



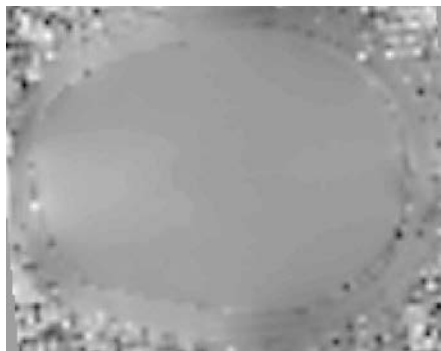
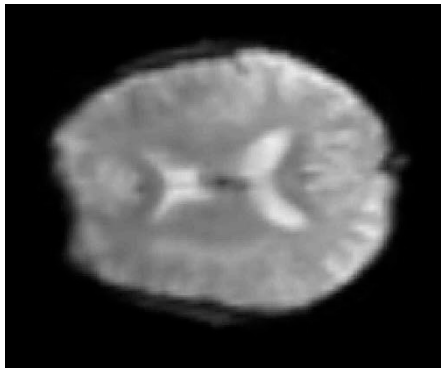
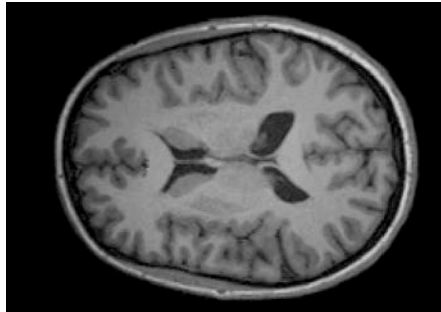
# Pre-processing

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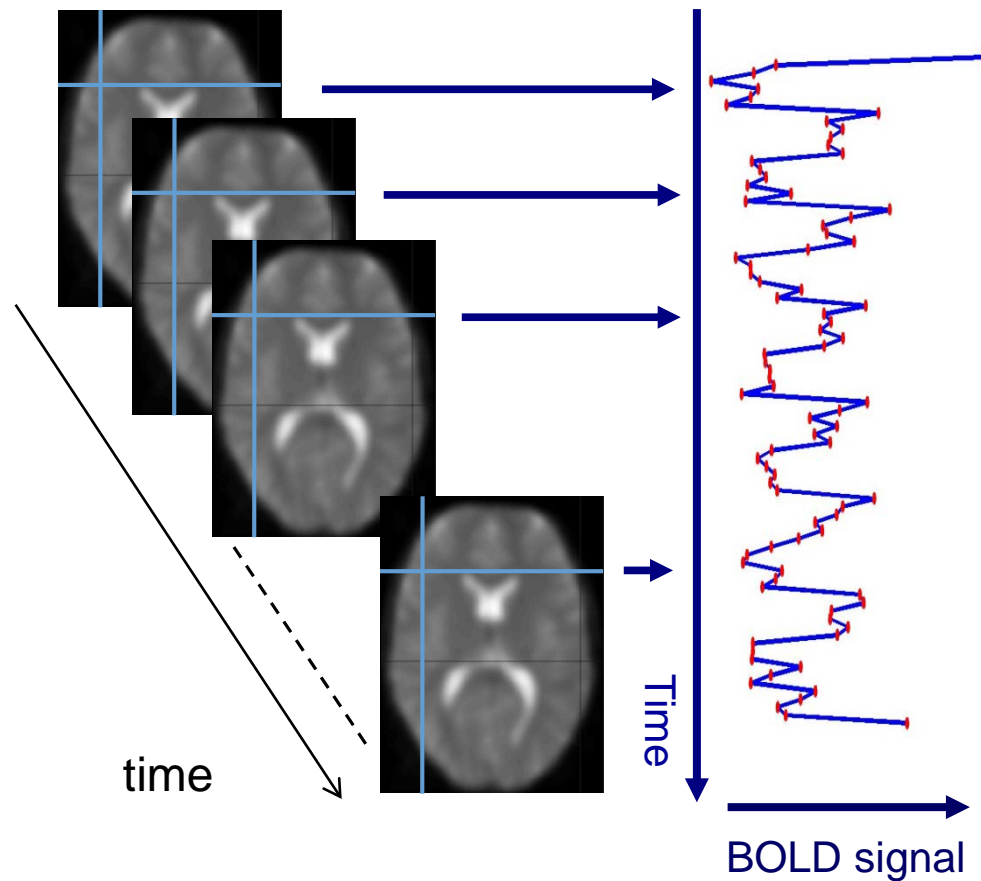
With thanks to Russell Thompson, Matthew Brett, Rik Henson and the authors of the HBF

# Data – Types



- **Anatomical data: T<sub>1</sub>-weighted, 3D, 1/subject or session**
  - (ME)MPRAGE sequence, undistorted
  - High spatial resolution (~1 mm isotropic)
  - Optimised for structural contrast<sup>1</sup>
  - Acquisition time ~5 minutes
- **Functional data: T<sub>2</sub>\*-weighted, 4D, 1/measurement**
  - EPI sequence, distorted
  - Lower spatial resolution (2-3 mm non-isotropic)
  - Optimised for functional contrast<sup>2</sup>
  - Acquisition time ~2 seconds (20-30 slices)
- **Fieldmaps: 2×3D, 1/session**
  - Dual-echo GE sequence, undistorted
  - Lower spatial resolution (same as fMRI)
  - Map of magnetic field inhomogeneities
  - Acquisition time ~1 minute.

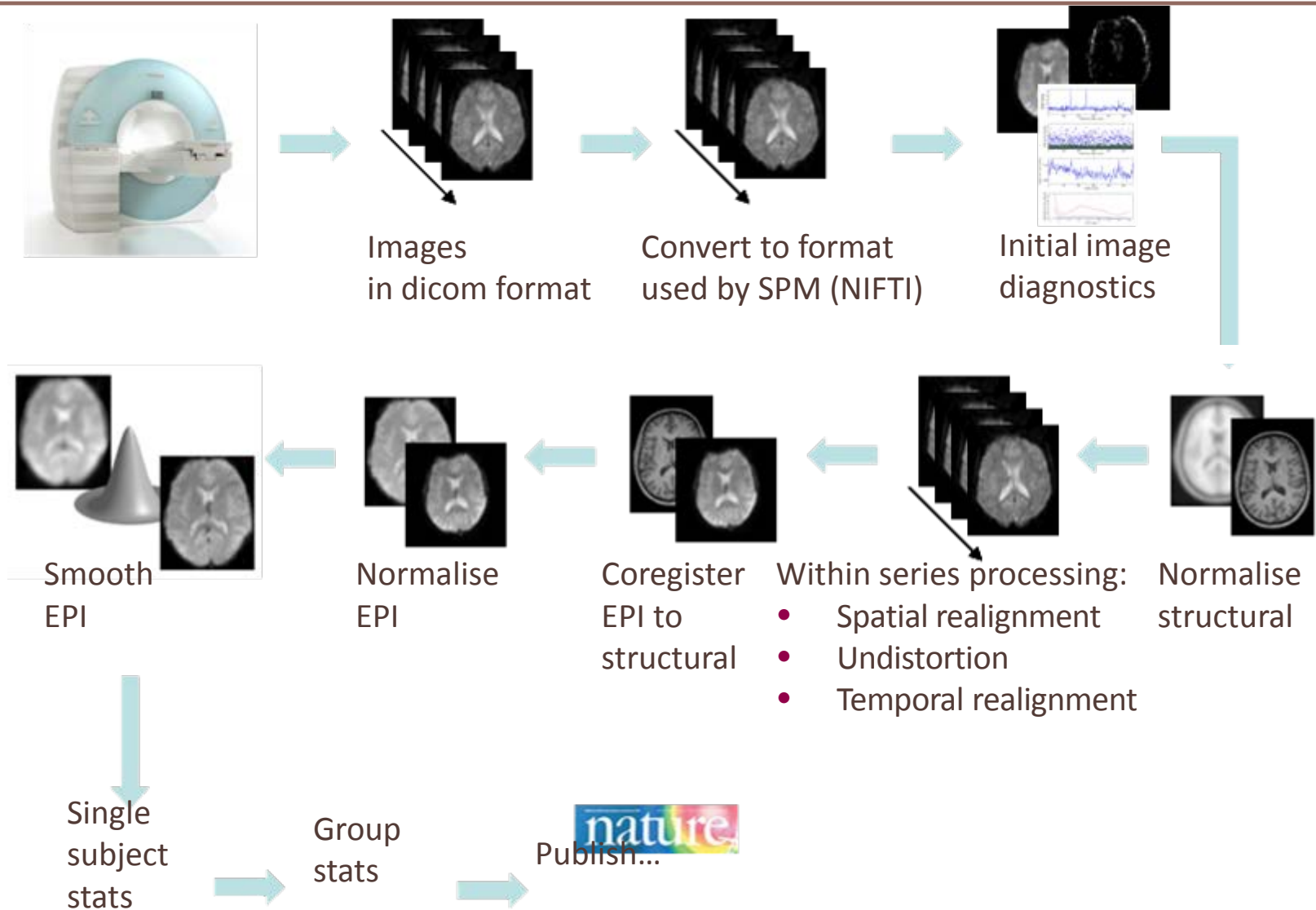
# Data – Functional



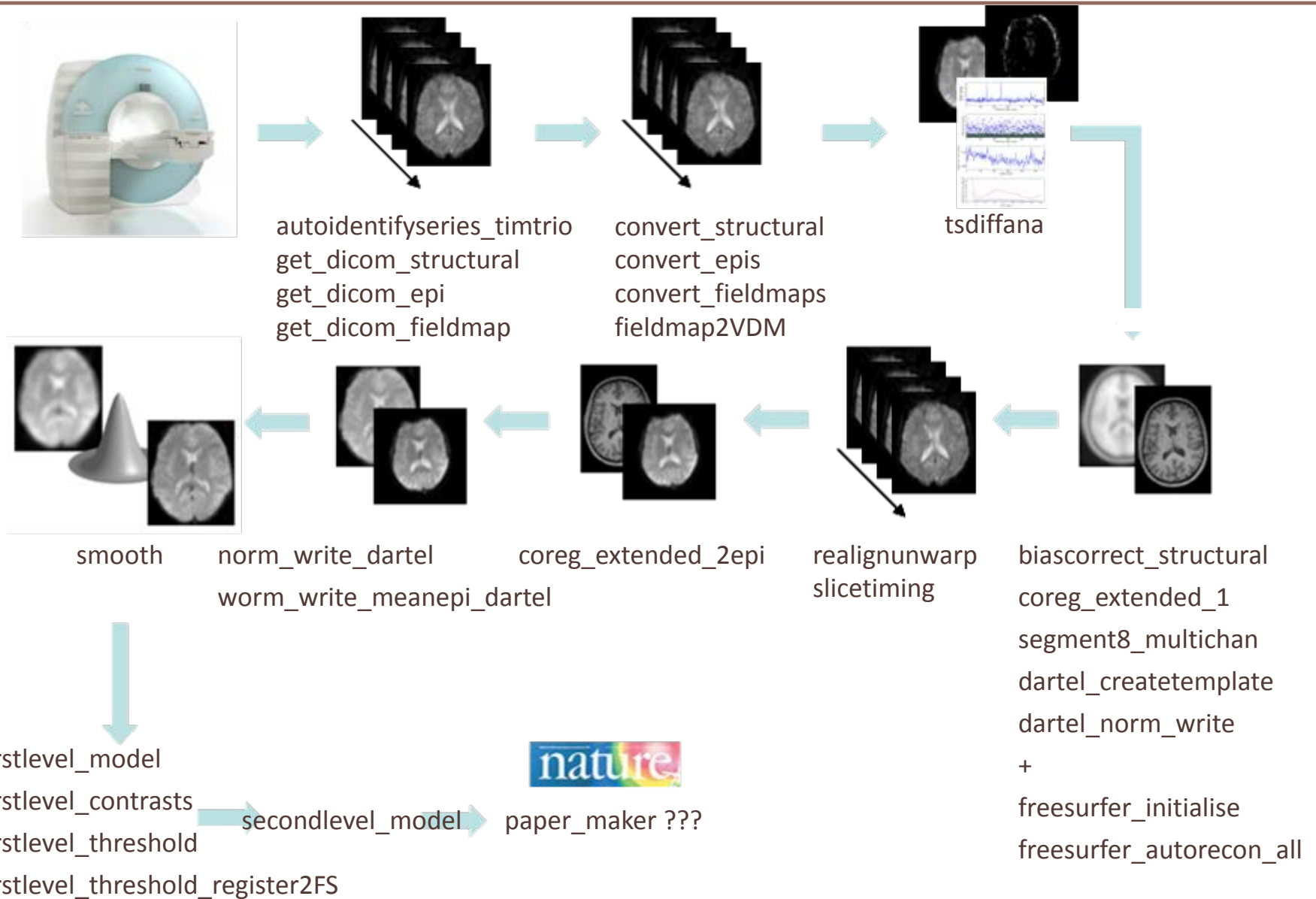
- **Time series**

- showing BOLD signal changes
- in each point in the brain  
3D
- at each repetition (~2 seconds)  
+1D

# Overview

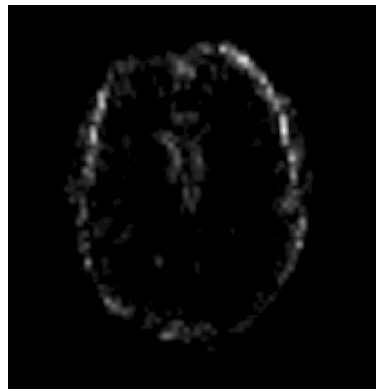
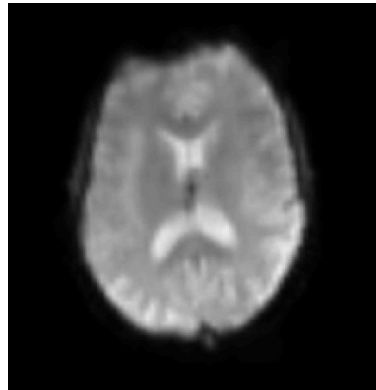


# Overview – aa modules (aamod\_\*)

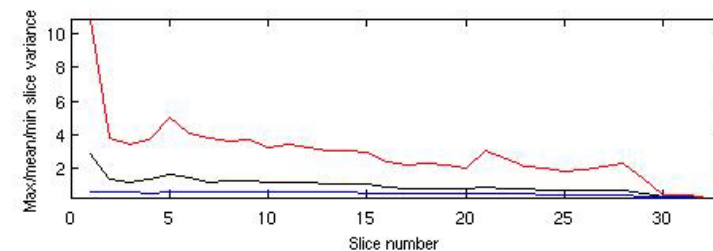
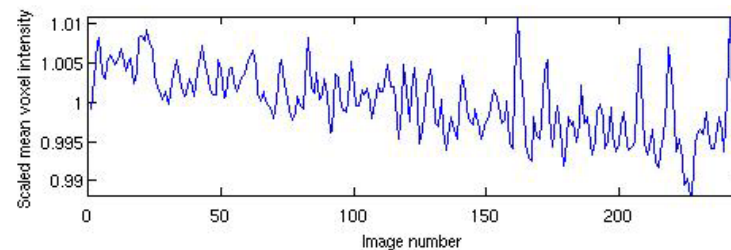
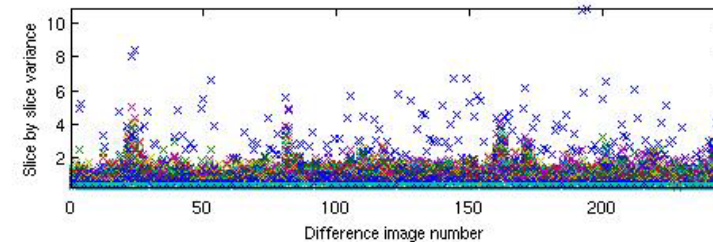
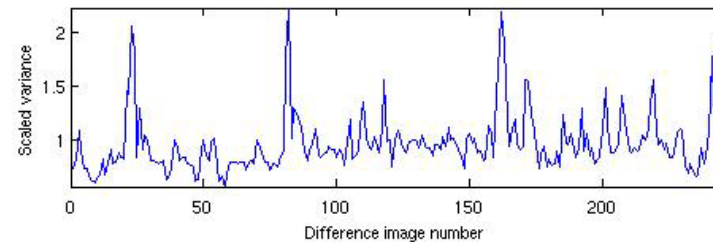


# Preprocessing – Initial diagnostics

Mean and variance images:



Diagnostic plots:



Scaled variance of difference from the 1<sup>st</sup> vol.:

- Volumewise

- Slicewise

Descriptive stats:

- Volumewise

- Slicewise



# Preprocessing – Normalization

## Challenge

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- **People have different shaped brains**
- **Goal: transforming brain so its shape matches that of a template**
  - Group studies
  - Cross study comparison, meta analysis
- **Template: universal space**
  - Talairach and Tournoux, 1988 (based on a single subject)
  - Montreal Neurological Institute: MNI152
    - Averaged from  $T_1$  images of 152 subjects
  - Information eXtraction from Images (London): IXI (in SPM12)
    - Also in MNI
    - Fewer subjects, but may be more representative locally
    - More classes (segmentation)



# Preprocessing – Normalization

## Approaches

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- **Direct:**
  1. EPI  $\rightarrow$  MNI modality + resolution/smoothness + shape
- **Indirect (Coreg<sup>1</sup>+Norm):**
  1. EPI  $\rightarrow$  Structural modality + resolution
  2. Structural  $\rightarrow^2$  MNI smoothness + shape
- **Indirect+ (Coreg<sup>1</sup>+DARTEL+Norm)<sup>3</sup>:**
  1. EPI  $\rightarrow$  Structural modality + resolution
  2. Structural  $\rightarrow^2$  Study template smoothness + shape (int.)
  3. Study template  $\rightarrow$  MNI shape (int.)



# Preprocessing – Normalization

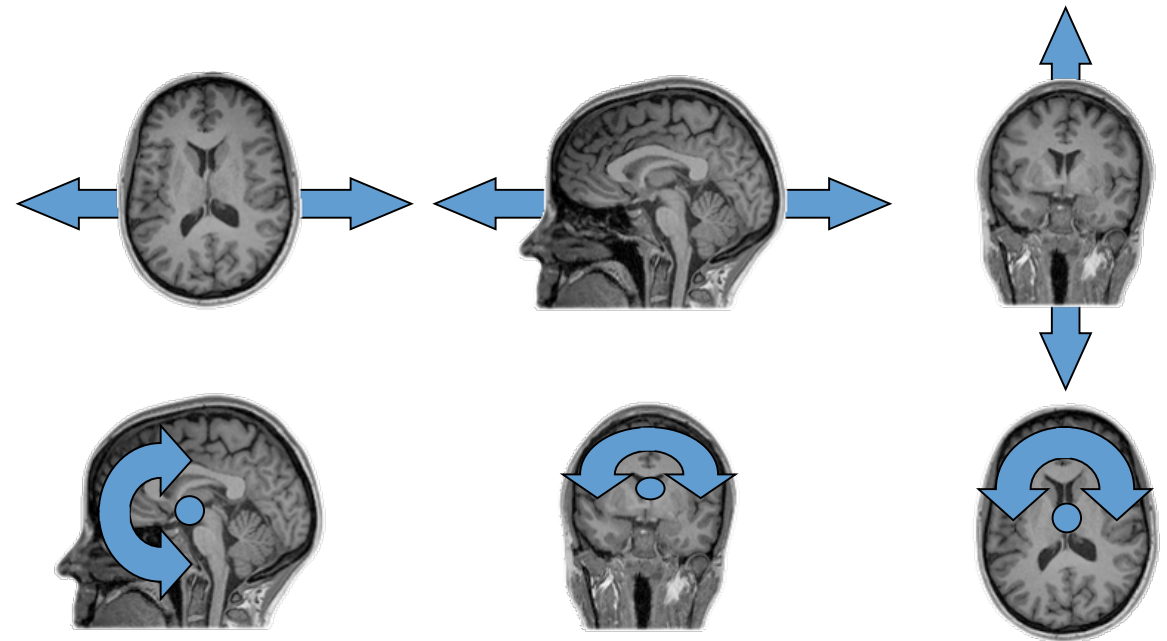
## Transformation

- **Affine (12 DOF) registration:**

- 3 translations

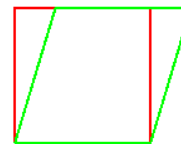
- 3 rotation

Rigid-body  
(6DOF)

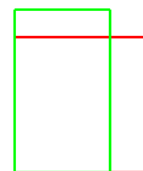


- 3 shears

- 3 zooms



Shear



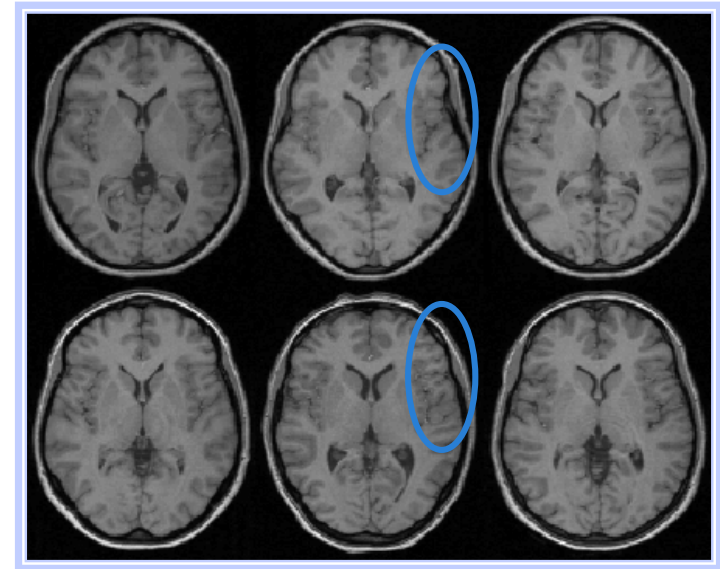
Zoom

# Preprocessing – Normalization

## Transformation

- **Linear transformations:**

- Assumes linear relationship
  - between position and transformation
- Able to match overall size and shape,
  - but not small details



- **Nonlinear transformations:**

- Deformation fields: nonlinear relationship between position and transformation
  - large DOF → overfitting (unnecessary warps) make brains exactly the same



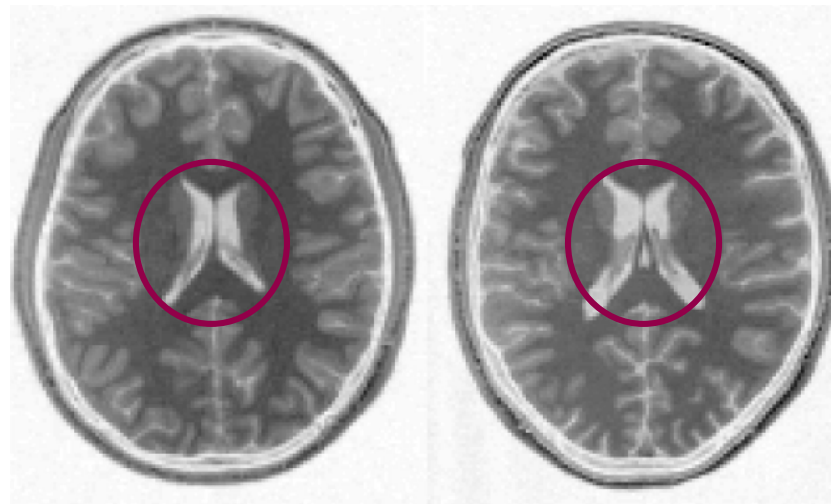
- Regularisation: transformation within a certain range based on *a priori* knowledge<sup>1</sup>

# Preprocessing – Normalization

## Transformation

- **Nonlinear transformations:**

Template

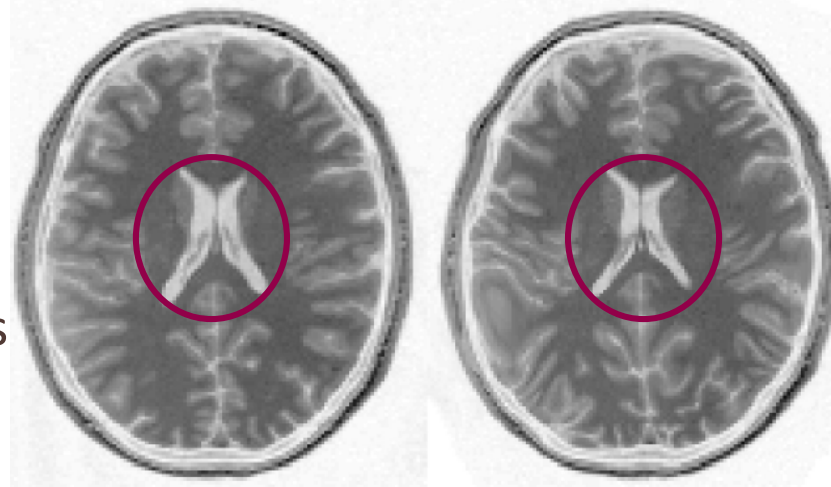


Affine only

- some differences in shape

Affine + nonlinear with regularization

- good match to overall shape
- some differences in details



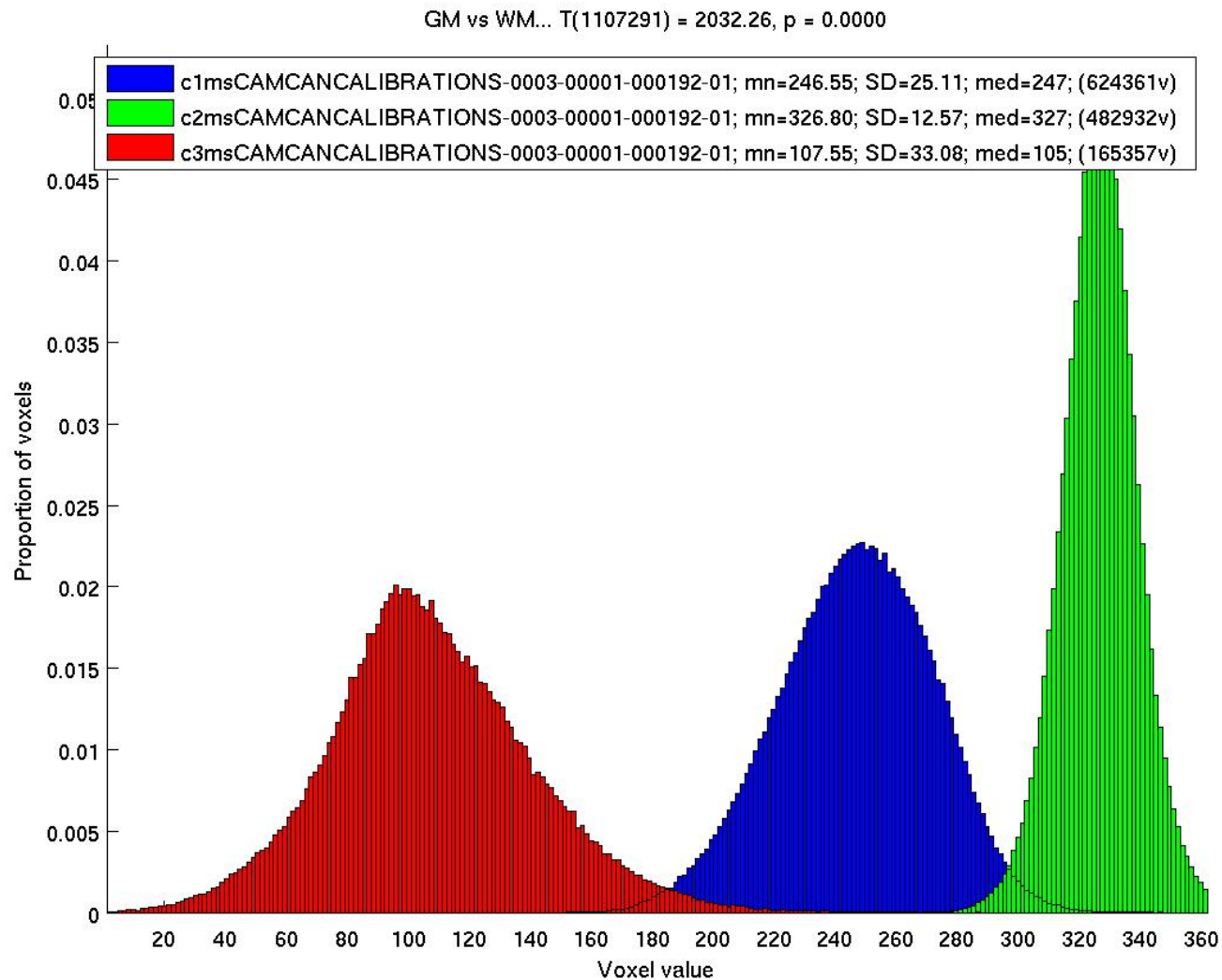
Affine + nonlinear without regularization

- overfitting

# Preprocessing – Normalization

## Diagnostics

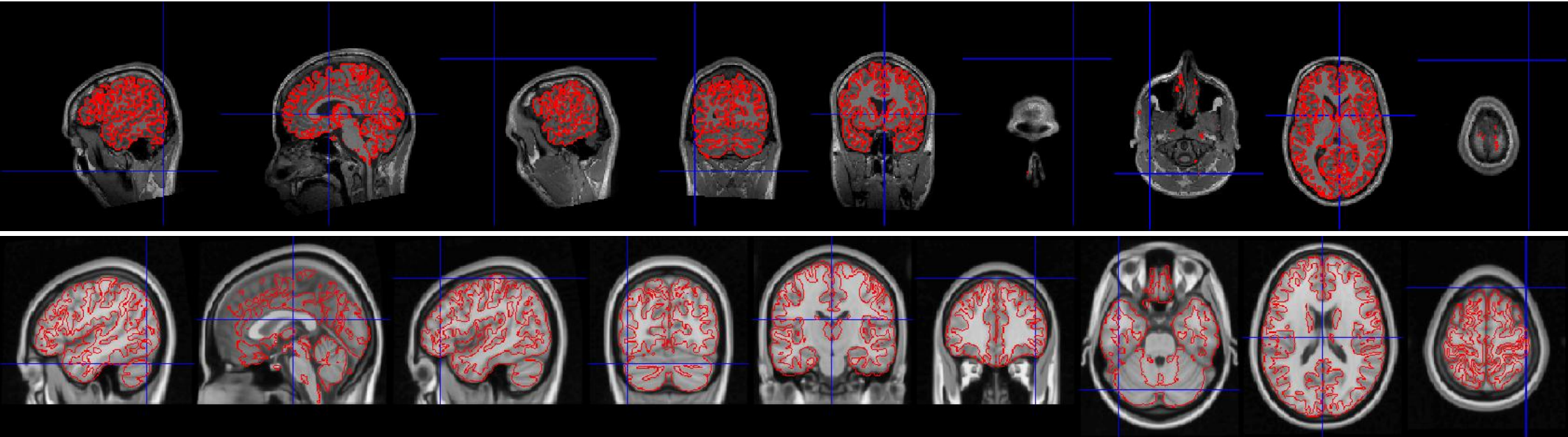
- Segmentation



# Preprocessing – Normalization

## Diagnostics

- **Segmentation**



- **Normalisation (structural)**
  - (manually)

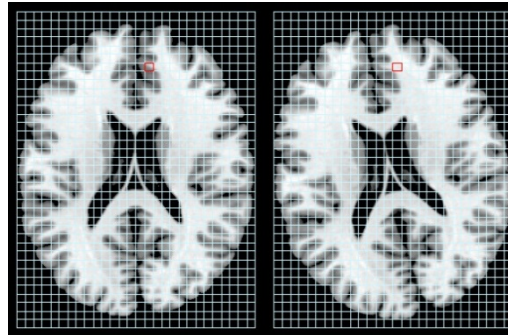


# Preprocessing – Motion correction

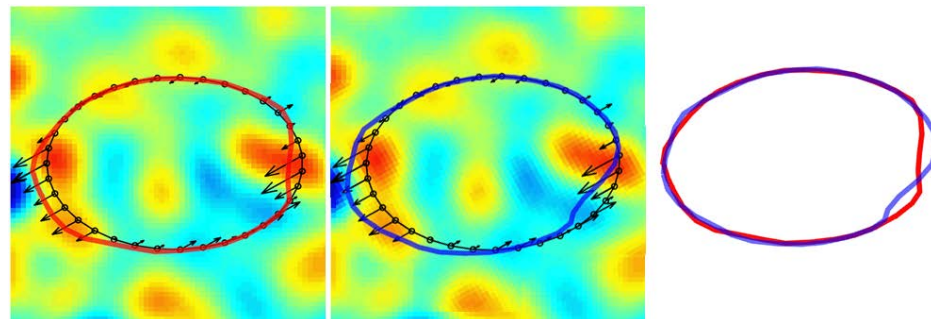
## Challenge

- **Movement confounds data:**

- Signal recorded from different position
  - Correspondence
  - PVE (e.g. WM – GM)



- Signal recorded at a different field strength
  - Local inhomogeneities in the magnetic field affecting the brain area



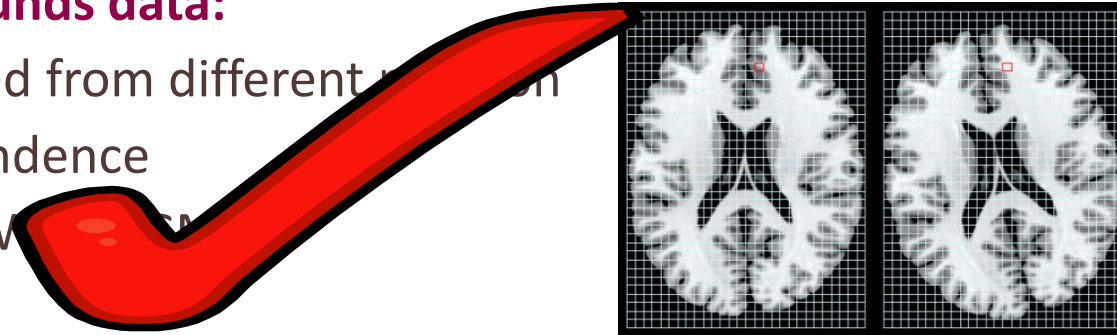
- Aliasing caused by gap between the slices

# Preprocessing – Motion correction

## Challenge

- **Movement confounds data:**

- Signal recorded from different positions
- Correspondence
- PVE (e.g. Voxel shift)



same modality, same resolution, same shape



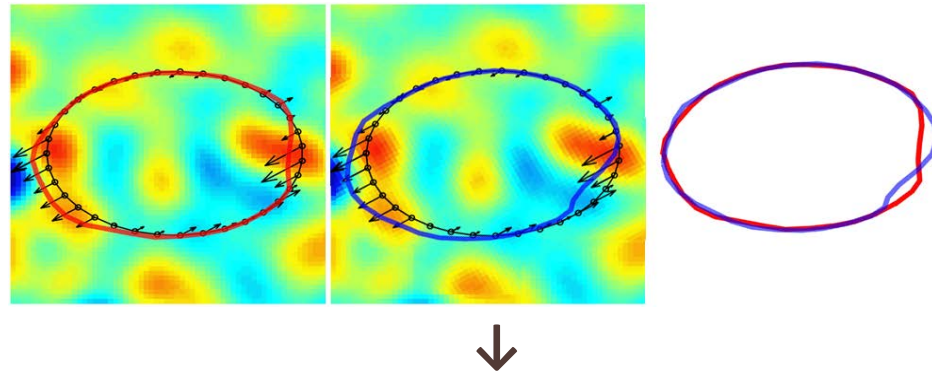
**Rigid-body (6DOF)**

# Preprocessing – Motion correction

## Challenge

- **Movement confounds data:**

- Signal recorded at a different field strength
  - Local inhomogeneities in the magnetic field affecting the brain area



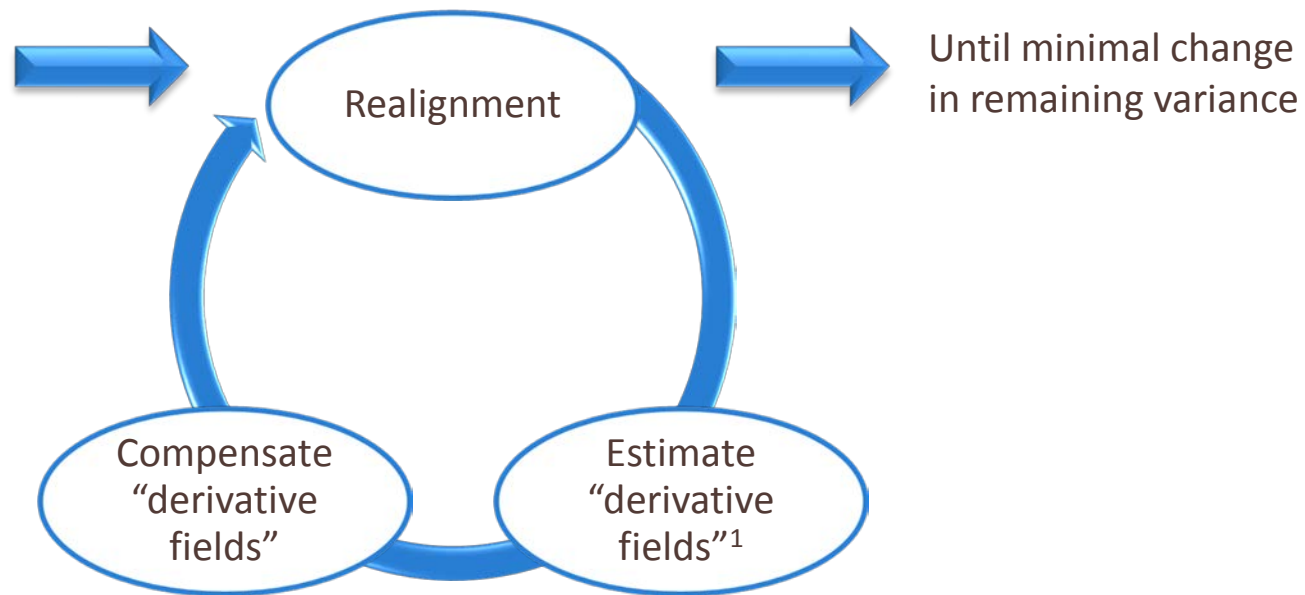
- **Include the realignment parameters as covariates in the statistical model**

- Capture any movement related variance in the data.
- However!
  - Reduces design's degree of freedom (usually > 100)
  - Problematic if movement is correlated with effects of interest
    - (e.g. button pushes, verbal responses etc.)
  - Can remove the effects of interest.



# Preprocessing – Motion correction: +Unwarping

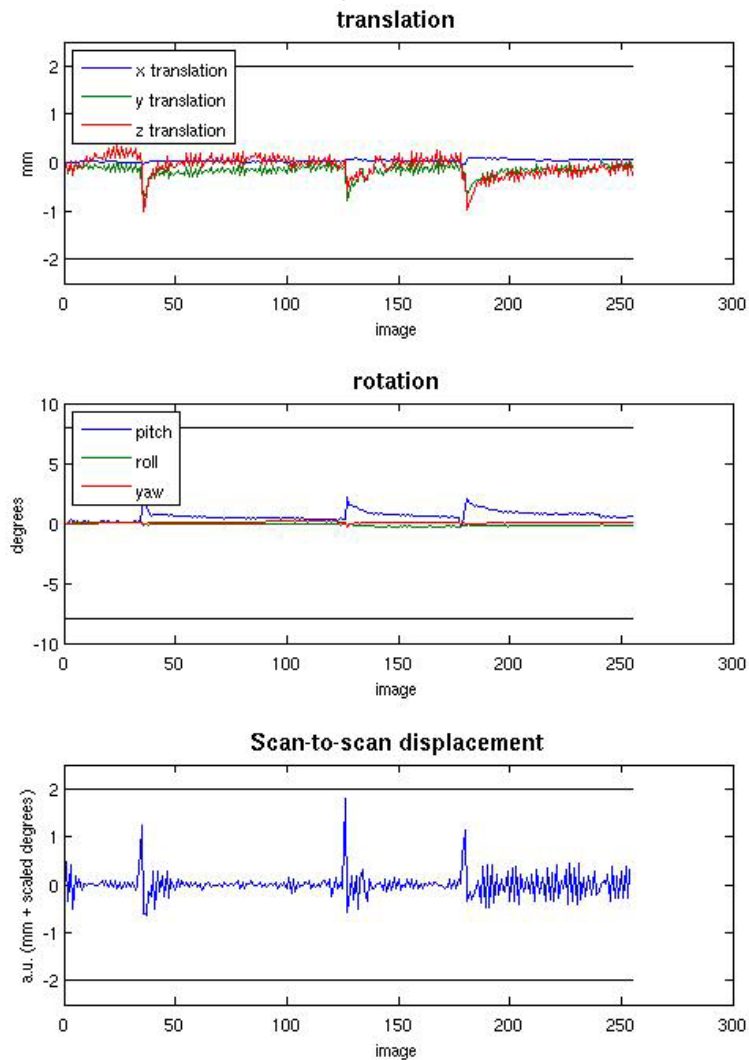
- **Motion correction with Unwarping:**
  - Iteratively estimate the effects and compensate for them



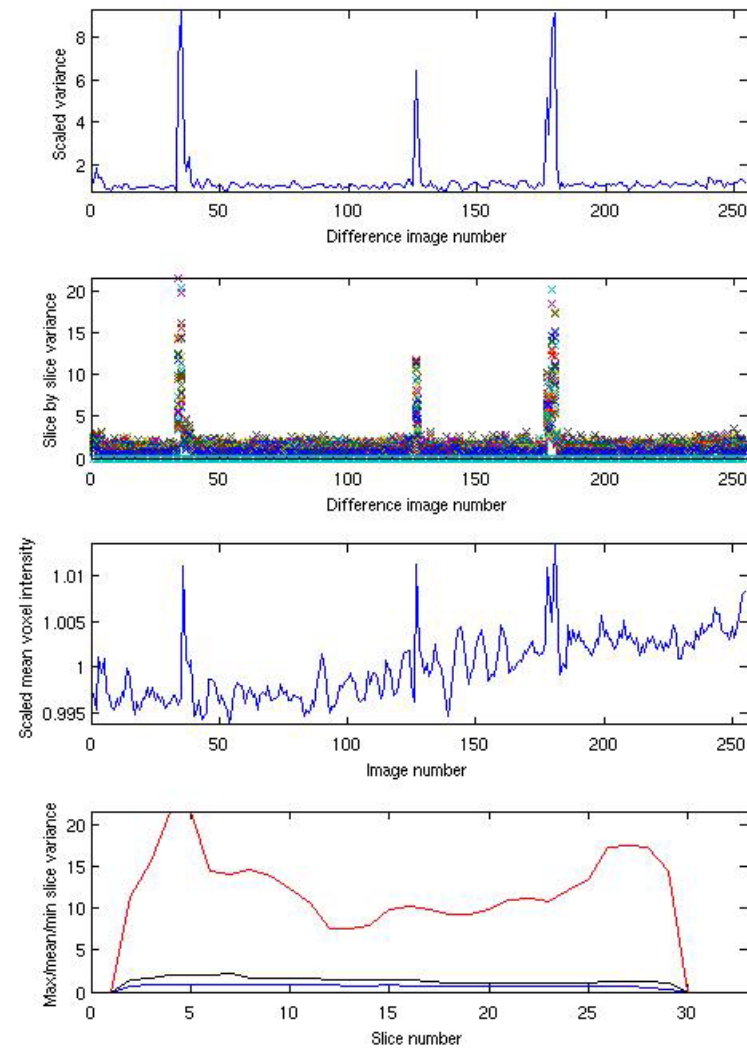
# Preprocessing – Motion correction

## Diagnostics

### MoCo parameters



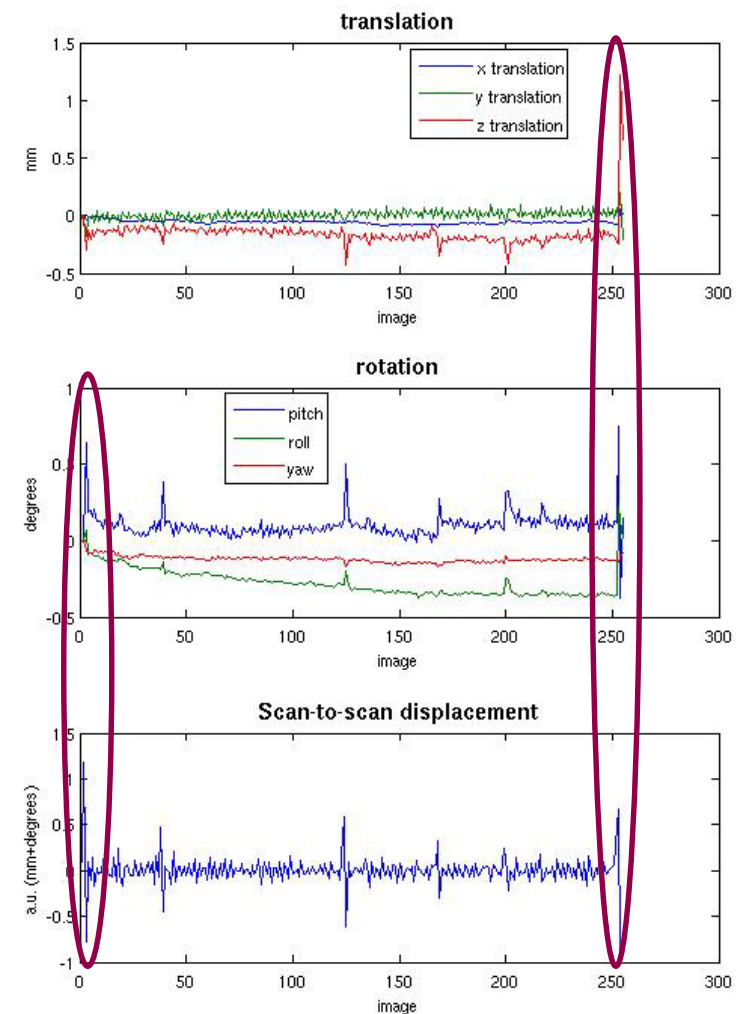
### QA



# Preprocessing – Motion correction

## Diagnostics

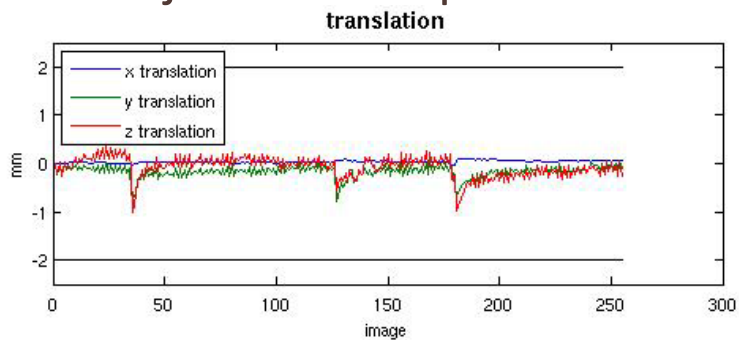
- **Best solution: reduce movement to the minimum**
  - Comfort<sup>1</sup>
  - Discourage talk during breaks (between-session movement<sup>2</sup>)
  - Dummy scans
  - “End of measurement”
- **Reject data to reduce heterogeneity (Summary)**
  - Scans
  - Subjects



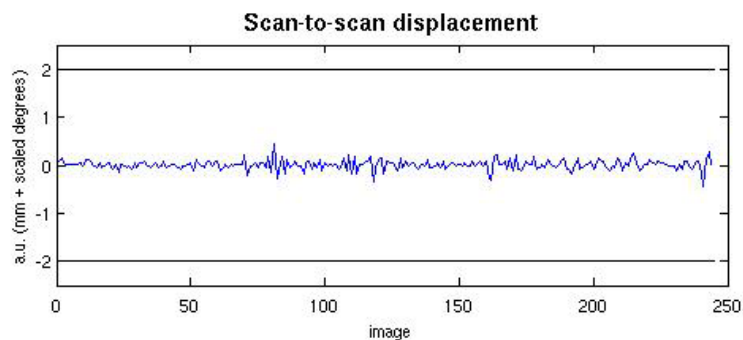
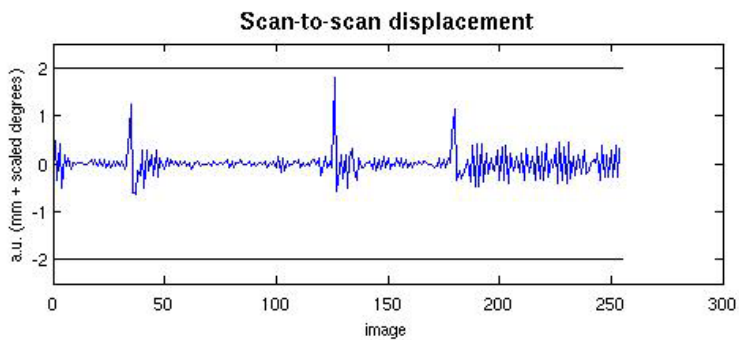
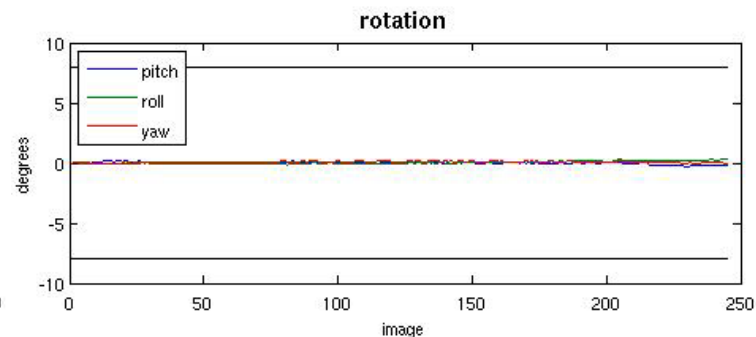
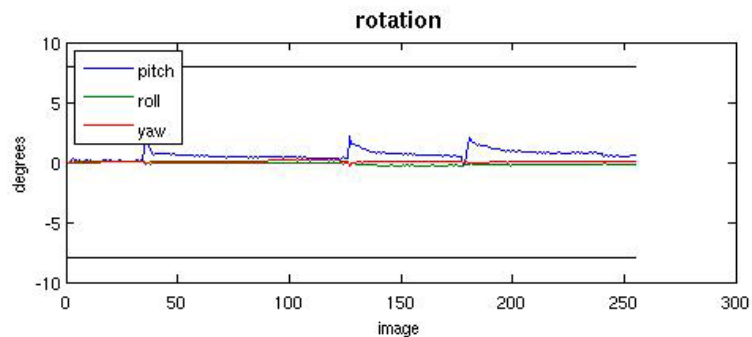
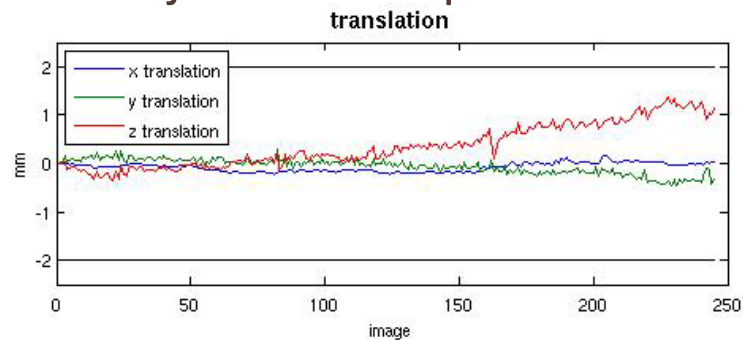
# Preprocessing – Motion correction

## Diagnostics

Subject1 MoCo parameters



Subject2 MoCo parameters

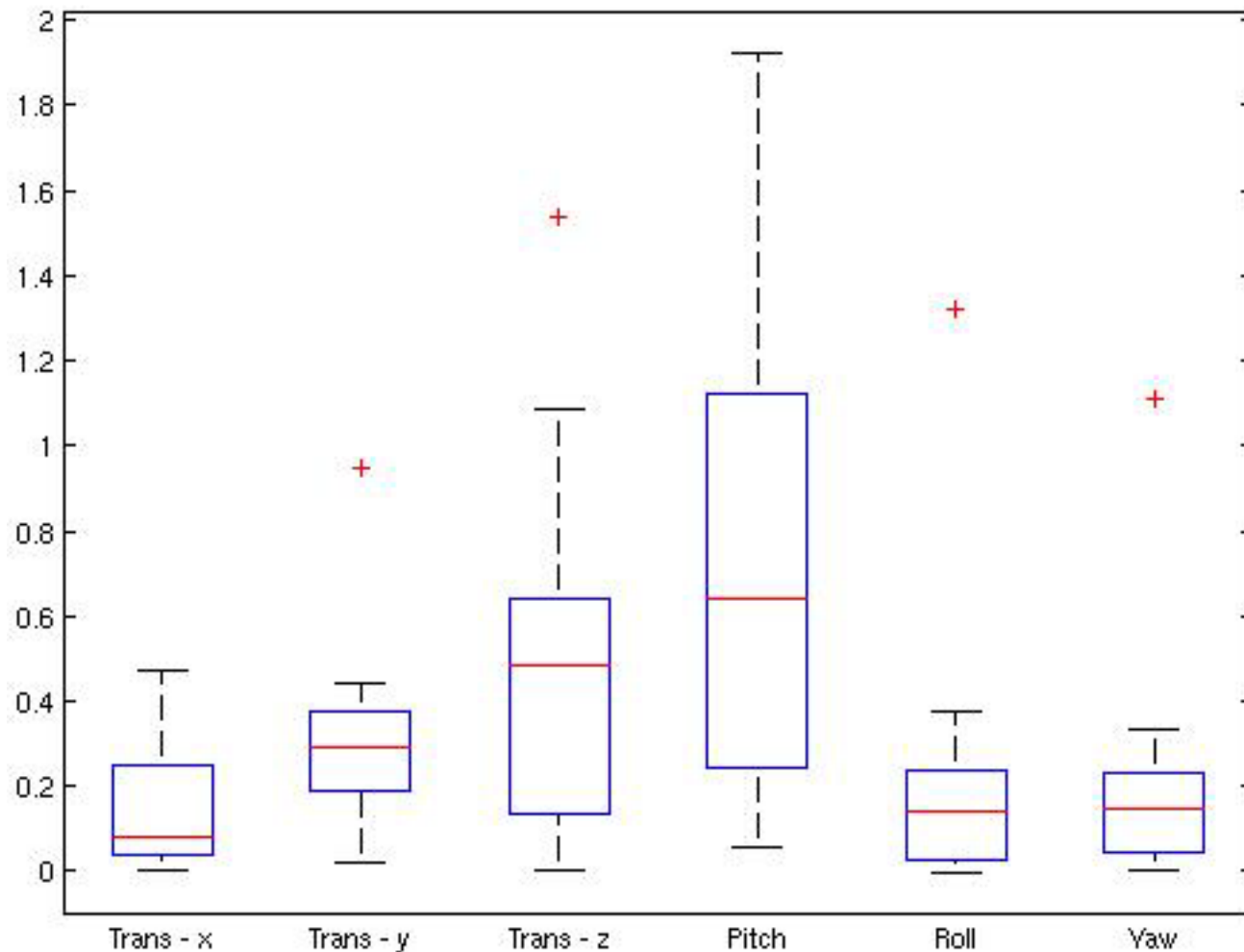


# Preprocessing – Motion correction

## Diagnostics

- **Summary (outliers)**

- Trans - x: None
- Trans - y: 12
- Trans - z: 1
- Pitch: None
- Roll: 19
- Yaw: 19



# Preprocessing – Temporal realignment

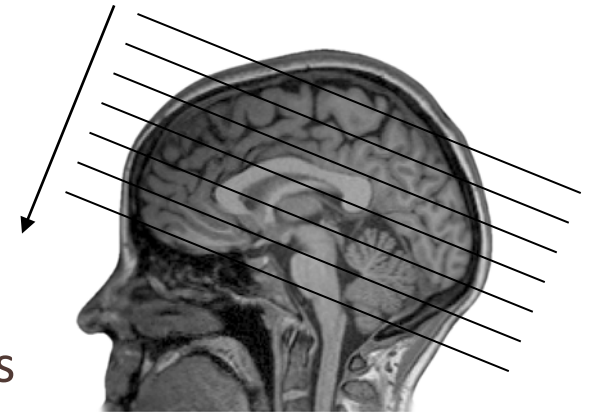
## Challenge

- **Acquisition**

- 2D EPI sequence collect volume slice-by-slice
- Each slice is acquired at a different time
- TR = 2s, 32 slices:
  - 62.5 ms between-slice difference
  - ~1.9 s difference between the first and the last slices



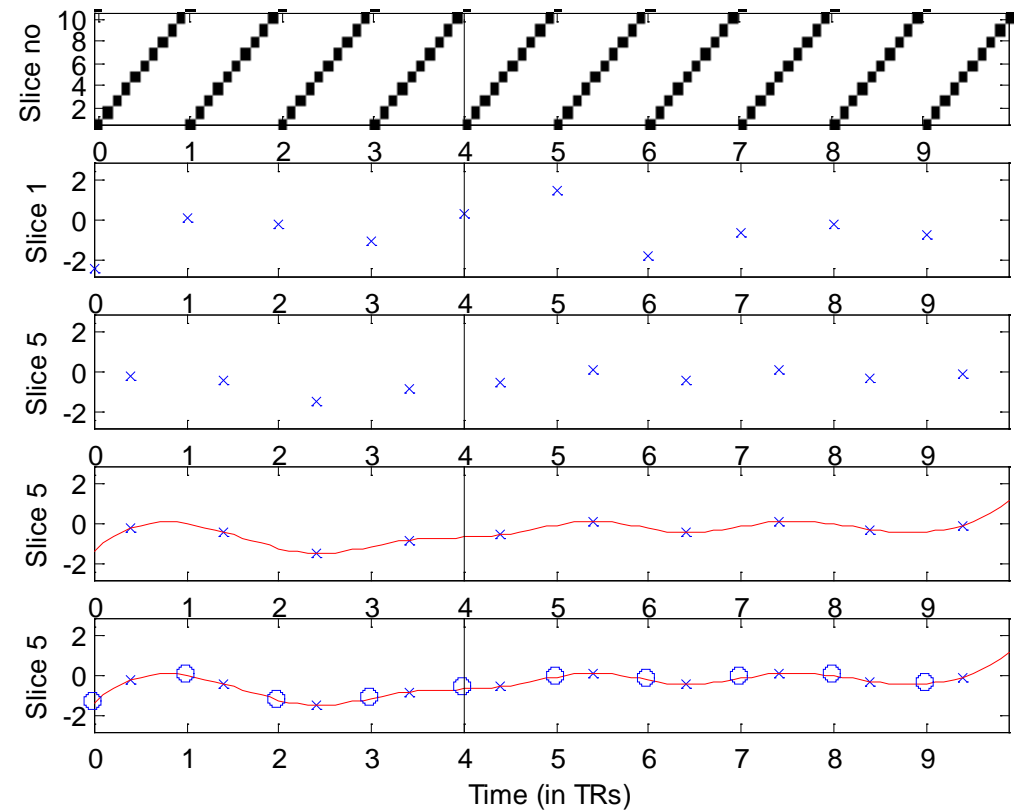
- Confound precise timing if TR is long ( $> 1s$ )
  - Event-related vs. epoch-based



# Preprocessing – Temporal realignment

## Solution

- **Slice time correction**
  - Interpolate timecourse<sup>1</sup>
  - Preprocessing:
    - Calculate time shift
    - “Tags” slices
  - Interpolation during HRF-estimation



# Preprocessing – Temporal realignment

## Input

---

- **Sliceorder/Slice timings**
  - Timings are more accurate than orders
  - Specified manually (automatic in *aa!*)
- **Reference slice: all other slices will be “adjusted” to it**
  - Middle slice: ↓ the maximum interpolation necessary → ↓ interpolation artefacts
  - It will not be altered: Chose according to your area of interest!
  - Scanner sync pulse is at the acquisition of the first slice
    - Stimuli timing adjusted to the first slice
    - or
    - Model needs to be adjusted (automatic in *aa!*)



# Preprocessing – Coregistration

## Challenge

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- **Goal: the functional in the same space as the structural**
  - Overlay functional results onto the structure to enhance localisation
  - Use anatomy as a precursor to spatial normalization
    1. Normalise the structural image<sup>1</sup>
    2. Apply the parameters to the functional data
- **Data types**
  - Reference image: Structural:  $T_1$ -weighted, high resolution, fewer artefacts
  - Source image: Functional:  $T_2^*$ -weighted, low resolution



modality + resolution (but same shape)



**Rigid-body (6DOF)**



# Preprocessing – Coregistration

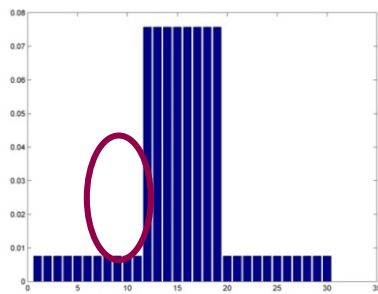
## Source image

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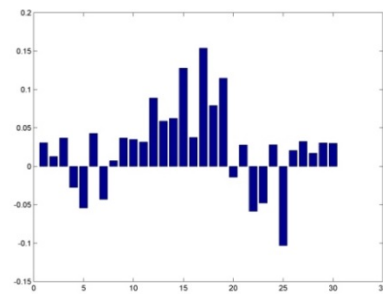
- **Functional image to estimate transformation**
  - example EPI from ca. the middle – FSL
  - mean EPI (temporally averaged) – SPM, aa
    - Smaller (effective) spatial resolution
    - Smaller noise
- **Requirement**
  - Reasonably good starting point (local optima)
    - Similar acquisition position (AutoAlign)
    - Reorient (?)
  - Adequate overlapping with structural
    - Partial-brain fMRI → two-step coregistration via a “whole-brain EPI”<sup>1</sup>
      1. Partial-brain EPI → whole-brain EPI
      2. Whole-brain EPI → Structural

# Preprocessing – Smoothing

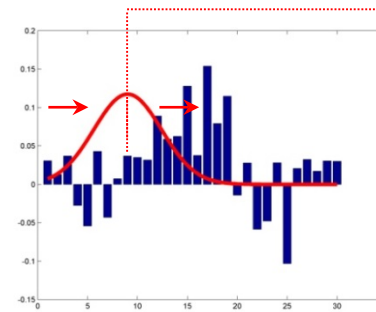
- **Spatial weighted averaging: usually Gaussian kernel**
  - Value at each voxel: a weighted average of the values in surrounding voxels



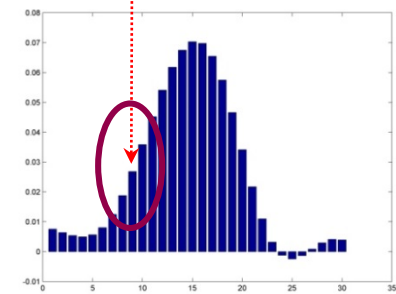
Original signal



Signal plus noise



Apply kernel  
to each point



Recovered signal

- $\uparrow$  signal-to-noise ratio: assuming random noise
- Spreads signal (**depends on kernel size**):
  - $\uparrow$  between-subject spatial correspondence (by blurring minor differences)
  - $\downarrow$  effective spatial resolution (RESEL)  $\downarrow$  the number of multiple comparisons
  - “False” positives!

# Preprocessing – Smoothing

## Kernel Size

- **Amount to smooth:**
  - Full Width at Half Maximum height (FWHM)
  - Ideally: hypothesis-dependent<sup>1</sup>
    - According to the spatial extent of the signal
    - Neuroanatomical assumptions
      - Visual areas: smaller kernel
      - Prefrontal: larger kernel
  - Methodologically: GRFT-dependent (inference)
    - Ensure minimum smoothness ( $\text{RESEL} \geq 3 \times \text{voxel}$ )
    - Iterative?
  - Practically:
    - Resolution-dependent:  $1.5 \times \text{voxel-size}$
    - 8-10 mm is common (SPM default, history!)

