

Multi-modal integration

Rik Henson

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Data-driven vs Model-driven

1. Data-driven in sense that no model that links specific features of one modality with features of another (still employ some form of statistical model), eg ICA, CCA

2. Model-driven in sense that either:
 - 2.1 tests feature relations across modalities, eg SEM

 - 2.2 has a generative model of both modalities, eg PEB

Symmetric vs Asymmetric

1. Symmetric integration (“fusion”) fits each modality simultaneously
2. Asymmetric integration uses one modality to model another modality

(Most data-driven approaches are symmetric; many, but not all, model-driven approaches are asymmetric)

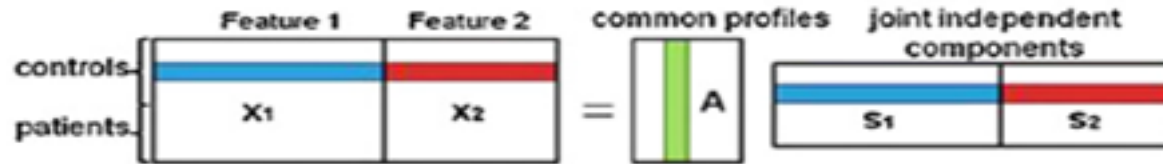
Some Data-Driven Methods

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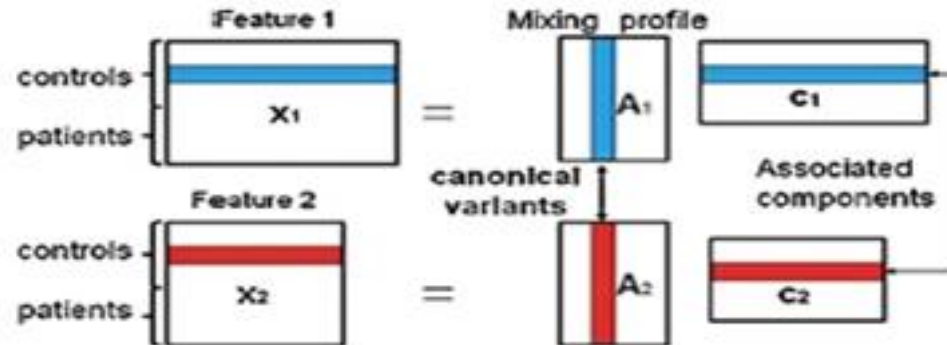
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1. Linked Matrix Factorisation methods (ICA, CCA, PLS)
2. Representational Similarity Analysis (RSA)
3. Graph Theory

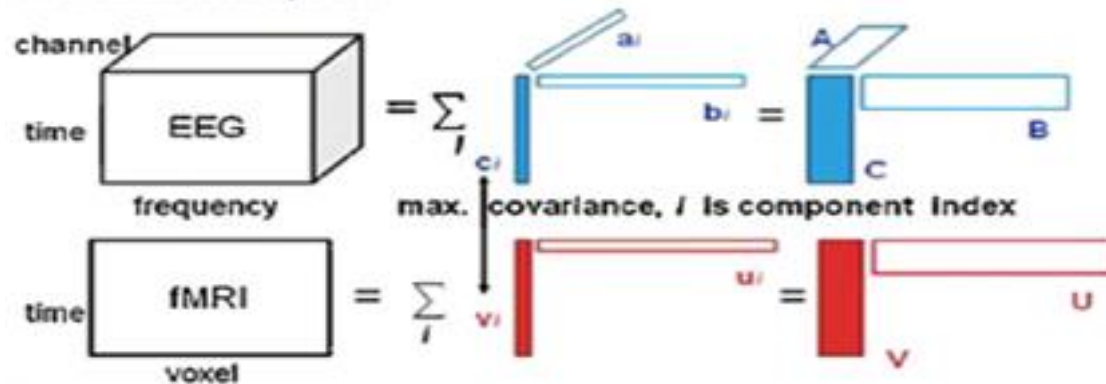
Joint ICA



mCCA

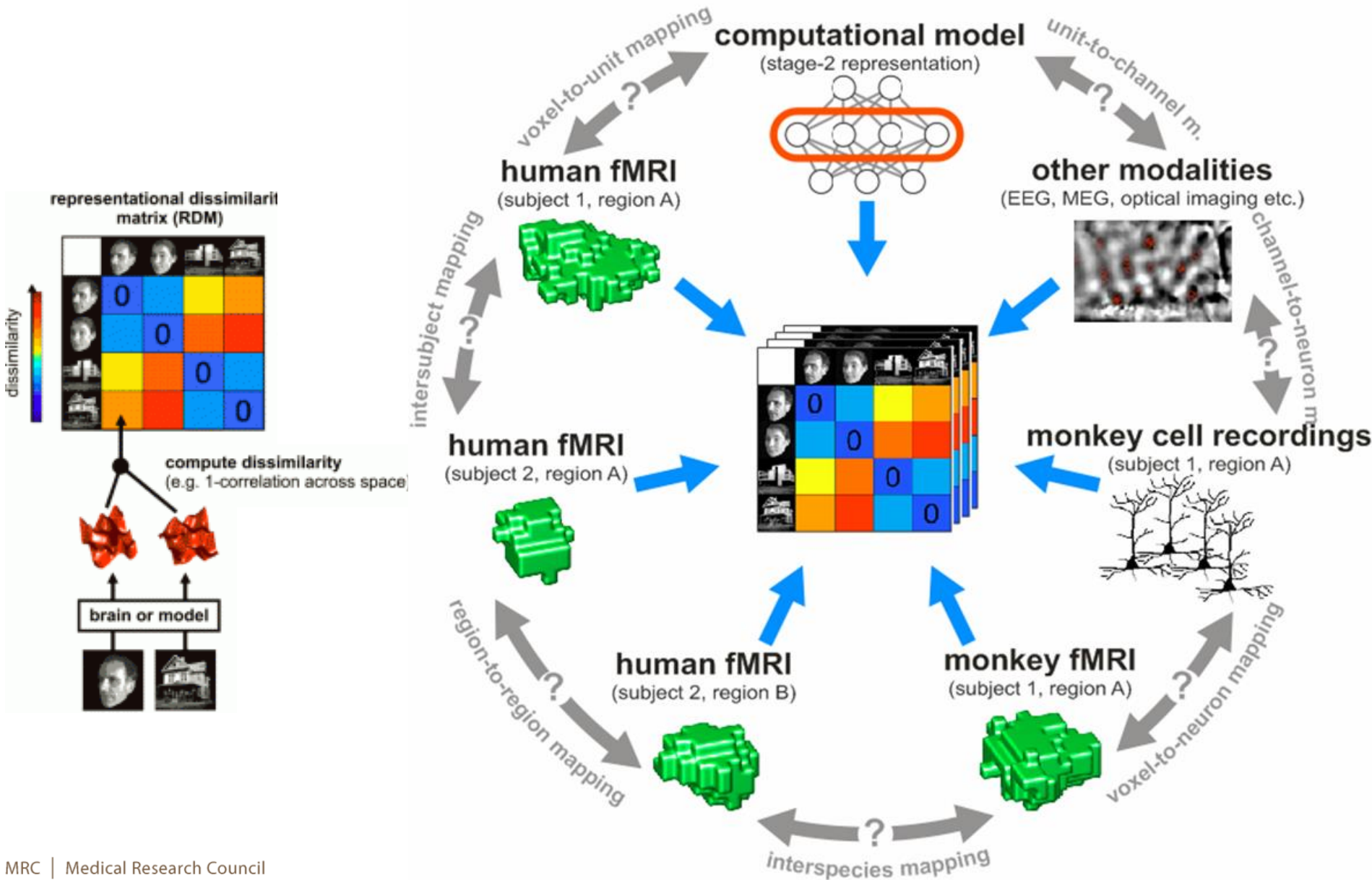


Partial Least Squares



Some Data-Driven Methods

1. Linked Matrix Factorisation methods (ICA, PLS, CCA)
2. **Representational Similarity Analysis (RSA)**
3. Graph Theory

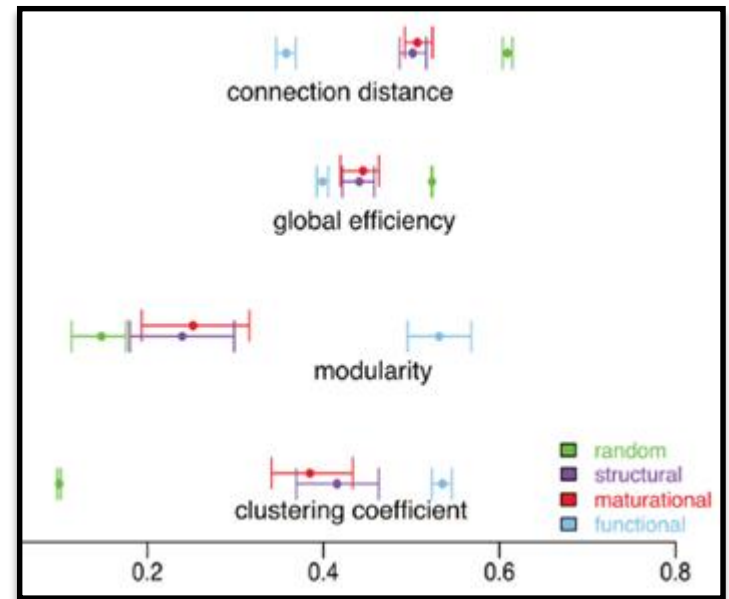
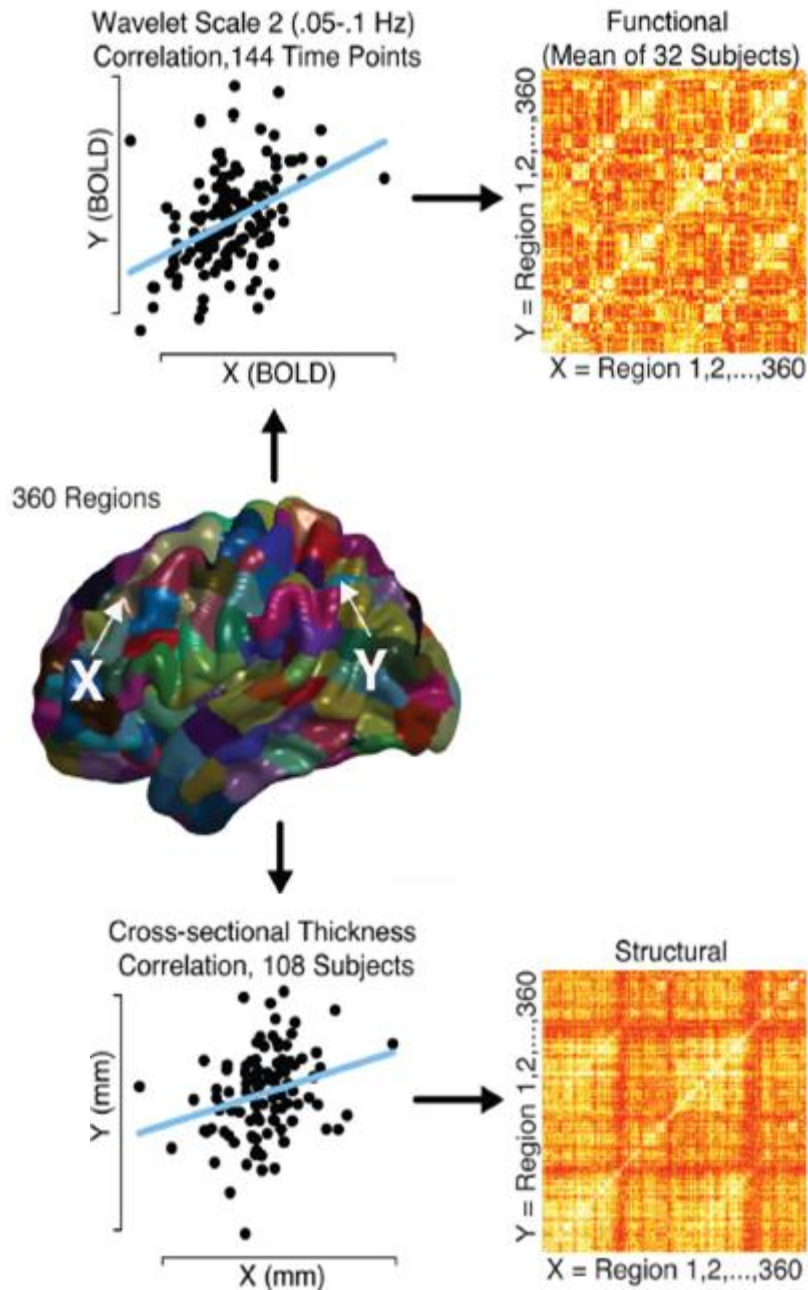


Some Data-Driven Methods

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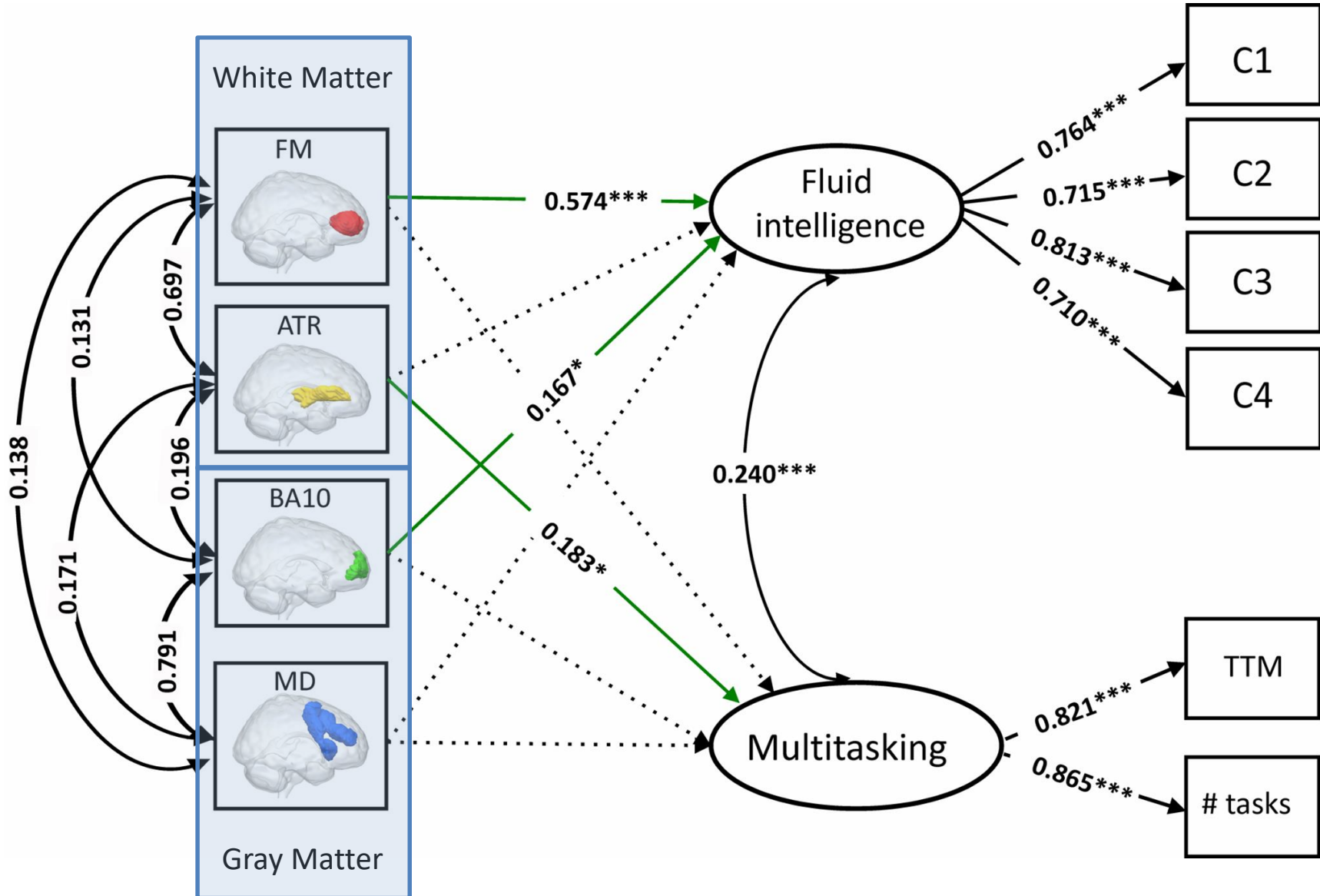
1. Linked Matrix Factorisation methods (ICA, PLS, CCA)
2. Representational Similarity Analysis (RSA)
3. Graph Theory



...or can even compare graphs with different nodes, eg fMRI ROIs and MEEG sensors...

Data-driven vs Model-driven

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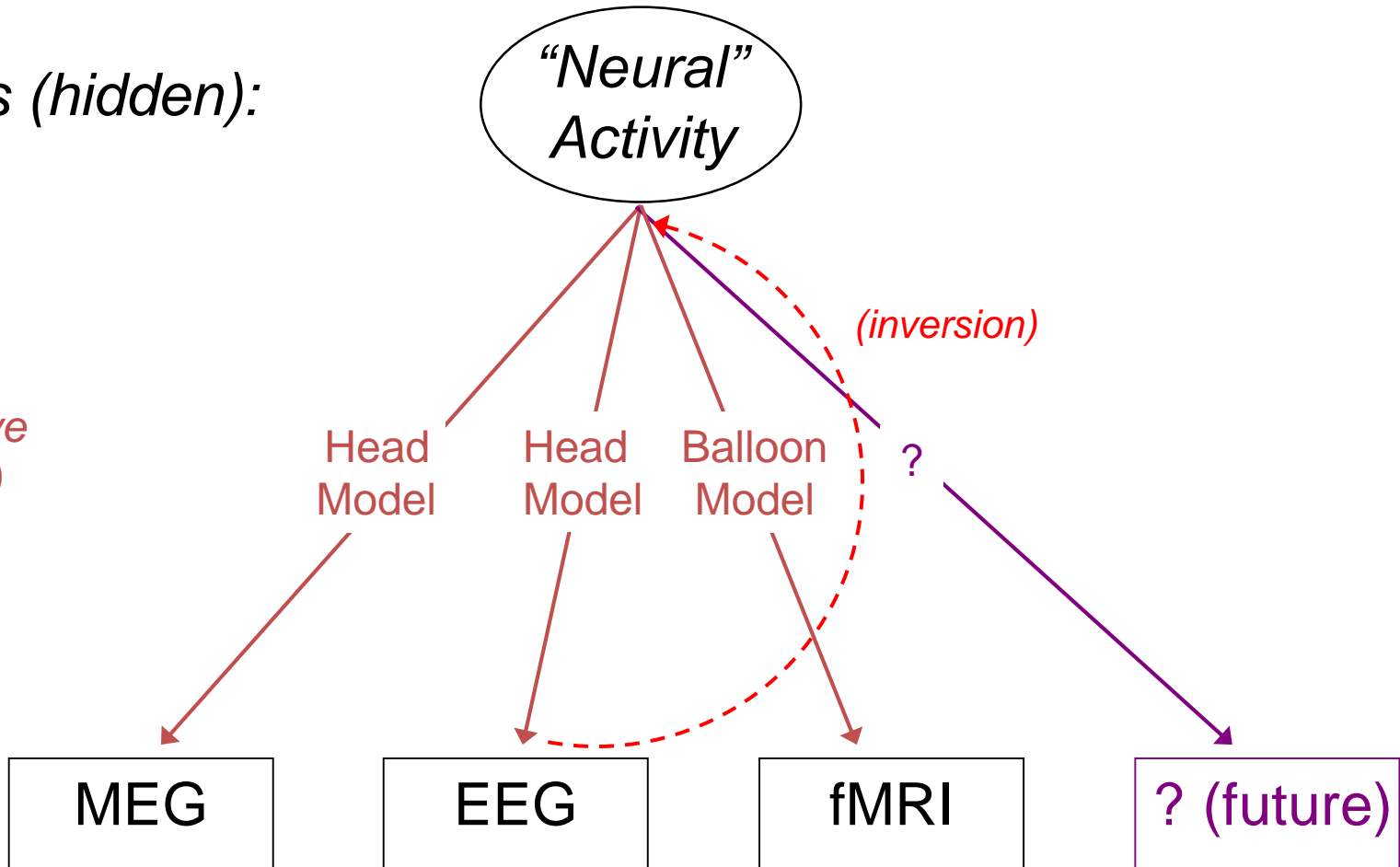
Multi-modal integration of MEG, EEG & fMRI

Multi-modal Integration

Causes (hidden):

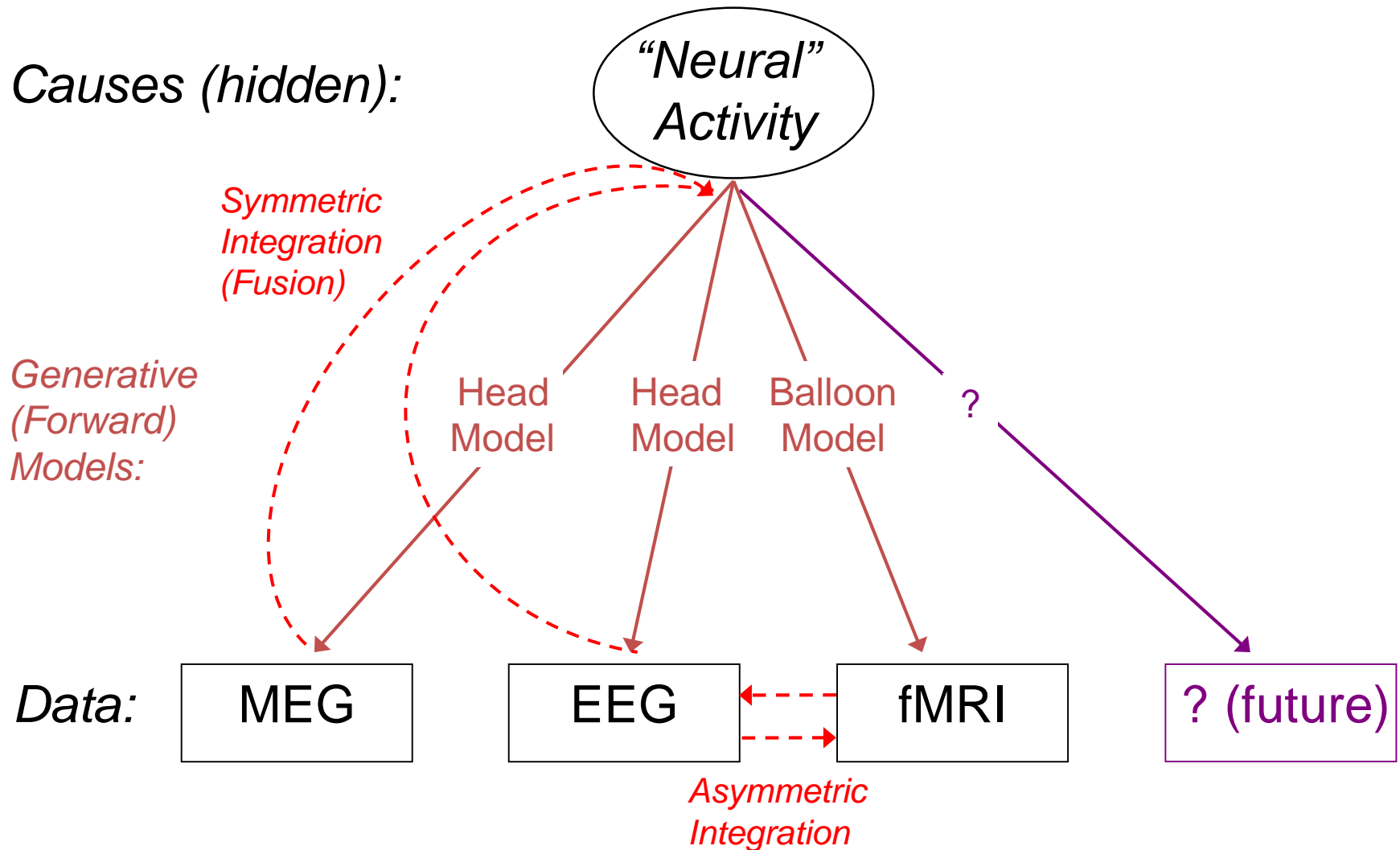
*Generative
(Forward)
Models:*

Data:



Multi-modal Integration

Causes (hidden):



Examples

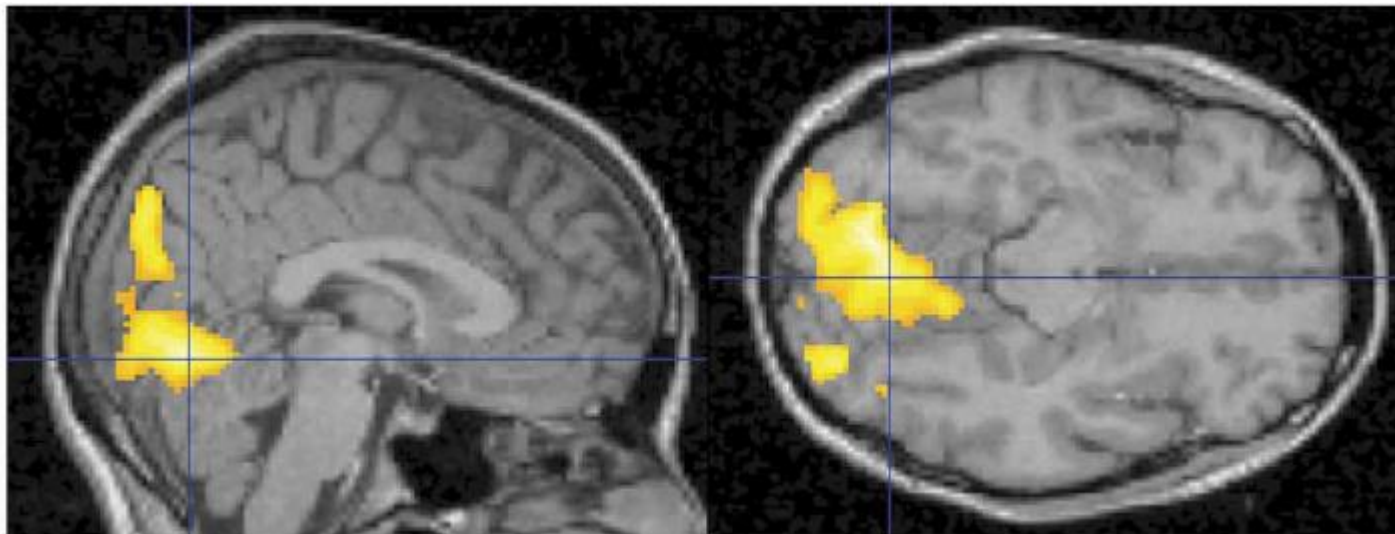
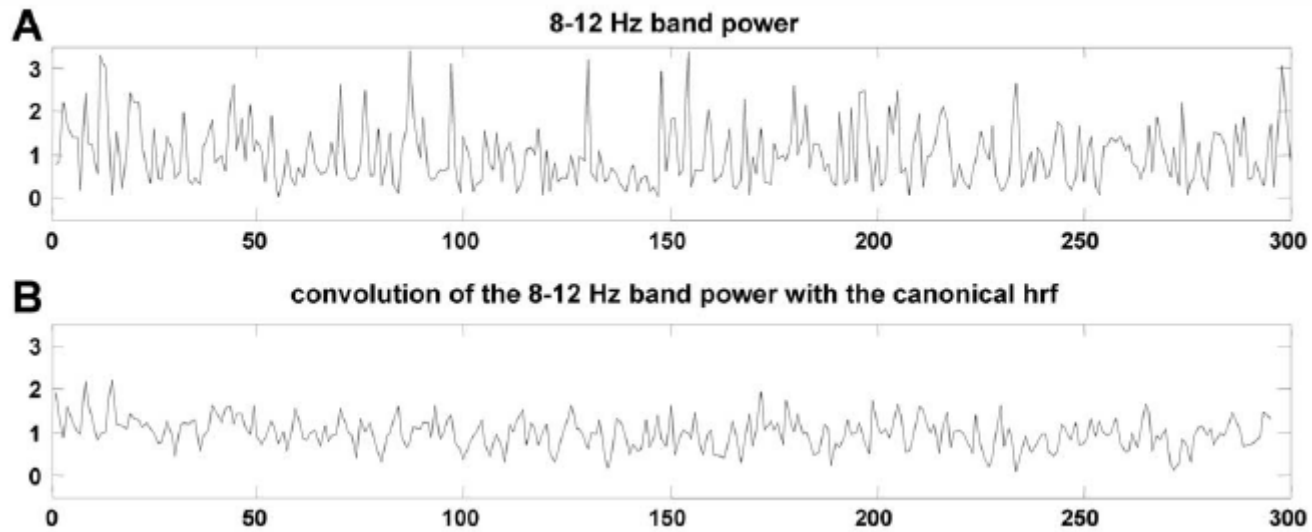
1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Concurrent EEG and fMRI

H. Laufs et al. / NeuroImage 19 (2003) 1463–1476



Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Examples

1. EEG \rightarrow fMRI asymmetric integration

(Background: The M/EEG inverse problem)

3. MEG \leftrightarrow EEG symmetric integration (fusion)

Given n sensors and p sources fixed in location and orientation (e.g, on a cortical mesh), then linear Forward Model (for single timepoint):

$$\begin{bmatrix} d_1 \\ \vdots \\ d_n \end{bmatrix} = \begin{bmatrix} L_{11} & L_{12} & \cdots & L_{1p} \\ \vdots & \ddots & & \vdots \\ L_{n1} & \cdots & \cdots & L_{np} \end{bmatrix} \begin{bmatrix} s_1 \\ s_2 \\ \vdots \\ s_p \end{bmatrix} + \begin{bmatrix} e_1 \\ \vdots \\ e_n \end{bmatrix}$$

d = Data

s = Sources

L = Leadfields

e = Error (noise)

n sensors

$p \gg n$ sources

n sensors \times p sources

n sensors...

Equivalent matrix format:

$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

Assume sensor noise is zero-mean Gaussian with error covariance $\mathbf{C}^{(e)}$:

$$\mathbf{e} \sim N(\mathbf{0}, \mathbf{C}^{(e)})$$

Assume sources similarly Gaussian with source covariance $\mathbf{C}^{(s)}$:

$$\mathbf{s} \sim N(\mathbf{0}, \mathbf{C}^{(s)})$$

M/EEG Linear Forward Model Assumptions to Solve

$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$
 $\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$

d = Data
 s = Sources
 L = Leadfields
 e = Error (noise)

n sensors
 $p \gg n$ sources
 n sensors \times p sources
 n sensors...

General solution is:

Hauk (2004), Neuroimage

$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d}$$

λ = Regularisation (hyperparameter)

But how calculate $\mathbf{C}^{(e)}$ and $\mathbf{C}^{(s)}$?

MEG Linear Forward Model Assumptions to Solve

One approach is to model sources and noise by variance components:

$$\mathbf{C} = \sum_i \lambda_i \mathbf{Q}_i$$

\mathbf{C} = Sensor/Source covariance

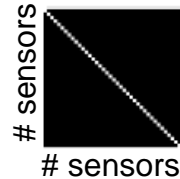
\mathbf{Q} = Covariance components

λ = Hyper-parameters

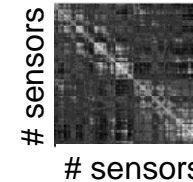
Friston et al (2008) Neuroimage

1. Sensor components, $\mathbf{Q}_i^{(e)}$ (error):

“IID” (white noise):

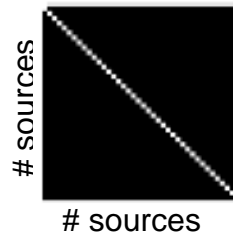


Empty-room:

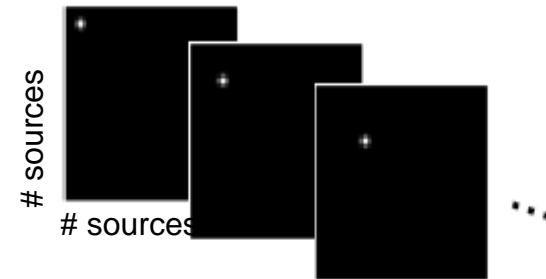


2. Source components, $\mathbf{Q}_i^{(s)}$ (priors/regularisation):

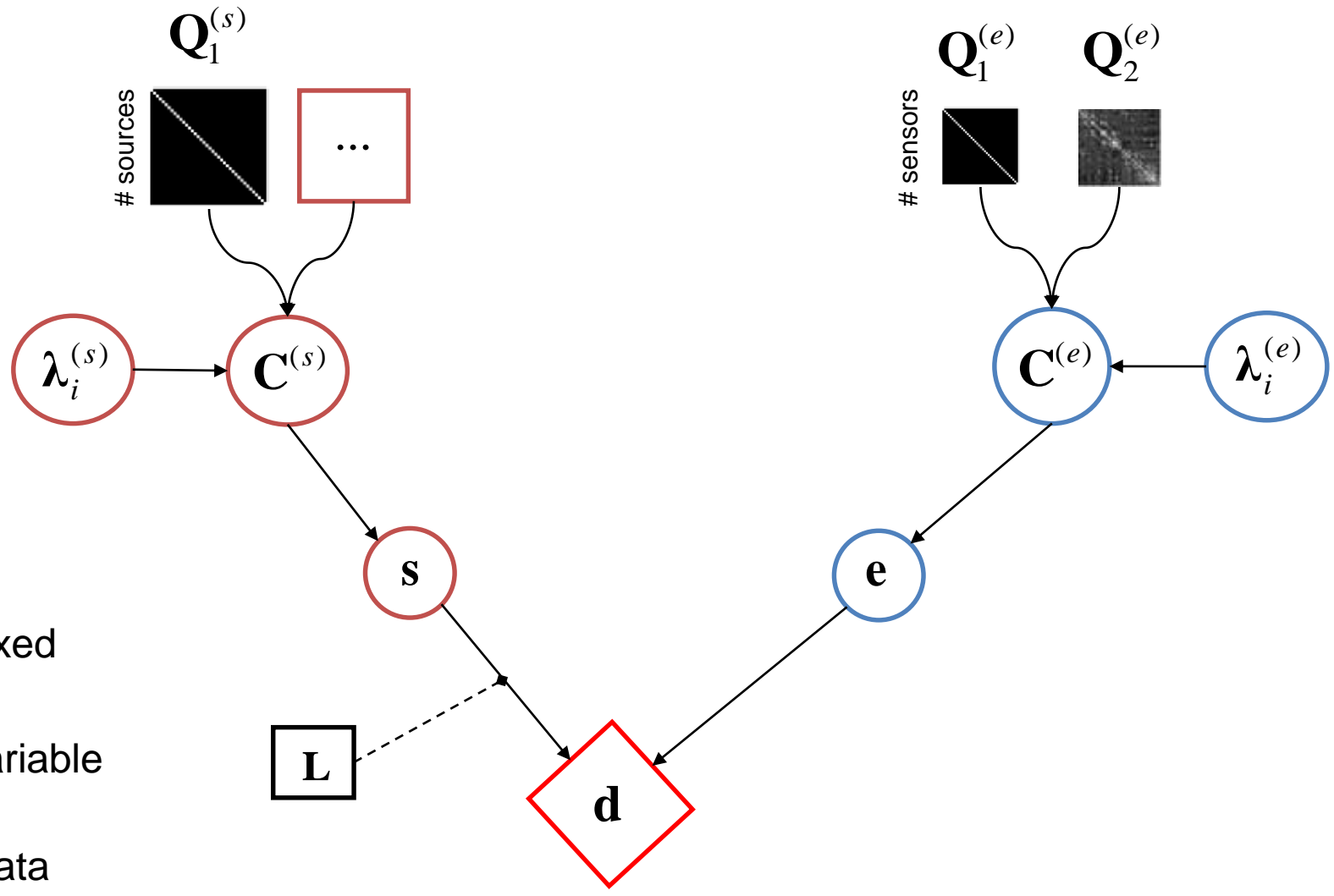
“IID” (min norm):



Multiple Sparse Priors (MSP):



MEG Generative Model



M/EEG Linear Forward Model Assumptions to Solve

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$$\mathbf{d} = \mathbf{L}\mathbf{s} + \mathbf{e}$$

$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$
 $\mathbf{s} \sim N(0, \mathbf{C}^{(s)})$

d = Data
 s = Sources
 L = Leadfields
 e = Error (noise)

n sensors
 $p \gg n$ sources
 n sensors \times p sources
 n sensors...

General solution is:

Hauk (2004), Neuroimage

$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d}$$

λ = Regularisation (hyperparameter)

But how calculate $\mathbf{C}^{(e)}$ and $\mathbf{C}^{(s)}$?

Specify multiple (covariance) priors, and estimate their weighting (hyperparameters) by maximising **model evidence**

(using a variational Bayesian approach, eg EM algorithm)

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Asymmetric Integration of MEG+fMRI Background

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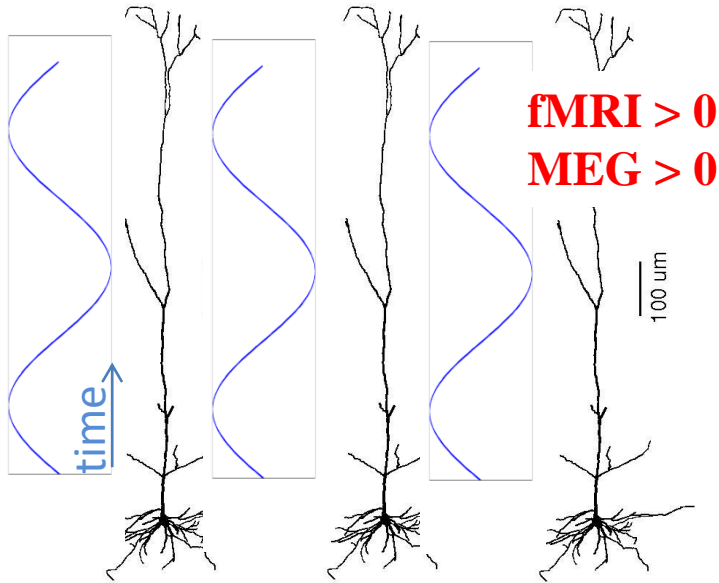
- fMRI has superior spatial resolution (~mm) than M/EEG, but inferior temporal resolution (integrating over seconds)
- fMRI and M/EEG measure similar, but not identical, neural activity
- Eg, some source configurations give detectable fMRI signal, but no detectable M/EEG signal...
- ...and vice versa

Asymmetric Integration of MEG+fMRI Background

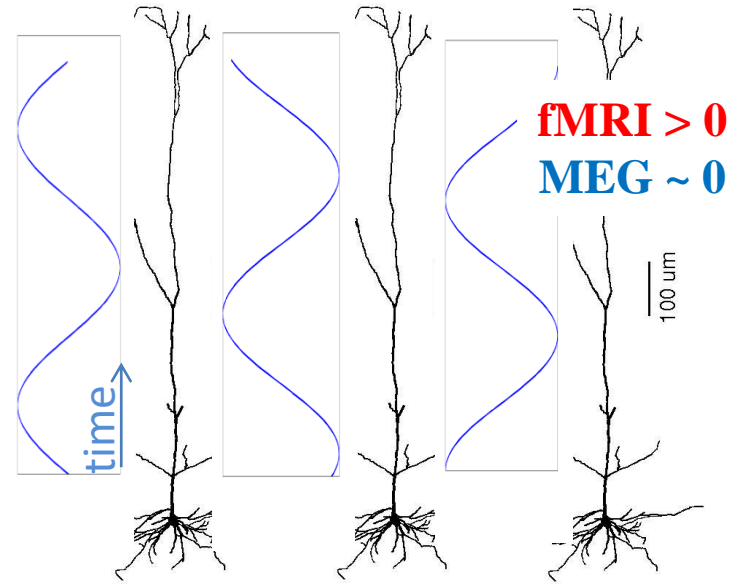
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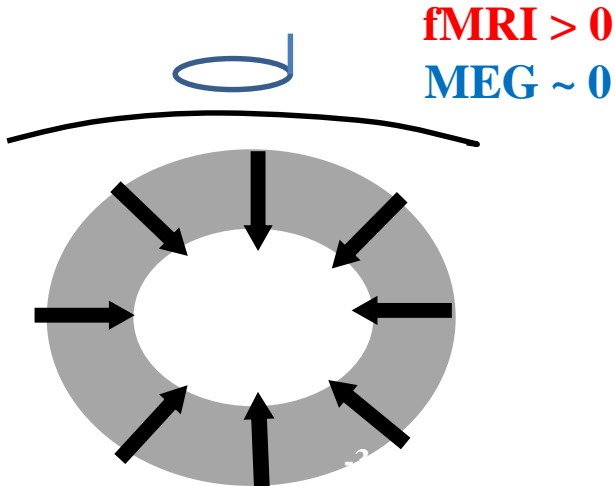
Synchronous



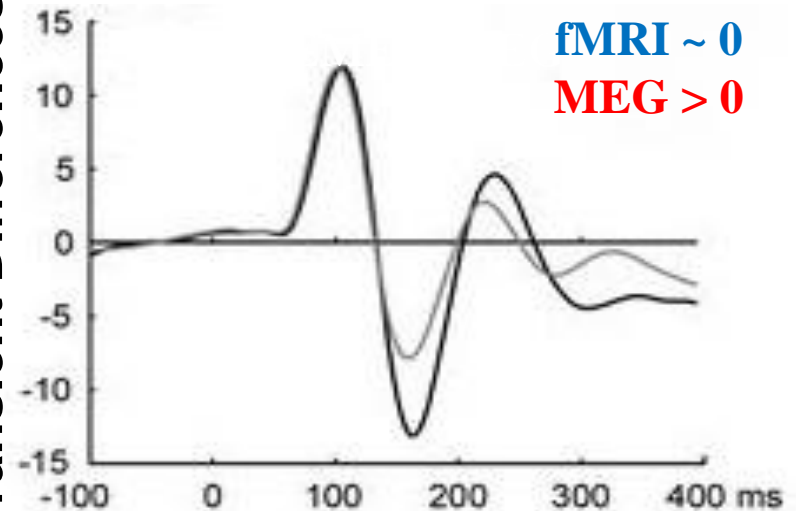
Asynchronous



Closed Fields?



Transient Differences



Asymmetric Integration of MEG+fMRI Background

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- fMRI has superior spatial resolution (~mm) than M/EEG, but inferior temporal resolution (integrating over seconds)
- fMRI and M/EEG measure similar, but not identical, neural activity
- Eg, some source configurations give detectable fMRI signal, but no detectable M/EEG signal...
- ...and vice versa
- Use fMRI as a **soft**, rather than **hard**, constraint on localisation of sources of M/EEG data...

Specifying (co)variance components (priors/regularisation):

$$\mathbf{C} = \sum_i \lambda_i \mathbf{Q}_i$$

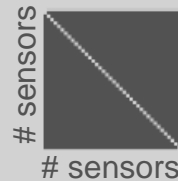
\mathbf{C} = Sensor/Source covariance

\mathbf{Q} = Covariance components

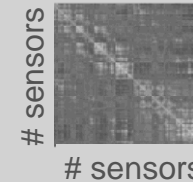
λ = Hyper-parameters

1. Sensor components, $\mathbf{Q}_i^{(e)}$ (error):

“IID” (white noise):

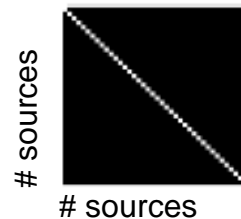


Empty-room:

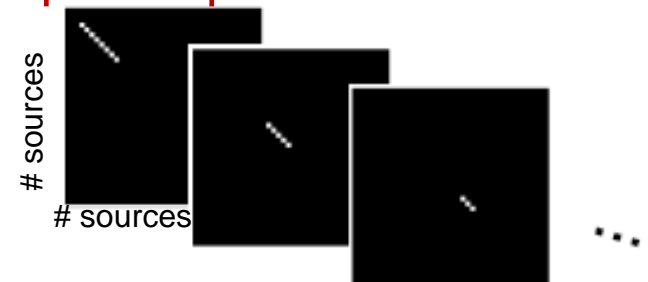


2. Each suprathreshold fMRI cluster becomes a separate prior $\mathbf{Q}_i^{(s)}$

“IID” (min norm):



fMRI Priors:



General solution again:

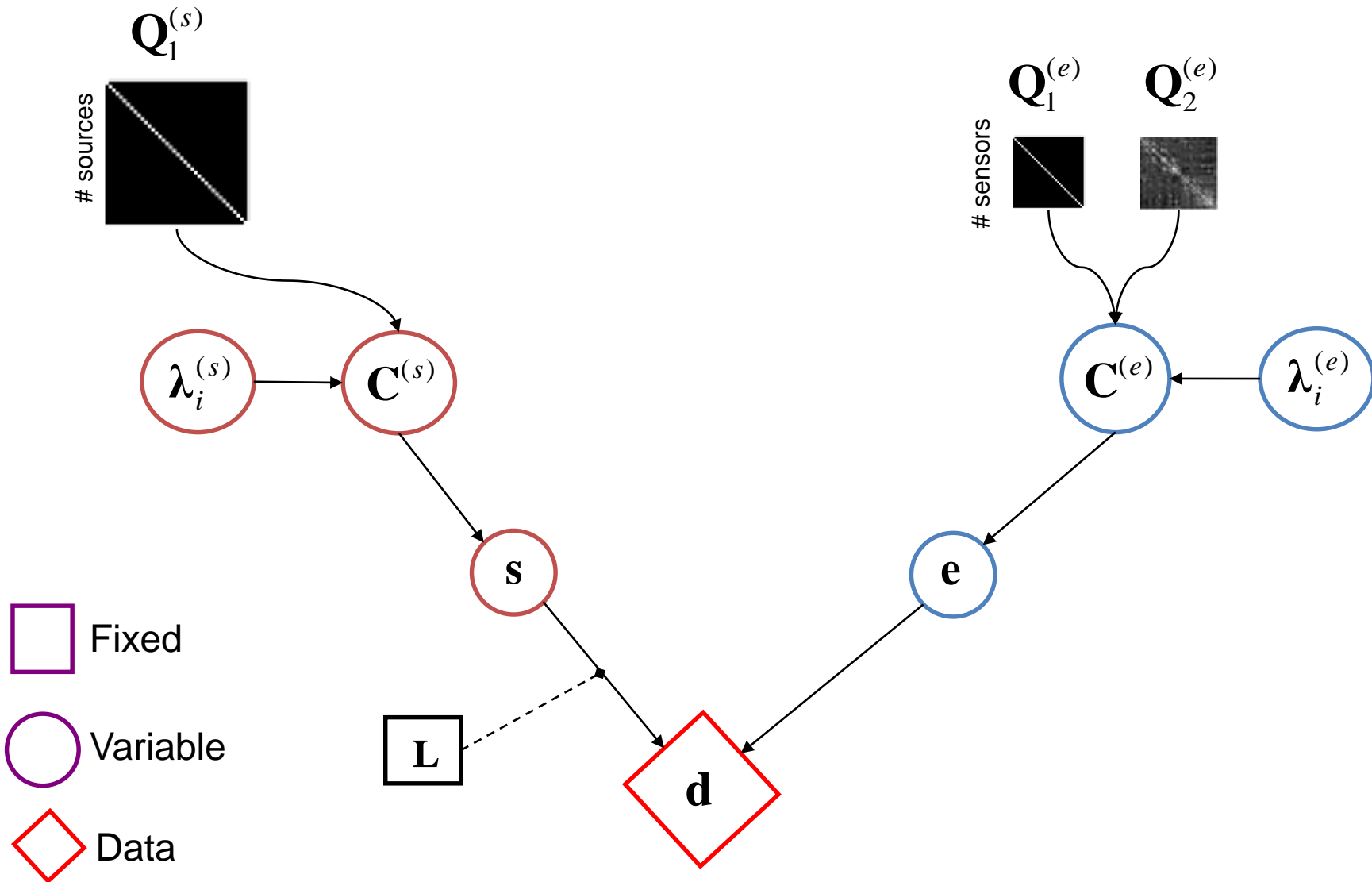
$$\hat{\mathbf{s}} = \mathbf{C}^{(s)} \mathbf{L}^T (\mathbf{L} \mathbf{C}^{(s)} \mathbf{L}^T + \lambda \mathbf{C}^{(e)})^{-1} \mathbf{d}$$
$$\mathbf{e} \sim N(0, \mathbf{C}^{(e)})$$
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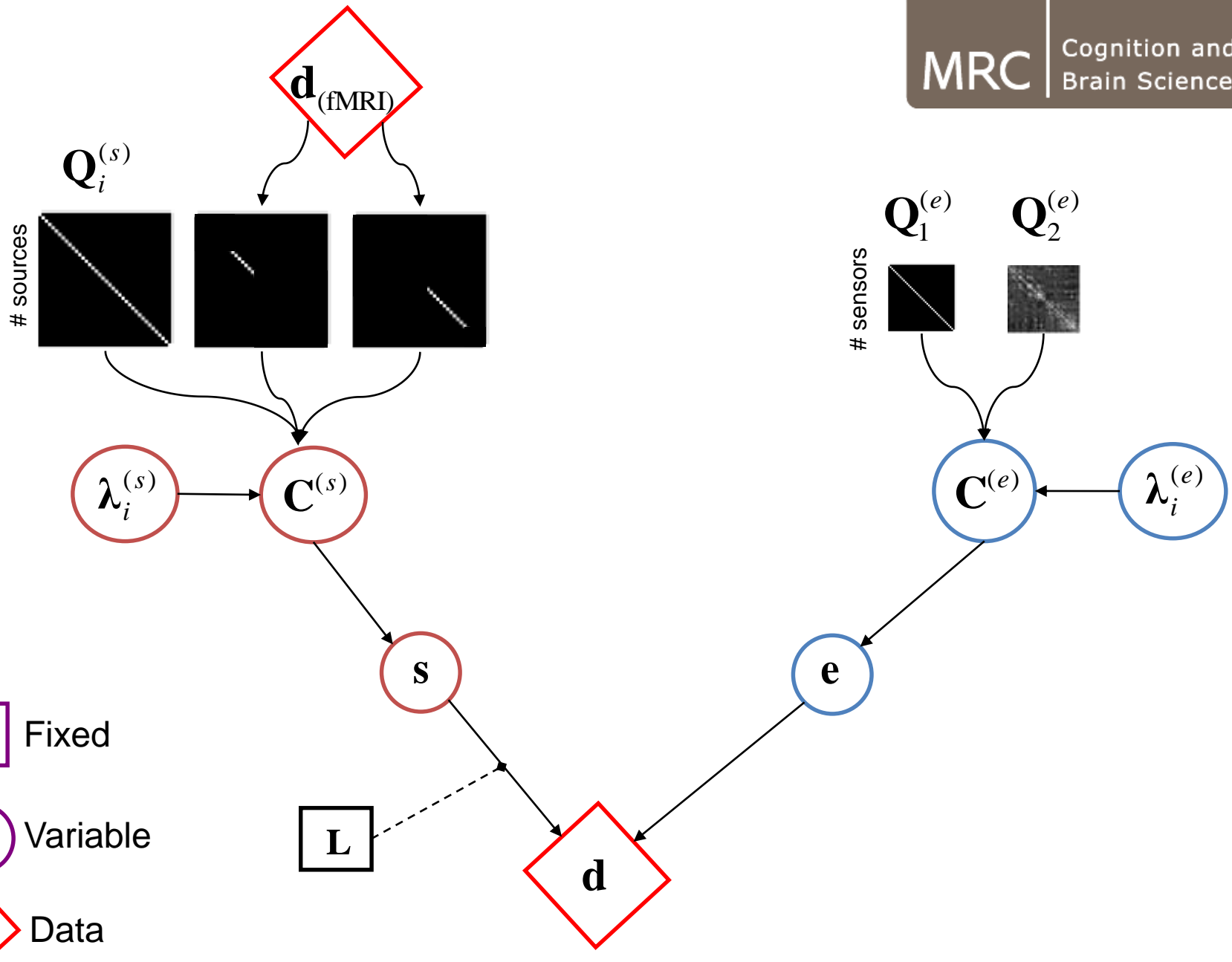
Now source covariance expressed as number of fMRI clusters:

$$\mathbf{C}^{(s)} = \lambda_1^{(s)} \mathbf{Q}_{(fMRI1)}^{(s)} + \lambda_2^{(s)} \mathbf{Q}_{(fMRI2)}^{(s)} + \dots$$

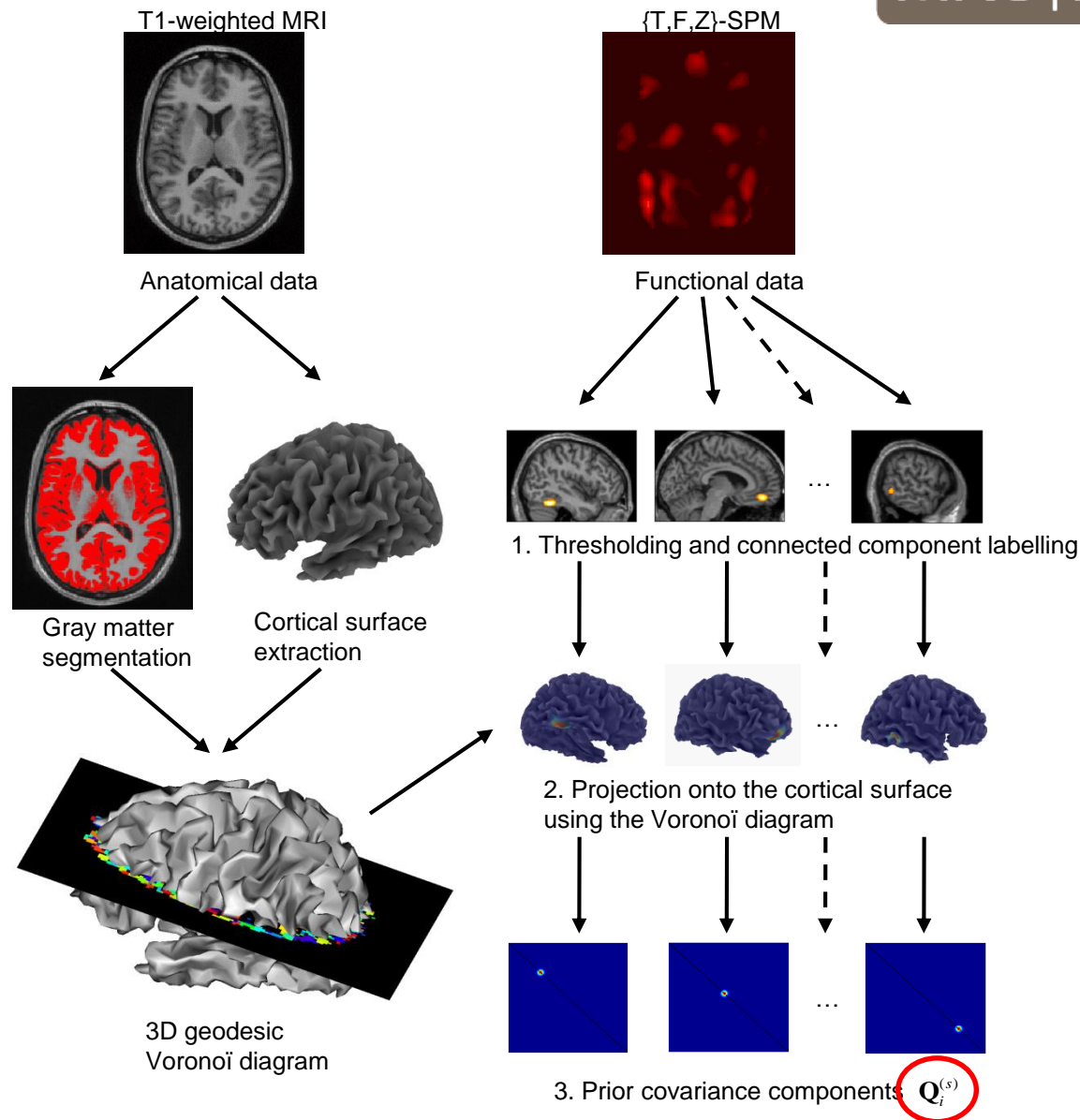
When $\mathbf{Q}_i^{(s)}$ does not help maximise model evidence, $\lambda_i^{(s)} \rightarrow 0$,
i.e. constraints ignored...

...catering for situations where fMRI signal does not reflect same activity as in M/EEG signal (e.g. occurring later than time-window than M/EEG data)

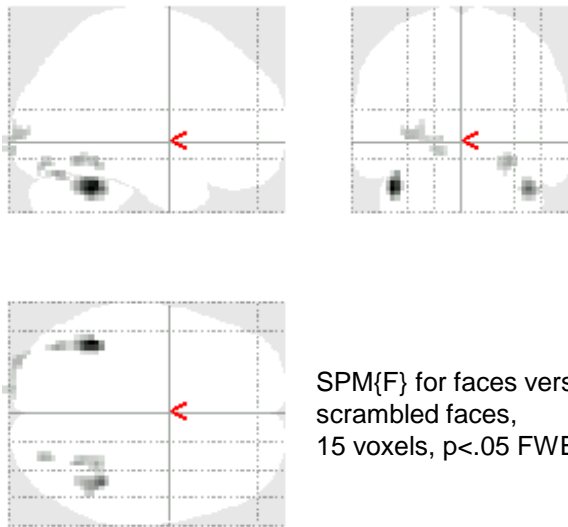




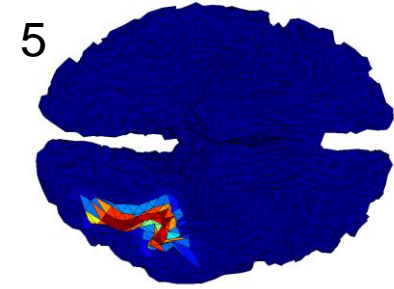
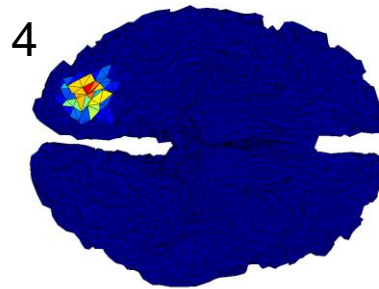
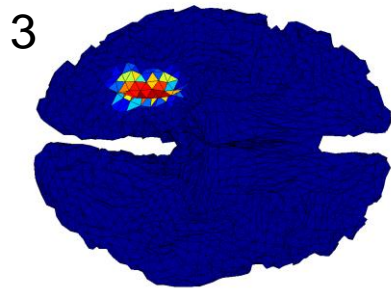
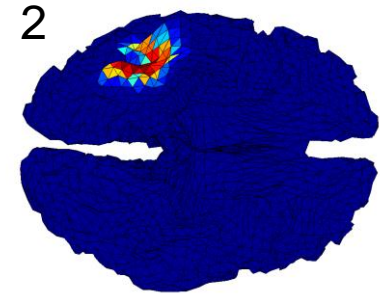
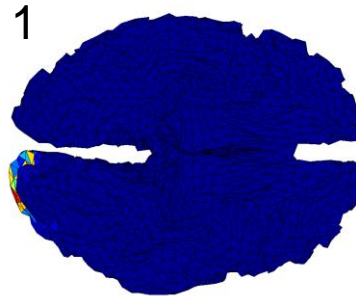
Asymmetric Integration of M/EEG+fMRI



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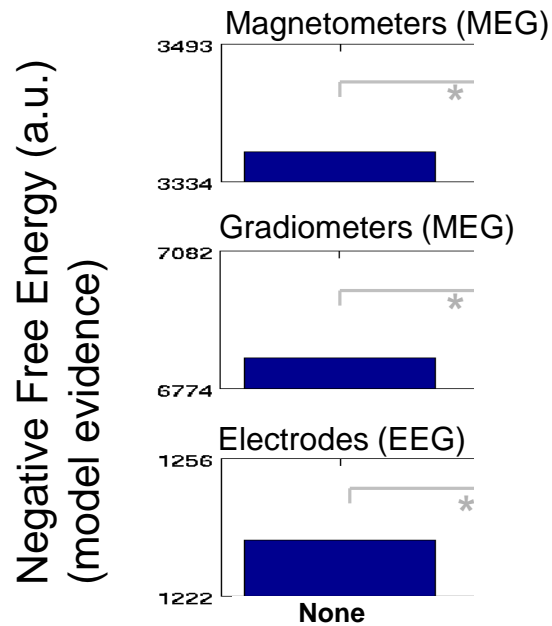


SPM{F} for faces versus scrambled faces,
15 voxels, $p < .05$ FWE

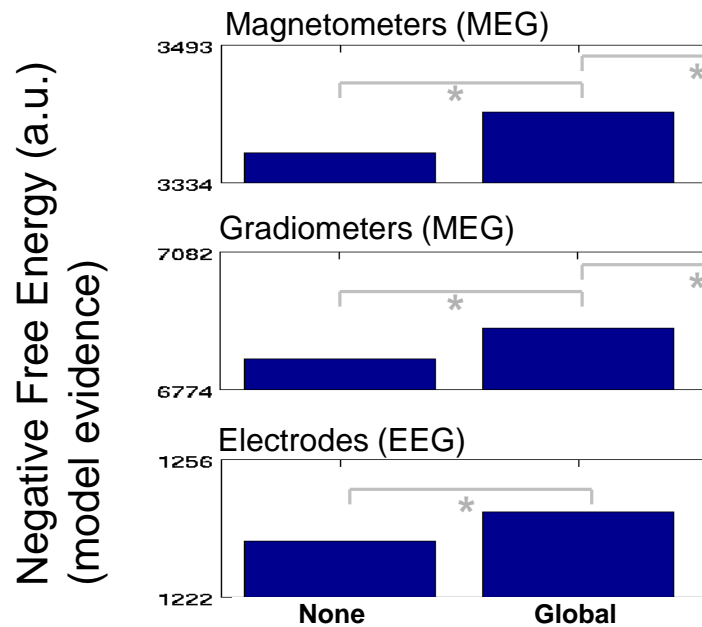


5 clusters from SPM of fMRI data from separate group of (18) subjects in MNI space

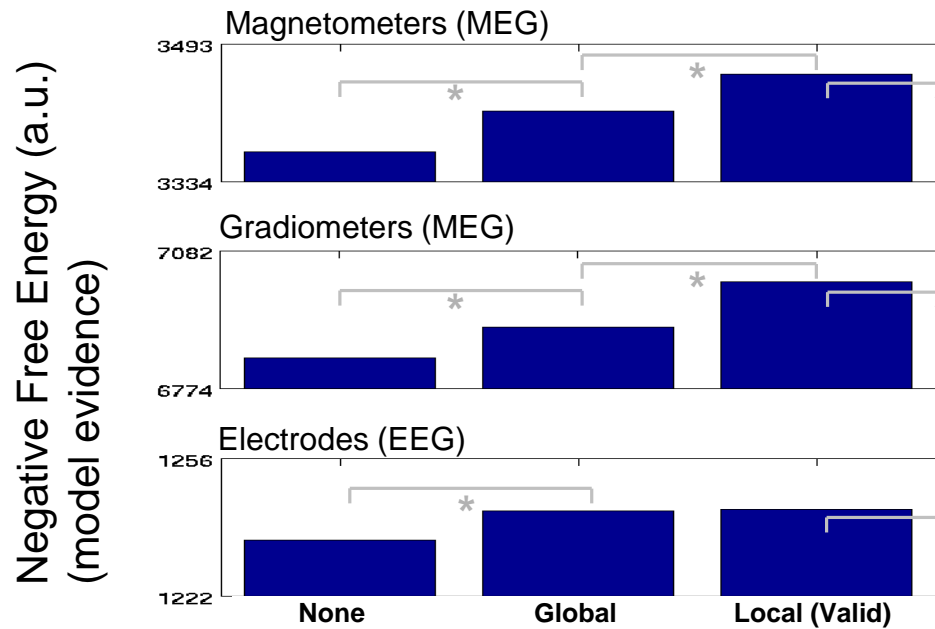
Asymmetric Integration of M/EEG+fMRI



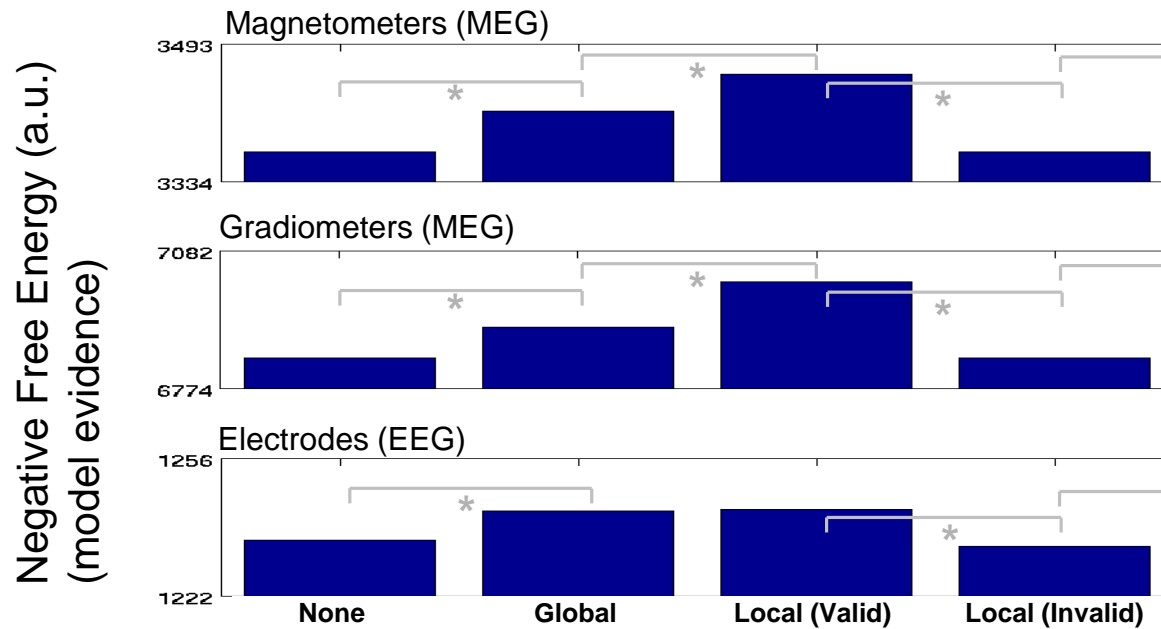
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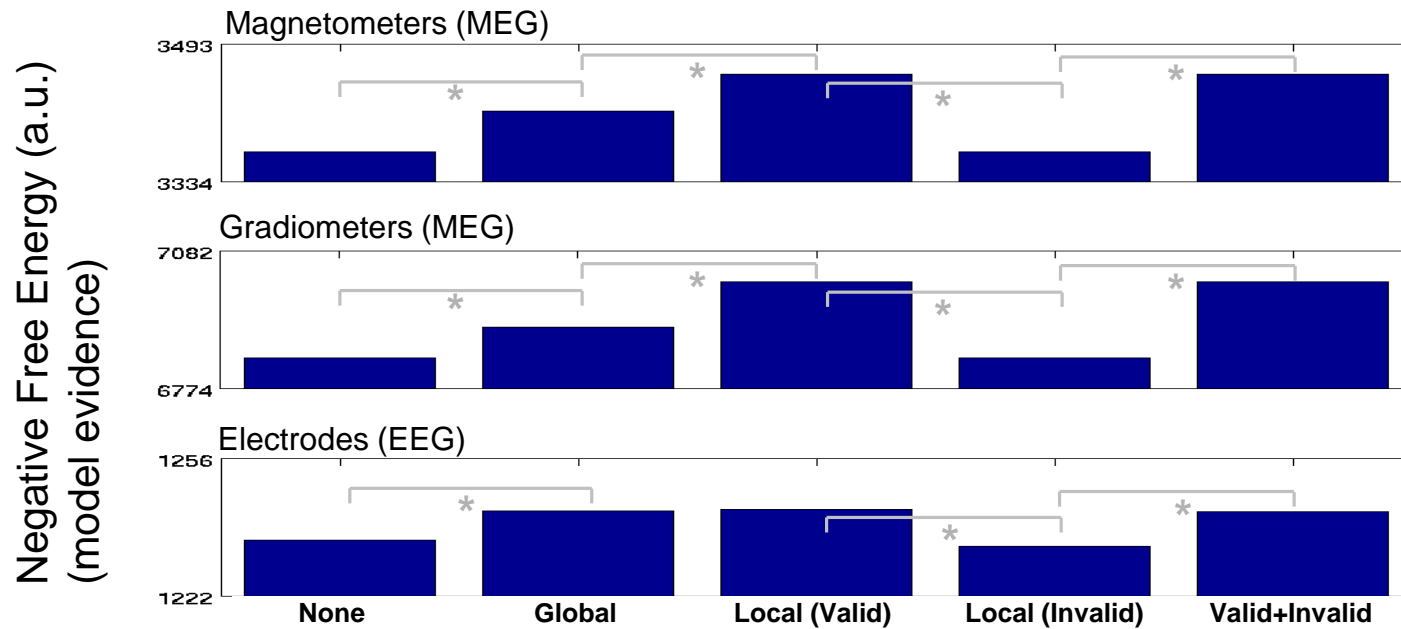
Asymmetric Integration of M/EEG+fMRI



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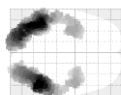
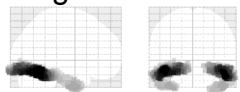
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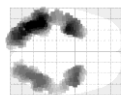
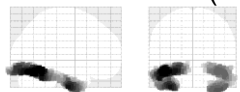
Asymmetric Integration of M/EEG+fMRI

IID sources and IID noise (L2 MNM)

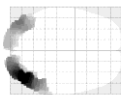
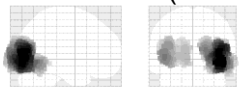
Magnetometers (MEG)



Gradiometers (MEG)



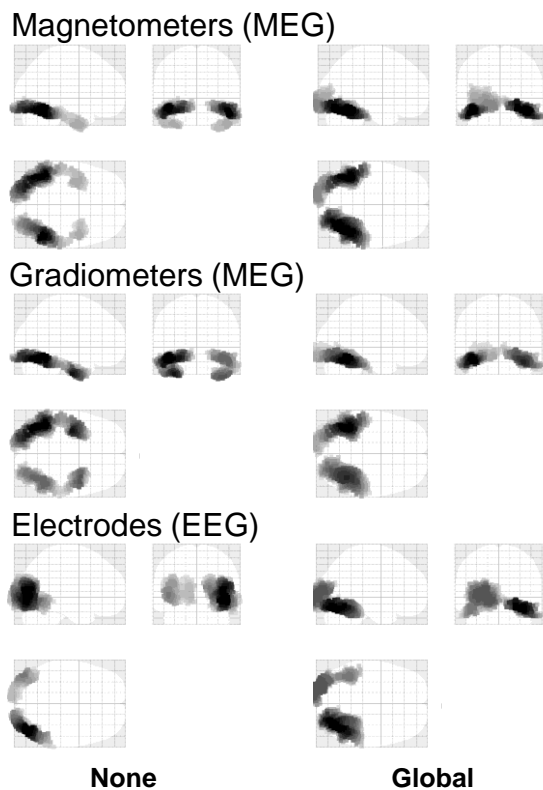
Electrodes (EEG)



None

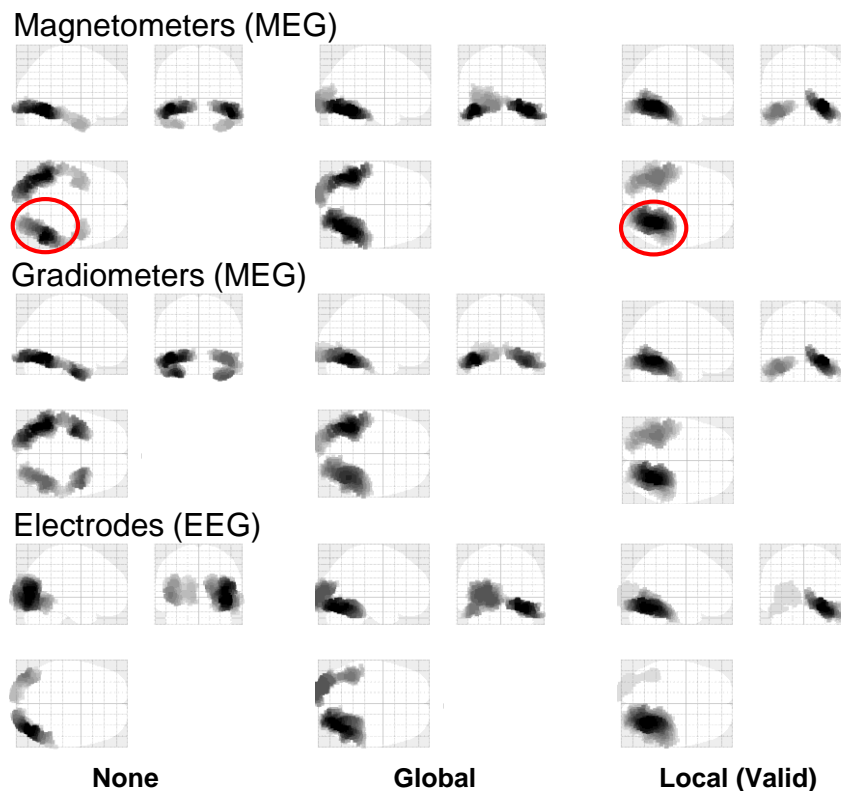
Asymmetric Integration of M/EEG+fMRI

IID sources and IID noise (L2 MNM)



Asymmetric Integration of M/EEG+fMRI

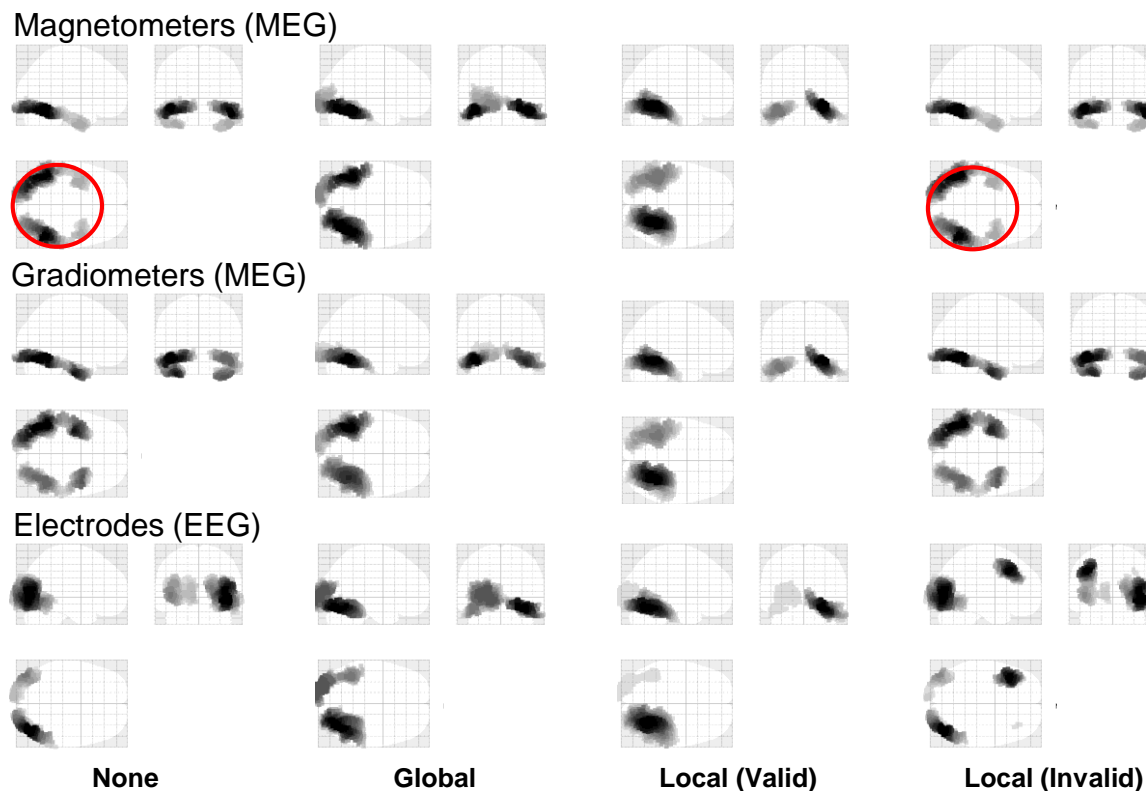
IID sources and IID noise (L2 MNM)



fMRI priors counteract superficial bias of Min Norm

Asymmetric Integration of M/EEG+fMRI

IID sources and IID noise (L2 MNM)



Invalid priors generally discounted (at least for MEG)

- Adding a single, global fMRI prior increases model evidence
- Adding **multiple** valid priors increases model evidence further
- Adding invalid priors does not necessarily increase model evidence, particularly in conjunction with valid priors
Helpful if some fMRI regions produce no MEG/EEG signal (or arise from neural activity at different times)
- Can counteract superficial bias of, e.g, minimum-norm
- Makes some allowance for different sensitivities of fMRI and M/EEG to certain types of neural activity

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)

Symmetric Integration of MEG+EEG Background

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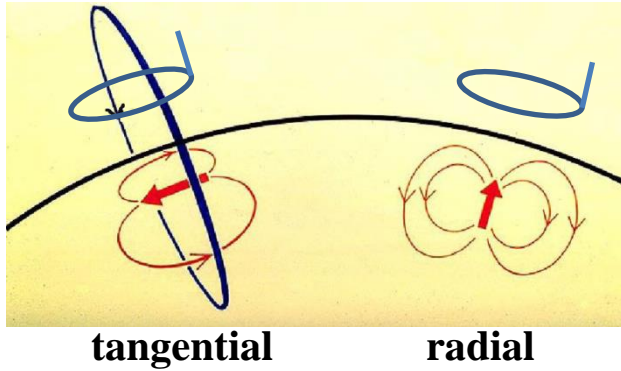
- MEG generally has superior spatial resolution than EEG (less blurred by skull/scalp)
- MEG cannot detect radial component of current sources; EEG can!

Symmetric Integration of MEG+EEG Background

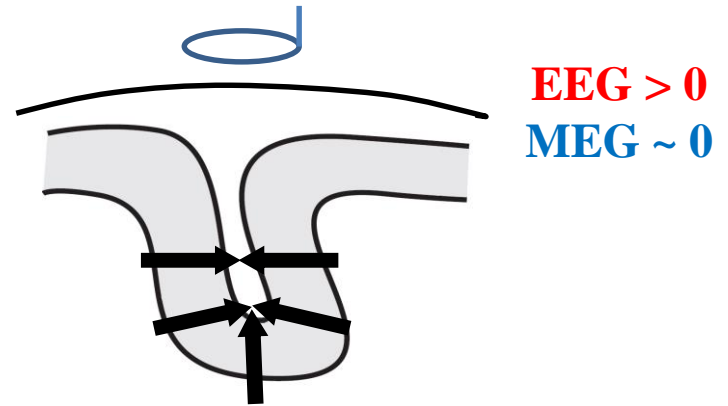
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Dipolar Sources

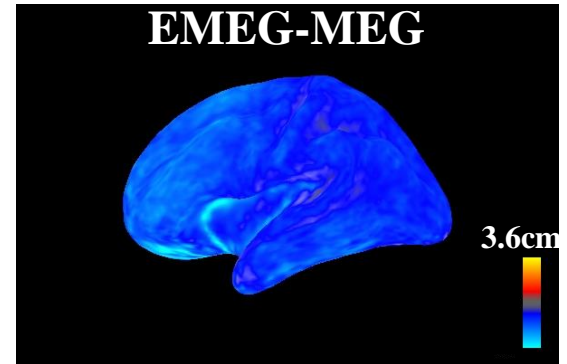
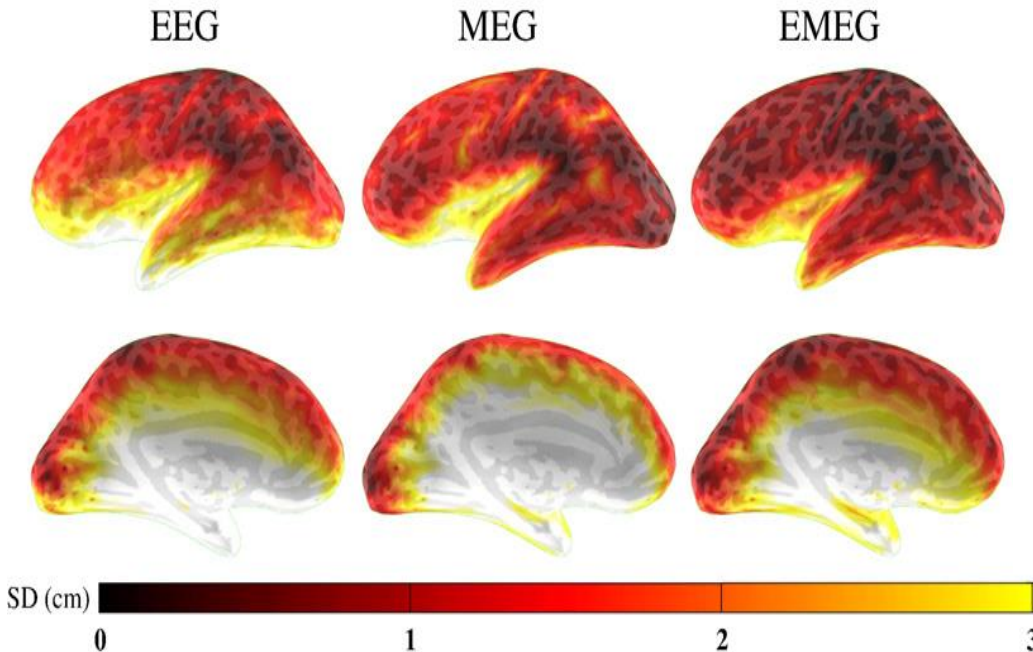


Extended Sources



Ahlfors et al., HBM 2010

Spatial Extent



Stenroos & Hauk, in prep

Symmetric Integration of MEG+EEG

Background

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- MEG generally has superior spatial resolution than EEG (less blurred by skull/scalp)
- MEG cannot detect radial component of current sources; EEG can!
- And few practical problems acquiring concurrent EEG (apart from extra time attaching electrodes)
- ...but EEG data is more sensitive to head geometry and conductivity (potentially biasing any joint-localisation)...
- ...and has different noise characteristics...

Symmetric Integration of MEG+EEG Generative Model

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For fusing MEG and EEG, we can simply concatenate the MEG+EEG data:

$$\begin{bmatrix} \mathbf{d}_{(MEG)} \\ \mathbf{d}_{(EEG)} \end{bmatrix} = \begin{bmatrix} \mathbf{L}_{(MEG)} \\ \mathbf{L}_{(EEG)} \end{bmatrix} \mathbf{s} + \begin{bmatrix} \mathbf{e}_{(MEG)} \\ \mathbf{e}_{(EEG)} \end{bmatrix} \quad \begin{array}{l} \mathbf{e} \sim N(0, \mathbf{C}^{(e)}) \\ \mathbf{s} \sim N(0, \mathbf{C}^{(s)}) \end{array}$$

Noise expressed by MEG and EEG terms (e.g, white noise):

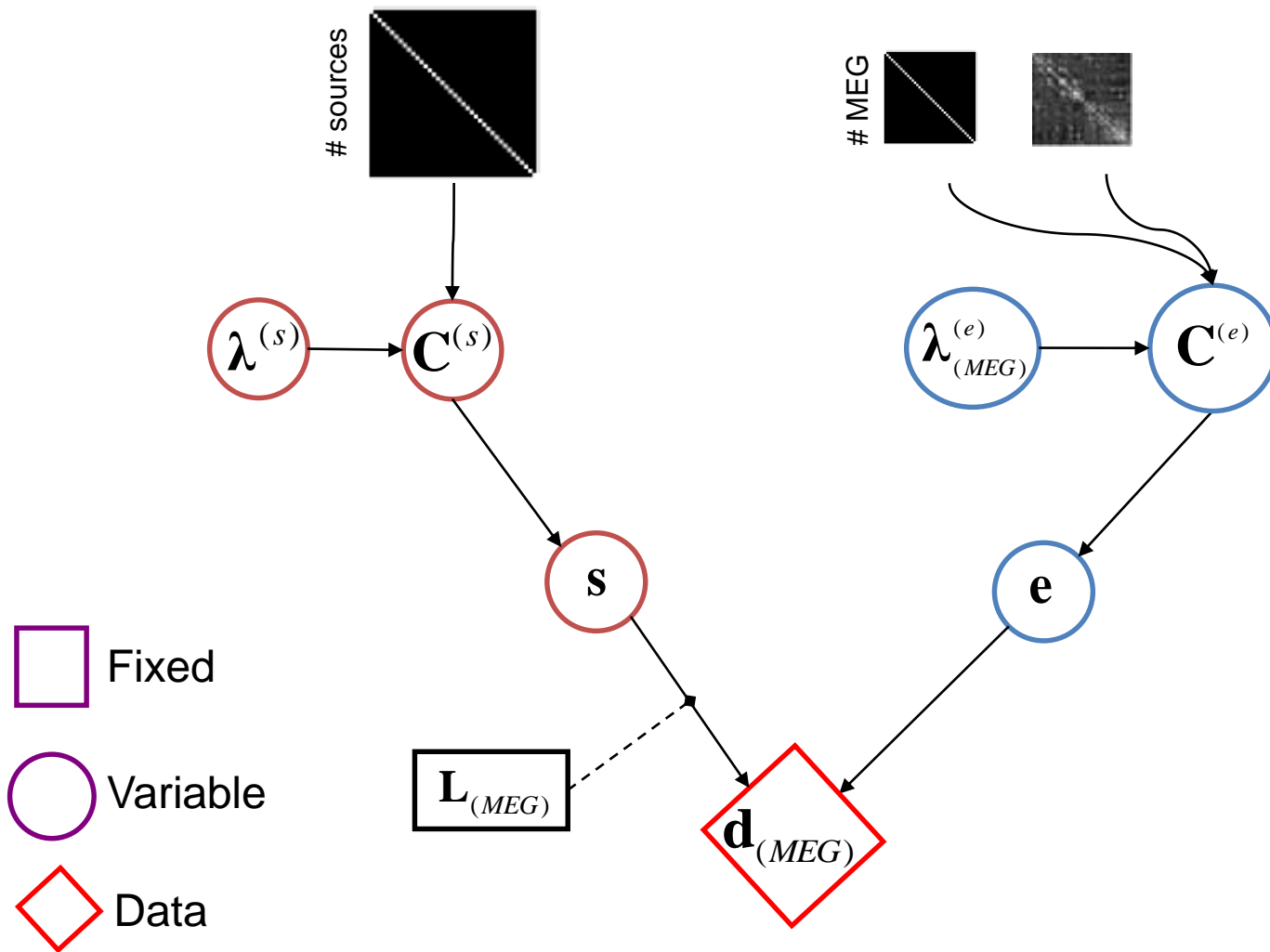
$$\hat{\mathbf{C}}^{(e)} = \lambda_1^{(e)} \mathbf{Q}_{(MEG)}^{(e)} + \lambda_2^{(e)} \mathbf{Q}_{(EEG)}^{(e)} \quad \mathbf{Q}_{(MEG)}^{(e)} = \begin{array}{c} \# \text{ sensors} \\ \blacksquare \\ \# \text{ sensors} \end{array} \quad \mathbf{Q}_{(EEG)}^{(e)} = \begin{array}{c} \# \text{ sensors} \\ \blacksquare \\ \# \text{ sensors} \end{array}$$

The separate hyperparameters allow for different noise levels (SNR)

Symmetric Integration of MEG+EEG Generative Model

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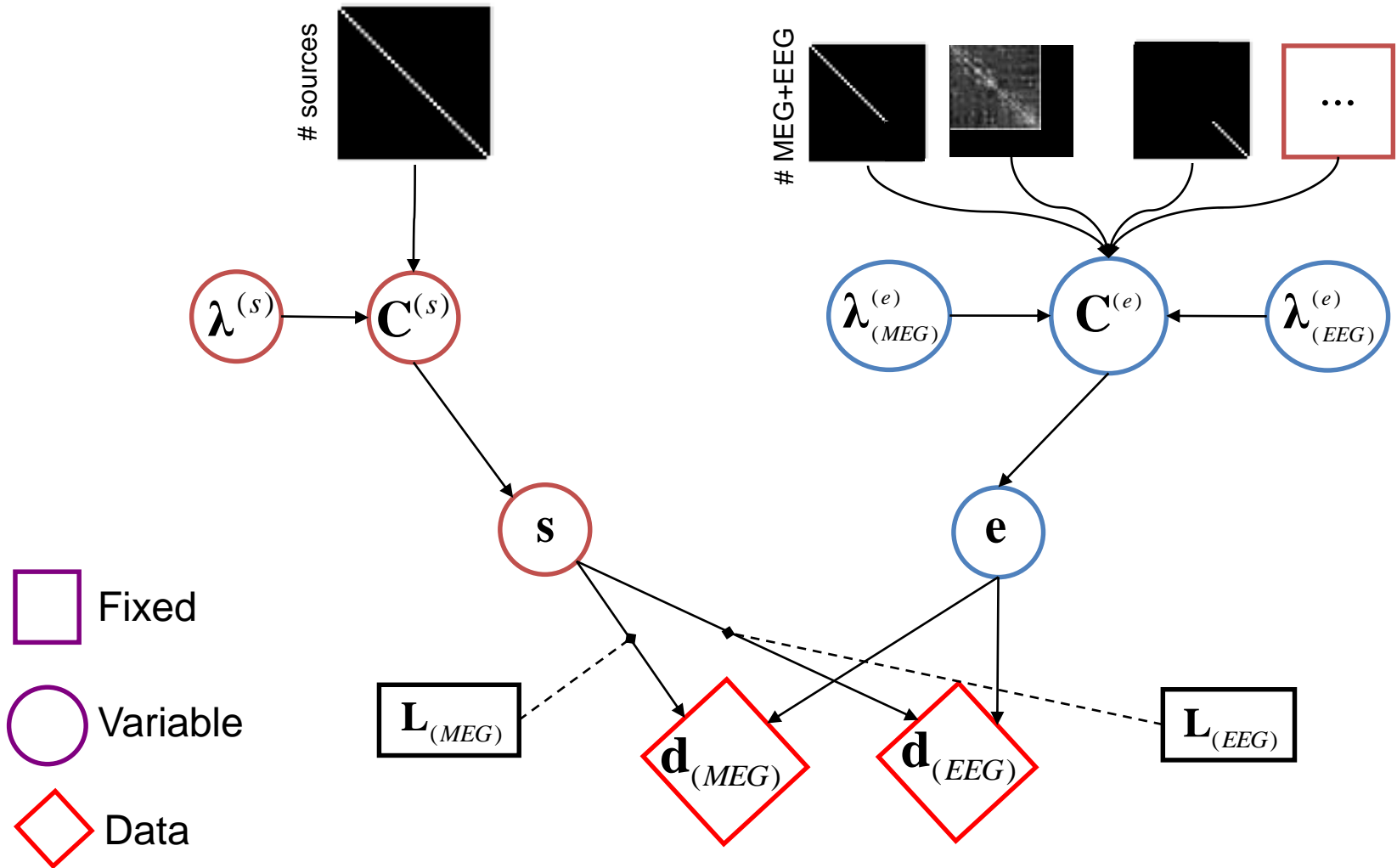
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Symmetric Integration of MEG+EEG Generative Model

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One final problem...

- Though this allows for different additive noise levels in MEG and EEG...
- ...we are assuming mapping from common electrical sources to sensor values (in terms of Tesla and Volts) is known precisely...
- ...whereas in reality, this depends on several unknowns (e.g, precise conductivity of skull/scalp)
- One solution is to scale data/leadfields to have same variance:

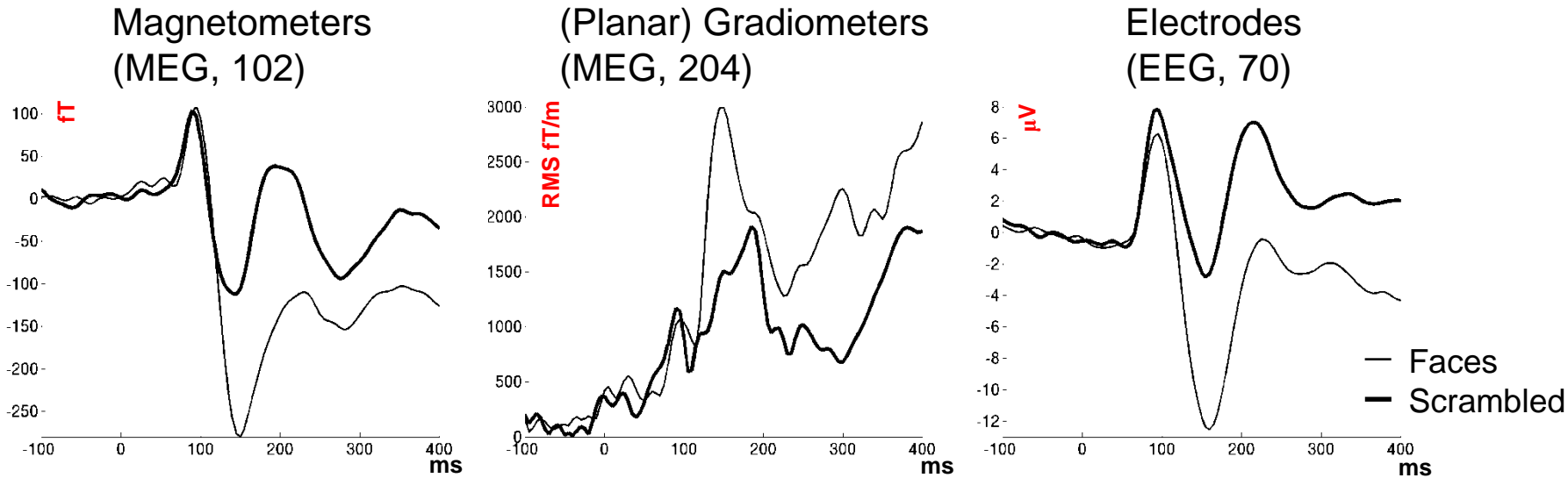
$$\tilde{Y}_i = \frac{Y_i}{\sqrt{\frac{1}{n_i} \text{tr}(Y_i Y_i^T)}}$$

$$\tilde{L}_i = \frac{L_i}{\sqrt{\frac{1}{n_i} \text{tr}(L_i L_i^T)}}$$

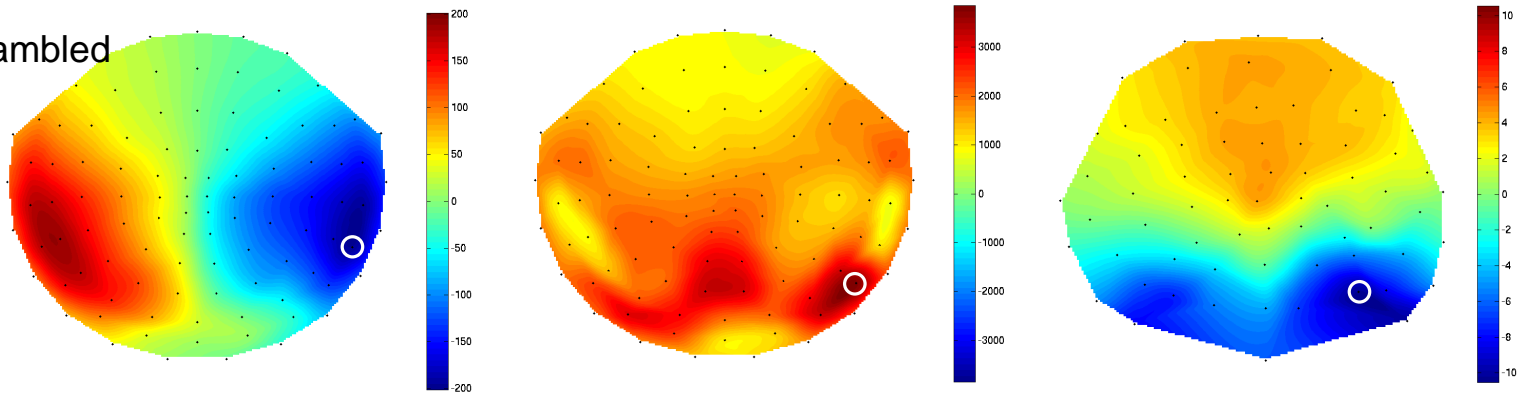
i = i th modality, ie MEG or EEG
 n_i = Number of sensors for modality i

Symmetric Integration of MEG+EEG Example

ERs from 12 subjects for 3 simultaneously-acquired Neuromag sensor-types:

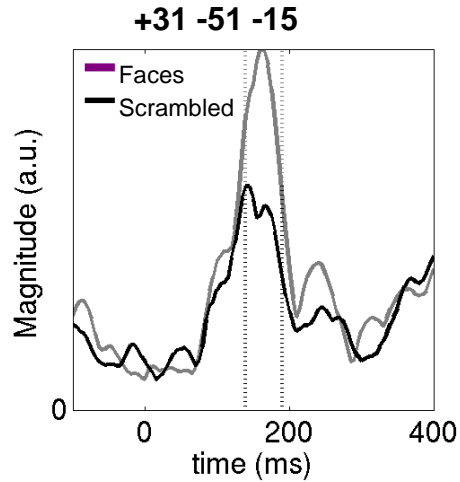
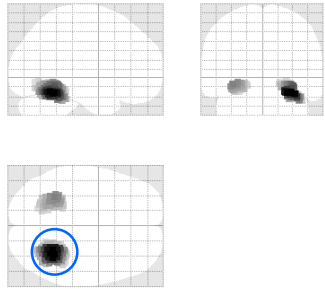


Faces - Scrambled
150-190ms

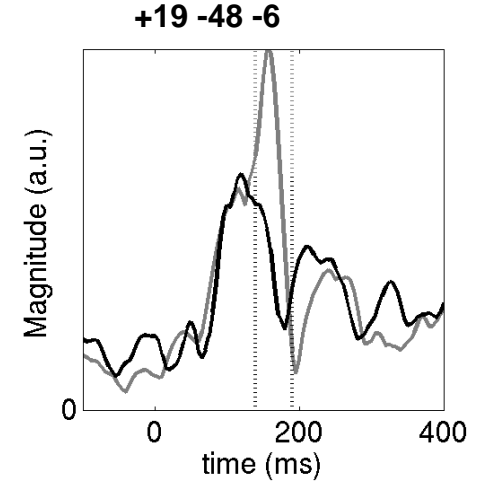
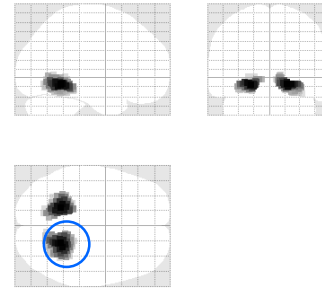


Symmetric Integration of MEG+EEG

MEG mags

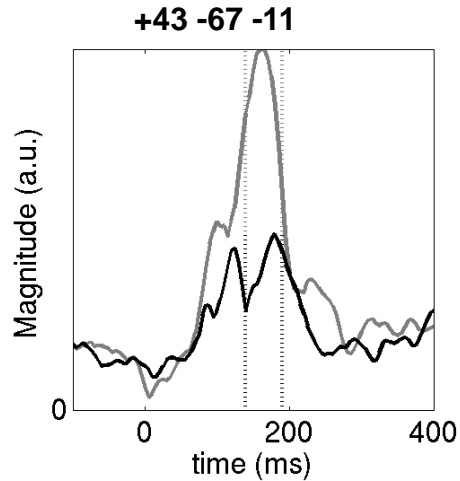
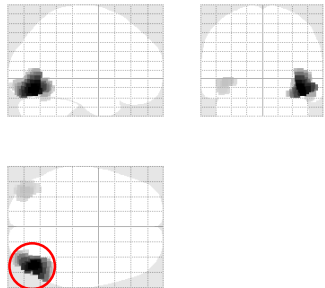


MEG grads

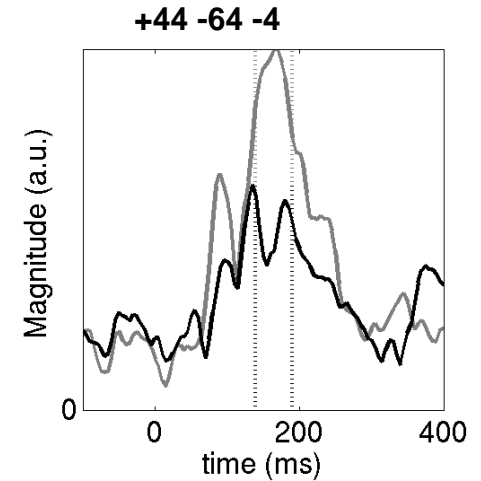
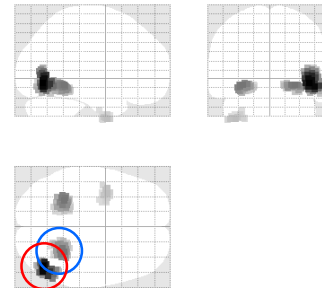


Faces – Scrambled, 150-190ms

EEG



FUSED



- Estimate noise covariance from pre-stimulus baseline (**b**):

$$\mathbf{C}^{(e)} = \begin{bmatrix} \text{cov}(\mathbf{b}_{(MEG)}) & \mathbf{0} \\ \mathbf{0} & \text{cov}(\mathbf{b}_{(EEG)}) \end{bmatrix}$$

Molins et al (2008), Neuroimage

(which can also be used to pre-whiten data and leadfields, scaling to noise units)...

...but downside is that **baseline contains source activity**, so not estimate of true sensor noise

- Maximise mutual information between MEG and EEG

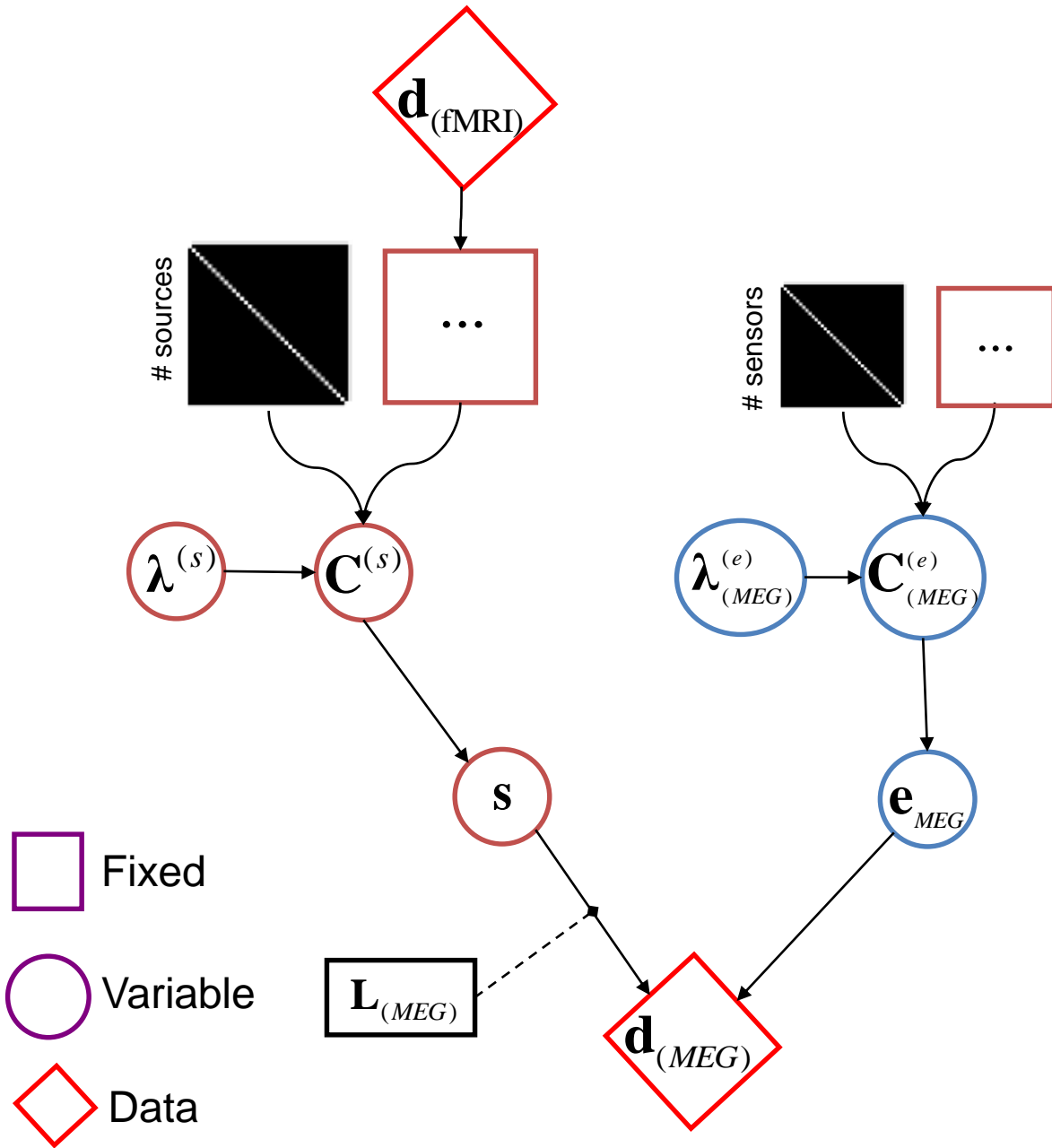
Baillet et al (1999), IEEE

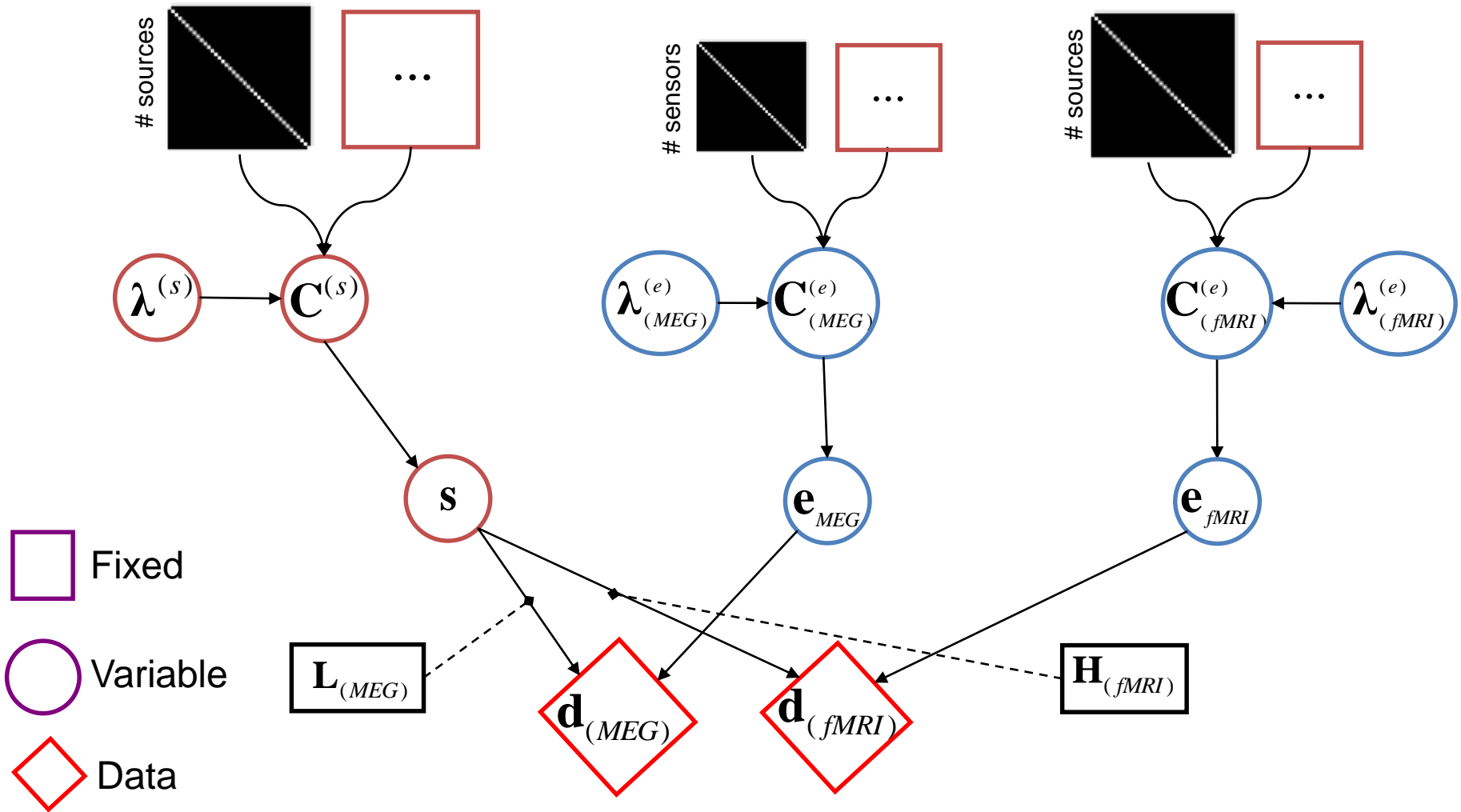
- Re-parameterise leadfields in terms of radial/tangential components

Huang et al (2007), Neuroimage

Examples

1. EEG \rightarrow fMRI asymmetric integration
2. fMRI \rightarrow M/EEG asymmetric integration
3. MEG \leftrightarrow EEG symmetric integration (fusion)
4. fMRI \leftrightarrow MEG \leftrightarrow EEG fusion?





Data-driven, symmetric approaches:

- Linked Matrix Factorisation methods (ICA, CCA, PLS)
- Representational Similarity Analysis (RSA)
- Graph Theory

Model-driven, asymmetric approaches:

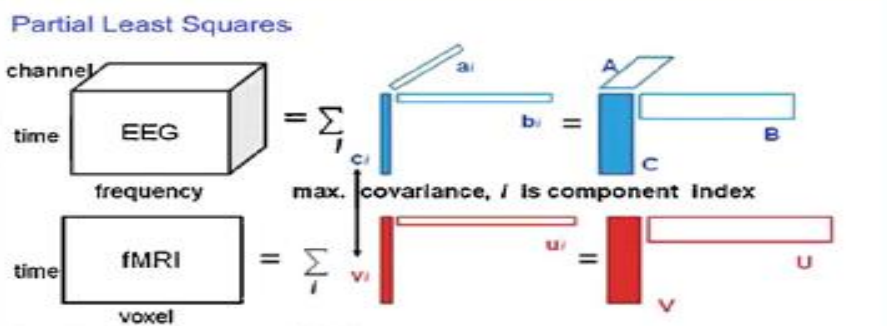
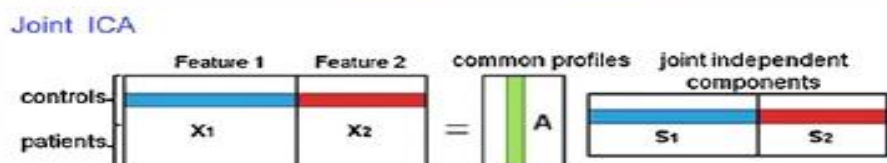
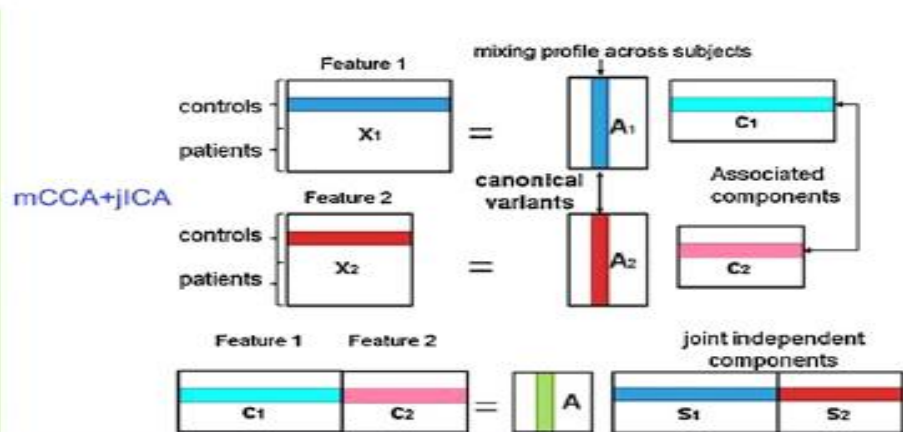
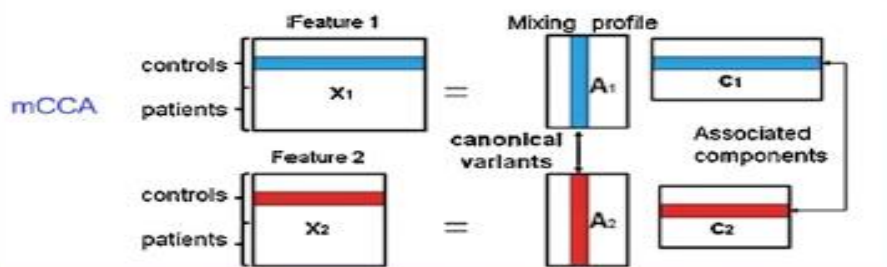
- Regression / Mediation / SEM

Model-driven, symmetric approaches:

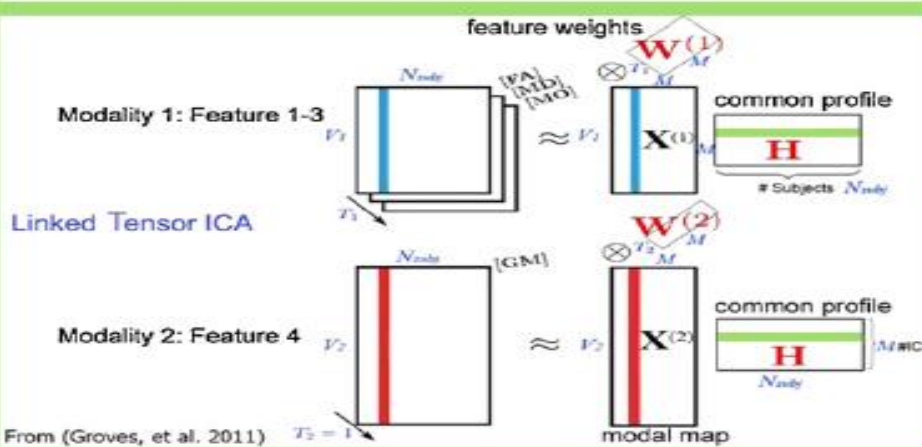
- Generative models (eg PEB)

The End

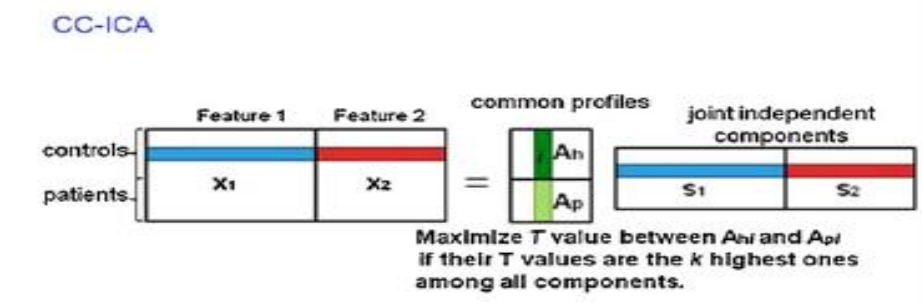
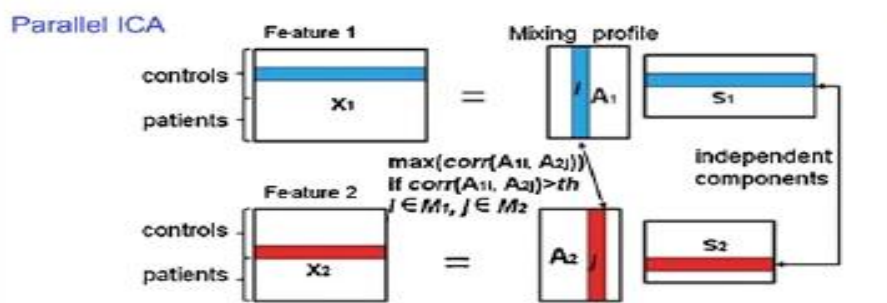
Blind Multivariate Fusion Methods



From (Martinez-Montes, et al. 2004)



Semi-Blind Multivariate Fusion Methods



Inverse Problem: Standard L_2 -norm

$$\mathbf{Y} = \mathbf{L}\mathbf{J} + \mathbf{E} \quad \mathbf{E} \sim N(\mathbf{0}, \mathbf{C}^{(e)})$$

$$\mathbf{J} = \arg \min \left\{ \left\| \mathbf{C}^{(e)-1/2} (\mathbf{Y} - \mathbf{L}\mathbf{J}) \right\|^2 + \lambda \left\| \mathbf{W}\mathbf{J} \right\|^2 \right\}$$

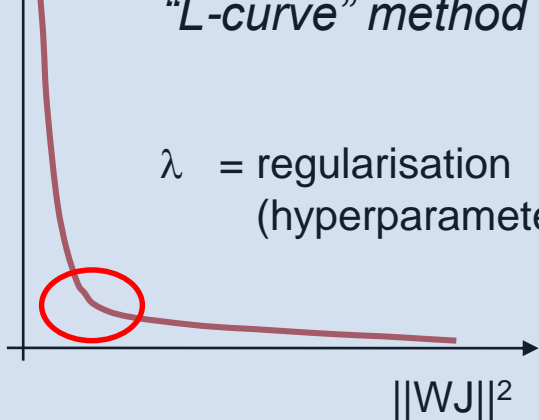
$$= (\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T [\mathbf{L} (\mathbf{W}^T \mathbf{W})^{-1} \mathbf{L}^T + \lambda \mathbf{C}^{(e)}]^{-1} \mathbf{Y}$$

“Tikhonov Solution”

$\|\mathbf{Y} - \mathbf{L}\mathbf{J}\|^2$

“L-curve” method

λ = regularisation
(hyperparameter)



$$\mathbf{W} = \mathbf{I}$$

“Minimum Norm”

$$\mathbf{W} = \mathbf{D}\mathbf{D}^T$$

“Loreta” (\mathbf{D} =Laplacian)

$$\mathbf{W} = \text{diag}(\mathbf{L}^T \mathbf{L})^{-1}$$

“Depth-Weighted”

$$\mathbf{W}_p = \text{diag}(\mathbf{L}_p^T \mathbf{C}_y^{-1} \mathbf{L}_p)^{-1}$$

“Beamformer”

$$\mathbf{W} = \dots$$

Inverse Problem: Equivalent PEB

Parametric Empirical Bayesian (PEB) 2-level hierarchical form:

$$\mathbf{Y} = \mathbf{L}\mathbf{J} + \mathbf{E}^{(e)} \quad \mathbf{E}^{(e)} \sim N(0, \mathbf{C}^{(e)})$$

$$\mathbf{J} = \mathbf{0} + \mathbf{E}^{(j)} \quad \mathbf{E}^{(j)} \sim N(0, \mathbf{C}^{(j)})$$

$\mathbf{C}^{(e)} = n \times n$ Sensor (error) covariance

$\mathbf{C}^{(j)} = p \times p$ Source (prior) covariance

Likelihood:

$$p(\mathbf{Y} | \mathbf{J}) = N(\mathbf{L}\mathbf{J}, \mathbf{C}^{(e)})$$

Prior:

$$p(\mathbf{J}) = N(0, \mathbf{C}^{(j)})$$

Posterior:

$$p(\mathbf{J} | \mathbf{Y}) \propto p(\mathbf{Y} | \mathbf{J})p(\mathbf{J})$$

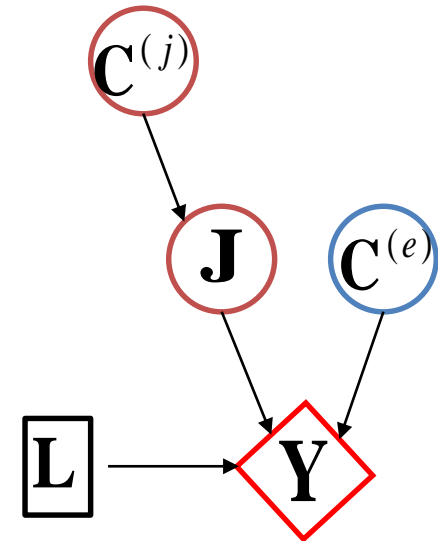
Maximum A Posteriori (MAP) estimate:

$$\hat{\mathbf{J}} = \mathbf{C}^{(j)}\mathbf{L}^T [\mathbf{L}\mathbf{C}^{(j)}\mathbf{L}^T + \mathbf{C}^{(e)}]^{-1}\mathbf{Y}$$

cf Classical Tikhonov:

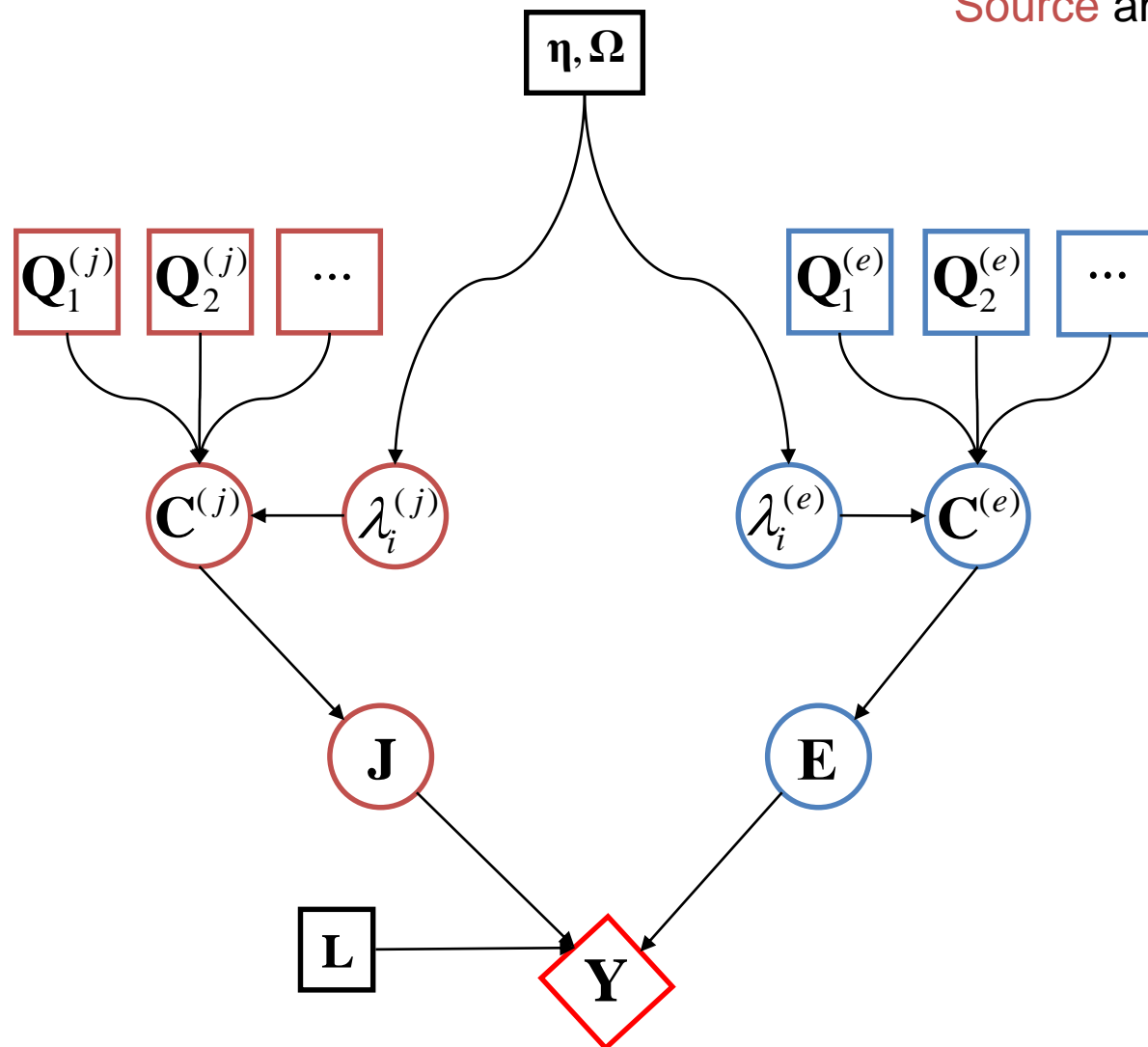
$$(\mathbf{W}^T\mathbf{W})^{-1}\mathbf{L}^T [\mathbf{L}(\mathbf{W}^T\mathbf{W})^{-1}\mathbf{L}^T + \lambda\mathbf{C}^{(e)}]^{-1}\mathbf{Y}$$

$$\Rightarrow \mathbf{C}^{(j)} = (\mathbf{W}^T\mathbf{W})^{-1}$$



PEB: Full Generative Model (DAG)

Source and sensor space



1. Obtain Restricted Maximum Likelihood (ReML) estimates of the hyperparameters (λ) by maximising the variational “free energy” (F):

$$\hat{\lambda} = \max_{\lambda} p(\mathbf{Y} | \lambda) = \max_{\lambda} F$$

2. Obtain Maximum A Posteriori (MAP) estimates of parameters (sources, \mathbf{J}):

$$\hat{\mathbf{J}} = \max_{\mathbf{J}} p(\mathbf{J} | \mathbf{Y}, \hat{\lambda}) = \max_{\mathbf{J}} F$$

3. Maximal F approximates Bayesian (log) “model evidence” for a model, m :

$$\ln p(\mathbf{Y} | m) = \ln \int \int p(\mathbf{Y}, \mathbf{J}, \lambda | m) d\mathbf{J} d\lambda \approx F(\mathbf{Y}, \hat{\mathbf{a}}, \hat{\Sigma}) \quad m = \{\mathbf{L}, \mathbf{Q}, \boldsymbol{\eta}, \boldsymbol{\Omega}\}$$

$$F(\mathbf{Y}, \hat{\mathbf{a}}, \hat{\Sigma}) \propto \underbrace{-\text{tr}(\mathbf{C}^{-1} \mathbf{Y} \mathbf{Y}^T) - \ln |\mathbf{C}|}_{\text{Accuracy}} \underbrace{- (\hat{\mathbf{a}} - \boldsymbol{\eta})^T \boldsymbol{\Omega}^{-1} (\hat{\mathbf{a}} - \boldsymbol{\eta}) + \ln |\hat{\Sigma} \boldsymbol{\Omega}^{-1}|}_{\text{Complexity}}$$

Accuracy

Complexity

(...where $\hat{\mathbf{a}}$ and $\hat{\Sigma}$ are the posterior mean and covariance of hyperparameters)

PEB: Multiple Sparse Priors

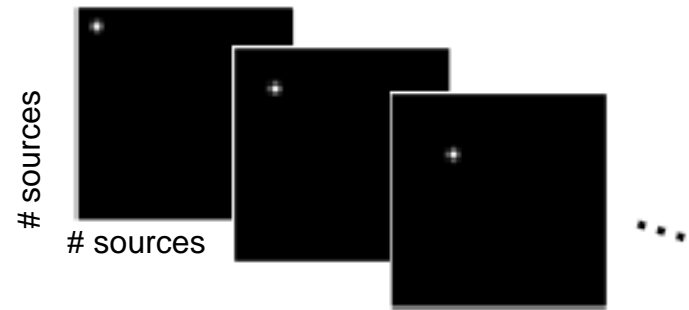
Hyperpriors allow the extreme of 100's source priors, or MSP

Three prior models

MNM $Q^\epsilon = I$

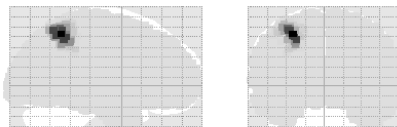
COH $Q^\epsilon = \{G, I\}$

MSP $Q^\epsilon = \{q_1 q_1^T, \dots, q_N q_N^T\}$

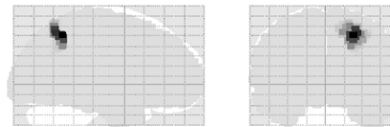


$$G(\sigma) = [q_1, \dots, q_N] = \sum_{i=0}^8 \frac{\sigma^i}{i!} A^i \approx \exp(\sigma A)$$

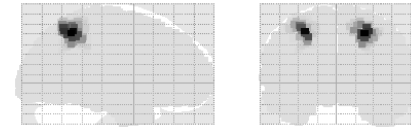
Left patch



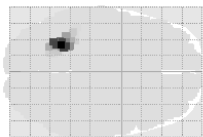
Right patch



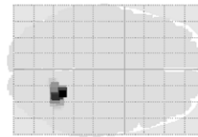
Bilateral patches



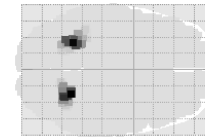
...



...



...



...

PEB: Multiple Sparse Priors

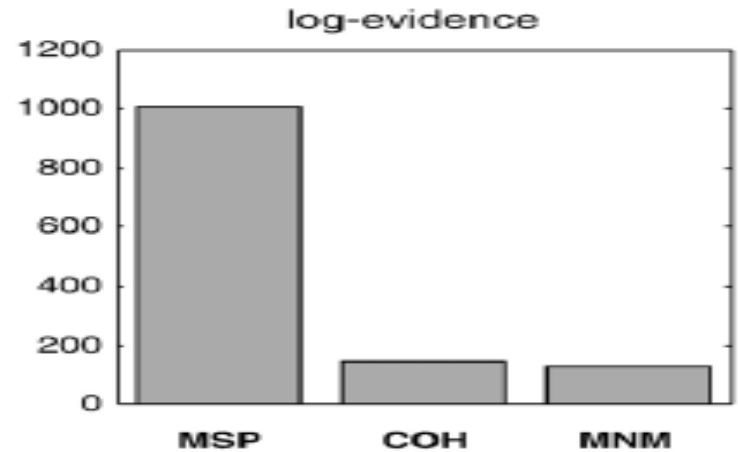
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Three prior models

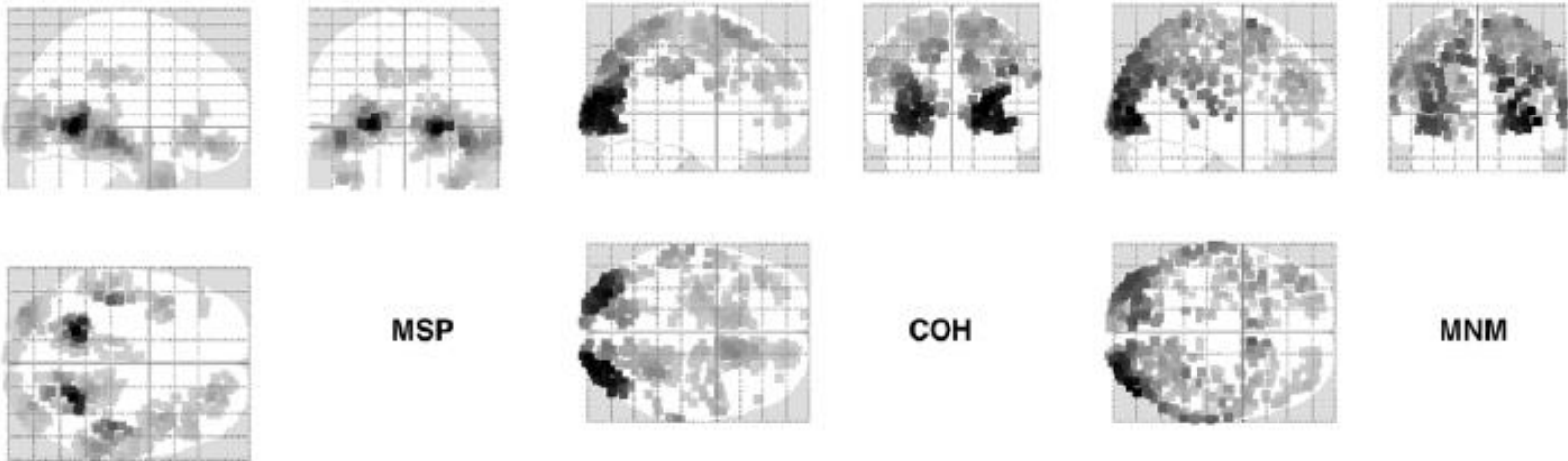
MNM $Q^\epsilon = I$

COH $Q^\epsilon = \{G, I\}$

MSP $Q^\epsilon = \{q_1 q_1^T, \dots, q_N q_N^T\}$



$$G(\sigma) = [q_1, \dots, q_N] = \sum_{i=0}^8 \frac{\sigma^i}{i!} A^i \approx \exp(\sigma A)$$



Summary:

- **Automatically** “regularises” in principled fashion...
- ...allows for **multiple** constraints (priors)...
- ...to the extent that multiple (100’s) of sparse priors possible (MSP)...
- ...(or multiple error components or multiple fMRI priors)...
- ...furnishes estimates of **model evidence**, so can compare constraints

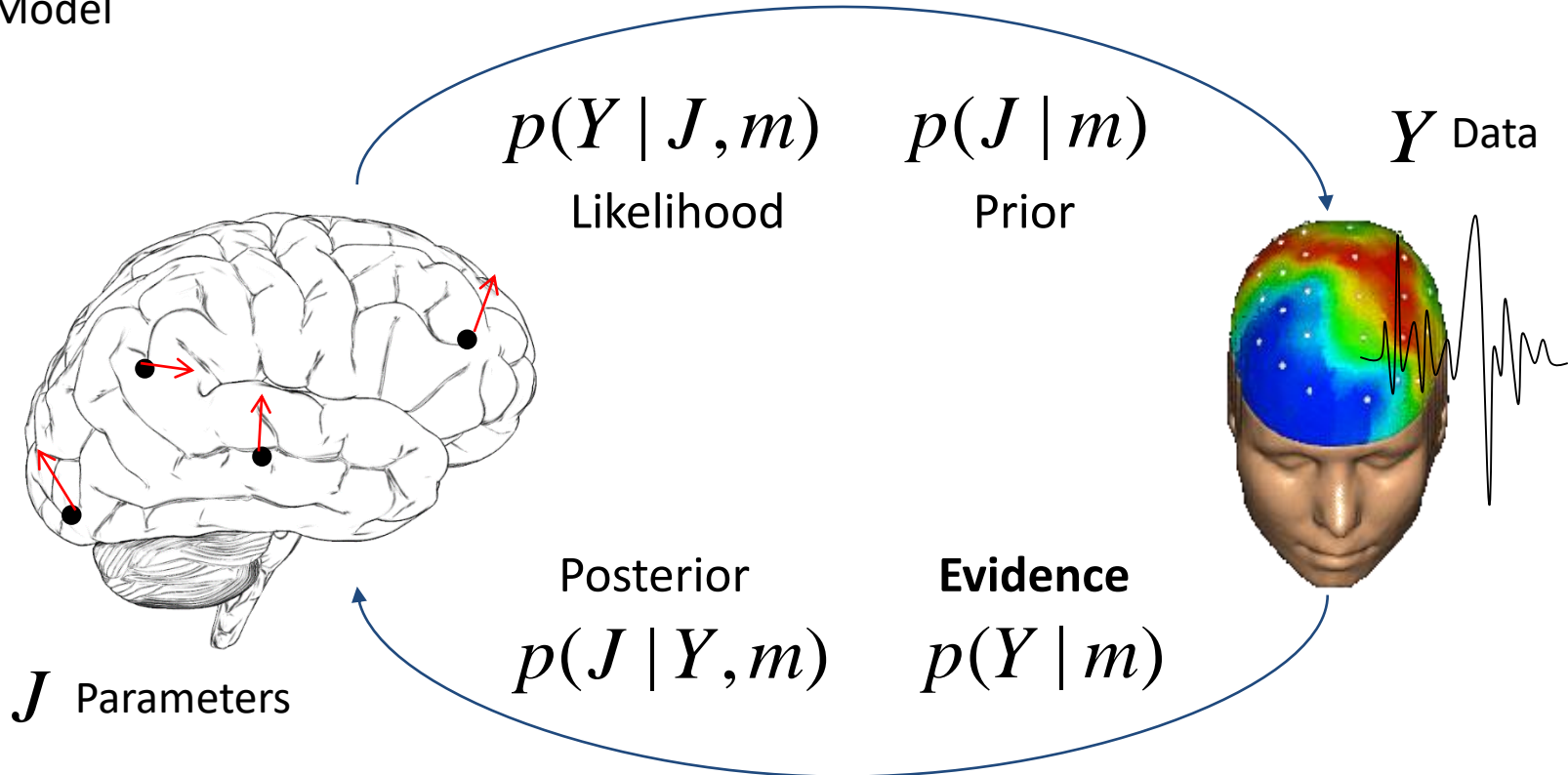
Bayesian Perspective

MRC

Cognition and
Brain Sciences Unit

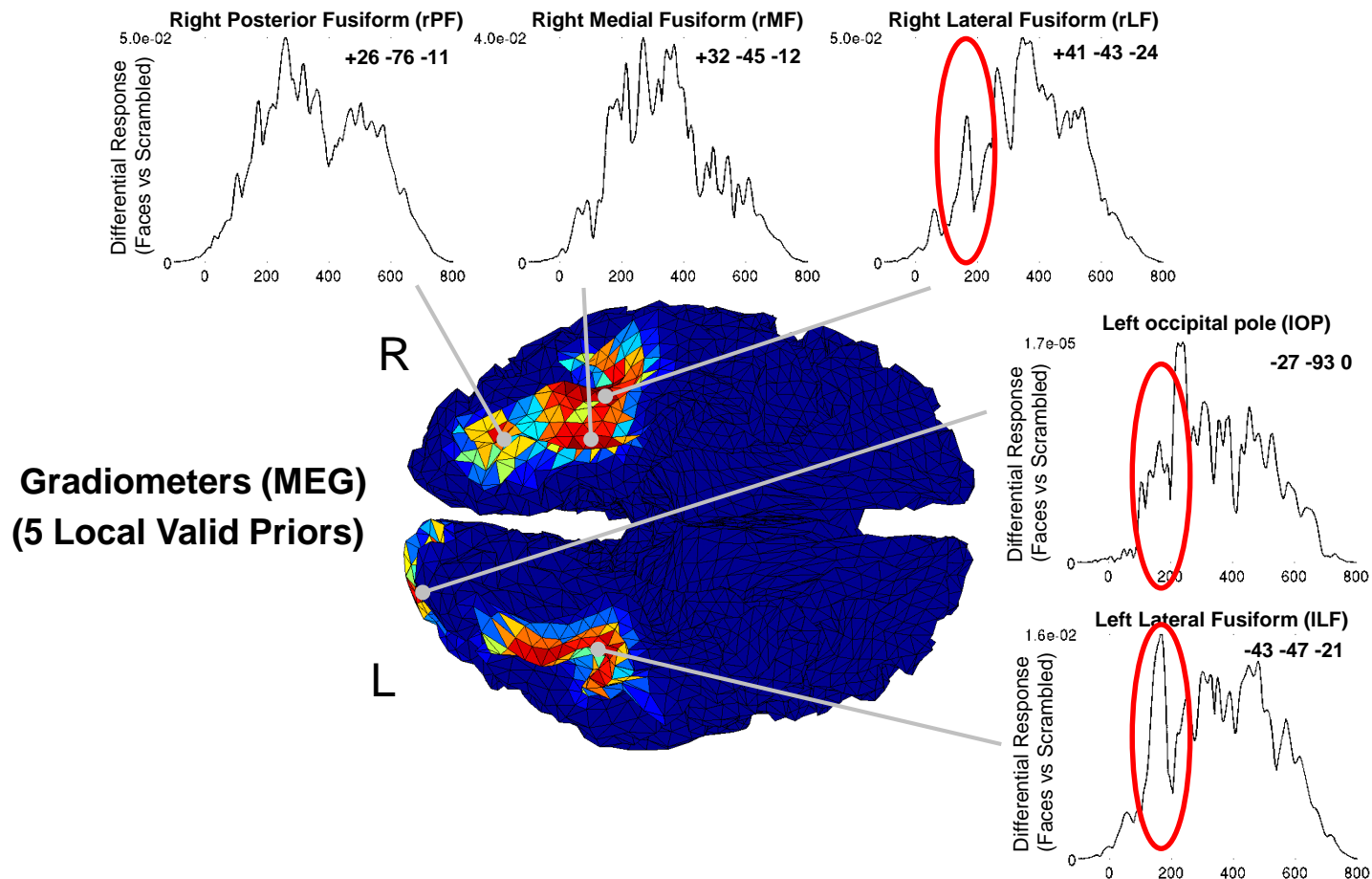
Forward Problem

m Model



Inverse Problem

Asymmetric Integration of M/EEG+fMRI

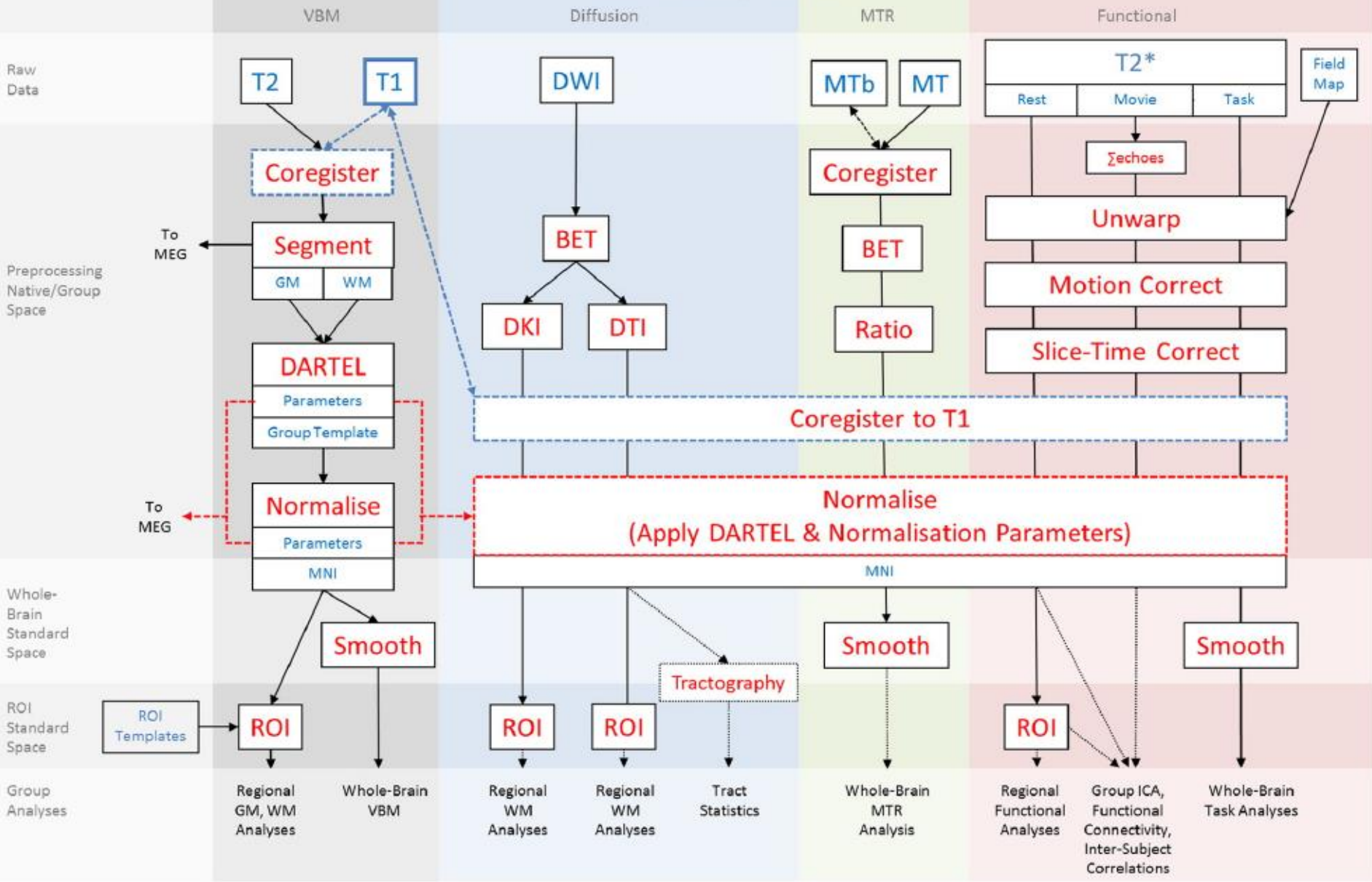


NB: Priors affect variance, not precise timecourse...

Some Model-Based Examples (local CamCAN examples)

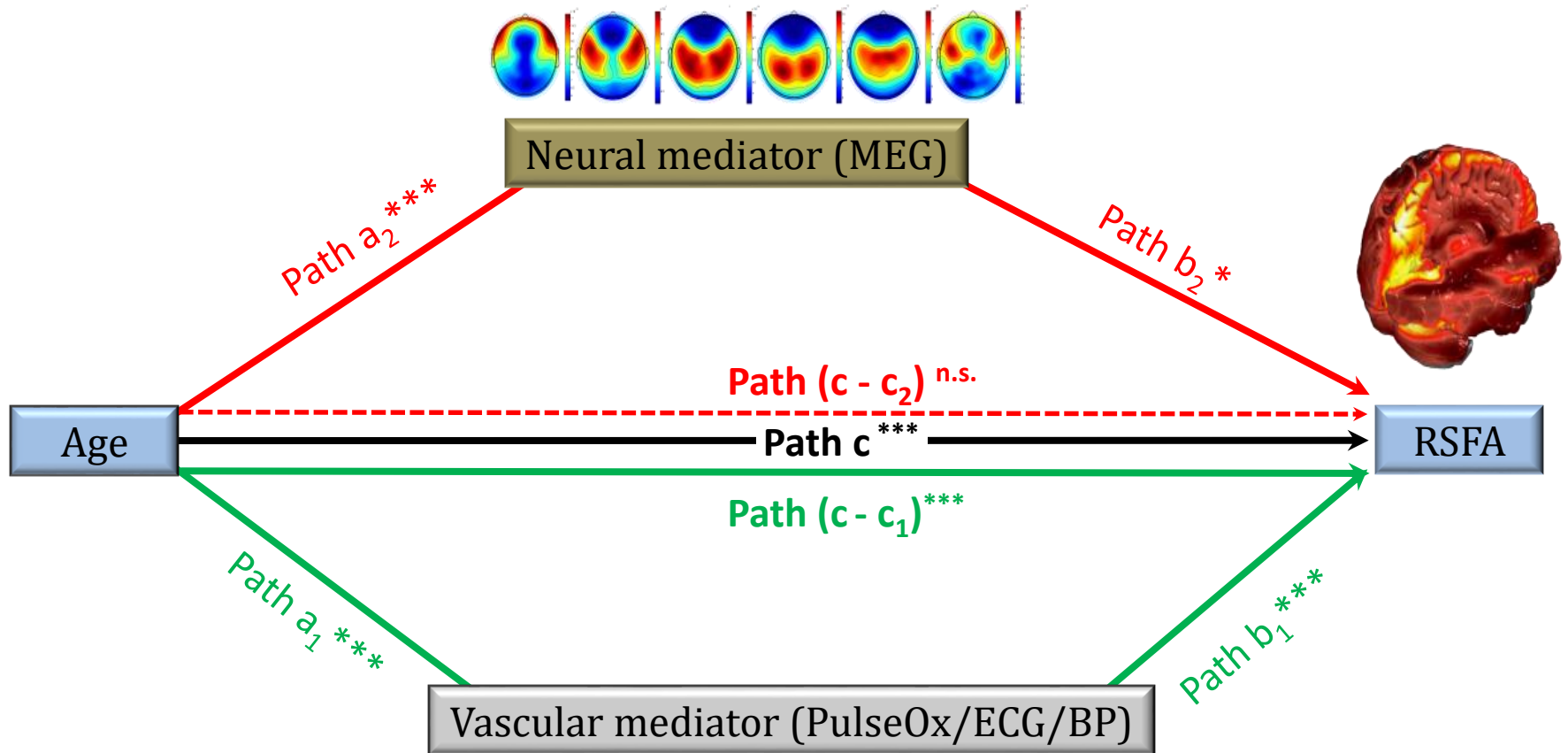
1. Combining T1-, T2-, Diffusion- and MT-weighted images for segmentation and normalisation
2. Univariate mediation: Using MEG to separate effects of age on neural vs vascular responsivity in fMRI
3. Univariate mediation: Using DKI to investigate effects of age on MEG latency
4. Multivariate Structural Equation Modelling (SEM) to separate GM and WM contributions to executive function

MRI Processing Pipelines



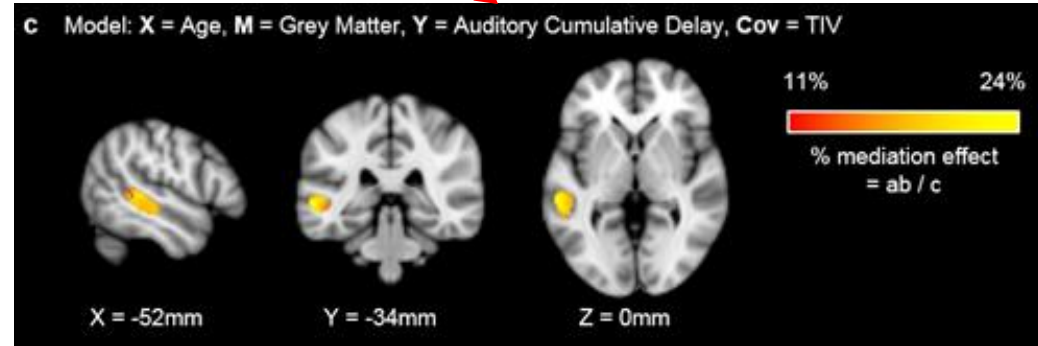
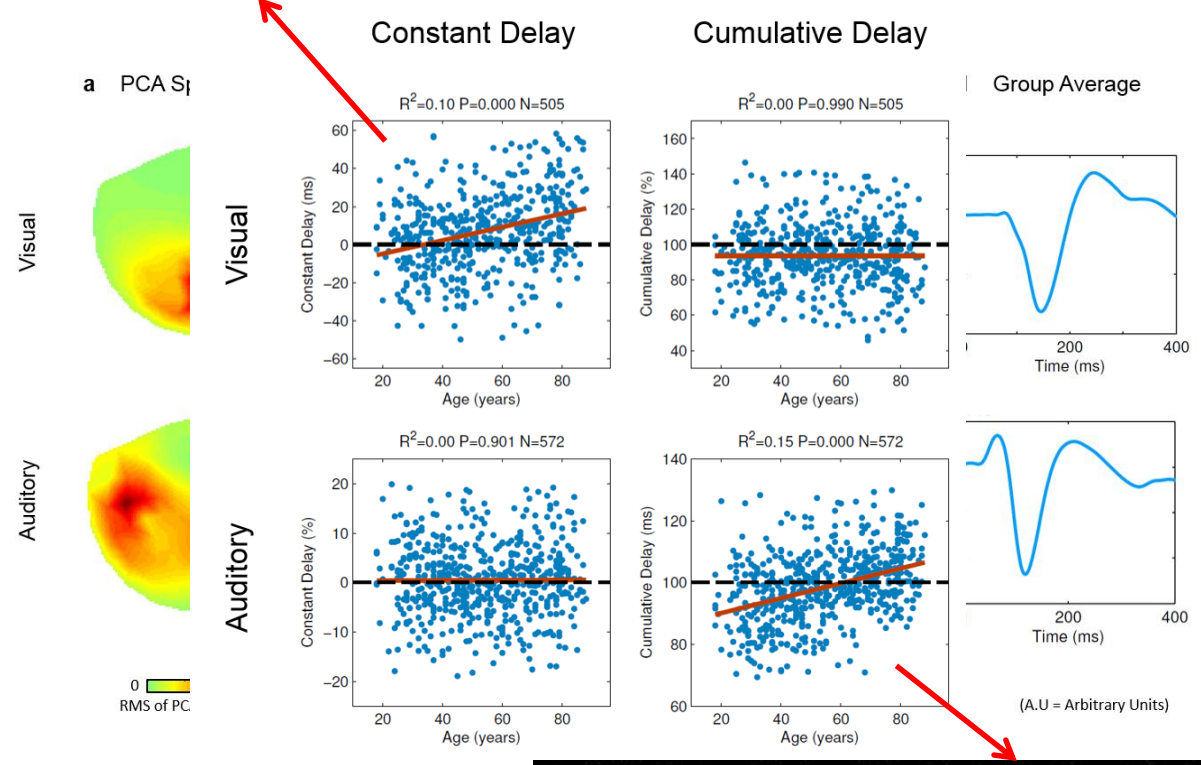
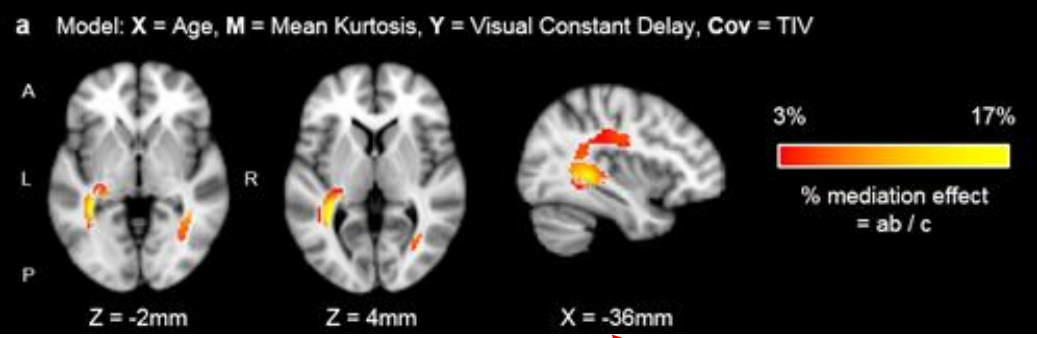
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Some Model-Based Examples (local CamCAN examples)

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