

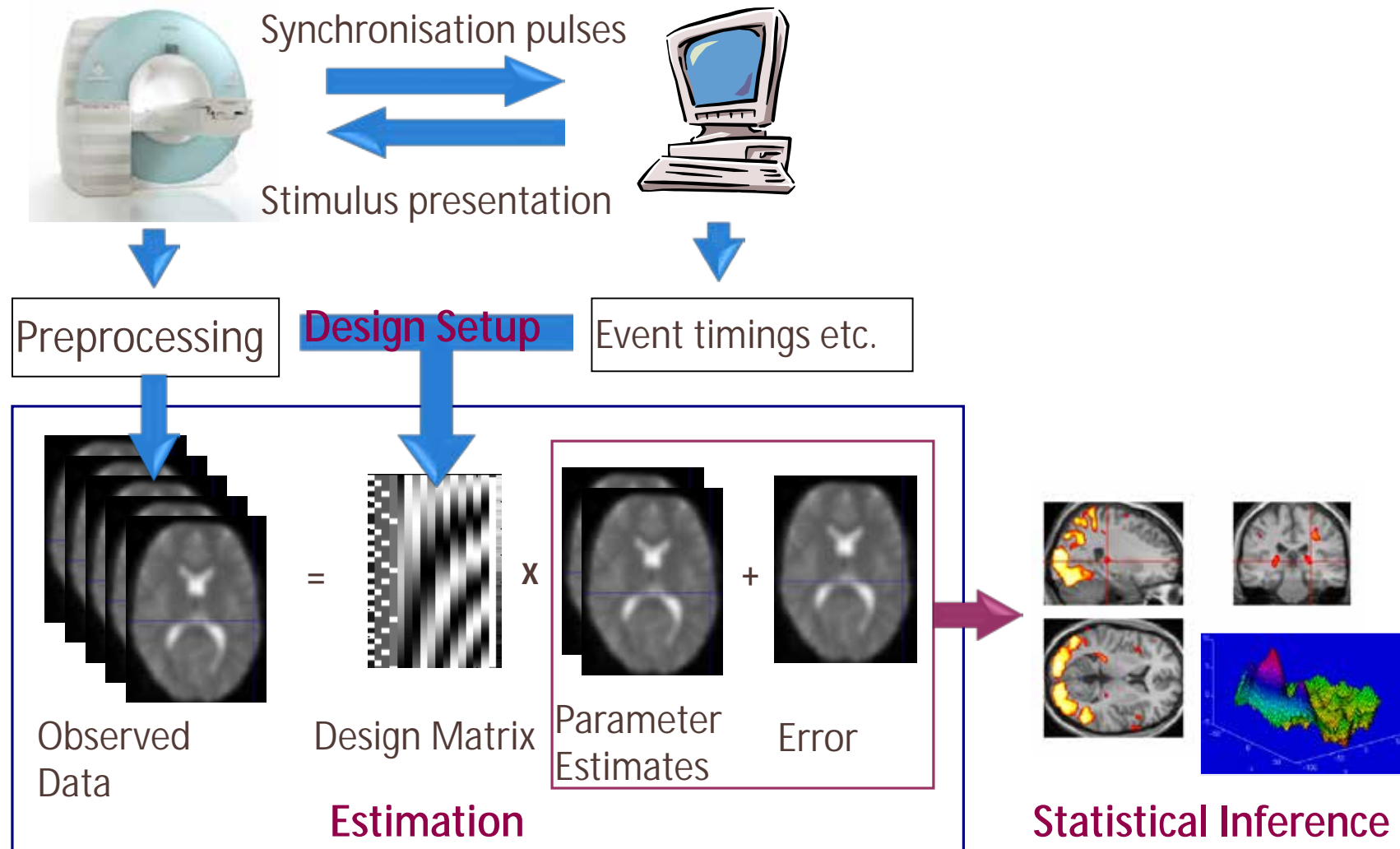
Single subject analysis using GLM

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With thanks to Russell Thompson, Rik Henson, Matthew Brett and the authors of the HBF

A functional experiment



General Linear Model – Theory

- **GLM**
 - models observed data (dependent variable) – Y
 - as a linear combination (parameter estimate – β) of
 - regressors/predictor variables/explanatory variables (EV) (independent variables) – X

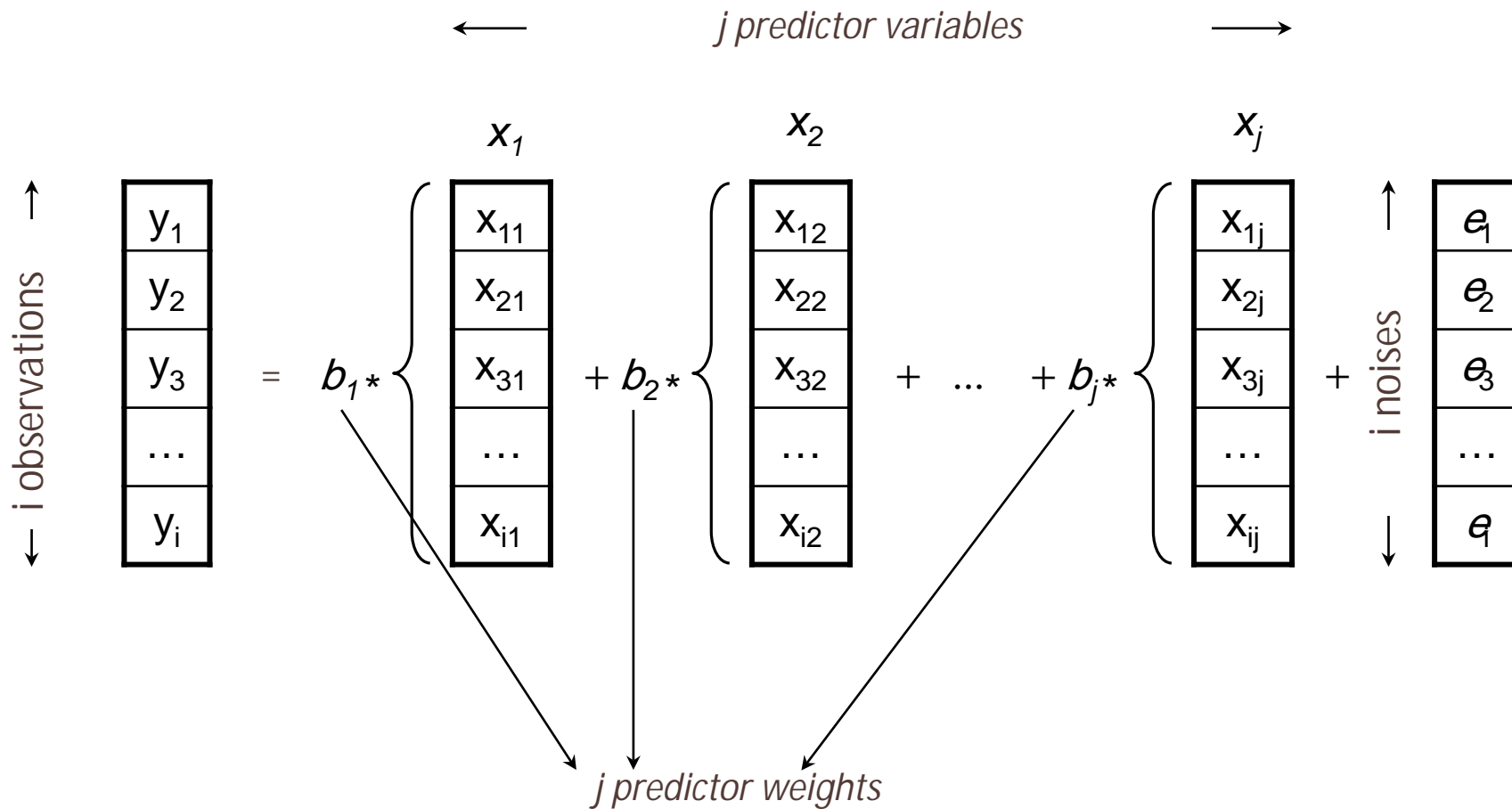
$$Y = X\beta + \epsilon$$

- AN(C)OVA, t-test, (multiple) regression, LDA, CCA are also GLMs.
- Relationship between a dependent variable and one or more independent variables

General Linear Model – Theory

- GLM

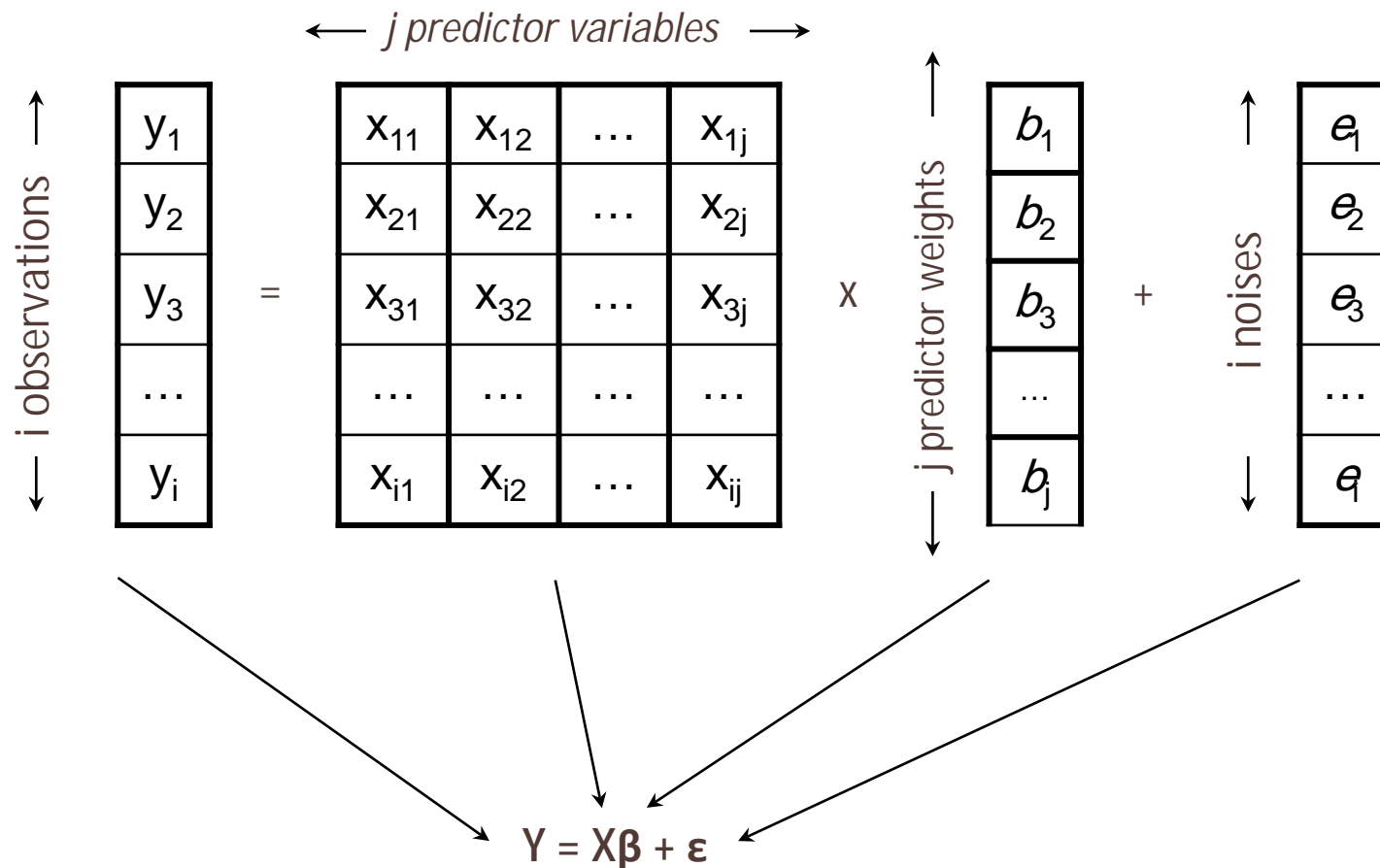
- For i observations modelled using j predictor variables:



General Linear Model – Theory

- GLM

- For i observations modelled using j predictor variables:



General Linear Model – Application

- **Mass univariate approach:**
 - Model $X_{1-i,1-j}$ estimated for each voxel independently (multiple tests)
 - For each voxel:
 - Y_{1-i} : timeseries of i observations at a single voxel
 - B_{1-j} for each of the j predictors



- Series of β_{1-j} images (beta0001-beta000j)

General Linear Model – Application

- **Model:**
 - Contains all known source of variance:
 - Controlled factors (e.g. stimuli)¹
 - All nuisance variables¹
 - Assumption about noise (ϵ)
 - High-pass filter
 - Temporal autocorrelation
 - Spikes (aa)
 - Movement parameters (SPM)
 - PhysIO Toolbox
 - Imaging Wiki/PhysNoise
 - GLMDenoise (aa)
 - FIX (FSL)





General Linear Model – Application

- **Model vs. Design:**
 - Model
 - Event-related (duration = 0)
 - Epoch-based (duration > 0)
 - Can be modelled with events
 - To model HRF along the epoch (e.g. FIR)
 - But: $\hat{\beta}pR_{\text{event}} \sim \hat{\beta}pR_{\text{epoch}} / n\text{Event}^1$
 - Design
 - Blocked (fix SOA)
 - Randomized (variable SOA) – jittering
 - Lower predictability (à subject is more engaged)
 - Higher estimability (β samples from various phases of the HRF)

General Linear Model – Application

- Model vs. Design:

Model \ Design	Epoch-based	Event-related
Blocked (fix SOA)	“block-design”	“non-jittered event-related design”
Randomized (variable SOA)	“randomised block-design”	“jittered event-related design”

General Linear Model – Application

- **BOLD response – Kernel:**

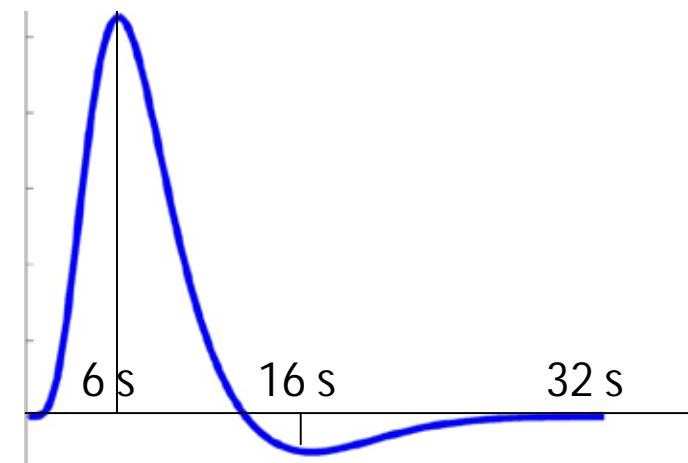
- stereotyped pattern of response (based on primary sensory areas)

- Canonical Haemodynamic Response Function (HRF) – $spm_hrf(TR,p)$

- Double-gamma function

- uses 7 parameters

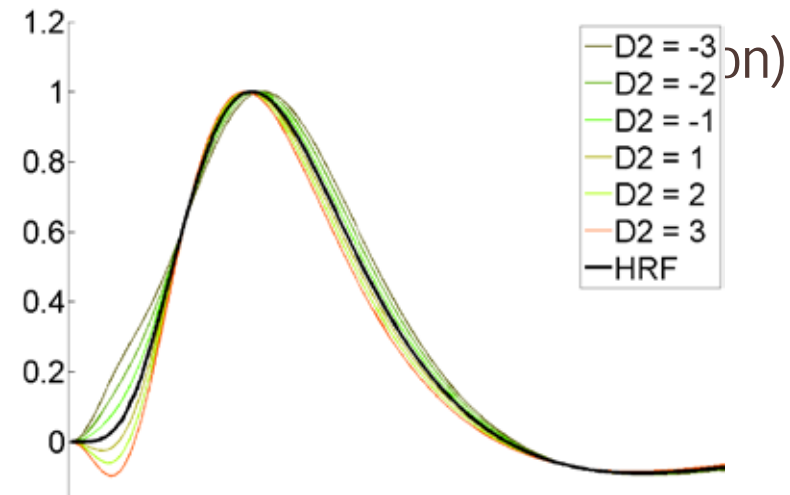
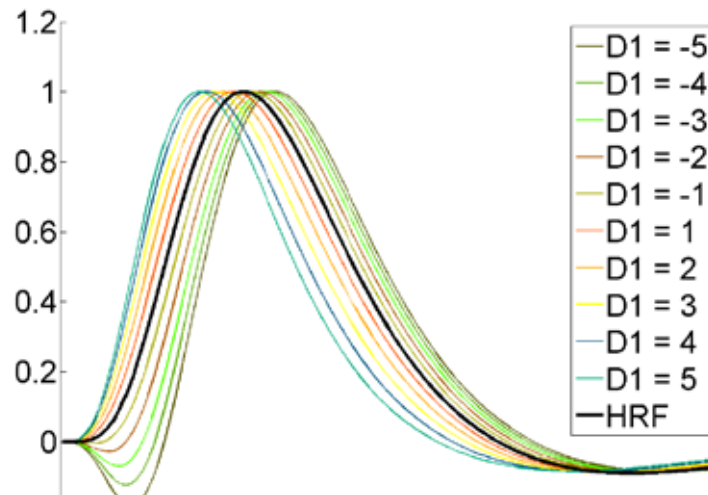
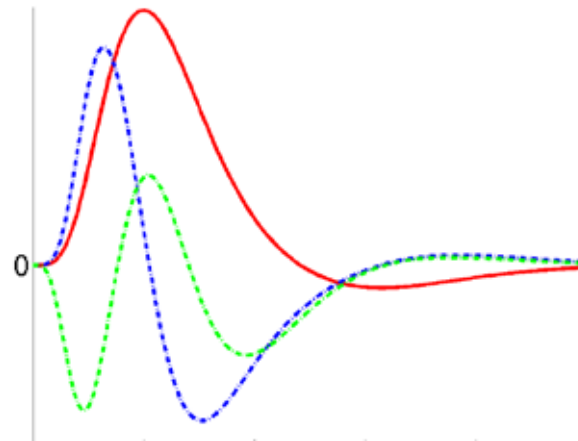
- p(1) - delay of response (relative to onset) 6
- p(2) - delay of undershoot (relative to onset) 16
- p(3) - dispersion of response 1
- p(4) - dispersion of undershoot 1
- p(5) - ratio of response to undershoot 6
- p(6) - onset (seconds) 0
- p(7) - length of kernel (seconds) 32



General Linear Model – Application

- **HRF**

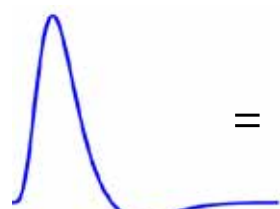
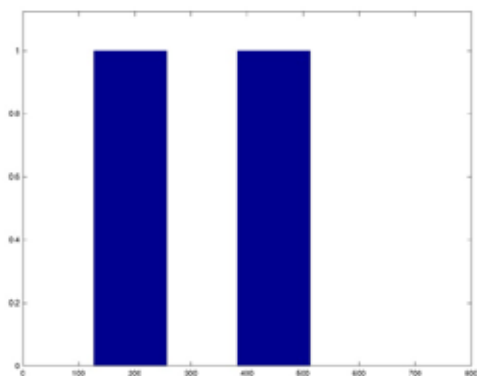
- Derivatives (to “adjust” HRF¹):



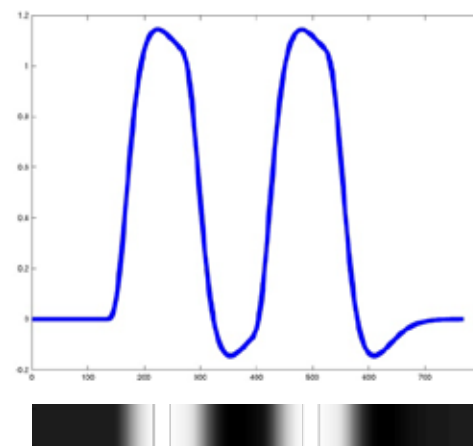
General Linear Model – Application

- BOLD response - Convolution:

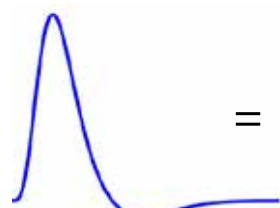
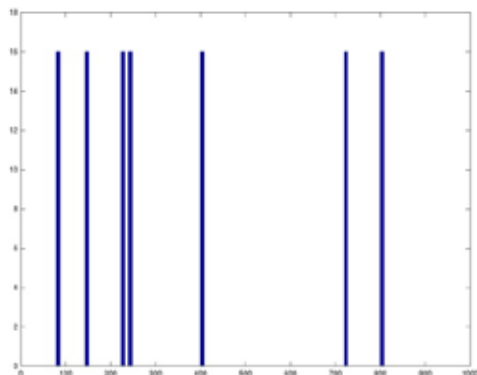
- Epochs



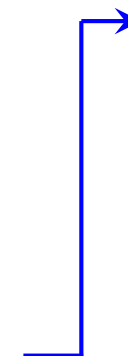
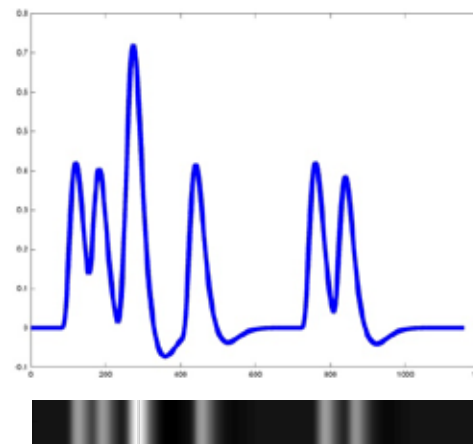
=



- Events



=



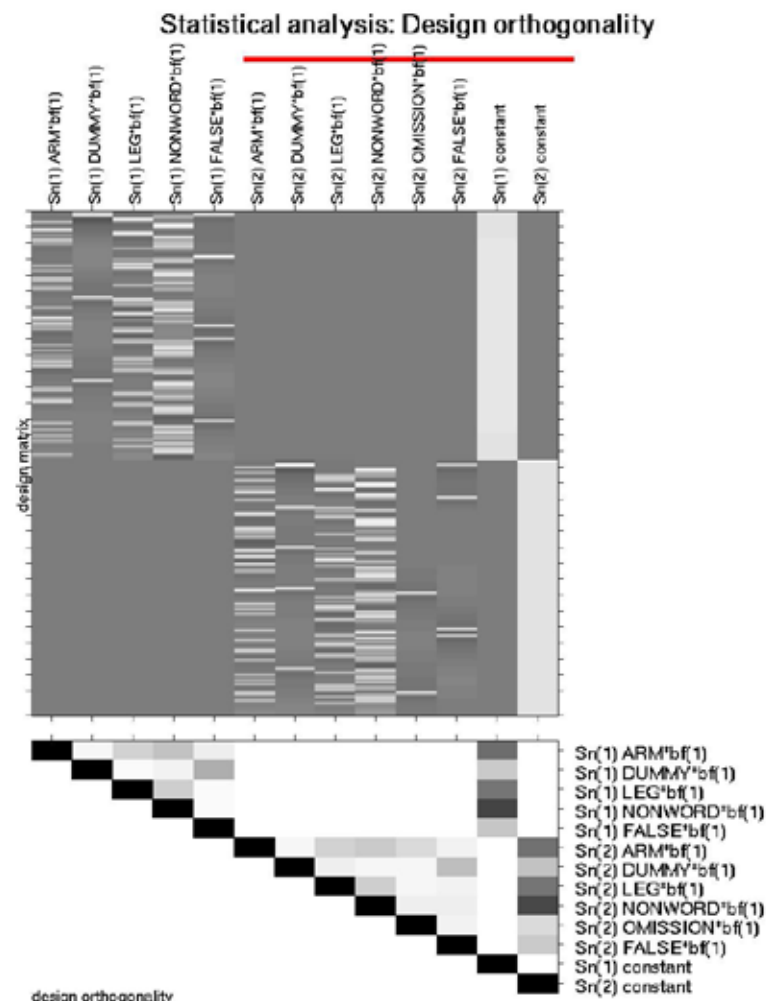
General Linear Model – Application

- **Non-orthogonality**

- Pairwise correlation (SPM)
- Rank deficiency (more general)
 - If any column of X is a linear combination of any others



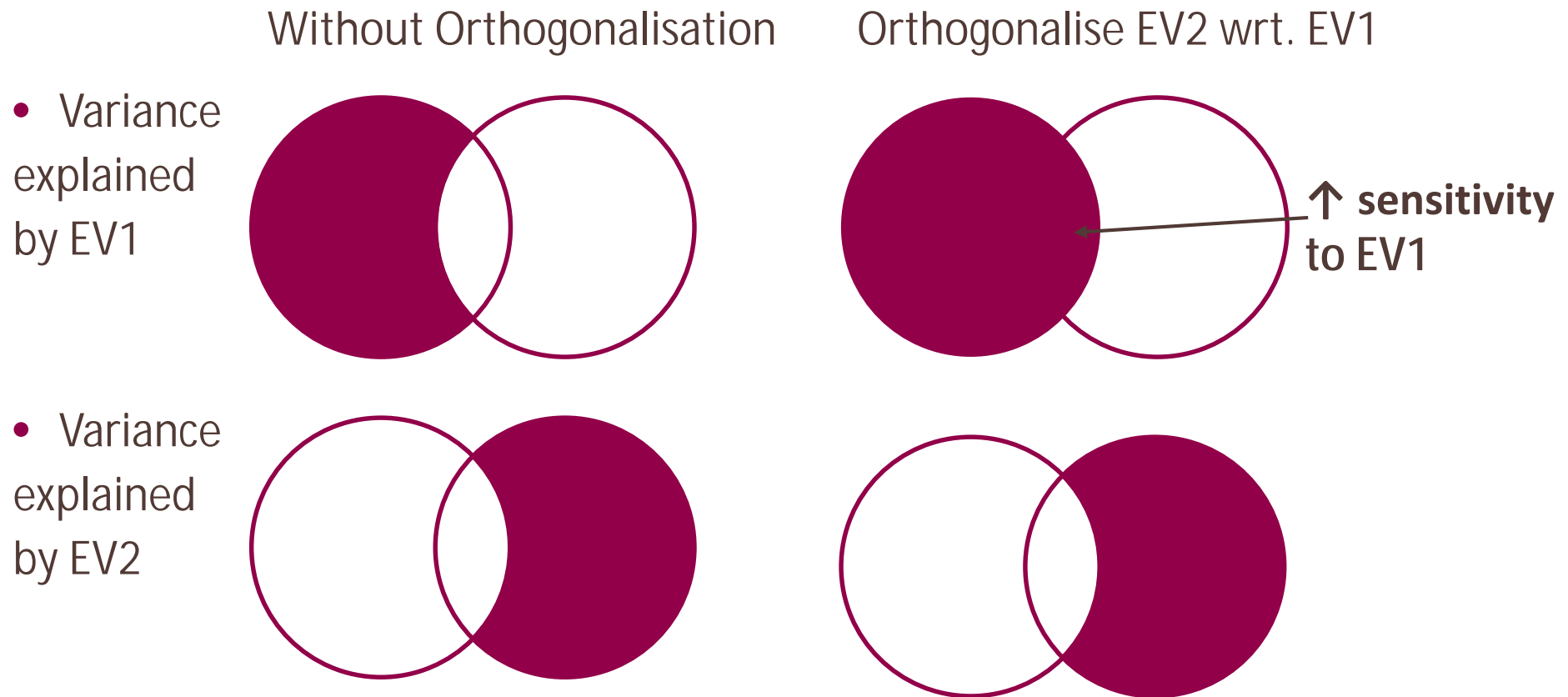
- Some parameters cannot be estimated uniquely (e.g. in case of EV1 and EV2)
 - ↓ efficiency for EV1, EV2 and EV1+EV2
 - Good efficiency for EV1-EV2



Measure : abs. value of cosine of angle between columns of design matrix
Scale : black - colinear (cos=+1/-1)
white - orthogonal (cos=0)
gray - not orthogonal or colinear

General Linear Model – Application

- **Orthogonalisation**
 - Assigning shared explained variance



General Linear Model – SPM input

- **Regressor = predictor variables/explanatory variables** – One β for each regressor
 - Condition \otimes HRF
 - Name
 - Onset
 - Duration
 - Modulation
 - Covariate: it will not be convolved with HRF
- **aa_user_fmri.m**
 - `aas_addevent(aap, 'aamod_firstlevel_model', mriname, sessname, onsets, durations, modulation)`
 - `aas_addcovariate(aap, 'aamod_firstlevel_model', mriname, sessname, covarName, covarVector, HRF, interest)`



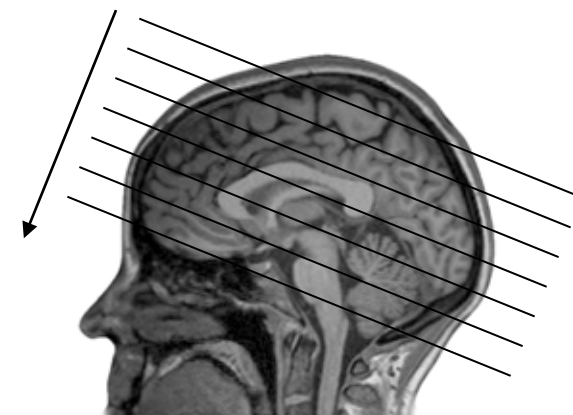
General Linear Model – SPM input

- **Modulation: effect with many level (or continuous)**
 - Parametric modulation
 - Stimulus strength
 - Response accuracy
 - Temporal modulation = Parametric modulation using onset as parameter
 - Habituation
 - Learning
 - Polynomial Expansion: higher-order effects
- Disadvantages
 - Correlated regressors → Orthogonalisation
 - < SPM12: always on (left to right)¹
 - SPM12: switchable
 - Difficult to set up interactions between factors

General Linear Model – SPM input

- “**Microtiming**” ~ **Slicetiming**¹

- Microtime resolution: time bins within one TR
 - Highest temporal precision = TR / MicRes
 - Divided equally for the whole TR
- Microtime onset: first time bin



- ²Sparse EPI: e.g. $TR = 3s$, $TA = 2s$, 20 slices



- Use middle slice (#10) as reference:

Slicetiming		Microtiming²	
Slice order	20:-1:1	Microtime resolution	30
Reference slice	10	Micortime onset	10



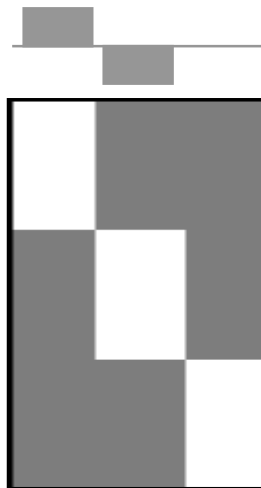
General Linear Model – SPM output

- beta_XXXX – $\hat{\beta}$ (XXXX: for each EV)
- mask – brain mask (voxels included in the analysis)¹
- ResMS – $\hat{\epsilon}$ (mean squared)
 - Heterogeneity may indicate unexplained variance in the data
- RPV – RESELS Per Voxel (local smoothness)
 - $RPV = FWHM_{in\ voxel}^{-3}$
 - ≤ 0.037 (RESEL ≥ 3 voxel) to ensure the minimum smoothness for GRFT²

General Linear Model – Contrasts

- **Specific hypotheses to be tested using t or F statistics**
 - How each predictor (column of the design matrix) plays a role
 - E.g. condition 1 > condition 2 à contrast [1 -1 0]

$$\mathbf{c} = \begin{bmatrix} 1 & -1 & 0 \end{bmatrix}$$



- **aa_user_fmri.m**
 - `aas_addcontrast(aap, 'aamod_firstlevel_contrasts', mri_name, format, vector, conname, contype)`



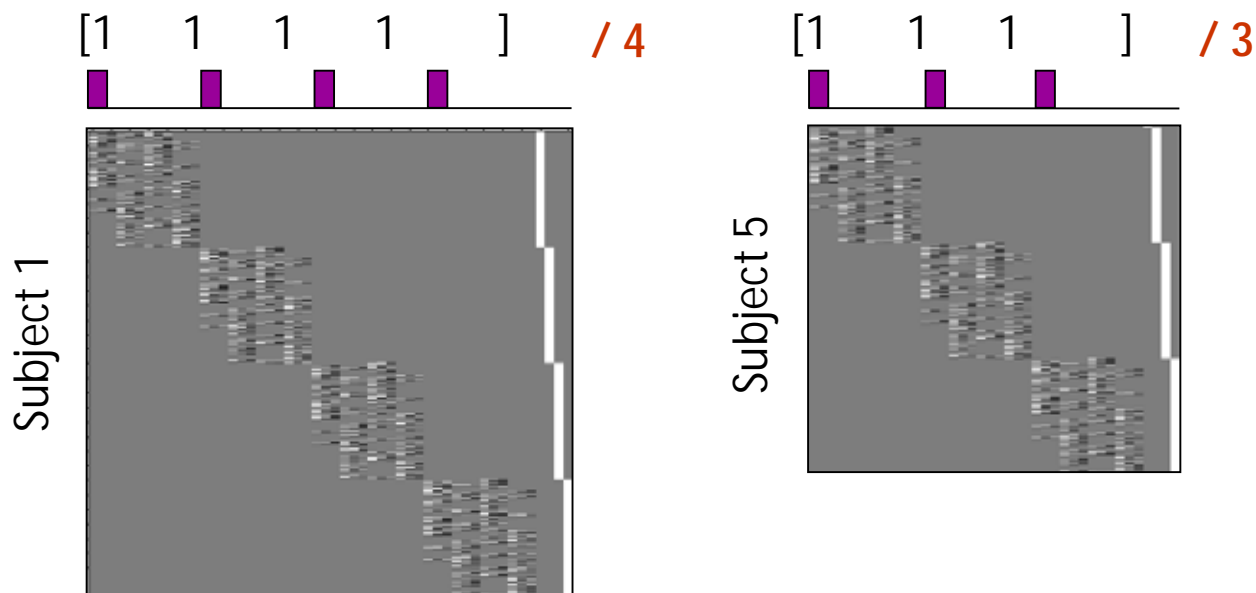
General Linear Model – Contrasts

- **F contrast:**
 - Model comparison: How much variance is explained by the model including the conditions of interest (e.g. movement parameters)?
 - Non-directional
 - Can contain more rows (OR)
 - [1 0 0; % EV1 > baseline OR
 - 0 1 0] % EV2 > baselineHow much variance is explained by EV1 and EV2? Should we include them in the model?¹
 - SPM output:
 - `ess*.img` (Extra Sum of Squares)
 - `spmF*.img` (F-map \rightarrow p)
- **T contrast:**
 - Hypothesis test: How do the conditions of interest relate to each other and/or to the baseline?
 - Directional
 - Can contain only one row
 - SPM output:
 - `con*.img` (Contrast)
 - `spmT*.img` (T-map \rightarrow p)

General Linear Model – Contrasts

- **T contrast:**

- The contrast vector sums to 0, 1 or -1
- Positive weights sum to 1
- Negative weights sum to -1
- Scaling issue
 - T-stat does not depend on scaling (of both the regressors and the contrast).
 - Contrast¹ depend on scaling² → consistency across subjects!





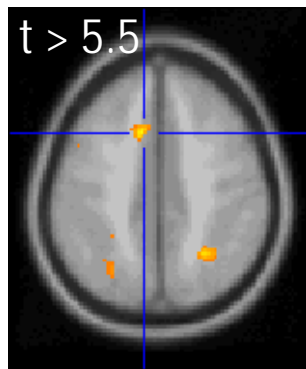
General Linear Model – Contrasts

- **T contrast:**
 - Examples¹:
 - $[1\ 0\ 0]$: condition 1 > unmodelled/implicit baseline
 - $[2\ -1\ -1]$: condition 1 > sum of conditions 2 and 3
 - $[1\ -0.5\ -0.5]$: condition 1 > average of conditions 2 and 3
 - $[-3\ -1\ 1\ 3]$: linear increase over 4 conditions

Statistical Inference

- **How much is enough?**
 - Converting a continuous statistical value (p) to a binary decision \rightarrow cut-off

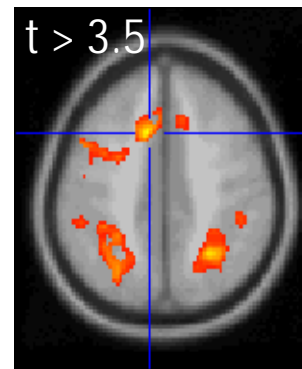
High Threshold



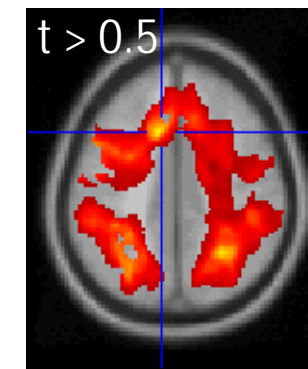
Good Specificity
Poor Sensitivity
(risk of false negatives)

Very Certain¹

Medium Threshold



Low Threshold



Good Sensitivity
Poor Specificity
(risk of false positives)

Quite Uncertain¹

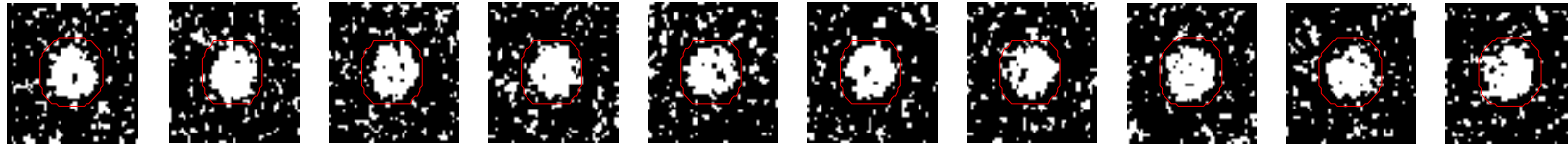


Statistical Inference

- **How to make certainty comparable?**
- **Multiple comparison**
 - Testing 100,000 random voxels at $p = 0.05$ à 5000 “significant” by chance (false positives, or “type I” errors)¹
- **FamilyWise Error Rate (FWER):**
 - Chance of any false positive in the “family” (any similar measurement)
- **False Discovery Rate (FDR):**
 - Chance/Proportion of false positives in the rejected tests (i.e. suprathreshold results)
 - To enable in SPM:
 - *global defaults*
 - *defaults.stats.topoFDR = 0;*

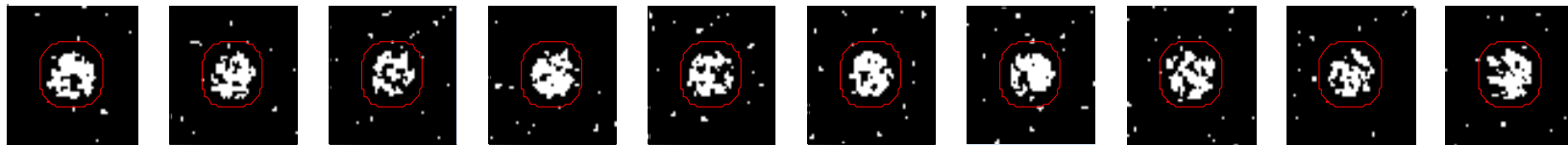
Statistical Inference

Control of Per Comparison Rate (i.e. none) at 10%



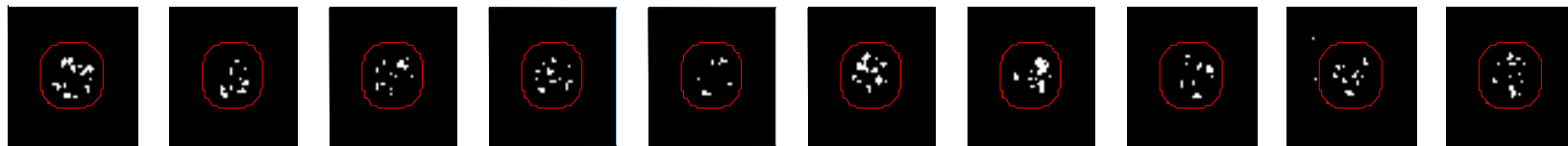
11.3% 11.3% 12.5% 10.8% 11.5% 10.0% 10.7% 11.2% 10.2% 9.5%
Percentage of Null Pixels that are False Positives

Control of False Discovery Rate at 10%



6.7% 10.4% 14.9% 9.3% 16.2% 13.8% 14.0% 10.5% 12.2% 8.7%
Percentage of Activated Pixels that are False Positives

Control of Familywise Error Rate at 10%



Occurrence of Familywise Error

FWE

Statistical Inference

- **FWE**

- Bonferroni correction: $p_{(\text{corrected})} = p_{(\text{uncorrected})} / n_{\text{comparisons}}$
 - Overly conservative in fMRI due to spatial dependence:
 - Nearby voxels are correlated: smoothness
 - Smoother data = More voxels in correlation \rightarrow fewer indep. elements
- ↓
- Gaussian Random Field Theory (GRFT) – default in SPM
 - Estimate the true number of independent/RESolution Elements (RESEL) using GRFT \rightarrow RPV.img: RESEL Per Voxel (local smoothness)
 - Corrects for the number of RESELS \rightarrow Less conservative than Bonferroni



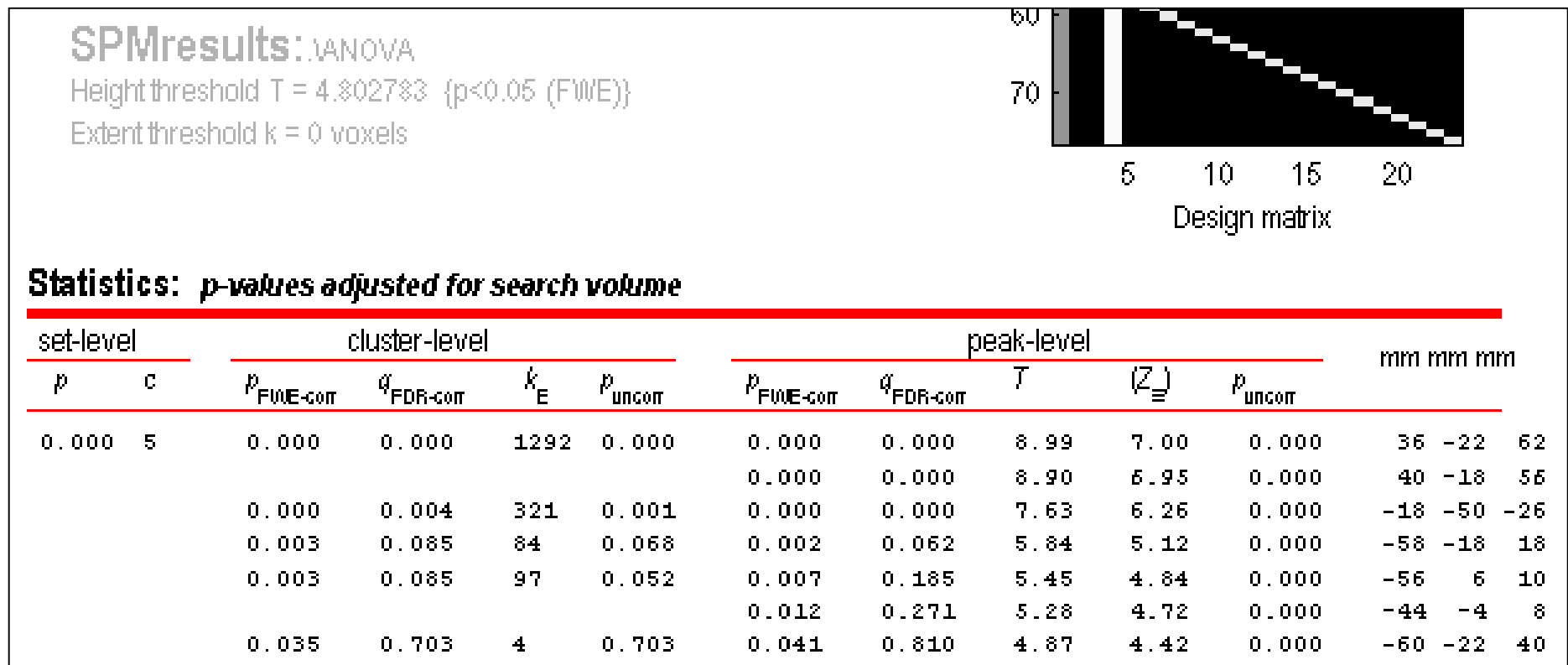
Statistical Inference

- **aa default**
 - aamod_firstlevel_threshold.xml
- **aa_user_fmri.m / aap_parameters.mat**
 - aap.tasksettings.aamod_firstlevel_threshold.threshold.correction = 'none';
 - aap.tasksettings.aamod_firstlevel_threshold.threshold.p = 0.001;
 - aap.tasksettings.aamod_firstlevel_threshold.threshold.extent = 0;

Statistical Inference

Levels of inference

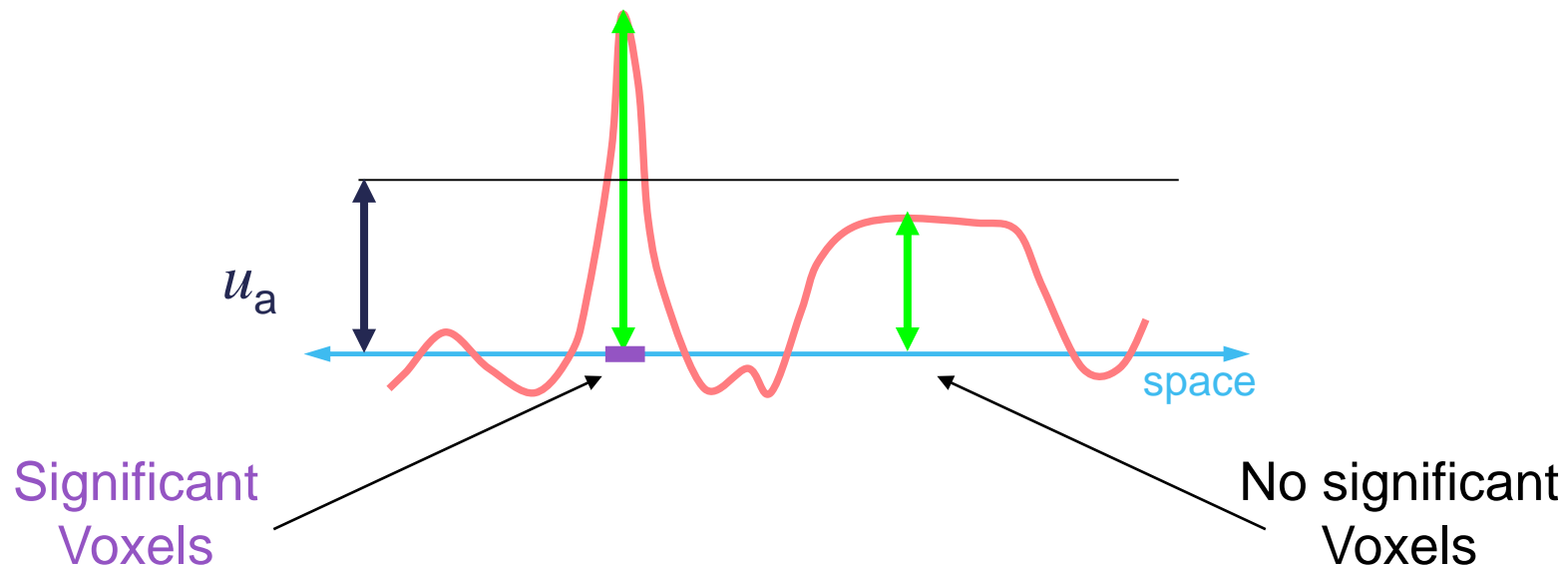
- Peak
- Cluster
- Set



Statistical Inference

Levels of inference

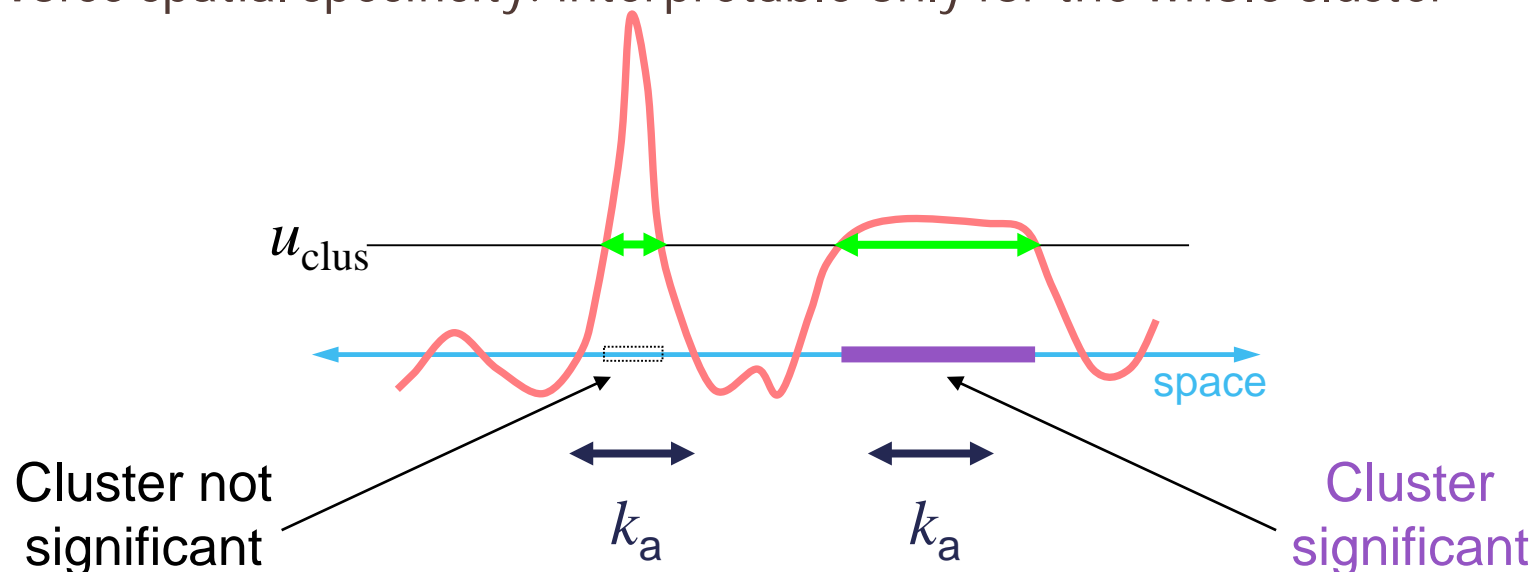
- **Peak-level (voxel-level) inference**
 - Probability p of that or higher peak voxel intensity (i.e. T/F-value)
 - Retains voxels above the threshold ($p \leq u_a$)
- Best spatial specificity: interpretable for each voxel



Statistical Inference

Levels of inference

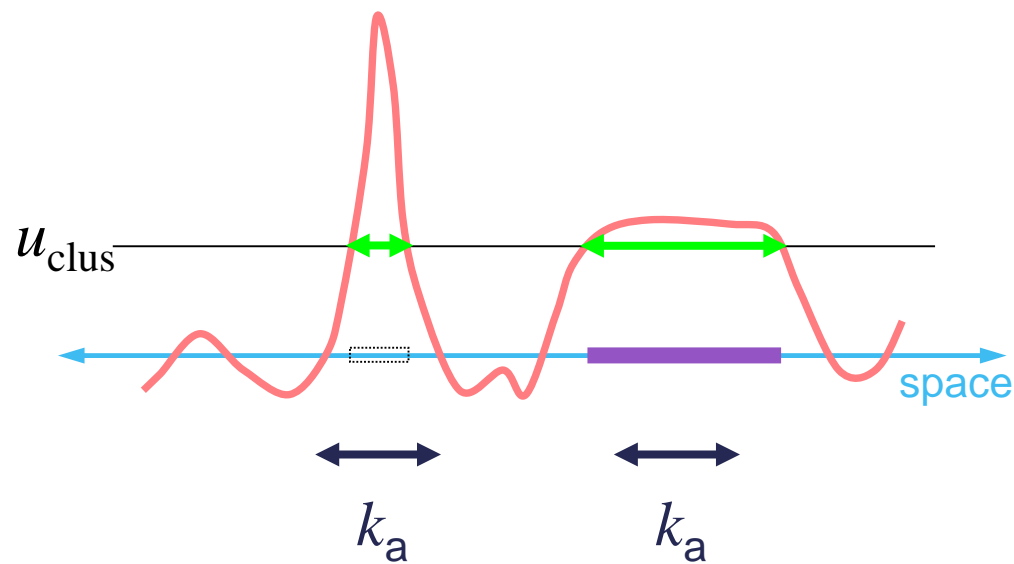
- **Cluster-level inference (default in FSL)**
 - Probability p of that or larger number of neighbouring significant voxels
 - Two thresholds
 - Define significant voxels by “cluster-forming” threshold ($p \leq u_{clus}$)
 - Retains only large clusters ($p \leq P(k_a)$)
- Worse spatial specificity: interpretable only for the whole cluster



Statistical Inference

Levels of inference

- **Set-level inference**
 - Probability p of that or larger number of significant clusters
 - Worst spatial specificity: interpretable only globally

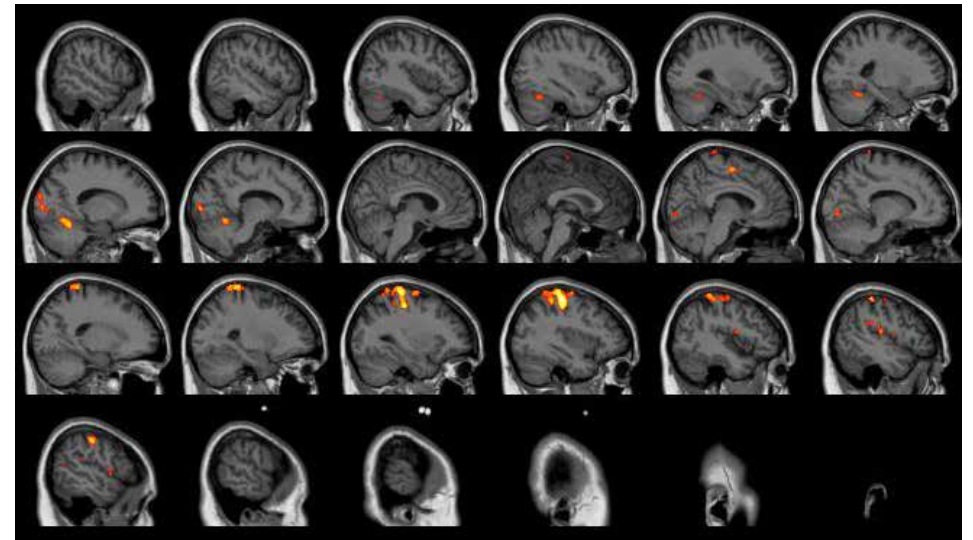
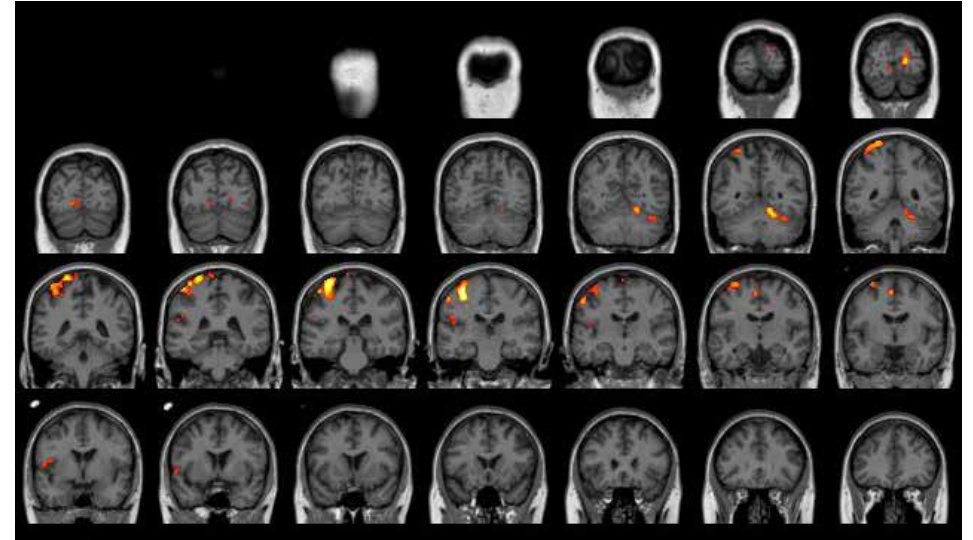
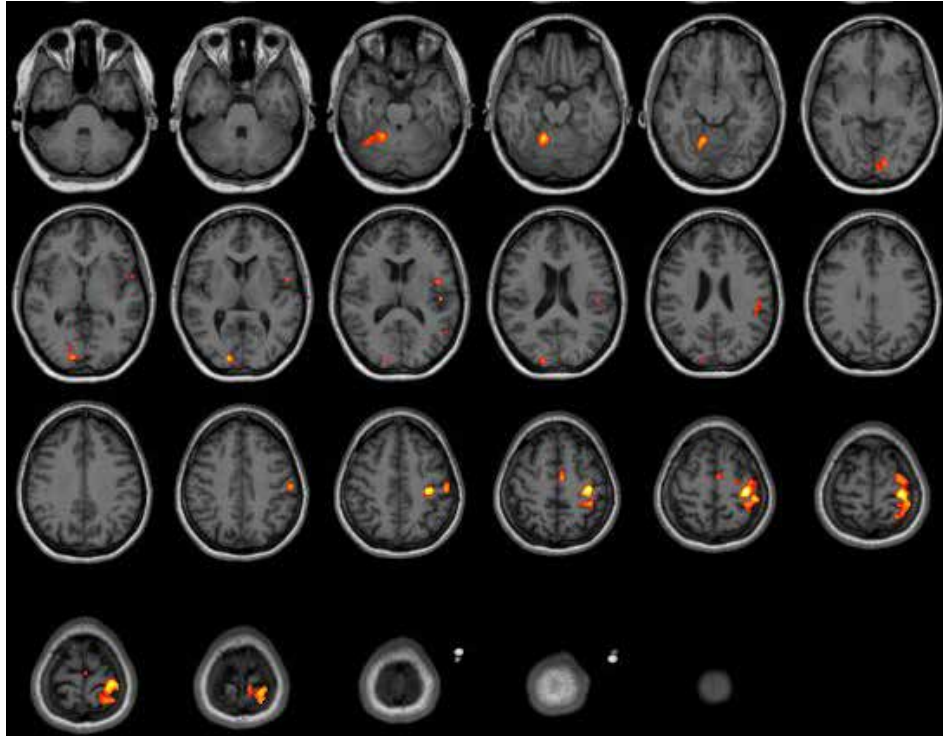


Only 1 significant cluster

Statistical Inference

Visualisation

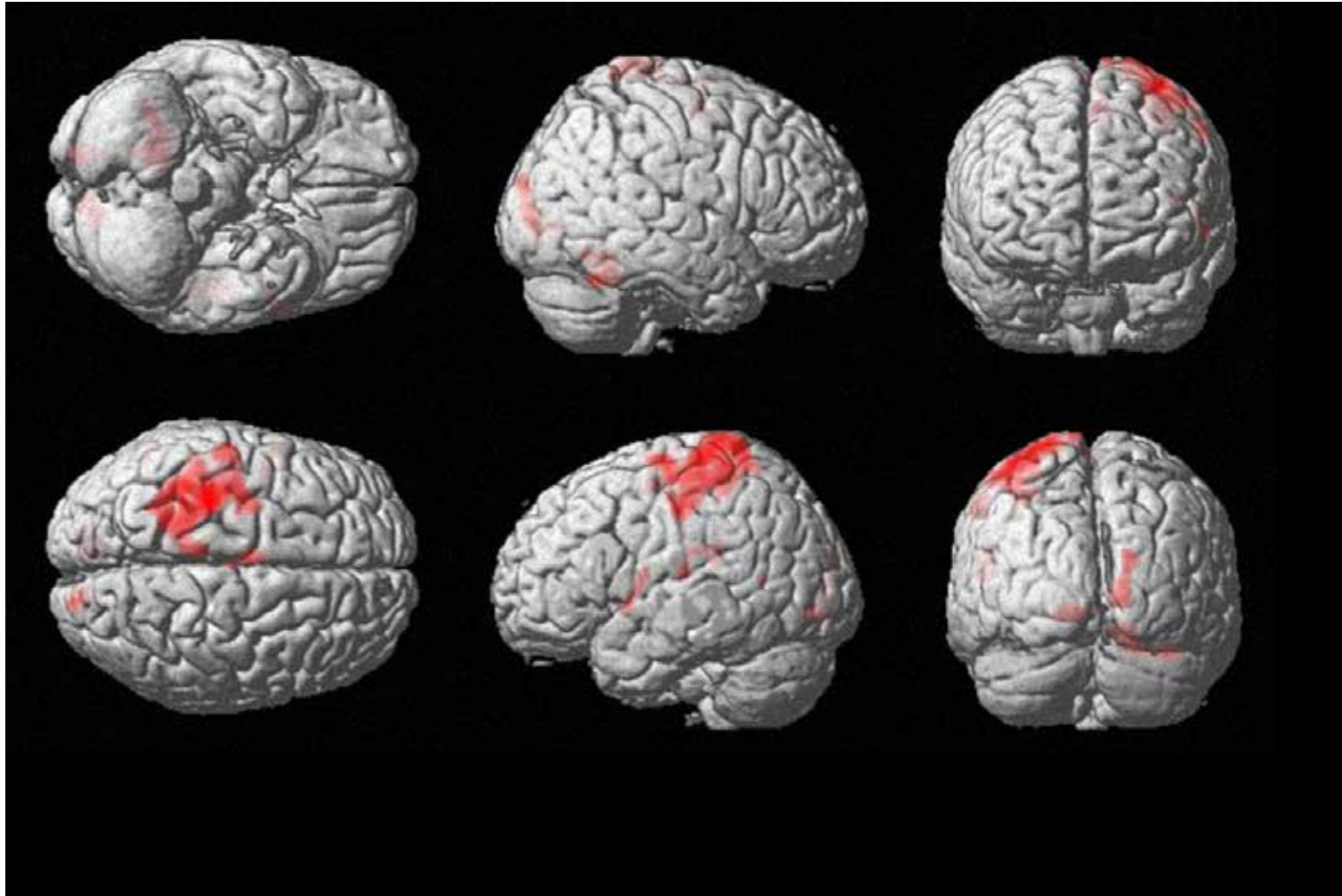
- `aamod_firstlevel_threshold`



Statistical Inference

Visualisation

- `aamod_firstlevel_threshold`



Statistical Inference

Visualisation

- **aamod_firstlevel_threshold_register2FS**
 - Launch a VNC session on a **login-gpu01-03** machine
 - *ssh login-gpu0X* à remember the machine name (e.g. login-gpu01)
 - *vncstart* à remember the desktop number (50+account number; e.g. 51)
 - TurboVNC (e.g. login-gpu01:51)
 - FreeView
 - *cdw*
 - *cd Material/4_aa/AA_fMRI/aamod_firstlevel_threshold_register2FS_00001/S1*
 - *vglrun freeview*
 - View à Viewport Layout à 1 & 3 Horizontal
 - View à Viewport Layout à 3D
 - View à Show Slices (3D View): off



Statistical Inference

Visualisation

- **aamod_firstlevel_threshold_register2FS**
 - Load volume (brain.mgz) and overlay (rthr*.nii)
 - File à Load Volume à brain.mgz
 - File à Load Volume à ../stats/rthrT_0001.nii à Color map: Heat
 - Load Surface (lh.*) and overlay (rthr*2FS_lh.mgh)
 - File à Load Surface à lh.pial
 - Curvature: binary
 - Overlay à Load generic... à ../stats/rthrT_00012FS_lh.mgh
 - Configure Overlay à Min = 3