf{J}, \mathbf{C}^{(e)})$$

Prior:

$$p(\mathbf{J}) = N(0, \mathbf{C}^{(j)})$$

Posterior:

$$p(\mathbf{J} | \mathbf{Y}) \propto p(\mathbf{Y} | \mathbf{J})p(\mathbf{J})$$

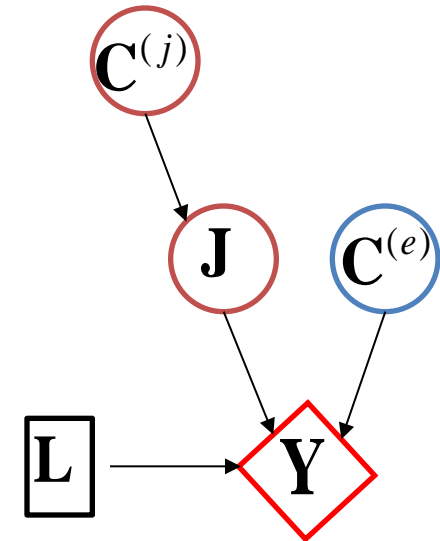
Maximum A Posteriori (MAP) estimate:

$$\hat{\mathbf{J}} = \mathbf{C}^{(j)}\mathbf{L}^T [\mathbf{L}\mathbf{C}^{(j)}\mathbf{L}^T + \mathbf{C}^{(e)}]^{-1}\mathbf{Y}$$

cf Classical Tikhonov:

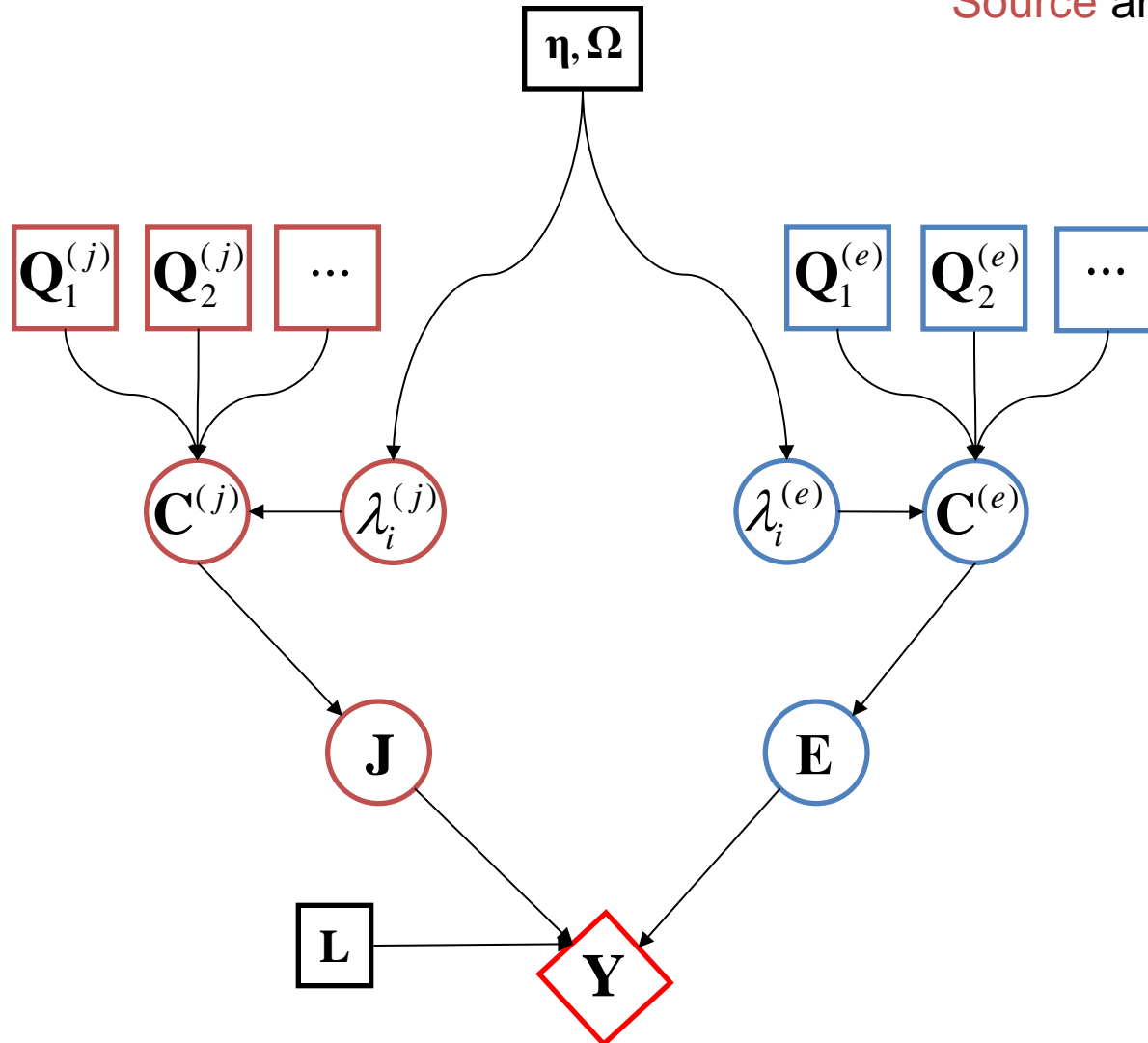
$$(\mathbf{W}^T\mathbf{W})^{-1}\mathbf{L}^T [\mathbf{L}(\mathbf{W}^T\mathbf{W})^{-1}\mathbf{L}^T + \lambda\mathbf{C}^{(e)}]^{-1}\mathbf{Y}$$

$$\Rightarrow \mathbf{C}^{(j)} = (\mathbf{W}^T\mathbf{W})^{-1}$$



PEB: Full Generative Model (DAG)

Source and sensor space



1. Obtain Restricted Maximum Likelihood (ReML) estimates of the hyperparameters (λ) by maximising the variational “free energy” (F):

$$\hat{\lambda} = \max_{\lambda} p(\mathbf{Y} | \lambda) = \max_{\lambda} F$$

2. Obtain Maximum A Posteriori (MAP) estimates of parameters (sources, \mathbf{J}):

$$\hat{\mathbf{J}} = \max_{\mathbf{J}} p(\mathbf{J} | \mathbf{Y}, \hat{\lambda}) = \max_{\mathbf{J}} F$$

3. Maximal F approximates Bayesian (log) “model evidence” for a model, m :

$$\ln p(\mathbf{Y} | m) = \ln \int \int p(\mathbf{Y}, \mathbf{J}, \lambda | m) d\mathbf{J} d\lambda \approx F(\mathbf{Y}, \hat{\mathbf{a}}, \hat{\Sigma}) \quad m = \{\mathbf{L}, \mathbf{Q}, \boldsymbol{\eta}, \boldsymbol{\Omega}\}$$

$$F(\mathbf{Y}, \hat{\mathbf{a}}, \hat{\Sigma}) \propto \underbrace{-\text{tr}(\mathbf{C}^{-1} \mathbf{Y} \mathbf{Y}^T) - \ln |\mathbf{C}|}_{\text{Accuracy}} \underbrace{- (\hat{\mathbf{a}} - \boldsymbol{\eta})^T \boldsymbol{\Omega}^{-1} (\hat{\mathbf{a}} - \boldsymbol{\eta}) + \ln |\hat{\Sigma} \boldsymbol{\Omega}^{-1}|}_{\text{Complexity}}$$

Accuracy

Complexity

(...where $\hat{\mathbf{a}}$ and $\hat{\Sigma}$ are the posterior mean and covariance of hyperparameters)

PEB: Multiple Sparse Priors

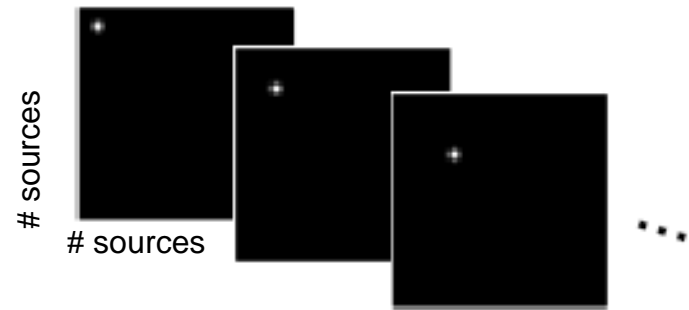
Hyperpriors allow the extreme of 100's source priors, or MSP

Three prior models

MNM $Q^\epsilon = I$

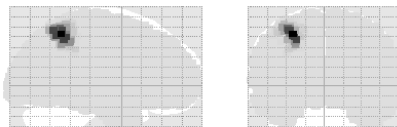
COH $Q^\epsilon = \{G, I\}$

MSP $Q^\epsilon = \{q_1 q_1^T, \dots, q_N q_N^T\}$

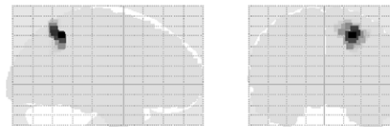


$$G(\sigma) = [q_1, \dots, q_N] = \sum_{i=0}^8 \frac{\sigma^i}{i!} A^i \approx \exp(\sigma A)$$

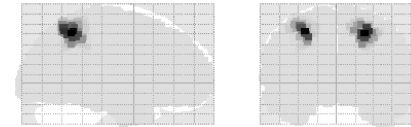
Left patch



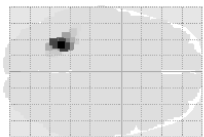
Right patch



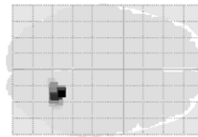
Bilateral patches



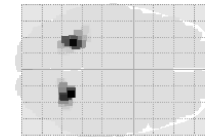
...



...



...



...

PEB: Multiple Sparse Priors

Hyperpriors allow the extreme of 100's source priors, or MSP

Three prior models

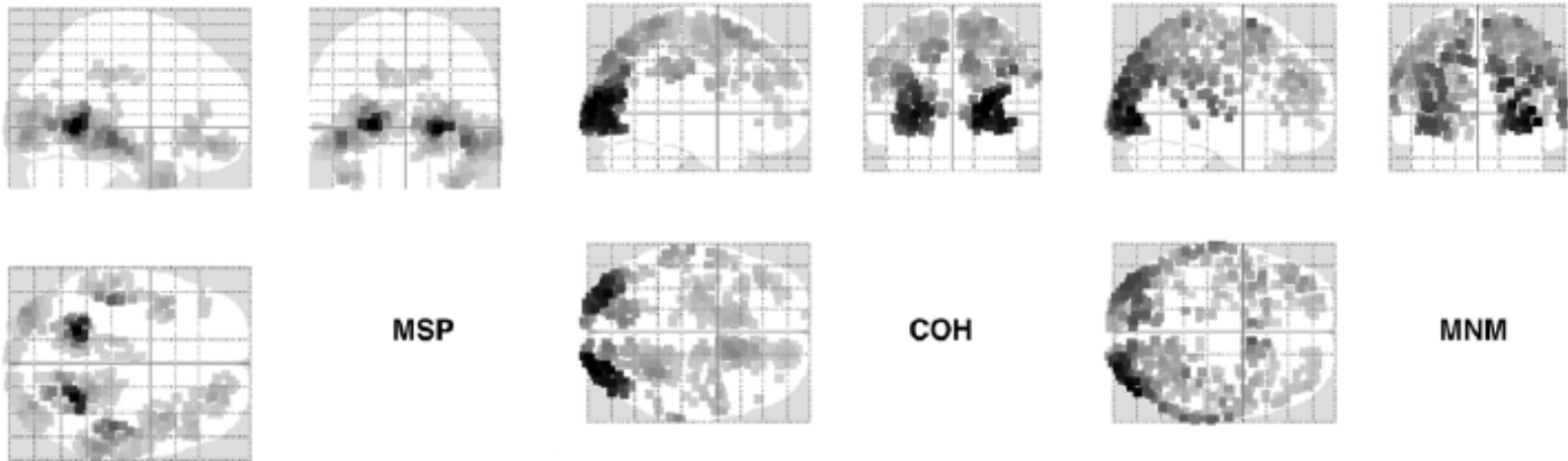
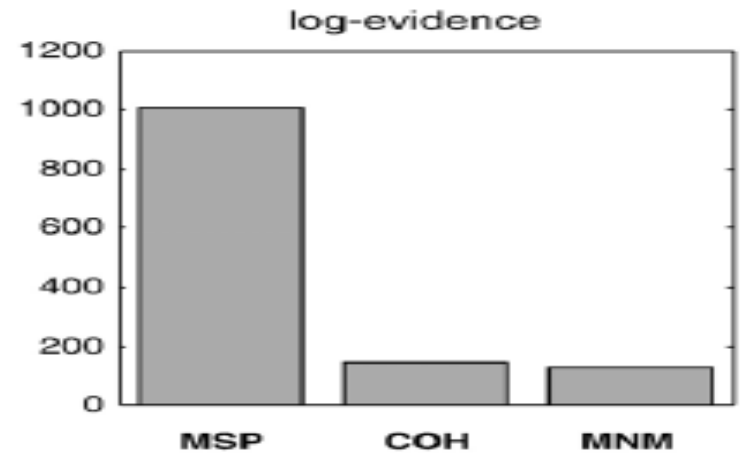
MNM $Q^\epsilon = I$

COH $Q^\epsilon = \{G, I\}$

MSP $Q^\epsilon = \{q_1 q_1^T, \dots, q_N q_N^T\}$



$$G(\sigma) = [q_1, \dots, q_N] = \sum_{i=0}^8 \frac{\sigma^i}{i!} A^i \approx \exp(\sigma A)$$



Summary:

- **Automatically** “regularises” in principled fashion...
- ...allows for **multiple** constraints (priors)...
- ...to the extent that multiple (100’s) of sparse priors possible (MSP)...
- ...(or multiple error components or multiple fMRI priors)...
- ...furnishes estimates of **model evidence**, so can compare constraints

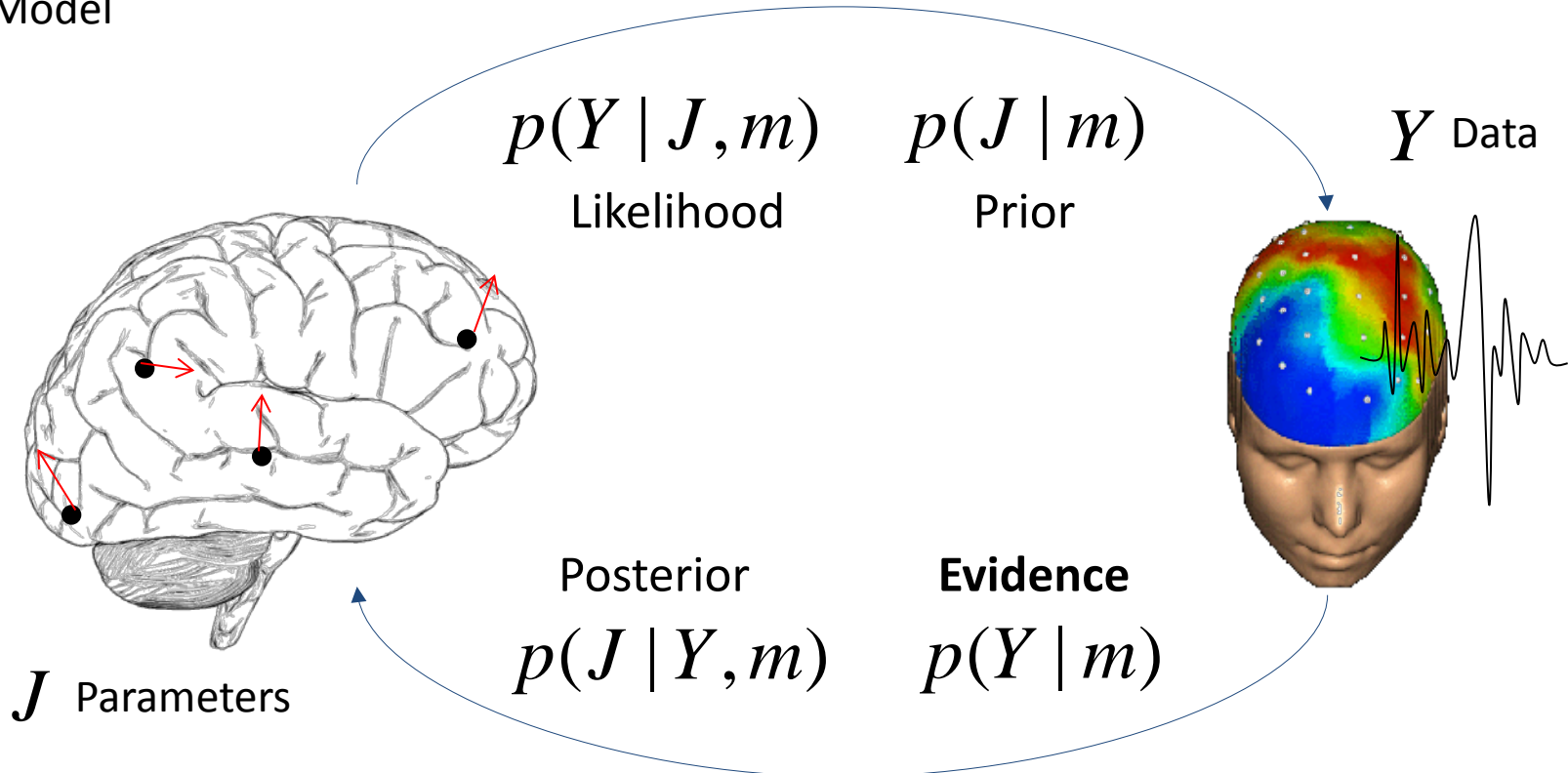
Bayesian Perspective

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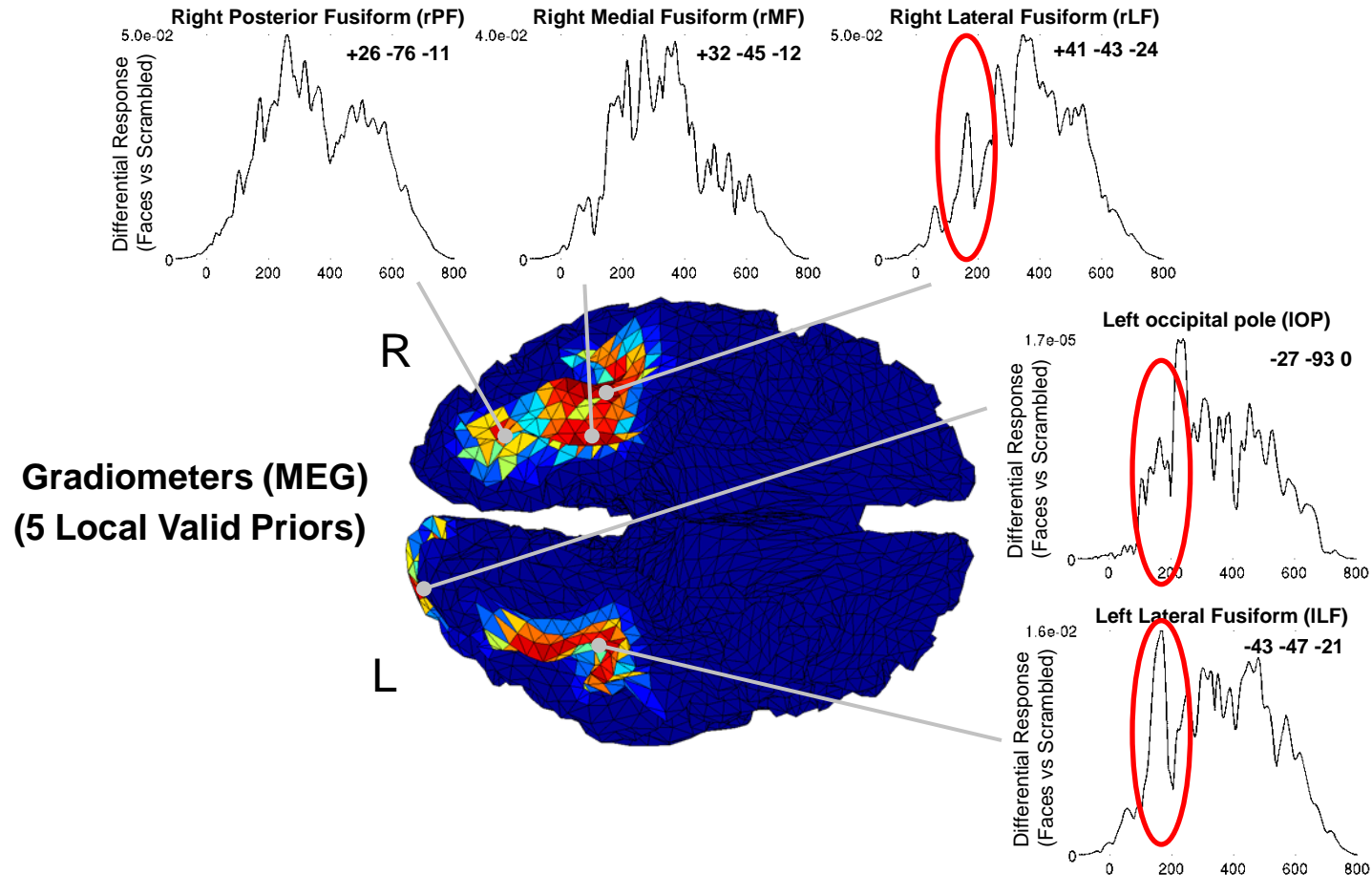
Forward Problem

m Model



Inverse Problem

Asymmetric Integration of M/EEG+fMRI



NB: Priors affect variance, not precise timecourse...